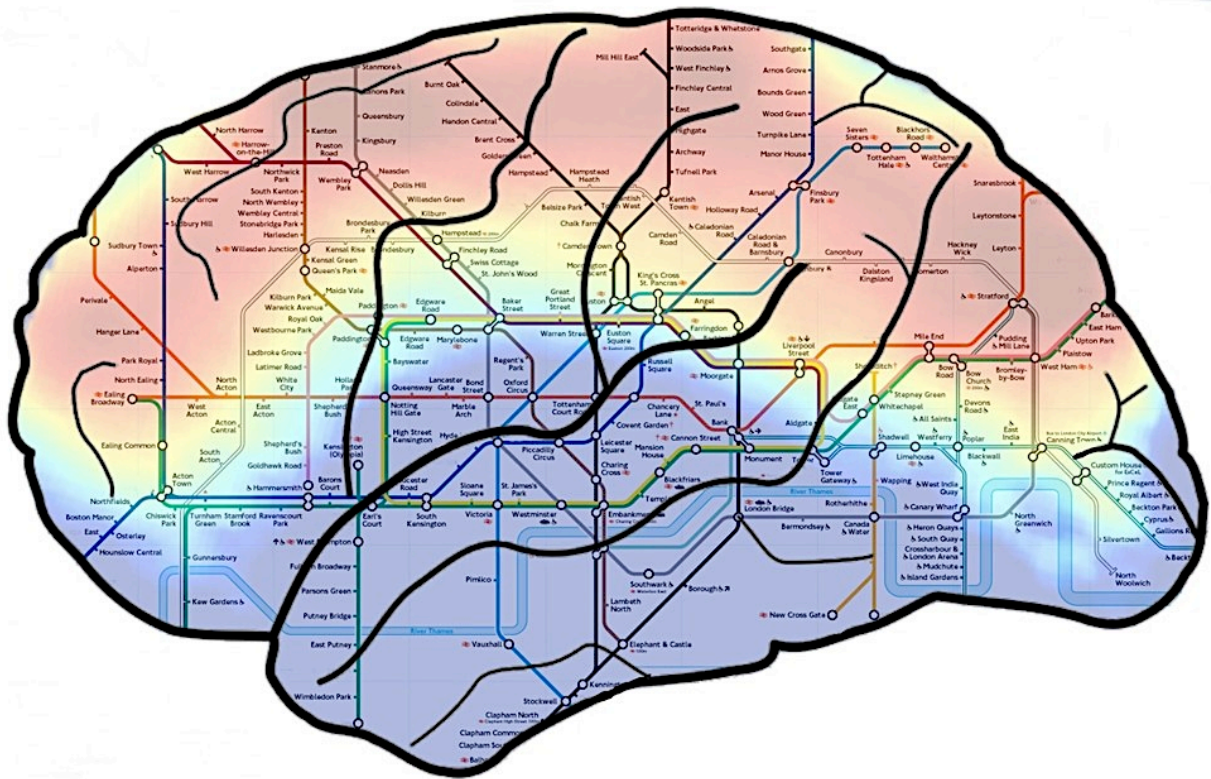


# Abstract Book



## Functional Near Infrared Spectroscopy Conference

University College London

26<sup>th</sup>-28<sup>th</sup> October 2012

Program Chair

Clare Elwell

Organizing Committee

Richard Aslin

David Boas

Joseph Culver

Clare Elwell

Maria Angela Franceschini

Ted Huppert

Charles Nelson

Hellmuth Obrig

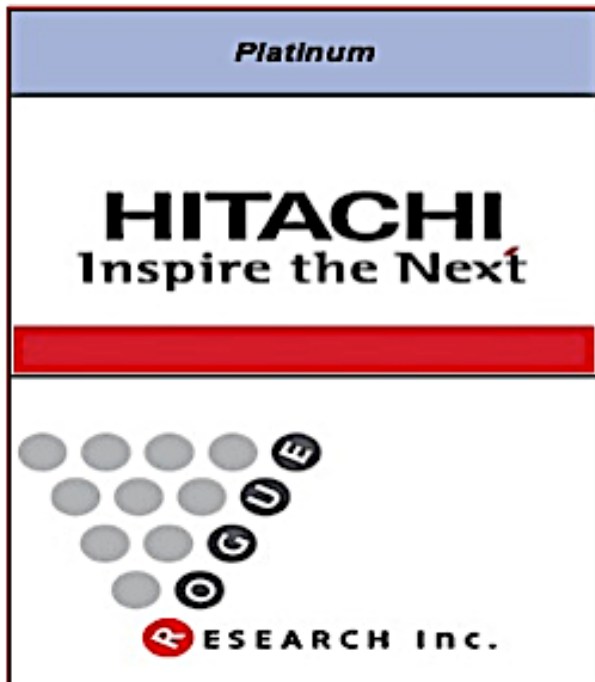
Gentaro Taga

Martin Wolf

## Hosts



## Sponsors



# SCHEDULE

	Session	Speaker	Location	Page #
<b>Friday 26th October</b>	<b>2:00pm</b> <b>REGISTRATION OPENS</b>		<b>North Cloisters</b>	
	<b>5:15pm</b> <b>Welcome and Introduction of Sponsors</b>	<b>Clare Elwell</b>	<b>Cruciform Lecture Theatre</b>	
	<b>5:30pm</b> <b>KEYNOTE: "Trends in Functional Near Infrared Spectroscopy"</b>	<b>David Boas</b>	<b>Cruciform Lecture Theatre</b>	<b>Page 13</b>
	<b>6:30pm</b> <b>WELCOME RECEPTION Sponsored by Hitachi Medical Corporation and Rogue Research Inc.</b>		<b>North Cloisters</b>	
<b>Saturday 27th October</b>	<b>HARDWARE DEVELOPMENTS</b> <i>Chair: Heidrun Wabnitz</i>		<b>Cruciform Lecture Theatre</b>	
	<b>8:00 - 8:30am</b> <b>Invited Talk: "Ischemic stroke &amp; hybrid diffuse optics combining diffuse correlation spectroscopy (DCS) and diffuse optical spectroscopy (DOS-NIRS)"</b>	<b>Turgut Durduvan</b>		<b>Page 15</b>
	<b>8:30-8:45</b> Time resolved functional near infrared spectroscopy by means of time gated system at small interfiber distance	Davide Contini		<b>Page 16</b>
	<b>8:45-9:00</b> Imaging multiple functional networks with diffuse optical tomography	Adam T. Eggebrecht		<b>Page 17</b>
	<b>MULTI-MODAL MONITORING</b> <i>Chair: Maria Angela Franceschini</i>		<b>Cruciform Lecture Theatre</b>	
	<b>9:00 - 9:30am</b> <b>False Positives in fNIRS: Identifying and Quantifying Systemic Influences on Neurovascular Coupling in fNIRS Data during Cognitive Tasks.</b>	<b>Ilias Tachtsidis</b>		<b>Page 19</b>
	<b>9:30 - 9:45am</b> Neurovascular Coupling Varies with Level of Global Cerebral Ischemia in a Rat Model	Wesley B Baker		<b>Page 20</b>
	Impact of Extracranial Vessels on Task-Evoked Artefacts in Functional Near Infrared Spectroscopy for Multiple Tasks	Evgeniya Kirilina		<b>Page 21</b>
	<b>10:00 - 10:45am</b> <b>COFFEE Sponsored by Spectratech Inc.</b>		<b>North Cloisters</b>	
	<b>DATA ANALYSIS</b> <i>Chair: Joseph Culver</i>			
	<b>10:45 -11:15am</b> <b>Methodological challenges in the application of fNIRS for infant cognitive neuroscience</b>	<b>Emmanuel Dupoux</b>	<b>Cruciform Lecture Theatre</b>	<b>Page 23</b>
	<b>11:15 - 11:30am</b> Low frequency oscillations measured in the periphery with near infrared spectroscopy (NIRS) are strongly correlated with blood oxygen level-dependent functional magnetic resonance imaging (BOLD fMRI) signals	Yunjie Tong		<b>Page 24</b>
	<b>11:30 - 11:45pm</b> Integrated Data Analysis Environment for fNIRS	Takusige Katura		<b>Page 25</b>
	<b>11:45 - 12:00pm</b> Is it possible to extract cortical depth information from traditionally 2D optical imaging spectroscopy using concurrent fMRI data?	A.J.Kennerley		<b>Page 26</b>
	<b>12:00 - 12:15pm</b> Non-contact photogrammetric spatial registration system for fNIRS featuring color-coded markers	Daisuke Tsuzuki		<b>Page 27</b>
	<b>12:15 - 12:30pm</b> Functional Connectivity of the PFC via Partial Correlation Analysis	Z. Einalou		<b>Page 28</b>
	<b>12:30 - 12:45pm</b> Hierarchical Bayesian estimation with ARD prior improves depth accuracy and spatial resolution of diffuse optical tomography	Takeaki Shimokawa		<b>Page 29</b>
	<b>12:45 - 1:45pm</b> <b>LUNCH Sponsored by TechEn, Shimadzu and ISS</b>		<b>North Cloisters</b>	
	<b>NEURODEVELOPMENT (I)</b> <i>Chair: Richard Aslin</i>		<b>Cruciform Lecture Theatre</b>	
	<b>1:45 - 2:15pm</b> <b>A cognitive neuroscience approach to the early identification of autism</b>	<b>Charles Nelson</b>		<b>Page 31</b>
	<b>2:15 - 2:30pm</b> Evoked changes in oxygen consumption in premature neonates	Nadege Roche-Labarbe		<b>Page 32</b>
	<b>2:30 - 2:45pm</b> Building from Basics: fNIRS recordings from 6-month olds investigate sensory cortex selectivity and response suppression	Lauren L. Emberson		<b>Page 33</b>
	<b>2:45 - 3:00pm</b> The specificity of the neural response to language at birth	Lillian May		<b>Page 34</b>
	<b>3:00 - 5:00pm</b> <b>POSTER VIEWING OF EVEN NUMBERED POSTERS</b> <b>TEA Sponsored by Loptek</b>		<b>North Cloisters and Old Refectory</b>	
	<b>NEURODEVELOPMENT (II)</b> <i>Chair: Gergely Csibra</i>		<b>Cruciform Lecture Theatre</b>	
	<b>5:00 - 5:30pm</b> <b>NIRS imaging of spatiotemporal activity in the developing brain</b>	<b>Gentaro Taga</b>		<b>Page 36</b>
	<b>5:30 - 5:45pm</b> Cortical Mapping of 3D Optical Topography in infants	Maria D Papademetriou		<b>Page 37</b>
	<b>5:45 - 6:00pm</b> Interaction between brain maturation and experience: hemodynamic responses to speech categories in full term and preterm neonates	Minagawa-Kawai		<b>Page 38</b>
	<b>6:00 - 6:15pm</b> Developmental Changes in Frontal-Parietal Activation Associated with Visual Working Memory Capacity	John Spencer		<b>Page 39</b>
	<b>6:15 - 6:45pm</b> <b>KEYNOTE LECTURE: Brain connectivity inference for fMRI data</b> <i>Chair: Jeremy Hebden</i>	<b>Will Penny</b>	<b>Cruciform Lecture Theatre</b>	<b>Page 41</b>
	<b>7:00 - 11:30pm</b> <b>SOCIAL EVENT: AN EVENING IN A GREAT BRITISH PUB</b>		<b>Jeremy Bentham Pub, University Street</b>	

<u>Sunday 28th October</u>	<u>Session</u>	<u>Speaker</u>	<u>Location</u>	<u>Page #</u>
	<b>CLOCKS GO BACK ONE HOUR ON SUNDAY MORNING</b>			
	<b>APPLICATIONS: ADULT (I)</b>		Cruciform Lecture Theatre	
	<i>Chair: Daniel Leff</i>			
8:00 - 8:30am	<b>Application of functional near infrared spectroscopy in Psychiatry</b>	<b>Andreas Fallgatter</b>		Page 43
8:30 - 8:45am	Physiological Correlates of Perceptual Learning	Uma Shahani		Page 44
8:45 - 9:00am	Neural correlates of spontaneous deception	Kang Lee		Page 45
9:00 - 9:15am	Frontal activation scales with working memory load: a near-infrared spectroscopy study	Frank A. Fishburn		Page 46
9:15 - 9:30am	The effect of inner speech on arterial pCO <sub>2</sub> , cerebral hemodynamics and	Martin Wolf		Page 47
9:30 - 11:30am	<b>POSTER VIEWING OF ODD NUMBERED POSTERS</b> <b>COFFEE Sponsored by NIRx</b>		North Cloisters and Old Refectory	
	<b>APPLICATIONS : ADULT (II)</b>		Cruciform Lecture Theatre	
	<i>Chair: Hellmuth Obrig</i>			
11:30 - 12:00pm	<b>Adult Clinical Applications of Near Infrared Spectroscopy</b>	<b>Martin Smith</b>		Page 49
12:00 - 12:15pm	Assessments of memory impairments associated with posttraumatic stress disorder (PTSD) by near infrared spectroscopy	Fenghua Tian		Page 50
12:15 - 12:30pm	Simultaneous EEG and fNIRS assessment of language processing: A tool to investigate changes in aphasia during (sub)acute stroke?	Sonja Rossi		Page 51
12:30 - 12:45pm	Characterising the response of cytochrome c oxidase to changes in cerebral oxygen supply and demand in the healthy adult brain	Christina Kolyva		Page 52
12:45 - 1:00pm	Investigating the origin of hemodynamic fluctuations using high-resolution diffuse optical tomography in humans	Christina Habermehl		Page 53
1:00 - 2:00pm	<b>LUNCH Sponsored by TechEn, Shimadzu and ISS</b>			
2:00 - 2:30pm	<b>KEYNOTE LECTURE: Interpreting NIRS data: the modelling challenge</b>	<b>Murad Banaji</b>	Cruciform Lecture Theatre	Page 55
	<i>Chair: Clare Elwell</i>			
	<b>APPLICATIONS: NEONATAL AND PAEDIATRIC</b>		Cruciform Lecture Theatre	
	<i>Chair: Martin Wolf</i>			
2:30 - 3:00pm	<b>Clinical application of Near infrared Spectroscopy in the Neonate</b>	<b>Frank Van Bel</b>		Page 57
3:00 - 3:15pm	A Study of Preschool Irritability: NIRS Brain Imaging of correlates of clinical irritability	Susan B. Perlman		Page 58
3:15 - 3:30pm	Development of a Multimodal Functional Brain Imaging Laboratory for Newborn Infants	T Austin		Page 59
3:30 - 3:45pm	<b>Round Up and Close</b>	<b>Clare Elwell</b>		

# Poster Presentations

Even numbers will present on Saturday the 27th. Odd numbers will present on Sunday the 28th.

## Hardware Developments

1	Heidrun Wabnitz	"A non-contact fNIRS scanner: First <i>in-vivo</i> tests"	Page 61
2	Luke Dunne	"Design of a new fNIRS multi-wavelength, multi-channel time resolved spectrometer using a supercontinuum laser for measuring brain tissue haemodynamics and metabolism"	Page 62
3	Louis Gagnon	"Multiple short separation measurements for removal of systemic oscillation in NIRS data"	Page 63
4	Marcin Pastewski	"A wireless, self-calibrating sensor for fNIRS studies in preterm infants"	Page 64
5	Yui Yamaguchi	"Development of new fNIRS-EEG system for seamless whole brain study"	Page 65
6	Udo Weigel	"DOCNEURO: Towards pre-commercial, clinical prototype development of hybrid diffuse correlation spectroscopy (DCS) and frequency domain diffuse optical spectroscopy (DOS) for bed-side neuromonitoring"	Page 66
7	Sophie Piper	"A wearable multi-channel NIRS imaging system for brain imaging in freely moving subjects"	Page 67
8	Raphael Zimmermann	"Silicon photomultipliers bear potential for fNIRS instrumentation"	Page 68
9	Masashi Kiguchi	"New techniques for advanced optical topography"	Page 69
10	Fumio Kawaguchi	"Development of multichannel fNIRS system with transcranial pulse oximetry function using CDMA technique"	Page 70
11	Paolo Giacometti	"Head probe for combined near-infrared spectroscopy and electroencephalography"	Page 71
12	Blasie Frederick	"A low cost NIRS spectrometer for monitoring global physiological hemodynamic fluctuations"	Page 72
13	Angela Harrivel	"Improved light injection and detection methods for fNIRS headgear for use in avionics and astronautics"	Page 73
14	Chester Wildey	"Advances in customized headgear and optode-hair penetration"	Page 74
15	Felipe Orihuela-Espina	"Towards a device capable of detecting the fast optical signal and its application to stroke rehabilitation"	Page 75
16	Chester Wildey	"Smaller, lighter, cheaper. A new fNIRS system from MRRA Inc."	Page 76
17	Arthur "Buzz" DiMartino	"TechEn: Advancing fNIRS technology for results"	Page 77

### **Multi-Modal Monitoring**

<b>18</b>	Theodore Huppert	"Multimodal investigation of neural-vascular coupling during somatosensory stimulation and resting state using concurrent MEG-NIRS and MRI-NIRS"	Page 79
<b>19</b>	Ilias Tachtsidis	"Investigation of brain tissue oxygenation, cytochrome-c-oxidase and intracellular metabolites during perinatal cerebral hypoxia-ischaemia"	Page 80
<b>20</b>	Makii Muthalib	"Multimodal correlation analysis between fNIRS, fMRI and EEG during motor tasks"	Page 81
<b>21</b>	Kunal Shetty	"A study of executive control during intracorporeal minimally invasive suturing (ICS)"	Page 82
<b>22</b>	Anique Driessen	"Simultaneous (Q)EEG and NIRS measurements during eyes open and eyes closed resting state conditions in healthy volunteers"	Page 83
<b>23</b>	Katherine Perdue	"Comparison of NIRS, EEG and MEG sensitivity to spatial scale of brain activity"	Page 84
<b>24</b>	Kunal Shetty	"Effects of visuomotor rotation in laparoscopic surgery on the prefrontal cortex (PFC)"	Page 85

### **Data Analysis**

<b>25</b>	Alp Özdemir	"High frequency content in blood volume signal is predictive of migraine without aura"	Page 87
<b>26</b>	Uma Shahani	"Haemodynamic responses to moving sinusoidal gratings"	Page 88
<b>27</b>	Felix Scholkmann	"A new approach to extract stimulus-evoked hemodynamic responses in fNIRS signals using Ensemble Empirical Mode Decomposition"	Page 89
<b>28</b>	Hamid Dehghani	"Development and utilisation of computational models for tomographic fNIRS imaging and co-registration with multi-modal data"	Page 90
<b>29</b>	Mehrdad Dadgostar	"Comparison of denoising algorithms in fNIRS"	Page 91
<b>30</b>	Na Yu	"Wavelet cross correlation for identification of interference between systemic physiological processes and brain haemodynamics measured by time-domain fNIRS during frontal lobe activation"	Page 92
<b>31</b>	Florian Haeussinger	"Influence of static and dynamic physiological parameters on the measurement of neural activation with functional near-infrared spectroscopy (fNIRS)"	Page 93
<b>32</b>	Juliette Selb	"Contamination of NIRS functional connectivity maps by superficial vasculature symmetries"	Page 94
<b>33</b>	Willaim Simpson	"Kernel distributed lag model applied to fNIRS recordings from visual cortex"	Page 95
<b>34</b>	Sinem Burcu Erdogan	"Analysis of task-dependent scalp signal contribution in fNIRS by use of reciprocal information from fMRI"	Page 96

<b>35</b>	Toshifumi Sano	"Using variable hemodynamic response functions to optimize differential temporal information of hemodynamics in functional near-infrared spectroscopy"	Page 97
<b>36</b>	Ata Akin	"Consistency of functional connectivity maps"	Page 98
<b>37</b>	Christoph Schmitz	"Enhancement of hemodynamic contrast in the cancerous breast by carbogen inspiration"	Page 99
<b>38</b>	Makiko Imai	"Region-specific cortico-cortical synchronization and desynchronization of hemodynamic changes"	Page 100
<b>39</b>	Sabrina Brigadoi	"The importance of motion artifacts correction in cognitive studies"	Page 101
<b>40</b>	David Highton	"Model enhanced interpretation of NIRS signals in brain injured patients"	Page 102
<b>41</b>	Arcangelo Merla	"GLM based detection of fast optical signals in visual cortex"	Page 103
<b>42</b>	Tanveer Talukdar	"Continuous correction of differential path length factor in near-infrared spectroscopy"	Page 104
<b>43</b>	Kazuki Kurihara	"Segmentation of magnetic resonance images for individual head models for DOT"	Page 105
<b>44</b>	Lucian Comandar	"Development of a flexible neurofeedback system for brain-machine interface using fNIRS"	Page 106
<b>45</b>	Angela Harrivel	"Artifact removal for assessment of cross-network anticorrelation with fNIRS"	Page 107
<b>46</b>	Randall Barbour	"A computing environment for multimodal integration of EEG and fNIRS"	Page 108
<b>47</b>	Theodore Huppert	"Group level analysis methods in NIRS"	Page 109
<b>48</b>	Shunsuke Ichimura	"Morphological modification of brain structure for optical brain activation imaging"	Page 110
<b>49</b>	Nima Hemmati	"Correlation based signal improvement (CBSI) combined with motion artifact removal algorithm (MARA) for enhancing synthetic fNIRS signals"	Page 111
<b>50</b>	Satoru Kohno	"Quantitative indexes of artifacts for NIRS signals"	Page 112
<b>51</b>	Masaya Ohtake	"Head phantom including multiple absorption inclusions for near infrared topography"	Page 113
<b>52</b>	Fenghua Tian	"Depth-compensated tomography (DC-Tomo) based on standard brain atlas"	Page 114
<b>53</b>	Kevin Mandrick	"fNIRS data analysis by Slope: an alternative method to distinguish the level of cortical activation pattern during functional tasks"	Page 115
<b>54</b>	Hirokazu Tanaka	"Task-related component analysis for functional neuroimaging and application to near-infrared spectroscopy data"	Page 116

### **Neurodevelopment (I) and (II)**

55	Fumitaka Homae	"Fronto-posterior connectivity during phonological processing in the infant brain"	Page 118
56	Hellmuth Obrig	"Prelexical cues in first language acquisition: Training induced changes in the processing of phonotactically legal and illegal consonant clusters"	Page 119
57	Heather Bortfeld	"Classifying hemodynamic responses to auditory input in preverbal infants"	Page 120
58	Sho Tsuji	"Six-month-olds' brains respond more to highly frequent vowels"	Page 121
59	Camillia Bouchon	"Vowels and consonants at birth: a NIRS study"	Page 122
60	Teresa Wilcox	"Experience-dependent changes in infant brain and behavior: The case of color priming"	Page 123
61	Yukifumi Monden	"Randomized, double blind, placebo controlled, crossover design to evaluate MPH effect in ADHD children using fNIRS monitoring during Go/NoGo task"	Page 124
62	Teresa Wilcox	"Different patterns of activation in temporal cortex to function vs. non-function events"	Page 125
63	Laura Edwards	"Hemodynamic correlates of ratio-based numerical discrimination in infancy: An fNIRS study"	Page 126
64	Alejandrina Cristia	"DBIfNIRS: A community-augmented online database of infant functional near infrared spectroscopy studies"	Page 127
65	Nawal Abboub	"Perception of rhythmic grouping: An optical imaging study"	Page 128
66	Teresa Wilcox	"Age-related changes in the functional organization of object processing pathways"	Page 129
67	Madeleine Verriotis	"Multimodal EEG-NIRS studies of noxious and sensory stimulation in newborn infants"	Page 130
68	John Spencer	"Integrating behavioral and neural dynamics over development in the dimensional change card sort (DCCS) task"	Page 131
69	Laura Anderson	"Neural responses to point-light displays of biological motion in the first year of life: a functional near-infrared study"	Page 132
70	Maria Arredondo	"Location, location, location-Where are we in the brain?"	Page 133
<b><u>Applications: Adult (I)</u></b>			
71	Fabio Scarpa	"Assessment of hemodynamic activity modulations: investigating visual short-term memory mechanisms through fNIRS and EEG"	Page 135
72	Hiroaki Suzuki	"Measurements of hemoglobin concentration of the deep brain tissue using near-infrared time-resolved spectroscopy"	Page 136



<b>73</b>	Meryem Yücel	"Brain response to painful versus non-painful electrical stimuli"	Page 137
<b>74</b>	Simone Cutini	"An exploratory fNIRS study with immersive virtual reality"	Page 138
<b>75</b>	Marie McGrath	"Examining resting state functional activity in the medial prefrontal cortex using fNIRS: A "proof-of-concept" study"	Page 139
<b>76</b>	Mayank Rehani	"Driving errors and cerebral hemodynamics during simulated driving with and without hands-free telecommunication: It's not about where your hands are, it's about where your mind is"	Page 140
<b>77</b>	Cathy Mondloch	"The neural correlates of the face attractiveness aftereffect: A functional near-infrared spectroscopy (fNIRS) study"	Page 141
<b>78</b>	Yagesh Bhambhani	"Cerebral & muscle hemodynamics during unilateral knee extensions at different loads & velocities"	Page 142
<b>79</b>	Sara Basso Moro	"Verbal and visual working memory investigated by multi-channel time-resolved functional near-infrared spectroscopy"	Page 143
<b>80</b>	Francesca Ferri	"Being social: a NIRS study on the social simon effect"	Page 144
<b>81</b>	Hercules Grant	"Cerebral hemodynamic responses during carbon dioxide rebreathing, aerobic exercise and cognitive activity"	Page 145
<b>82</b>	Silvia Bisconti	"Prefrontal cortex is not activated by observation of disgusting and pleasant pictures: a multi-channel time-resolved functional near-infrared spectroscopy study in healthy subjects"	Page 146
<b>83</b>	Jeff Dunn	"Quantification of cerebral hemoglobin in adult brain using near-infrared spectroscopy"	Page 147
<b><u>Applications: Adult (II)</u></b>			
<b>84</b>	Meeri Kim	"Cerebral hemodynamics at altitude: Effects of hyperventilation and acclimatization on cerebral blood flow and oxygenation"	Page 149
<b>85</b>	Arnab Ghosh	"Reduction of cytochrome c oxidase during vasovagal hypoxia-ischaemia in human adult brain: a case study"	Page 150
<b>86</b>	Matthew Cloud	"Longitudinal fNIRS stroop study of adult traumatic brain injured patients in post-acute treatment"	Page 151
<b>87</b>	Eiju Watanabe	"Presurgical diagnosis of the epileptogenic focus using near-infrared spectroscopy mapping"	Page 152
<b>88</b>	Christoph Schmitz	"Enhancement of hemodynamic contrast in the cancerous breast by controlled articulation"	Page 153
<b>89</b>	Daniel Milej	"Validation of the time-resolved optical measurement combined with ICG-bolus tracking in assessment of brain perfusion in posttraumatic brain injury patients"	Page 154

90	Ingo Helmich	"Differential cortical mechanisms of tool use related gesture production"	Page 155
91	Anouk Vermeij	"Very-low-frequency oscillations of cerebral hemodynamics and blood pressure are influenced by aging and cognitive activation"	Page 156
92	Jeff Dunn	"Functional near-infrared spectroscopy shows altered functional connectivity in the brain of patients with multiple sclerosis"	Page 157
93	Alessandro Torricelli	"Cortical response during motor task in adult volunteers and epileptic patients with movement disorders: a multimodality fNIRS-EEG, fMRI-EEG and TMS clinical study"	Page 158
94	Jeff Dunn	"Methylphenidate-mediated reduction in prefrontal hemodynamic responses to working memory task: A functional near-infrared spectroscopy study"	Page 159
95	Michal Kacprzak	"Analysis of frequency components in optical signals measured by time-resolved near infrared spectroscopy on adults head: preliminary study"	Page 160
96	Yoko Hoshi	"Cerebral vasoreactivity to carbon dioxide and neural activation in schizophrenia: a study with near-infrared time resolved spectroscopy"	Page 161
97	Christian Rummel	"Multi-channel and multi-distance NIRS during neuroangiography: Feasibility and technical aspects"	Page 162
98	Daan Meester	"Prefrontal cortex activity and H-reflex variability during dual and single task treadmill walking in healthy subjects"	Page 163
99	Rebecca Dewey	"fNIRS of auditory, visual and somatosensory responses in normal-hearing individuals"	Page 164
100	Christian Rummel	"NIRS during neuroangiography: First results and potential added value"	Page 165
101	Xin Zhang	"Abnormal activation pattern of schizophrenia in performing Tower of London test"	Page 166
102	Jose Leon-Carrion	"The rate of deoxy-Hb changes can be used as a neuromarker to detect the emergence from deep to light anesthesia"	Page 167
103	Arnold Wilkins	"Uncomfortable visual stimulation and the shape of the haemodynamic response"	Page 168
<b><u>Applications: Neonatal and Paediatric</u></b>			
104	Theodore Huppert	"Investigation of resting state and visual evoked functional activity in neonates during concurrent NIRS and MRI"	Page 170
105	Mahdi Mahmoudzadeh	"The impact of neonatal intraventricular hemorrhage on auditory hemodynamic response"	Page 171

<b>106</b>	George Aleandrakis	"Concurrent functional near-infrared spectroscopy and motion tracking to assess functional improvement of children with cerebral palsy after constrained induced motion therapy"	Page 172
<b><u>Other</u></b>			
<b>107</b>	Tingting Zhu	"Optimal wavelength combinations for resolving in-vivo concentration changes of haemoglobin and cytochrome-c-oxidase with fNIRS"	Page 174
<b>108</b>	Heidrun Wabnitz	"Performance assessment of time-domain fNIRS instruments in the 'nEUROpt' project"	Page 175
<b>109</b>	Andrew Macnab	"Near infrared spectroscopy of the bladder to monitor physiologic function in health and disease"	Page 176
<b>110</b>	Yukari Tanikawa	" <i>In vivo</i> time-resolved DOT images of human forearm under exercises"	Page 177
<b>111</b>	Theodore Huppert		Page 178
<b>112</b>	Gerrita van Spijker	"Exploring the effects of Nilvadipine on blood pressure, cerebral blood flow and cerebral autoregulation in patients with mild to moderate Alzheimer's Disease: a NILVAD add-on study"	Page 179
<b>113</b>	Kevin Mandrick	"Hemodynamic cerebral responses as a function of the neurovascular coupling to brain activation: NIRS signal changes"	Page 180
<b>114</b>	Ata Akin	"Analysis of Stroop Test fNIRS data by use of singular value decomposition"	Page 181
<b>115</b>	Terence Leung	"Cerebral oxygenation measurement with acousto-optics: a simulation study"	Page 182

Oral Session  
**Keynote**  
Friday, 26<sup>th</sup> October  
5:30pm

# Trends in Functional Near Infrared Spectroscopy

David Boas

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fNIRS continues to experience exponential growth as it approaches 20 years since the first studies of functional brain activation were published in 1993. The manually culled results of a PubMed search of (“Near Infrared Spectroscopy” or “NIRS” or “Optical Topography” or “Optical Tomography”) and “Brain” support this exponential growth model in terms of number of

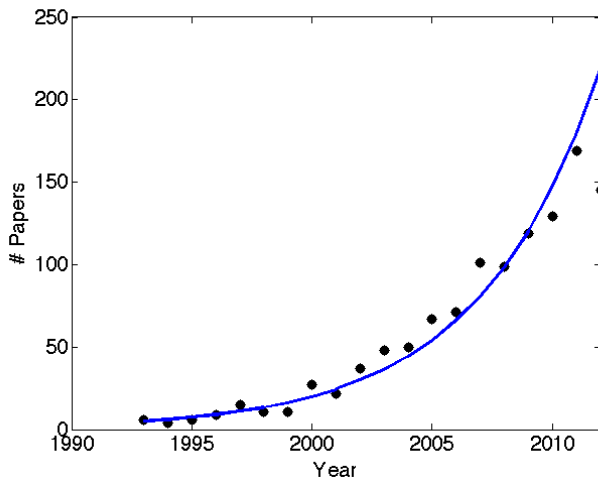


Figure 1. Number of fNIRS papers published each year. Note that this only contains 8 months of 2012.

publications per year, as shown in figure 1. Note that 2012 only contains 8 months of publications and thus is projected to increase by 50%. The line is an exponential fit with a doubling time of 3.5 years. Will we have 400 publications in 2015?

This database of results contains 1150 publications, with only 149 from the first ten years. The first ten years already broadly covered fNIRS applications domains with papers containing brain activation paradigms with visual, motor/sensory, cognitive, language, auditory, and psychological stimuli; exploring clinical applications for schizophrenia, depression, Alzheimer’s disease, epilepsy, and stroke; exploring multi-modal integration with fMRI, PET, TCD, MEG,

EEG, TMS, and DBS; as well as studying brain activation in infants. These domains were explored further over the next 10 years with particular emphasis on cognitive stimuli; schizophrenia and stroke; multi-modal integration with fMRI, EEG, and TMS; strong growth in infant studies; and a recent explosion of resting state functional connectivity studies.

The successfully translation from technology development to application is further supported by 8 of the top 10 journals publishing fNIRS papers coming from the neuro and health sciences, with only 2 coming from technology disciplines.

During my talk, I will discuss these trends, some of the work coming out of our group at MGH, exciting new opportunities that are emerging, as well as the grass-roots efforts to further strengthen and grow our community.

1) 159	Neuroimage
2) 68	J Biomed Opt
3) 47	Conf Proc IEEE Eng Med Biol Soc
4) 41	Neurosci Lett
5) 40	Adv Exp Med Biol
6) 31	Neuroreport
7) 23	Brain Res
8) 21	Human Brain Mapping
9) 20	Neurosci Res
10) 18	PLoS ONE

Oral Session  
**Hardware Developments**  
Saturday, 27<sup>th</sup> October  
8:00am  
*Chair: Heidrun Wabnitz*

# Ischemic stroke & hybrid diffuse optics combining diffuse correlation spectroscopy (DCS) and diffuse optical spectroscopy (DOS-NIRS)

**Turgut Durduran**

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I will present a brief summary of the development of diffuse correlation spectroscopy (DCS) (also known as “diffuse wave spectroscopy”) for non-invasive measurement of cerebral blood flow (CBF) in human brain [1, 2]. DCS was introduced for “deep-tissue” biomedical optics by Arjun Yodh’s laboratory at University of Pennsylvania, Philadelphia [3] where we have shown that by combining DCS with simultaneous diffuse optical spectroscopy (DOS/NIRS), changes in cerebral blood flow (CBF), oxy-hemoglobin (HbO<sub>2</sub>) and deoxy-hemoglobin (Hb) concentrations and total hemoglobin concentration (THC) can be measured and the cerebral metabolic rate of oxygen extraction (CMRO<sub>2</sub>) can be calculated. This combined approach is termed “hybrid diffuse optics” since we are combining two diffuse optical methods to get a more complete picture of the brain physiology.

The technology has, since, was validated against an array of other modalities and was introduced to the clinics for applications ranging from peripheral vascular diseases to oncology to neuro-monitoring [1, 2]. The validation studies have demonstrated that DCS can indeed non-invasively measure changes in CBF even in adult brain, albeit with some limitations. In this presentation, I will focus on its utility in clinical ischemic stroke monitoring from the emergency care to acute, bed-side management to risk assessment. I will describe a time-line of common clinical care that an ischemic stroke patient receives upon arrival to the unit and use examples from various studies to demonstrate the potential for these technologies in clinical settings for early diagnosis, management and risk assessment. Finally, I will outline the next-generation instrumentation and the immediate and long-term goals.

This work was partially funded by Fundació Cellex Barcelona, Marie Curie IRG (FP7, RPTAMON), Instituto de Salud Carlos III (FIS), Ministerio de Ciencia e Innovación (Ramon y Cajal Fellowship, ACIO), OPTIMILK, LASERLAB (FP7), European regional development funds (FEDER), Institució CERCA and National Institutes of Health (NIH). It is the product of many years of collaborations with many faculty, researchers and students from University of Pennsylvania, Children’s Hospital of Philadelphia and Hospital de la Santa Creu i Sant Pau. In particular, AG Yodh, JA Detre, JH Greenberg, DJ Licht, JM Fabregas, RM Delgado have been the leaders of this effort.

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## **Time resolved functional near infrared spectroscopy by means of time gated system at small interfiber distance**

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Functional near infrared spectroscopy (fNIRS) is an emerging new tool to non-invasively monitor task-related hemodynamic changes in the human brain, due to the ability of photon migration measurements to investigate inner structures of biological tissues. As a matter of fact, for the brain the potentially interesting optical changes or alterations occurring in the cortex are masked by the scalp, skull and clear layer that cover the brain cortex. In this work we focused on small (few millimeters) source-detector distance time-resolved measurements, which are predicted to have better contrast, better spatial resolution, and lower noise than the typical measurements performed at few centimeters. A common assumption, in fact, is that the larger is the source-detector (inter-fiber) distance, the deeper is the visited region. Even if this is true for continuous-wave measurements, in time domain the mean depth visited by collected photons is independent from the inter-fiber distance, while it increases for longer arrival times of photons.

The instrumental set-up we consider is an improved version of the one used for the first experimental feasibility of such a kind of measurements. We developed an instrument based on a fiber laser providing two independent output at 710nm and 820nm with a repetition frequency of 40MHz and a FWHM of few tens of picoseconds. In our instrumental set-up we exploited a fast-gating (<500ps) front-end electronics enabling a silicon Single-Photon Avalanche Diode (SPAD) for time-correlated single-photon counting. By means of this detector, we can acquire “late” (strongly attenuated) photons of the diffused light collected few millimeters apart from the injection point. Such photons traveled long paths through the head, then exploring the brain cortex. This is possible because the fast-gated SPAD rejects the huge amount of “early” photons which otherwise would saturate the detection electronic chain. Two fast time-gated detectors are used to acquire independently late photons at the two wavelengths in order to estimate concentrations of oxy- and deoxy-hemoglobin during brain activity. This prototype, differently from the previous ones, can follow the hemodynamic behavior of tissues for both oxy- and deoxy-hemoglobin at the same time with measurement at small distance between injection and detection points.

We validated the instrument on tissue phantoms attaining photon-timing resolutions of 100ps (FWHM) and photon-counting dynamic ranges of around  $10^8$  (160dB). Preliminary results in-vivo show for the first time the possibility to detect the dynamic of oxygenated and deoxygenated hemoglobin concentration during a cerebral activation with an interfiber distance of few millimeters.



## Imaging multiple functional networks with diffuse optical tomography

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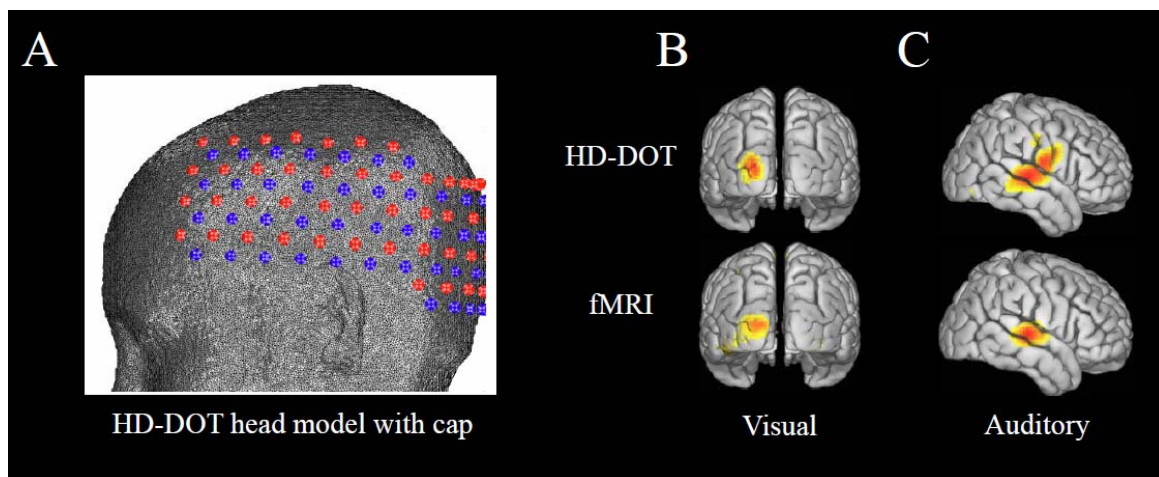
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High-density diffuse optical tomography (HD-DOT) methods have improved localization and resolution compared to traditional near infrared spectroscopy (NIRS). However HD-DOT systems have generally suffered from a limited field of view (FOV) and studies have focused on sensory and motor areas. In order to consider a wider range of clinical applications, it is necessary to sample a large contiguous FOV that permits the study of multiple functional brain networks in parallel. We have developed an HD-DOT system and cap that spans over 50% of the superficial cortical surface (**Fig. 1A**), covering occipital, temporal, and much of the parietal and frontal lobes. In this study, the DOT image reconstructions are calculated within the subject-specific anatomical space; data are affine transformed into a standard MNI atlas space to create group averages of the activations. Stimuli include somatosensory, visual (**Fig. 1B**), auditory (**Fig. 1C**), and language tasks. Locations of activation within the language processing system are clearly separable into passive auditory and visual processing regions and regions responsible for the generation of language. Activation locations are validated with subject-matched non-concurrent fMRI. In parallel, we evaluate brain networks with spontaneous resting-state functional connectivity methods. The seeds chosen in the field of view of the HD-DOT system provide access to the visual, motor, and language networks. Seed-based correlation maps of resting-state networks generated from HD-DOT data are then compared with fMRI. Cortical maps from both modalities show clear differentiation between the three networks investigated.



**Figure 1:** Our high-density diffuse optical tomography (HD-DOT) system covers much of the superficial cortical surface. **(A)** A subject-specific T1-weighted MRI-based mesh with the positions of source (red) and detector (blue) fibers of our system. **(B)** Example of an activation in response to a flickering checkerboard stimulation located within the right visual field. **(C)** Example of an activation in response to an auditory stimulus composed of a series of words. All activation are thresholded at 50% of the maximum value for that given activation. Data are presented on the MIN152 atlas cortical surface.

Oral Session  
**Multi-Modal Monitoring**  
Saturday, 27<sup>th</sup> October  
9:00am  
*Chair: Maria Angela Franceschini*

False Positives in fNIRS: Identifying and Quantifying Systemic Influences on Neurovascular Coupling in fNIRS Data during Cognitive Tasks.

### **Ilias Tachtsidis**

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Brain functional studies of task-specific activation using functional neuroimaging rely on the existence of a close coupling between neuronal electrical excitation and regional changes in brain metabolism and regional cerebral blood flow, sometimes referred to as activation-flow coupling or neurovascular coupling. Regional haemodynamic changes are used as a surrogate marker for changes in regional brain function that occur due to changes in metabolism during excitatory or inhibitory neurotransmission, both of which are energy consuming processes. Functional near-infrared spectroscopy (fNIRS) is used to non-invasively measure the changes in oxygenated and deoxygenated haemoglobin ([HbO<sub>2</sub>], [HHb]) and hence investigate the brain haemodynamic changes, which occur in response to functional activation at specific regions of the cerebral cortex. The fNIRS signal is an indirect measure of neuronal activity.

Neuronal excitation causes oxidative metabolism increases that lead to brain vascular responses; blood vessels dilate causing an increase in cerebral blood flow and cerebral blood volume. This oversupply of oxygenated blood causes the [HbO<sub>2</sub>] to increase and the [HHb] to reduce. In order for this response to be monitored unambiguously it is important that the haemodynamic task related activity is occurring on top of an unchanged global systemic and brain resting state. Comparisons of the fNIRS signals implicitly assume that the coupling between [HbO<sub>2</sub>], [HHb] and neuronal activity (neurovascular coupling) is equivalent during the duration of activation in individual and between individuals. However, changes in cerebrovascular dynamics due to task related systemic cardiovascular changes can lead to results that are unrelated to neuronal activity; in addition to producing extracranial vasculature changes that can lead to fNIRS signal contamination.

fNIRS is increasingly being used to investigate higher level cognitive functions, some of which might produce significant changes in systemic variables. For several years now (see references) we have investigated the relationship between task related brain fNIRS and systemic changes in a large group of young healthy adults during cognitive functional tasks that included anagram solving and video gaming. Our results suggest that task related changes seen in systemic variables in some volunteers might contribute to the changes in the fNIRS signals leading to false positives.

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# Neurovascular Coupling Varies with Level of Global Cerebral Ischemia in a Rat Model

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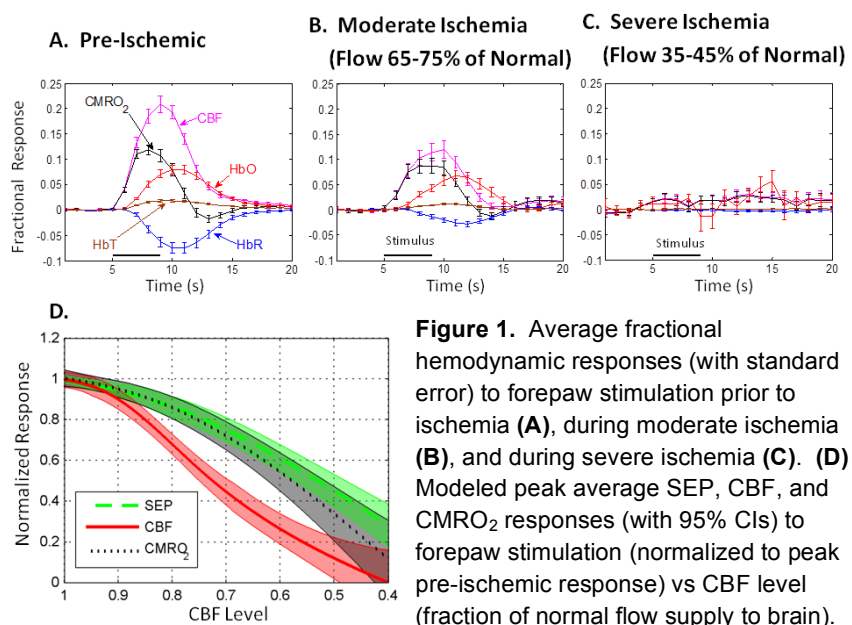
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In healthy brains, localized increases in neuronal activity are strongly correlated, both spatially and temporally, with localized increases in cerebral blood flow (CBF) and cerebral metabolic consumption of oxygen (CMRO<sub>2</sub>). Thus, quantification of hemodynamics due to increased neuronal activity, i.e., neurovascular coupling, has long been a topic of intense interest. In this study, we employ multimodal monitoring of hemodynamics and electrical activity to investigate the effects of global cerebral ischemia on neurovascular coupling in a rat animal model (N = 46). To make these measurements, we combined the well-established optical techniques of laser speckle contrast imaging and optical imaging of intrinsic signals, which involve planar illumination of the brain surface with NIR and visible

illumination to construct two-dimensional images of tissue oxy-hemoglobin concentration (HbO), deoxy-hemoglobin concentration (HbR), total hemoglobin concentration (HbT), and CBF. CMRO<sub>2</sub> was calculated from these measurements via a compartmental model. We also measured the electrical somatosensory evoked potentials (SEP) to characterize neuronal activity. To our knowledge, this is the first study that examines functional activation during graded ischemia.



**Figure 1.** Average fractional hemodynamic responses (with standard error) to forepaw stimulation prior to ischemia (A), during moderate ischemia (B), and during severe ischemia (C). (D) Modeled peak average SEP, CBF, and CMRO<sub>2</sub> responses (with 95% CIs) to forepaw stimulation (normalized to peak pre-ischemic response) vs CBF level (fraction of normal flow supply to brain).

**Fig. 1** is a summary of the main results from this study. The pre-ischemic CBF response to stimulation is substantially larger than the pre-ischemic CMRO<sub>2</sub> response (**Fig. 1A**), which suggests that increases in oxygen delivery to cerebral tissue due to stimulation exceed increases in oxygen consumption. If this mismatch from CBF and CMRO<sub>2</sub> persists during cerebral ischemia, then repeated functional stimulation during a stroke could potentially increase the base level of oxygen in cerebral tissue. However, our results show that the mismatch between the CBF and CMRO<sub>2</sub> responses becomes smaller with increasing global ischemia (**Figs. 1B-C**). A mixed effects model was used to model the peak SEP, CBF, and CMRO<sub>2</sub> responses to forepaw stimulation as a function of the level of ischemia, i.e., the fraction of normal flow supply to the brain (**Fig. 1D**). The peak responses were normalized to their pre-ischemic responses to enable a direct comparison of the effects of ischemia between the different parameters. The CMRO<sub>2</sub> and SEP functional responses remained tightly coupled to each other at all levels of ischemia examined. Importantly, as the animals became ischemic, the CBF response was more strongly attenuated than was the CMRO<sub>2</sub> response. The HbO and HbR responses were also more strongly attenuated than the CMRO<sub>2</sub> response (data not shown). These results demonstrate independence between CMRO<sub>2</sub> and the other hemodynamic parameters, illustrating the importance of measuring both blood flow and blood oxygenation to calculate oxygen metabolism, rather than using blood flow or blood oxygenation as a surrogate for oxygen metabolism.

# Impact of Extracranial Vessels on Task-Evoked Artefacts in Functional Near Infrared Spectroscopy for Multiple Tasks.

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## Introduction:

A major limitation in functional Near Infrared Spectroscopy (fNIRS) is its high sensitivity to hemodynamics of non-cerebral superficial tissue layers including scalp, skull and pial vessels. While pulsatile noise components induced by heart beat and respiration can be effectively removed by filtering, Mayer waves and low frequency vascular fluctuations strongly interfere with cerebral hemodynamical signals (1,2). Moreover, facial blood flow is controlled by the autonomic nervous system, and is therefore systematically influenced by certain tasks. This fact results in false positives in fNIRS activation maps (1-4). In order to separate superficial contribution from cerebral response, precise knowledge about skin hemodynamic response is indispensable. In the present study we used concurrent multi-distance fNIRS and skin-sensitive functional Magnetic Resonance Imaging (fMRI) in order to quantify the contribution of superficial vessels in fNIRS and quantify their response to stimuli of different types. Since conventional fMRI usually exhibits poor sensitivity to the skin, we used a dedicated skin sensitive fMRI method based on multi-echo (5) and high-resolution 3D (6) echo planar imaging (EPI).

## Methods:

We combined multi-distance fNIRS and skin-sensitive fMRI in functional experiment using four different tasks: (i) working memory, (ii) emotional processing, (iii) speech production, (iv) gustatory stimulation. Concentration changes of oxygenated (oxy-Hb) and deoxygenated (deoxy-Hb) hemoglobin were recorded using NIROScout (NIRx, Berlin, Germany) with a dense grid of optodes consisting of fNIRS channels with short (15 mm) and long (30 mm) source-detector separations. Experiments were performed inside a 3T MR scanner (Siemens, Erlangen, Germany) using multi-echo EPI (5) in working memory experiments and high-resolutions 3D-EPI (6) providing 1.5x1.5x1.5 mm<sup>3</sup> resolution for all other tasks.

## Results:

We observed pronounced task-evoked superficial signals in the oxy-Hb time courses in near as well as in far fNIRS channels, for all subjects in all tasks. For deoxy-Hb we found similar behaviour, but with weaker signal intensities than for oxy-Hb. The oxy-Hb concentration changes in short-distance channels demonstrate strong correlation with fMRI signal of temporal skin vessels for gustatory stimulations and speech production task and with the supraorbital forehead veins for working memory tasks. The skin vessels response functions for both stimuli types could be obtained.

## Conclusion

We demonstrated that hemodynamics of facial veins contribute to task-evoked fNIRS signals. This superficial contribution depends on the face position and the type of stimulus. The skin vessel response function obtained in our experiment could be further used in GLM analysis of fNIRS data in order to separate task-evoked signals resulting from the skin and from brain signals.

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Oral Session  
**Data Analysis**  
Saturday, 27<sup>th</sup> October  
10:45am  
*Chair: Joseph Culver*

## **Methodological challenges in the application of fNIRS for infant cognitive neuroscience**

**Emmanuel Dupoux & Alex Cristia**

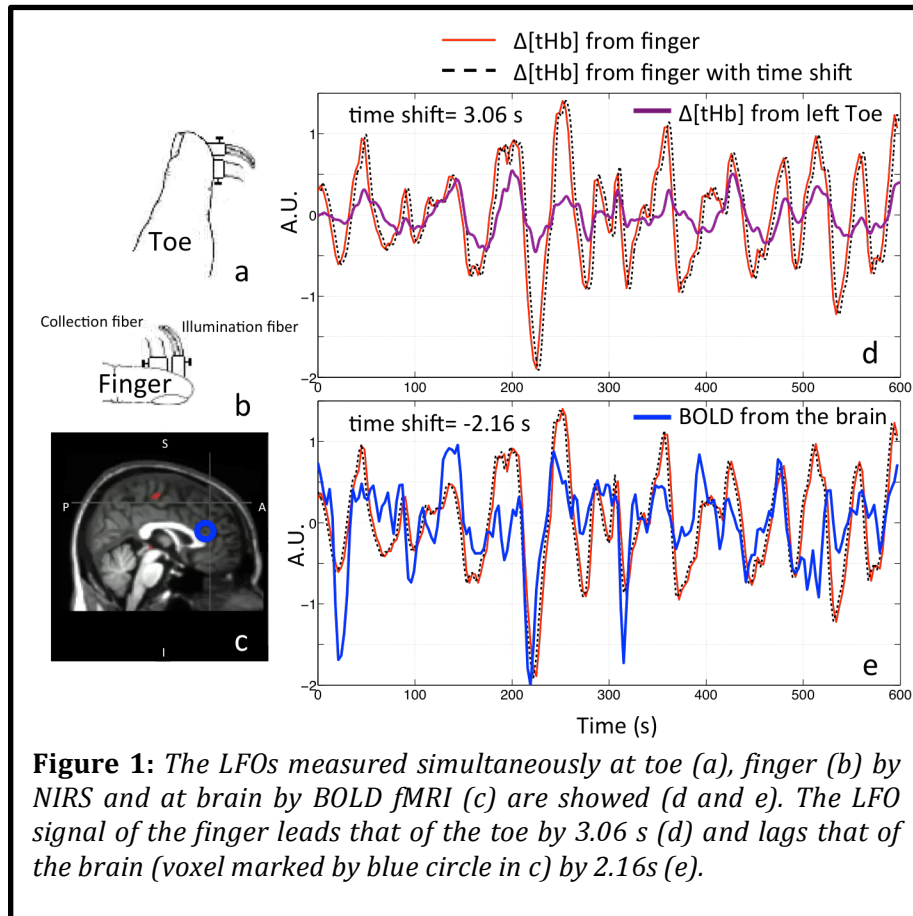
Functional Near InfraRed Spectroscopy (fNIRS) is a promising, rapidly expanding technique for the study of infant cognition. However, a number of methodological stumbling blocks remain to be lifted for the widespread acceptance of this technique by the cognitive neuroscience community at large. We illustrate three such stumbling blocks in three separate studies conducted in our group. The first one deals with brain lateralization for language in neonates and raises the issue of the shape of the Hemodynamic Response Function in newborns. The second addresses language discrimination and raises the issue of free parameters in data analysis and replicability. The third one addresses the representation of self body motion and raises the issue of head-brain co-registration. We propose that public repositories of published results should help to increase the quality of analysis and methods by enabling large scale meta-analyses.

**Low frequency oscillations measured in the periphery with near infrared spectroscopy (NIRS) are strongly correlated with blood oxygen level-dependent functional magnetic resonance imaging (BOLD fMRI) signals**

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**Abstract:** Low frequency oscillations (LFOs) in the range of 0.01-0.15Hz are commonly observed in functional imaging studies, such as blood oxygen level-dependent functional magnetic resonance imaging (BOLD fMRI) and functional near infrared spectroscopy (fNIRS). Some of these LFOs are non-neuronal



**Figure 1:** The LFOs measured simultaneously at toe (a), finger (b) by NIRS and at brain by BOLD fMRI (c) are showed (d and e). The LFO signal of the finger leads that of the toe by 3.06 s (d) and lags that of the brain (voxel marked by blue circle in c) by 2.16s (e).

and are closely related to autonomic physiological processes. In the current study, we conducted a concurrent resting state fMRI and NIRS experiment with healthy volunteers. LFO data was collected simultaneously at peripheral sites, e.g. middle fingertip and big toes by NIRS, and centrally in the brain by BOLD fMRI. The cross-correlations of the LFOs collected from the finger, the toes, and the brain were calculated. Our data shows that the LFOs measured in the periphery (NIRS signals) and in the brain (BOLD fMRI) were strongly correlated with varying time delays. This demonstrates that some portion of the LFOs actually reflect systemic physiological

circulatory effects. Furthermore, we demonstrated that NIRS is effective for measuring the peripheral LFOs, and that these LFOs and the temporal shifts between them are consistent in healthy participants, and may serve as useful biomarkers for detecting and monitoring circulatory dysfunction.

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**Reference:**

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# Integrated Data Analysis Environment for fNIRS

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Data analysis is important in the field of fNIRS because of rich source information in measured signals. There are considerable variations in obtained signals according to the experimental designs for data acquisition. Therefore in order to obtain reliable results exploring for adequate signal analysis methods and the best parameters for them is required.

To meet these requirements we developed platform software for testing analysis methods, “Platform for Optical Topography Analysis Tools” (POTATo) [1]. There are three conceptual architectures in the software; an analysis script creator, a visualization designing tool and a plug-in wizard. Analysis script creator automatically produces a code for analyzing data according to an analysis recipe which was designed by the user using Graphical User Interface (GUI). By referring to the created script, users can read all the analysis that POTATo does and also modify it. For visualization of data and analysis results we can use a Layout editor which enables us to design layout and drawing contents. Additional functionality for signal analysis is supported by the Plug-in wizard. By using this tool users can create and import additional analysis functions into POTATo. Some useful analysis functions have been implemented and provided as plug-in file sets including: “Motion detection using wavelet analysis” [2] which was developed for neonate measurement to detect not only spike-like changes but also slower changes; “T-Test with peak search” [3] which enables the detection of significant signal changes by searching time of peak value for each trial and subject; “Transfer entropy analysis” [4] which is similar to correlation analysis but this function returns the amount of information transferred from one to another data array; “Time delayed decorrelation and clustering” [5] which enables extracting activation signals from a group of subjects. The concept of integrated data analysis environment will help researchers to test and evaluate traditional and novel signal analysis methods on fNIRS data and to obtain fruitful results.

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## Is it possible to extract cortical depth information from traditionally 2D optical imaging spectroscopy using concurrent fMRI data?

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Optical imaging spectroscopy is a technique used in neuro-imaging for the quantification of changes in cerebral blood volume and oxygenation during neural activity, with high temporal and 2D spatial resolution. One disadvantage is that the technique relies on many assumptions concerning the light absorption and scattering properties of the imaged tissue. For example both baseline and relevant changes in blood volume and oxygenation are often assumed to be homogeneous throughout the brain tissue (Frostig et al., 1990; Malonek and Grinvald, 1996; Mayhew et al., 2000). This assumption is common place as one only needs an estimate of the path length (often from Monte Carlo simulations) to use a simple Beer-Lambert relationship to extract 2D images of chromophore (e.g. Hbr & HbO<sub>2</sub>) concentration changes from light attenuation data. However it is well known that cortical brain tissue has a heterogeneous distribution of vascular and physiological structures (Pawlik et al., 1981). This suggests that using a homogeneous tissue model in OIS to assess the hemodynamic changes (to neuronal activity) to help understand the nature and time course of the Blood oxygenation level dependent (BOLD) functional magnetic resonance imaging (fMRI) signal is inappropriate. In the current research we take the opposite approach and use concurrent fMRI data to help us to understand the nature and time course of the optical imaging ‘measurements’ in terms of cortical depth and tissue/absorption heterogeneity.

Three dimensional 7 Tesla fMRI measurements were used to parameterize and refine a multi layered heterogeneous tissue model for use in the Monte Carlo simulations (MCS) of light transport through tissue. Simulations showed that fMRI data can be used to estimate absorption depth sensitivity and response profiles. These profiles can be used in the Beer-Lambert law to weight the path length estimate from the MCS; thus dramatically changing the magnitude of the chromophore (e.g. Hbr & HbO<sub>2</sub>) concentration changes. We implemented concurrent fMRI and OIS, with light attenuation captured using interleaved illumination at four wavelengths (495, 586, 559 and 575nm), in an animal model. When hemodynamic measurements estimated from the heterogeneous optical imaging spectroscopy algorithm were input into Monte Carlo simulations of MR signal attenuation it resulted in consistent prediction of the concurrently measured BOLD signal. In contrast the homogeneous model under-estimates BOLD changes by approximately 40% (see figure 1). Furthermore the response depth profile was dynamic over time and thus we estimated depth information from a traditionally 2D imaging method. This has important implications for research investigating effects such as the negative BOLD effect which have been shown to originate deeper in the cortical tissue (Boorman et.al. 2010).

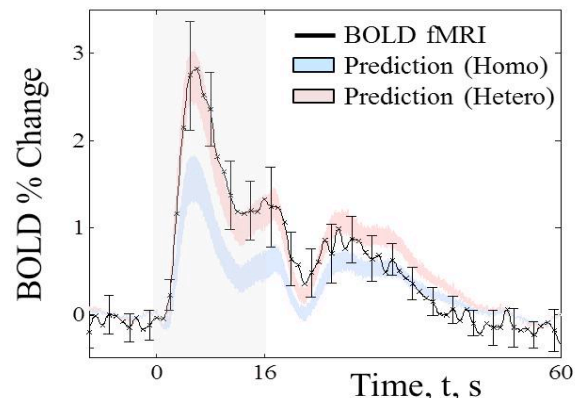


Figure 1 – Hemodynamic data is input into a MCS of MR signal attenuation to predict the concurrent BOLD fMRI signal. Good agreement only when using the heterogeneous tissue model.

Using the three dimensional characteristics of the functional magnetic resonance imaging signal we have improved and refined our optical imaging spectroscopy analysis. This work will be extended and exploited in our current research using MRI to parameterize a diffuse optical tomography algorithm in a project investigating the metabolic monitoring of cortical activity.

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## Non-contact photogrammetric spatial registration system for fNIRS featuring color-coded markers

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Functional near-infrared spectroscopy (fNIRS) is a neuroimaging technique which has several merits in comparison with other imaging methods. However, as a neuroimaging tool, fNIRS faced a fundamental dilemma. In its stand-alone setting, fNIRS can obtain only functional information and no structural information. Thus, we recently developed an anchor-based probabilistic registration method which based on canonical probabilistic registration method that uses MRIs in a reference database instead of the subject's own MRIs, and probabilistically registers the fNIRS optode or channel positions onto a standard template in standard stereotactic brain coordinate system such as Montreal Neurological Institute (MNI). In this session we present a new approach called the photogrammetric spatial registration that applies photogrammetric method to measure the three reference points (Nz, AL and AR) and optode positions (plus any given anchor points) on subject's head to achieve the anchor-based probabilistic registration. The proposed system utilizes a digital camera instead of a magnetic 3D-digitizer. The photogrammetric method is non-contact, and features use of color-coded targets that enable automatic rendering of acquired images. Although the current measurement system focuses on the usage of registration for fNIRS data on healthy adults heads, it would be applicable, with some minor modifications, in clinical studies and also useful in infant studies which require non-contact and remote sensing environment.

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# Functional Connectivity of the PFC via Partial Correlation Analysis

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In this study, we aimed to investigate the functional connectivity in the prefrontal cortex (PFC) during a modified version of the color-word matching Stroop task. Stroop task, which requires responding to a particular stimulus dimension while suppressing a competing stimulus dimension, is commonly used to evaluate PFC function [1, 2]. This task consists of three different stimulus conditions: Neutral (N), Congruent (C) and Incongruent (IC). Connectivity patterns obtained from hemodynamic response to each stimulus is expected to be different because of the contribution of partially different neural networks [1]. A continuous wave 16 channels near-infrared spectroscopy device (ARGES Cerebro, Hemosoft Inc., Turkey) was used to measure the changes in HbO<sub>2</sub> concentrations from 11 healthy volunteers. The probe was placed on the forehead with approximate cortical sampling regions as depicted in Figure 1 [3]. fNIRS data were band-pass filtered using a wavelet algorithm with frequency range of 0.003-0.08Hz. Partial correlation (PC) values were computed for each stimulus condition [4]. Since PC analysis helps to remove the effect of indirect paths, by applying this method, the PC between two channels is correlated, with the activity at all other 14 regions regressed out. We report in Table 1 the major PC change in two pairs of channels that reside on two hemispheres: 1<sup>st</sup> and 12<sup>th</sup> with  $F(2,33) = 4.1$ ,  $p = 0.025$  and 5<sup>th</sup> and 14<sup>th</sup> with  $F(2,33) = 3.84$ ,  $p = 0.031$ . The rest of the channel pairs have PC values in the range  $0.058 \pm 0.0647$  for N condition,  $0.057 \pm 0.0632$  for C condition and  $0.056 \pm 0.072$  for IC condition. PC values are negative for C condition, meaning a reversal of the temporal dynamics between those two channels, while they are positive for IC condition, representing a synchronous contribution of those two channels to the suppression of irrelevant stimulus dimension and decision making effort. The PC method is preferable to standard cross correlation due to its inherent elimination of the most common and underlying activity in all the channels and highlighting only the actual correlation between the two channels.

Table 1: Statistical properties of partial correlation

Stimulus Type	Channels: 5 <sup>th</sup> and 14 <sup>th</sup>	Channels: 1 <sup>st</sup> and 12 <sup>th</sup>
	Mean $\pm$ Std	Mean $\pm$ Std
Neutral	-0.098 $\pm$ 0.149	0.044 $\pm$ 0.119
Congruent	-0.024 $\pm$ 0.136	-0.085 $\pm$ 0.147
Incongruent	0.062 $\pm$ 0.138	0.0821 $\pm$ 0.177

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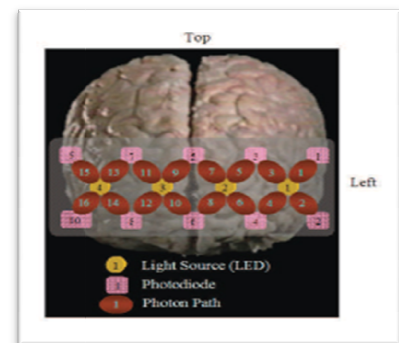


Figure1: Placement of the fNIRS probe on the PFC

# Hierarchical Bayesian estimation with ARD prior improves depth accuracy and spatial resolution of diffuse optical tomography

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Recently, high-density diffuse optical tomography (HD-DOT) has received much attention as an advanced technique for visualizing the cortical activities. The large number of overlapping measurement channels due to the use of high-density probe arrays permits the reconstruction of the internal activities, even with a reflectance-only measurement. However, accurate three-dimensional reconstruction is still a challenging problem. First, the exponentially decaying sensitivity causes a systematic depth-localization error. Second, the nature of diffusive light makes the image blurred. In this presentation, we propose a three-dimensional reconstruction method that overcomes these two problems by introducing sensitivity-normalized regularization and sparsity into the hierarchical Bayesian method [1]. We performed phantom experiments to validate the proposed method under three conditions of probe interval: 26 mm, 18.4 mm, and 13 mm. We found that two absorbers with distances shorter than the probe interval could be discriminated under the high-density conditions of 18.4-mm and 13-mm intervals. This discrimination ability was possible even if the depths of the two absorbers were different from each other (see Fig. 1). These results show the high spatial resolution of the proposed method in both depth and horizontal directions.

In addition, we extended this method to estimate the hemodynamic responses both in the cortex and in the superficial layers incorporating prior knowledge that the hemodynamic responses in the cortex is local and that in the superficial layers are rather global in the Bayesian method. We also show the preliminary results of the extended method.

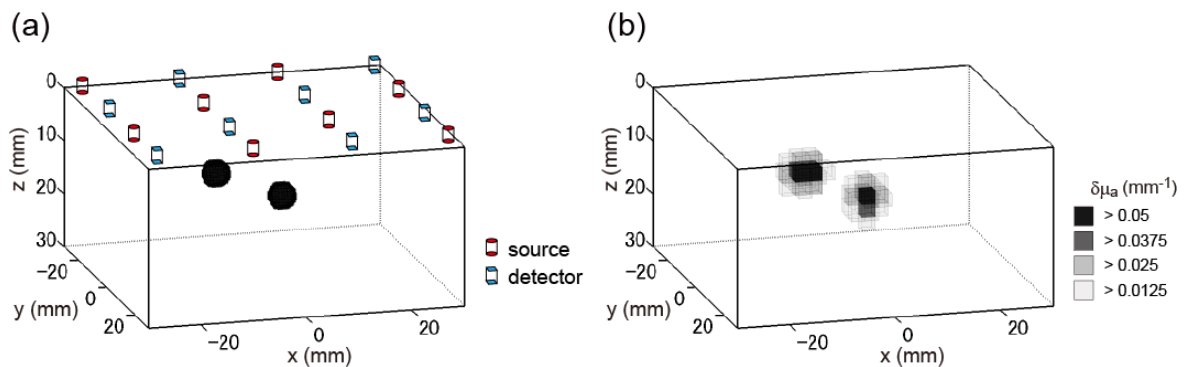


Fig. 1 (a) True absorber position. (b) Estimation result of the proposed method.

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Oral Session  
**Neurodevelopment (I)**  
Saturday, 27<sup>th</sup> October  
1:45pm  
*Chair: Richard Aslin*

## A cognitive neuroscience approach to the early identification of autism

Charles A. Nelson III

### Abstract:

There is wide support for the notion that the outcome of children diagnosed with autism is superior among those who receive early intervention. However, early intervention is predicated on early identification, and at the present time, the average age of diagnosis is 3 years. For a number of years now an international consortium of more than 18 sites has been studying infants at high risk for developing autism by virtue of having an older sibling with the disorder (placing the infant's chances of developing an ASD at 1:5). Despite great promise, there are few behavioral signs of the disorder that are predictive in infants less than 12-18 months. One reason for the failure to identify signs in younger infants is how limited the behavioral repertoire is in infants less than 12 or so months. In the program of research I will talk about, we hypothesize that examining the brain directly, bypassing behavior, may prove more efficacious, as changes in behavioral development typically follow changes in brain development. In this context I will describe preliminary findings from a longitudinal study focused on tracking high risk infants from 3-36 months of life, using a battery of EEG, ERP, and fNIRS tasks, although the major focus of this talk will be on our fNIRS data.

## Evoked changes in oxygen consumption in premature neonates

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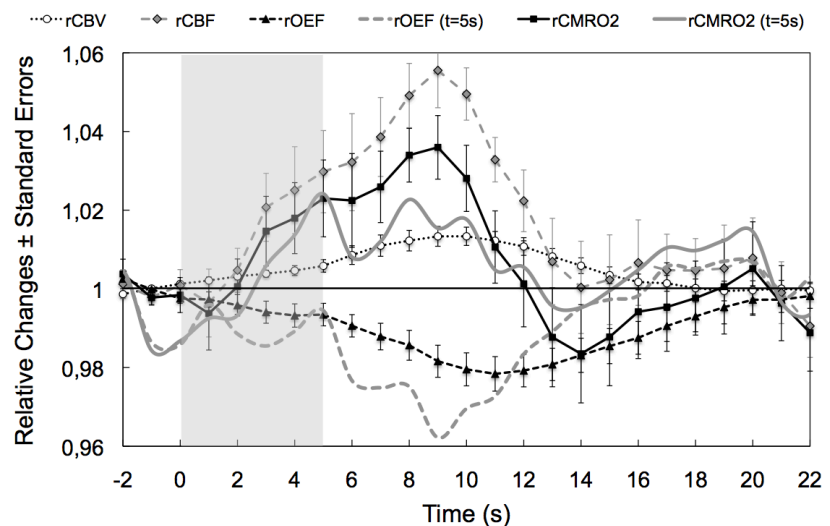
Corresponding author: N. Roche-Labarbe at [nadege.roche@unicaen.fr](mailto:nadege.roche@unicaen.fr)

The hemodynamic functional response is used as a reliable marker of neuronal activity in countless studies of brain function and cognition. In newborns and infants however, conflicting results have appeared in the literature concerning the typical response, and there is little information on brain metabolism and functional activation. Measurement of all hemodynamic components and oxygen metabolism is critical for understanding neurovascular coupling in the developing brain, and for using the functional response as a reliable functional imaging marker of brain development.

To this aim we combined multiple NIRS techniques: we used diffuse correlation spectroscopy (DCS) to measure relative cerebral blood flow changes (rCBF), frequency domain near infrared spectroscopy (FDNIRS) to measure baseline hemoglobin oxygenation (SO<sub>2</sub>), oxy- and deoxy-hemoglobin concentrations (HbO and HbR respectively) and cerebral blood volume (CBV), and continuous wave near infrared spectroscopy (CWNIRS) to measure relative hemoglobin concentration and oxygenation changes (rSO<sub>2</sub>). By combining all these measures we estimated relative changes in the cerebral metabolic rate of oxygen (rCMRO<sub>2</sub>) in the somatosensory cortex of 6 preterm neonates during passive tactile stimulation of the hand. We are the first to report functional changes in cerebral blood flow and cerebral oxygen consumption in premature newborns.

Our data shows in preterm neonates the typical pattern of hemodynamic response to sensory stimulation: an increase in rSO<sub>2</sub> and CBV. However, the “preterm” response however is slower (longer time to peak, see figure) compared with adults. We did not observe any inverted response pattern associated with stimulation. Blood flow starts increasing immediately after stimulus onset, and returns to baseline before blood volume. This is consistent with the model of pre-capillary arteriole active dilation driving the CBF response, with a subsequent CBV increase influenced by capillaries and veins dilating passively to accommodate the extra blood. The higher compliance of the veins relative to arterioles can explain the slower return to baseline of CBV with respect to CBF.

rCMRO<sub>2</sub> shows a biphasic pattern: an increase immediately after stimulus onset, followed by a significant post-stimulus undershoot due to blood flow returning faster to baseline than oxygenation. However, if we calculate rCMRO<sub>2</sub> taking into account the longer mean transit time through the venous compartment in preterm infants compared with adults ( $\tau \geq 5s$ ), the undershoot disappears (see figure). We observed an evoked flow-metabolism ratio of  $n=2.8$ , consistent with numerous studies in animals and human adults.





Building from Basics: fNIRS recordings from 6-month olds investigate sensory cortex selectivity and response suppression

**Lauren L. Emberson**, Holly Palmeri, & Richard N. Aslin

Brain and Cognitive Sciences Department, University of Rochester

While the last 15 years has seen a veritable explosion in both interest and knowledge about the neural mechanisms supporting cognition, methodological constraints have prevented investigations into the functional organization of the brain early in the lifespan. fNIRS is uniquely poised to facilitate such investigations by providing many of the benefits afforded by fMRI (e.g. unambiguous spatial location of neural responses) but without the same methodological hurdles (e.g. the need for rigid head stabilization). Of course, using fNIRS to investigate the neural mechanisms supporting infant cognition has its own set of methodological issues to tackle (see Aslin, in press for a review). Part of the challenge in establishing methodologically rigorous investigations is the fact that so little is known about the young, developing brain. Some early surprising findings (e.g. the involvement of the prefrontal cortex in simple habituation studies, e.g., Nakano, Watanabe, Homae, & Taga, 2009) suggest that the infant brain could be functionally quite different from the adult brain. Thus, it is unclear whether a given pattern of results has arisen from unanticipated methodological limitations or is a result of functional differences in the infant brain.

In an effort to gain traction on this issue, the current project employs established, rigorous behavioral paradigms from the adult cognitive neuroscientific literature to probe functional neural activity in infants at 6 months. These paradigms provide strong hypotheses that will support a comparison of the adult and infant brain. Here, we describe a part of this broader effort, in which we utilize a well-established phenomenon in adult fMRI studies, **response suppression**. Response suppression has been described as “[o]ne of the most robust experience-related cortical dynamics” (Grill-Spector, Henson, & Martin, 2006) and is defined as a reduction in neural response during the repetition of a stimulus compared to the presentation of variable stimuli. These differential neural responses occur in cortex that is selective for a particular stimulus.

We employed a response suppression paradigm to investigate responses of visual and auditory cortex to auditory or visual stimuli. Infants viewed smiling, female faces and heard familiar, two-syllable words spoken in infant-directed speech (e.g., “diaper”). Stimuli were presented in uni-modal blocks (**auditory** or **visual** stimuli presented at 1sec SOA) that were either **repeated** (a single face or word presented 8 times) or **variable** (eight different faces or eight different words). After each block, a jittered ISI was employed (mean duration = 6.5 secs, 4 to 9 secs). While this project is ongoing, data collected from 16 infants demonstrate that auditory presentation produces responses in the auditory cortex but not the visual cortex. Moreover, repeated auditory presentation results in a weaker fNIRS response than variable presentation in these channels. We interpret this as strong evidence for response suppression in auditory cortex. We also find responses in visual cortex to visual presentation but evidence for repetition enhancement rather than response suppression in occipital channels. Future analyses will probe these potential modality-differences in neural selectivity and response suppression.

Aslin, R. N. (in press). Questioning the questions that have been asked about the infant brain using NIRS. *Cognitive Neuropsychology*.

Grill-Spector, K., Henson, R., & Martin, A. (2006). Repetition and the brain: neural models of stimulus-specific effects. *Trends in Cognitive Sciences*, 10, 14-23.

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The specificity of the neural response to language at birth

**Lillian May** (1), Judit Gervain (2), Manuel Carreiras (3,4), Janet F. Werker (1)

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From birth, the human brain responds specially to language. Greater neural activation is reported in neonates when listening to forward language versus acoustically matched but non-linguistic backwards language (Pena et al., 2003). Recent research has indicated that this response to language at birth is not purely a result of language experience: the neonate brain responds to unfamiliar language in similar neural areas as familiar language, although less strongly (Sato et al., 2011; May et al., 2011). However, it is still unknown whether the neural response to language seen at birth is triggered only by language stimuli, or if stimuli sharing some properties of language might also elicit a similar brain response in neonates. To answer this question, we compared the newborn neural response to familiar language, unfamiliar language, and whistled language.

Silbo Gomero is a whistled surrogate language of Spanish, used in parts of the Canary Islands. As a surrogate language, it shares Spanish prosody and grammar, but uses whistled contours instead of speech sounds and has a very limited phonological inventory. Moreover, Silbo Gomero is never acquired as a first language. Crucially, the adult brain seems to require experience to process Silbo Gomero specially: only Silbo speakers – and not Spanish speakers - show greater left hemisphere activation to forward versus backwards Silbo (Carreiras, 2005).

In the present studies, we used functional Near Infrared Spectroscopy to examine cortical activation in English-exposed newborns in response to both forward and backward familiar language (English), unfamiliar language (Spanish), and whistled language (Silbo Gomero). Activation was measured across 12 optical channels in temporal regions of each hemisphere (24 channels in total). If the newborn brain response to language is triggered specifically by language stimuli, we expected to find strong activation for both familiar and unfamiliar language, but little or no activation to whistled language. In contrast, if the newborn brain responds to all communicative forms that contain prosodic and rhythmical properties of language, we expected to find activation to whistled language as well as to familiar and unfamiliar language.

In Study 1, we measured the neural response to forward and backward English (familiar language) as well as forward and backward Spanish (unfamiliar language), while in Study 2 we measured the neural response to forward and backward Spanish and forward and backward Silbo Gomero. Results revealed strong bilateral activation in similar anterior temporal regions to both forward English and forward Spanish. Additionally, we found greater activation to forward versus backward English, but no difference in the response to forward versus backward Spanish. When comparing the neonates' neural activation to Spanish versus Silbo Gomero we observed a significant difference in activation between languages: the neural response to Spanish was significantly larger than the response to Silbo, primarily in the anterior temporal regions. The neonate brain response to both forward and backward Silbo was very small across all regions.

Our results indicate that the newborn brain is broadly tuned to respond to both familiar and unfamiliar language, with an additional advantage for forward versus backwards only in response to familiar language, but that the neural response to language is not triggered by stimuli sharing only the rhythmical and prosodic properties of language. This suggests a high level of specificity in the neural response to language from the first days of life, and suggests that all properties of language—including phonological complexity-- may need to be present to activate this response.

Oral Session  
**Neurodevelopment (II)**  
Saturday, 27<sup>th</sup> October  
5:00pm  
*Chair: Gergely Csibra*

## **NIRS imaging of spatiotemporal activity in the developing brain**

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The multi-channel continuous wave NIRS technique has a great advantage in studying detailed hemodynamics in relation to cortical activity in young infants. The technique has been used to reveal not only functional activations in response to stimuli but also resting-state networks of spontaneous activity during sleeping in infants. It is notable that detecting timing information among different regions of the cortex does not necessarily need measurement of absolute values of hemodynamic signals, which has been a long-lasting problem of continuous wave NIRS. Here, I will discuss open issues concerning spatiotemporal property of hemodynamics in the developing brain.

- (1) Do subtle differences in timing of response to stimuli reflect flows of cortical activation? (Watanabe et al. Hum Brain Map 2012; Taga et al. Phil. Trans. R. Soc. A 2011)
- (2) Do specific patterns of response of oxy-Hb and deoxy-Hb changes represent cortical activation or deactivation? (Watanabe et al. Dev Psychobiol 2012)
- (3) Is the information on phase differences between oxy-Hb and deoxy-Hb changes useful to understand mechanisms of interaction between neural and metabolic processes? (Taga et al. Neurosci Lett 2000; Pierro et al. NeuroImage 2012)
- (4) Do the resting state network change depending on sleep states?
- (5) Do the resting state network reflect developmental disorders? (White et al. NeuroImage 2012)
- (6) Are the resting state networks different between preterm and term infants? (kato et al. Brain & Dev 2012; Arichi et al. NeuroImage 2012)
- (7) How the spontaneous hemodynamic changes affect responses to stimuli? (Colonnese & Khazipov NeuroImage 2012)
- (8) Is the resting state network modified by repetition of stimuli or by behavioral learning? (Homae et al. Front Psychol 2011)
- (9) Do the sequences of transient spatiotemporal patterns of hemodynamic changes encode functional information that the brain creates?
- (10) How does the development of the anatomical connectivity change the resting state network?

# Cortical Mapping of 3D Optical Topography in infants

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Over the last decade optical topography (OT) has to study functional brain imaging in infants. The technology can be used to study awake infants and address topics such as biological motion, face and voice processing. Even though OT has been used to map haemodynamic responses during activation with specific regions of the cortex, co-registration between the haemodynamic response measured at the surface of the head and the underlying cortical anatomy remains a challenge. This is primarily due to the lack in capacity for measuring brain structure for anatomical reference and the lack of common control points between the optical array, the head and the anatomical image. Furthermore, OT studies treat the data as single source-detector (channel) haemodynamic responses even if the data are measures from multiple channels at different separations. Conventional image reconstruction involves finding the optical properties of the medium from a set of measurements, which are then combined to calculate the chromophore concentrations. We use a multispectral imaging algorithm to reconstruct haemodynamic responses and obtain 3D optical topography images. In order to make a precise statement about cerebral specialisation during cortical activation it is necessary to co-register functional activation onto an anatomical atlas. In this paper we describe a method for co-registering 3D optical topography images on 3D brain volumes rendered from MRI scans. In this paper we are presenting a method for co-registering 3D optical topography images onto anatomical brain images obtained from MRI structurals of the individual infants.

Five 4-7 month old infants were included in the study. The experiment consisted of three types of auditory experimental trials – voice, non-voice and silence. The trials alternated beginning with 10-s baseline followed by 10-s experimental trial. The UCL optical topography system was used for data acquisition. Two optical imaging arrays were placed on each temporal lobe, providing a total of 19 channels per array. The probes were placed according to anatomical landmarks which were obtained by measuring each infants head circumference, distance between the forehead, ears and lower point of the back of the skull. Increases in oxyhaemoglobin concentration (HbO<sub>2</sub>) were measured and reconstructed using a multispectral imaging algorithm with spatially variant regularisation to optimise depth discrimination. Images were obtained showing the distribution of activation in a plane parallel to the surface, as well as changes in activation with depth. Structural MRIs of the subjects were also obtained. The scans were used to reconstruct 3D head and brain images of the participants. The anatomical landmarks used for placing the probes were marked on the head reconstructions as offsets from the anterior commissure. These marks were used to reconstruct the probes and channel positions on the head reconstructions. The images of the HbO<sub>2</sub> changes during activation were co-registered on the 3D brain reconstructions rendered from the MRI scans.

State-of-the-art optical topography systems, coupled with sophisticated data analysis and image reconstruction can provide a practical tool which can be used to answer research questions in developmental psychology.

Interaction between brain maturation and experience: hemodynamic responses to speech categories in full term and preterm neonates

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2. Institut d'étude de la cognition, Ecole Normale Supérieure
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The development of near-infrared spectroscopy (NIRS) has allowed us to effectively measure auditory-related neural system in very young human brains. Utilizing this advantage, we measured cerebral responses to vowel and intonation changes in full term neonates (37-41 weeks of gestation), preterm neonates (26-33 weeks of gestation) shortly after birth and preterm infants (26-33 weeks of gestation) at their due date. We document differences and similarities between the three groups with respect to (1) the time course and shape of the evoked hemodynamic response (oxygenated hemoglobin and deoxygenated hemoglobin) in comparison with the adult Hemodynamic Response Function (HRF), (2) response amplitudes and activated regions depending on the two change conditions, (3) the connectivity of frontal and temporal regions and (4) analysis of resting state is still ongoing. In this dataset, HRFs similar to the adults' was observed for full term neonates and preterm infants at due date., but not for preterm neonates Asymmetrical cerebral activations were also observed for the former two groups around the Supra Marginal Area in response to both types of changes. Interestingly, connectivity during presentation of speech was stronger for the preterm infants at due date than the other two groups, suggesting a critical role of auditory experience outside the utero. In current analyses, we are investigating resting state connectivity in all three groups. These results underline the interaction between maturation and auditory experience for the functional development of neonates' brain.

Developmental Changes in Frontal-Parietal Activation  
Associated with Visual Working Memory Capacity

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& Larissa Samuelson  
Department of Psychology & Delta Center, University of Iowa

For decades, we have known that children's visual working memory (VWM) capacity increases over development. Moreover, several theories have proposed that changes in working memory capacity underlie major transitions in thought. Nevertheless, there have been relatively few investigations of the neural systems that underlie the development of VWM capacity, particularly early in development when changes are most dramatic.

Work using fMRI with adults has shown that activation in the intra-parietal sulcus (IPS) and dorso-lateral prefrontal cortex (DLPFC) increases as working memory loads increase. For instance, in the change detection task, participants are asked to remember the features of a set of objects presented in a sample array. After a 1 second delay, they are shown a second test array and are asked whether the objects are the 'same' or 'different'. Activation in IPS increases with set size. Critically, neural activation asymptotes once the set size increases beyond the participant's VWM capacity. That is, for participants with a VWM capacity of 4 items, there is comparable activation in IPS at set sizes 4-8. Moreover, studies have shown that activation in DLPFC is robust, particularly at higher set sizes when the memory demands are severe.

In the present study, we asked whether these signatures of VWM processes are evident early in development during periods of rapid change in working memory capacity. 14 3-year-old children and 16 4-year-old children completed a change detection task with set sizes of 1, 2, and 3 objects in an event-related design. On each trial, the sample array was presented for 2s, there was a 1s delay, and then the test array appeared until participants responded. This was followed by a jittered inter-trial interval. In each run, children completed 6 'same' trials and 6 'different' trials at each set size. They completed a total of 4 runs across two visits to the lab. Behavioral data from these sessions replicated previous findings showing that 3-year-olds have a VWM capacity of roughly 1 item ( $M = 1.28$  items), while 4-year-olds have a VWM capacity of roughly 2 items ( $M = 1.73$  items).

NIRS data were recorded using a TechEn CW6 system with 16 detectors and 8 sources. We recorded from frontal (F5/F3; F4/F6) and parietal (P5/P3; P4/P6) areas in both hemispheres. The data were high pass filtered at .016 Hz and low pass filtered at .5 Hz. Pre-processing eliminated noisy signals (<80dB) and trials with motion artifact ( $dOD > .35$ ). Analyses focused on trials with correct behavioral performance. 76% of correct trials for 3-year-olds had usable NIRS data (11.3 trials/participant), while 65% of correct trials for 4-year-olds had usable NIRS data (11.4 trials/participant).

Results showed an increase in left parietal activation (near P3) as set size increased, with a statistically robust correlation ( $R^2 = 0.152$ ) between NIRS activation at high set sizes and behaviorally-measured VWM capacity. This was also the case in left frontal regions (near F5;  $R^2 = 0.332$ ). Right parietal activation (near P4) showed an increase in activation over set sizes, but this effect was primarily driven by the neural response on 'different' trials ( $R^2 = 0.368$ ). These data are generally consistent with data from adult fMRI studies; however, unlike studies in later development, our data suggest that the VWM system shows greater lateralization in early childhood.

Oral Session  
**Keynote**  
Saturday, 27<sup>th</sup> October  
6:15pm



TITLE: Brain connectivity inference for fMRI data

William Penny

ABSTRACT: I will describe a set of differential equations which describe how (i) stimulus activity gives rise to neurodynamics which in turn (ii) give rise to changes in blood volume and deoxyhemoglobin which in turn (iii) give rise to the BOLD fMRI signal. Parameters of this model are then estimated from fMRI data using a Bayesian estimation approach. This produces posterior estimates of model parameters and an approximation to the model evidence. Different assumptions about brain connectivity (or other aspects of the forward model) can then be formally compared using Bayesian model inference. This approach can be applied to NIRS by updating part (iii) of the forward model.

Oral Session  
**Applications: Adult (I)**  
Sunday, 28<sup>th</sup> October  
8:00am  
*Chair: Daniel Leff*

## Application of functional near infrared spectroscopy in Psychiatry

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Functional near infrared (fNIR) spectroscopy can be used for an in-vivo assessment of activation changes in brain tissue. Due to its simple and quick applicability as well as the absence of side effects, fNIR spectroscopy is particularly well tolerated by psychiatric patients and can hence markedly contribute to the understanding of the neurobiological basis of psychiatric disorders. Validity and reliability of fNIR spectroscopy measurements to assess task-related cognitive activation have been repeatedly confirmed among healthy subjects. Beyond that, the application of fNIR spectroscopy in order to detect altered cortical oxygenation in psychiatric patients during cognitive tasks has been highly intensified over the last two decades. In this context, hypofrontality, a decrease in frontal lobe activity that is associated with a number of clinical symptoms and psychiatric disorders, has been demonstrated in a wide range of fNIR spectroscopy studies with psychiatric patients. Despite its variety of beneficial properties, the most apparent disadvantages of NIR spectroscopy compared to other imaging techniques are its limited spatial as well as depth resolution and its restriction to cortical areas. Further technical development and a broadened implementation of combined measurements are necessary in order to uncover distinct brain activity alterations in different psychiatric disorders. In addition broad and longitudinal applications of fNIR spectroscopy measurements in psychiatric research are required in order to identify robust diagnostic markers which are needed to establish NIR spectroscopy as a valid interindividual screening instrument in psychiatry.

## PHYSIOLOGICAL CORRELATES OF PERCEPTUAL LEARNING

Uma Shahani<sup>1\*</sup>, Sobana Wijekumar<sup>1</sup>, Ross Aitchison<sup>1</sup>, Pamela Knox<sup>1</sup>, Anita Simmers<sup>1</sup>

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**Purpose:** To compare haemodynamic and electrophysiological responses in amblyopic and normally sighted participants whilst they did a perceptual learning task

**Methods:** Functional near infrared spectroscopy (fNIRS) and electroencephalography (EEG) (Wijekumar et al 2012) were used to record the extent of change in activation patterns in normal and amblyopic cortices while the observers were trained in a dichoptically presented game of tetris. fNIRS measured concentrations of oxyhaemoglobin (HbO), deoxyhaemoglobin (Hb) and total haemoglobin (THC) on a 2 channel oximeter (Oxiplex TS). EEGs were recorded on a multichannel Brain Vision EEG acquisition system.

Global motion thresholds were measured using a 2-Alternative Forced Choice (2-AFC) discrimination task in normal and amblyopic participants while viewing random dot kinematograms. The stimuli were viewed via eMagin Z800 3Dvisor goggles (HMD), which allowed the manipulation of individual input to either eye. Visual feedback was given in the form of the fixation dot changing in colour to reinforce correct responses. Binocular motion coherence thresholds were measured for each participant. The mean threshold number of dots was then used in a second program where the signal dots for motion coherence set at a high contrast were presented to the AE with noise dots increasing in contrast from 0% presented to the FE (randomly assigned in the visually normal participants). This technique of matching visibility 'balance point' between eyes allows for maximum binocular combination of the visual stimuli and is described by Knox et al (2012)

**Training:** A dichoptic perceptual training task of the game *tetris* that involved the manipulation of the position and orientation of falling 4-block shapes was undertaken for 5 days (3 x 15 minute sessions/day). The aim of the game was to form a complete wall of blocks with no gaps. It was modified so that the falling blocks were presented to the AE. The blocks that formed the wall were presented to the FE via the HMD goggles. Inter-ocular contrast thresholds measured previously were then used to match the visibility of the blocks in each eye by reducing the contrast of the blocks presented to the FE while the blocks presented to the AE were maintained at 70% contrast. This stimulus arrangement required binocular interaction to complete the task.

**Physiological Recordings:** fNIRS and electrophysiological recordings were taken from normal and amblyopic observers from over the primary visual cortex (V1) on Day 1, Day 3 and Day 5 of the training. Clinical assessments and behavioural data (task-based scores – levels reached) were also collected.

**Results:** VA and stereo acuity measures were taken both pre and post training. These showed improvements post training in amblyopic observers. Normal participants also showed an increase in performance at the task.

**fNIRS:** All three haemoglobin chromophores were recorded and normalized to a pre-stimulus baseline. Changes in HbO levels in response to the tetris stimulus on Day 1 were smaller in amblyopes than in normal participants. **Post training:** HbO levels increased as a result of training, being greatest on Day 3 of the training period. Normal participants showed a steady increase in HbO until Day 5 of the training period.

**Electroencephalography:** FFTs were performed on EEG records from O1, Oz and O2 in amblyopic and normal participants. No difference was seen between amblyopic and normal participants in the gamma band response (GBR) on Day 1. **Post Training:** Increased GBRs were observed from Day 1 to Day 5 over all examined areas and observers. A linear correlation was observed between behavioral, electrophysiological and fNIRS measures over V1.

**Conclusion:** Our results, which included behavioral, clinical and physiological measures, have shown that visual perception 'improves' as a consequence of perceptual learning.

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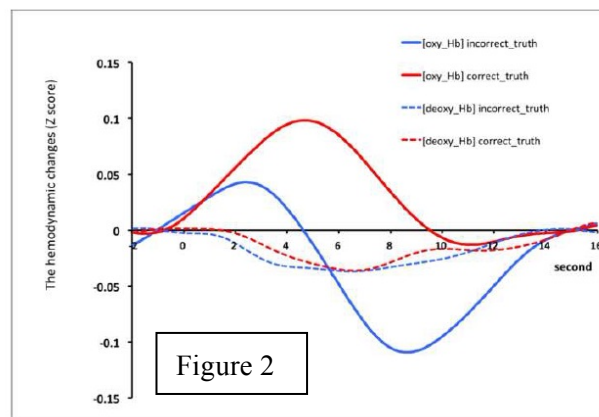
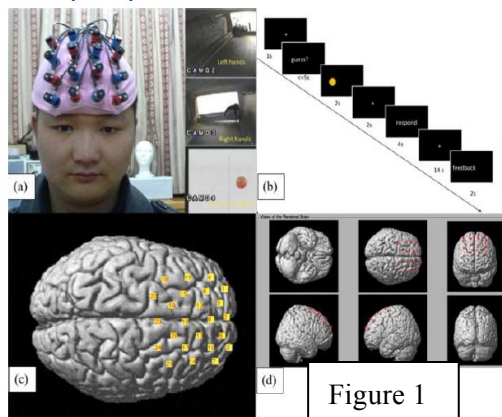
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## Neural correlates of spontaneous deception

Xiao Pan Ding<sup>1</sup>, Xiaoqing Gao<sup>2</sup>, Genyue Fu<sup>3</sup>, **Kang Lee**<sup>4</sup>

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Recently, research on the neural basis of deception has flourished. While most of the existing studies instructed participants when and how to lie, the present study focused on the neural correlates underlying spontaneous deception. Participants took part in a novel guessing game where they guessed which side a coin would appear on a computer screen by moving their left or right hand hidden in the drawers of a table (Figure 1). Then, the correct answer would appear on the screen. Participants could gain points if they had guessed correctly. Participants were asked to self-report whether their guesses were correct. Because participants' hand movements appeared invisible to the experimenter, participants had opportunities to report falsely that they guessed correctly when in fact they did not. Unbeknownst to the participants, their hand movements were recorded by hidden cameras inside the drawers and thus could be verified against their verbal report of correctness of their guesses. Participants were motivated to lie spontaneously because the more points they gained, the sooner they could finish the experiment and receive payment. We used the near-infrared spectroscopy (NIRS) methodology to collect neural responses when participants made incorrect guesses and lied, incorrect guesses and told the truth, and correct guesses and told the truth. We found that the incorrect-lie trials elicited significantly greater [oxy-Hb] changes in the prefrontal cortex, specifically in the left superior frontal gyrus, relative to the incorrect-truth trials (Figure 2). This finding suggests that spontaneous lying, like the instructed lies, is an executive functioning intensive task and engenders greater involvement of the prefrontal cortical executive function network. We also found that the correct-truth trials produced greater neural activities in the frontal area than both the incorrect-truth and incorrect-lie trials, suggesting the important roles of rewarding and self-evaluation systems in response to the success and failure of truth-telling and deception.



## Frontal activation scales with working memory load: a near-infrared spectroscopy study

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### Introduction

Working memory, the ability to maintain and manipulate information temporarily, is a fundamental component of higher level cognition. Working memory is commonly measured using the 'n-back' which requires subjects to remember a stimulus that occurred  $n$  trials ago. As the to-be-remembered stimulus is updated with every new trial, the subject must resist interference from irrelevant stimuli while constantly updating what is to be remembered. Thus, the amount of information that is maintained and manipulated varies with  $n$ , the working memory load. Functional magnetic resonance imaging (fMRI) studies show that working memory depends upon the frontal lobes, with activation of frontal regions increasing in response to working memory load [1],[2]. The present study attempts to replicate these findings using near-infrared spectroscopy (NIRS), as a cognitive load effect has not yet been demonstrated with this imaging modality.

### Method

Three subjects (2 female, 1 male) performed an n-back task with loads of 1-, 2-, and 3-back. Each load condition contained 100 randomized stimuli (40 targets, 60 nontarget) with a jittered interstimulus interval. Optical data were recorded on a two-wavelength (760 and 830 nm) continuous-wave CW5 imaging system (TechEn, Inc., Milford, Massachusetts). Four probes each holding 3 sources and 8 detectors were placed bilaterally on the scalp covering the inferior and middle frontal gyri as well as parietal cortex. Demodulation and low pass filtering (.8 Hz) were performed within the CW5 software. Artifact removal was performed using ICA (FastICA) and visual inspection. Signals were converted to oxygenated- and deoxygenated-hemoglobin concentrations using HOMer [3]. These data were then segmented, baselined, and averaged around the onsets of target stimuli. Each target trial was then averaged over a 7-second window, starting from 5 seconds after stimulus onset. Two-sample one-tailed t-tests were then used to compare each load condition for each channel. For a given contrast, each of the reported statistics represents the best channel from the best subject.

### Results

All subjects demonstrated a load effect on at least one frontal channel, for both oxygenated (an increase) and deoxygenated (a decrease) signals. Positive load effect was detected for 2-back > 1-back (Hb-oxy:  $t=2.39$ ,  $p<.05$ ; Hb-deoxy:  $t=-1.77$ ,  $p<.1$ ), 3-back > 2-back (Hb-oxy:  $t=2.83$ ,  $p<.01$ ; Hb-deoxy:  $t=-2.06$ ,  $p<.05$ ), and 3-back > 1-back (Hb-oxy:  $t=2.43$ ,  $p<.05$ ; Hb-deoxy:  $t=-2.46$ ,  $p<.05$ ).

### Discussion

These preliminary results are compatible with the existing fMRI literature, indicating that frontal activity increases with n-back load. This is the first demonstration that NIRS can be used to measure parametric increases of working memory load. Continuing research will provide better information about the spatiotemporal dynamics of this load effect and the extent of inter-subject differences.

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# The effect of inner speech on arterial pCO<sub>2</sub>, cerebral hemodynamics and oxygenation

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**Introduction:** We showed in previous studies that different speech tasks cause changes in cerebral oxy-, deoxy- and total hemoglobin concentration ([O<sub>2</sub>Hb], [HHb], [tHb]) [1, 2], which are accompanied by changes in arterial carbon dioxide pressure (PaCO<sub>2</sub>) [2], the latter possibly being the cause of the former. The aims of this study were 1) to possibly reduce the influence of PaCO<sub>2</sub> by using inner speech instead of externally voiced speech and 2) to test how inner speech affects cerebral [O<sub>2</sub>Hb], [HHb], [tHb].

**Material and methods:** In 7 adult volunteers each measurement lasted 38 min (8 min pre-baseline, 5 min task, 5 min recovery, 5 min task, 15 min post-baseline). Each subject performed 3 different tasks (inner recitation of hexameter (IRH) or prose (IRP) verses) and a control task (mental arithmetic (MA)) on different days according to a randomized crossover design. Absolute concentrations of cerebral [O<sub>2</sub>Hb], [HHb], [tHb] and tissue oxygen saturation (StO<sub>2</sub>) were measured using an ISS OxiplexTS NIRS instrument. NIRS sensors were placed over the left and right pre-frontal cortex (PFC). A Nellcor N1000 gas analyzer measured end-expiratory CO<sub>2</sub> pressure, which represents PaCO<sub>2</sub>. Statistical analysis was applied to the differences between pre-baseline, 2 task and 4 post-baseline periods. The 2 brain hemispheres and 3 tasks were tested separately.

**Results:** During the tasks: 1) PaCO<sub>2</sub> decreased significantly ( $p < 0.05$ ) during the IRH (~3 mmHg) and MA (~0.5 mmHg) task. 2) [O<sub>2</sub>Hb] and StO<sub>2</sub> decreased significantly during IRH (~1.5  $\mu$ M; ~1.5 %), IRP (~1  $\mu$ M; ~1.5 %) and MA (~1  $\mu$ M; ~1.5 %) tasks. During the post-baseline period: [O<sub>2</sub>Hb] and [tHb] of the left PFC decreased significantly after the IRP and MA task (~1  $\mu$ M and ~2  $\mu$ M, respectively).

**Conclusion:** The study showed that inner speech affects PaCO<sub>2</sub>, probably due to changes in respiration. Although a decrease in PaCO<sub>2</sub> is causing cerebral vasoconstriction and could potentially explain the decreases of [O<sub>2</sub>Hb] and StO<sub>2</sub> during inner speech, the changes in PaCO<sub>2</sub> were significantly different between the three tasks (no change in PaCO<sub>2</sub> for MA), but led to very similar changes in [O<sub>2</sub>Hb] and StO<sub>2</sub>. Thus, the cerebral changes cannot solely be explained by PaCO<sub>2</sub>.

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Oral Session  
**Applications: Adult (II)**  
Sunday, 28<sup>th</sup> October  
11:30am  
*Chair: Hellmuth Obrig*



## Adult Clinical Applications of Near Infrared Spectroscopy

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Near infrared spectroscopy (NIRS) is a non-invasive technique that offers the potential for bedside monitoring of cerebral oxygenation, haemodynamics and metabolic status over multiple regions of interest and across a wide spectrum of clinical scenarios. Despite the potential of NIRS to address many of the shortcomings inherent in other cerebral monitoring techniques, there has been limited adoption into clinical practice more than three decades since its first description [1].

In the last decade there has been a rapid expansion of clinical experience using NIRS to monitor cerebral oxygenation, particularly in cardiac surgery where there is some evidence that NIRS-guided brain protection protocols might lead to a reduction in peri-operative neurological complications [2]. There are no data to support the wider application of NIRS to monitor cerebral oxygenation during routine anesthesia and surgery despite claims of benefit by manufacturers of cerebral oximeters [3].

Cellular hypoxia/ischemia is a key component of the multiple pathophysiological processes in acute brain injury (ABI), and a logical application for NIRS is after ABI where secondary ischaemic injury is common and associated with adverse outcome. However, there has been limited research into the utility of NIRS in this area and no outcome studies. To date, studies of NIRS in adult ABI have been observational and highlight the problem of defining a threshold for hypoxia/ischaemia, particularly in the presence of acutely disordered cerebral metabolic function. NIRS measurement of cytochrome c oxidase concentration might provide additional information about metabolic failure after ABI and, in association with oxygenation variables, aid in the determination of NIRS-defined ischemia following ABI [4]. Cerebrovascular autoregulation is frequently impaired after ABI and this is also associated with poor outcome. NIRS can be used to monitor cerebrovascular reactivity [5] and might provide a sensitive assessment of autoregulation that will readily translate into clinical practice. The challenges of describing NIRS variables in the normal brain are accentuated by the presence of intracranial hematoma, cerebral edema and subarachnoid blood which may invalidate some of the assumptions upon which NIRS algorithms are based. Newer NIRS technology will play an important role in overcoming these issues [6].

NIRS and other multimodal monitoring techniques generate large and complex datasets whose interpretation is difficult and often incomplete. Furthermore, what can be measurable at the bedside and what clinicians really need to know are often very different. The development of mathematical models of brain hemodynamics and metabolism allows *in silico* derivation of physiological variables which can be compared with measured signals to facilitate their interpretation [7]. Such models will allow access at the bedside to simultaneously measured signals and model predictions of measured and unmeasured variables, thereby delivering enhanced information that can be used to support clinical decision making in real-time.

NIRS has many potential advantages over other neuromonitoring techniques but further investigation and technological advances are necessary before it can be introduced more widely into clinical practice [3].

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## Assessments of memory impairments associated with posttraumatic stress disorder (PTSD) by near infrared spectroscopy

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<sup>1</sup> Department of Bioengineering; <sup>2</sup> School of Social Work; <sup>3</sup> Department of Electrical Engineering  
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**Introduction:** Post-traumatic stress disorder (PTSD) is a common neuropsychiatric disorder that can be formed after exposure to any traumatic event that results in psychological trauma. Combat-related PTSD affects up to 20 percent of service members in the global war on terror and is often persistent in their return to civilian life. Numerous studies have reported the presence of cognitive dysfunction, particularly the memory impairments, associated with PTSD. In this study, we have used functional near infrared spectroscopy (fNIRS) to assess the PTSD-associated, memory-related dysfunction at the frontal cortex. Twelve student veterans with PTSD were recruited from UT Arlington campus. Their brain activations in response to a digit span task were measured by fNIRS and compared with those from fifteen healthy controls. At last, a neural network classifier in combination with feature selection, using piecewise linear orthonormal floating search, is utilized and examined for diagnostic assessments of PTSD.

**Methods:** The digit span task assesses the memory-related functions and consists of encoding, maintaining and recall processes. A sparse optode array, which consisted of 12 sources and 16 detectors, was used to acquire the fNIRS data at 10.8 Hz. Tomographic images were generated by our newly-developed depth-compensated tomography (DC-Tomo) method. Based on the tomographic image, GLM analysis was conducted to identify the regions of significant activation ( $t < -4$  or  $t > 4$ ) at each processing stage (i.e., encoding, maintaining and recall). For classification, fNIRS readings from both control and PTSD groups were analyzed after grouping multiple channels into clusters, some of which were identified for their significant differences in oxygenated hemoglobin concentrations (HbO<sub>2</sub>) between the two groups. Then, the corresponding HbO<sub>2</sub> values in those cluster regions were used to train a neural network classifier, along with 9-fold cross validation after feature selection was performed.

**Results:** Significant difference in behavioral scores (i.e., response time and error rate) were identified between healthy controls and veterans with PTSD. A strong correlation between response time and error rate was also observed. The regions of significant activation ( $t < -4$  or  $t > 4$ ) identified through GLM analysis are shown in Fig. 1. While healthy controls show representative activation on the dorsolateral frontal cortices, veterans with PTSD show reduced activation at the same location. Veterans with PTSD also show significant deactivation at the left frontopolar region. For classification, HbO features (0-30 s of the epoch) were selected from three clusters of measurements, as indicated in Fig. 1. Parameters that summarize the classification ability after feature selection are shown in Table 1, reporting excellent sensitivity, specificity, and accuracy in classifying PTSD subjects.

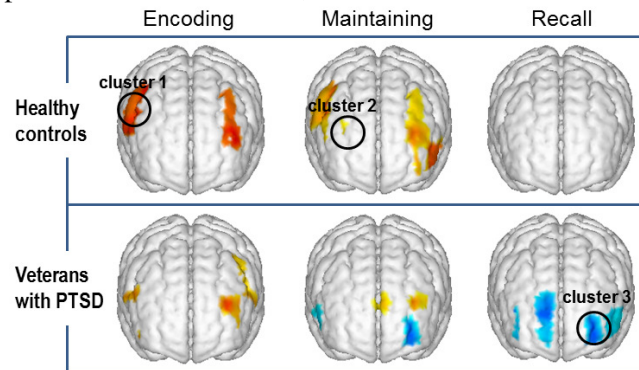


Fig 1. Regions of significant activation ( $t < -4$  or  $t > 4$ ) identified with GLM analysis. Black circles indicate three clusters of measurements for classification.

Table 1. Classification statistics obtained using MLR along with 9-fold cross validation.

Sensitivity (%)	Specificity (%)	Accuracy (%)	AUC
94 ± 11	82 ± 23	88 ± 14	84 ± 21

## SIMULTANEOUS EEG AND fNIRS ASSESSMENT OF LANGUAGE PROCESSING: A TOOL TO INVESTIGATE CHANGES IN APHASIA DURING (SUB)ACUTE STROKE?

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**Background:** Aphasia may be considered the most prominent neuropsychological sequel of ischemic stroke. During the acute and subacute phase of the disease the aphasic symptoms are highly dynamic. This high degree of clinical dynamics and variability in patients has been explored with regard to the neuronal correlates and predictors of such plasticity (Saur et al., 2010, Saur et al., 2006). Based on BOLD-contrast fMRI measurements a dynamic transitory shift in auxiliary right hemisphere recruitment has been suggested. Due to constraints of MRI-instrumentation such investigations are limited with regard to repetitive assessment and may not be feasible in larger clinical populations. Therefore we here explore the option to use two bed-side methods, namely EEG and fNIRS, to assess language processing in an undemanding design, compatible with bed-side assessment also on stroke units (Obrig and Steinbrink, 2011). **Methods and Results:** Semantically correct (*The pilot flies the plane*) and incorrect (*The pilot eats the plane*) sentences, either as forward or backward (*enalp eht stae tolip ehT*) speech were auditorily presented to 20 right-handed healthy young subjects (material from (Saur et al., 2006). Electroencephalography (EEG) and functional near-infrared spectroscopy (fNIRS) were simultaneously acquired over frontal, temporal and parietal regions bilaterally. Results showed a larger N400 followed by a larger P600 for semantically incorrect in contrast to correct forward sentences. This confirms the robustness of the paradigm with regard to the well-established N400-effect for semantic integration at the sentence level. The fNIRS results showed converging evidence for a stronger activation for semantically incorrect compared to correct sentences. Additionally, when comparing forward to backward speech fNIRS disclosed a left-lateralized response over frontal regions for the forward condition. This suggests recruitment of a language-relevant network in response to linguistically relevant stimuli. **Conclusions and Perspectives:** The study in healthy volunteers shows that two key neurophysiological correlates of language processing are accessible by simultaneous EEG-fNIRS measurements. Here EEG robustly evidences differences in lexico-semantic processing demands while NIRS provides evidence for differential lateralization in response to intelligible vs. unintelligible speech. The undemanding paradigm can be used in patients suffering from aphasia and the methodological approach allows for bed-side assessment. Ongoing measurements investigate the response pattern in chronic aphasic patients to eventually perform longitudinal studies during acute and subacute aphasia.

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## Characterising the response of cytochrome *c* oxidase to changes in cerebral oxygen supply and demand in the healthy adult brain

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**Background** Transcranial near-infrared spectroscopy (NIRS) may provide an assessment of cerebral oxygen metabolism by monitoring changes in the concentration of oxidised cytochrome *c* oxidase ( $\Delta[\text{oxCCO}]$ ). This measurement is technically complex both in terms of instrumentation and algorithm development, and despite its potential as a non-invasive bedside marker of oxygen utilisation, there is still debate about its use outside research settings. A hybrid optical spectrometer (pHOS) and accompanying algorithm specifically optimised for the measurement of  $\Delta[\text{oxCCO}]$  have recently been developed by our group. To contribute to the better understanding of this measurement and thus gain confidence in its regular use as a biomarker of cerebral metabolic status, we aimed to characterise the changes in  $\Delta[\text{oxCCO}]$  in response to changes in cerebral oxygen supply and demand in healthy adults.

**Methods** Cerebral oxygen delivery was decreased by reducing arterial oxygen saturation to 80% and increased by inducing systemic hyperoxia. Both hypoxia and hyperoxia were delivered in 15 healthy adults by appropriate manipulation of the inspired oxygen fraction. Brain functional activation through anagram solving was the paradigm used in an additional 11 healthy volunteers for stimulating frontal lobe functional activation, leading to an increase in cerebral oxygen demand. The pHOS measures light absorption and scattering at discrete wavelengths, as well as multi-distance broadband light attenuation, and was used for obtaining frontal lobe NIRS measurements from all subjects during the protocols.  $\Delta[\text{oxCCO}]$  and concentrations of total haemoglobin ( $\Delta[\text{HbT}]$ ) and haemoglobin difference ( $\Delta[\text{Hbdiff}]$ ) were derived with the UCLn algorithm, fitting the wavelength range 780-900 nm. Simultaneous systemic monitoring data were also available.

**Results** All reported results (mean  $\pm$  SD) are in the absence of optical scattering changes and from the detector furthest from the broadband light source, which is more likely to reflect cerebral events<sup>1</sup>. During hypoxia a  $0.54 \pm 0.46$   $\mu\text{molar}$  decrease in  $\Delta[\text{oxCCO}]$  ( $P < 0.001$ ) was measured in the presence of an increase in  $\Delta[\text{HbT}]$  and decrease in  $\Delta[\text{Hbdiff}]$  ( $P < 0.001$  for both), whereas during hyperoxia a  $0.24 \pm 0.20$   $\mu\text{molar}$  increase in  $\Delta[\text{oxCCO}]$  ( $P < 0.001$ ) was observed in the presence of the opposite  $\Delta[\text{HbT}]$  and  $\Delta[\text{Hbdiff}]$  haemodynamic response ( $P < 0.001$  for both). Such unambiguity in the group response of  $\Delta[\text{oxCCO}]$  was not observed during functional activation, despite the fact that the interrogated datasets demonstrated a uniform haemodynamic response consistent with functional activation (defined as a statistically significant increase in oxygenated haemoglobin and decrease or no change in deoxygenated haemoglobin). Closer examination of the individual rather than group data revealed that the  $\Delta[\text{oxCCO}]$  response measured in the presence of functional activation was heterogeneous, with the majority of subjects showing statistically significant increase in oxidation, but others having a statistically significant decrease.

**Conclusion** The observed  $\Delta[\text{oxCCO}]$  responses to hypoxia and hyperoxia have a rational physiological explanation, since the induced changes in cerebral oxygen delivery will have a direct impact on mitochondrial oxygen availability, and are in agreement with what has been reported previously<sup>1,2</sup>. The heterogeneity in the  $\Delta[\text{oxCCO}]$  response to functional activation, although somewhat surprising, also has physiological rationales, for example, the fact that functional activation can cause an increase in both oxygen and NADH levels, factors that will affect the cytochrome *c* oxidase oxidation state in opposite directions. This heterogeneity is not likely to have been induced by confounding factors in the measurements, especially as demonstrated by the uniformity and unambiguity of the response to global changes in cerebral oxygen delivery. These findings suggest that NIRS-measured  $\Delta[\text{oxCCO}]$  may be a useful marker of cerebral cellular oxygen metabolism.

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# Investigating the origin of hemodynamic fluctuations using high-resolution diffuse optical tomography in humans

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Max Planck Institute for Human Cognitive and Brain Sciences, Leipzig, Germany; <sup>4</sup>Center for Stroke Research Berlin (CSB),  
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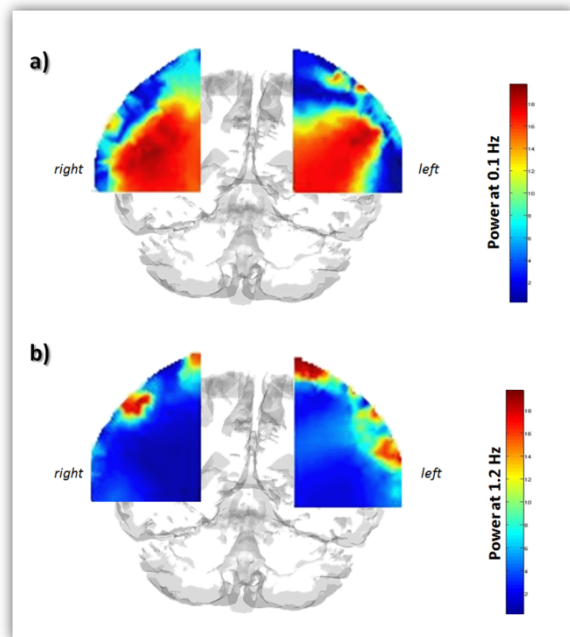
Near infrared spectroscopy and DOT signals are often contaminated with spontaneous low frequency oscillations (LFO) in the 0.1 Hz band and heart beat (HB) signals (1.2Hz). LFO are often described in human brain imaging studies [1] and may represent auto-regulatory processes of cerebral blood flow. Since 2D NIRS cannot separate superficial from deeper layers, we investigate the origin (brain or scalp) of LFO and HB in NIRS signals using 3D DOT.

We used a NIRScoutX (NIRx Medizintechnik, Germany) cw tomography imager (32 sources\* 32 detectors, 760 nm & 830 nm). We placed two grids of optical fibers bilateral, pericentrally over C3 and C4 (each side: 16s\*16d) achieving 2\*256 data channels with a 3.41 Hz sampling frequency. Three subjects performed a 10 min resting task.

Image reconstruction was performed for both hemispheres independently. We reconstructed time series of relative absorption changes using the normalized difference method [2]. The weight matrix was determined using BrainModeler (NIRx Medical Technology LLC) which provides a library of subvolumes from a MRI-scan based finite element mesh (FE) with precalculated inverse parameters. To investigate LFO and HB, the reconstructed time series were band pass filtered at 0.1Hz /1.2Hz and normalized (z-score). We calculated the power spectral density (PSD) for the reconstructed HbO time courses in every node of the FE mesh. For visualization purpose, the results (power at 0.1 Hz and 1.2Hz) were transformed into volumes and superimposed on a brain structure.

We found a high relative fraction of LFO in deeper layers, whereas HB could be seen mainly in superficial layers.

We demonstrate that DOT with a 3D image reconstruction allows a depth profiling of hemodynamic rhythms in the adult head. Monitoring these hemodynamic features and detecting changes in the individual patterns could be an additional module to noninvasively detect changes in cerebral blood flow, e.g. in neurointensive care patients.



**Fig. 1** Result of a PSD of HbO time courses for a) low frequency oscillations and b) heart beat

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Oral Session  
**Keynote**  
Sunday, 28<sup>th</sup> October  
2:00pm

# Interpreting NIRS data: the modelling challenge

**Murad Banaji<sup>1</sup>**

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As NIRS has progressed as a technology, the robust extraction of scientifically – and even clinically – relevant information from NIRS signals has become an increasingly challenging task. Each NIRS signal is the outcome of an interaction between complex underlying physiological processes and the physics of a complex measurement process. Simultaneous acquisition of several signals provides hope of more meaningful and accurate information, but also complicates matters: the signals are related to each other in various ways, and thus while providing more data, also require simultaneous interpretation. Entering into the mix are the inevitable gaps in our understanding of both physiology and measurement; inter- and intra-individual physiological variation; “noise” from various sources; and (especially in the human *in vivo* context) severe practical and ethical limitations to validation via more invasive measurement.

In this context, a natural framework for extraction of useful information from NIRS data involves the construction of *in silico* models, of both physiology and measurement. Constructing and simulating computer models holds out the hope of not only explaining measured data, but going on to make robust predictions of hard-to-measure but important quantities. Unfortunately, we are led quickly to an apparent vicious circle – where understanding physiology requires measurement whose interpretation is itself dependent on an understanding of the physiology. Some practical and philosophical issues associated with trying to escape from this vicious circle will be outlined. The conclusion will be that the modelling approach is both necessary and holds considerable potential, provided a set of principles are adhered to during the modelling and data analysis process.

Combining data-driven and physiology-driven approaches; if appropriate combining deterministic and stochastic approaches; adopting pragmatic, but consistent, approaches to questions of model construction, identification and validation; acknowledging and attempting to explain (rather than throwing out) inconsistent or surprising data, whether experimental or from simulation: all of these must at least be on the wish-list for the modelling/data-analysis project. Perhaps most important is taking a long-term view where model assumptions are presented transparently, models are seen at the outset as evolving objects designed to be shared, and a principled approach is adopted to model evolution and interaction with data over time.

Oral Session  
**Applications: Neonatal and Paediatric**  
Sunday, 28<sup>th</sup> October  
2:30pm  
*Chair: Martin Wolf*



## **Clinical application of Near infrared Spectroscopy in the Neonate**

**Frank van Bel and Petra Lemmers, Department of Neonatology, Wilhelmina Children's Hospital, Utrecht, The Netherlands**

Near InfraRed Spectroscopy (NIRS) is a non-invasive monitoring technique initially mainly used as a research technique to monitor changes in neonatal cerebral hemodynamics and oxygenation and is based on absorption of near infrared light by chromophores which are present in hemoglobin in the brain. Absorption changes can be converted by the NIRS apparatus in concentration changes of HbO<sub>2</sub> and HbR in the neonatal brain. It are mainly the acute changes of HbO<sub>2</sub> and HbR which can be detected nicely and that made this method applicable as a research tool.

However, for monitoring cerebral oxygenation and extraction over longer episodes in clinical practice on the Neonatal Intensive Care Unit (NICU) the assessment of changes in HbO<sub>2</sub> and HbR are not usable because these relative variables are prone to movement artefacts.

What really is needed is the possibility to monitor the integrity of neonatal brain function, providing us with parameters with absolute values which can be compared over extended periods of time and indicating the balance between O<sub>2</sub>-delivery and O<sub>2</sub>-consumption of the neonatal brain. Promising variables in this respect are regional (mixed: arterial, capillary and venous) cerebral O<sub>2</sub>-saturation (rScO<sub>2</sub>), measuring (changes in) cerebral O<sub>2</sub>-supply and secondly the rSO<sub>2</sub>-derived cerebral fractional tissue O<sub>2</sub>-extraction or cFTOE, which correlates with actual cerebral O<sub>2</sub>-extraction. They provide us with absolute values which are stable and reproducible. Normal values in the neonatal period for cerebral oxygenation are supposed to be between 55 and 75%. The main clinical applications of NIRS, using rScO<sub>2</sub> and cFTOE, in Neonatology are to monitor the balance between oxygen supply and oxygen extraction in the preterm baby in various pathological conditions such as severe respiratory distress syndrome, a hemodynamically significant patent ductus arteriosus and if related to simultaneous arterial pressure monitoring, NIRS-monitored rScO<sub>2</sub> can be used to assess whether of not cerebral vascular autoregulation is in tact. Also its use to predict secondary energy failure of the neuronal cells after severe birth asphyxia in term babies can be used as an additional prognostic tool to assess long-term neurodevelopmental outcome.

As stated by Greisen *cs* (Semin Fetal Neonat Med 2006), it is however important to realize that different types of NIRS devices and optodes are used with different algorithms to separate the signals of oxyhemoglobin and deoxyhemoglobin. Differences in results may therefore merely caused by differences in NIRS methodology and not based on (patho)physiologic changes in actual neonatal cerebral oxygenation and oxygen extraction.

## A Study of Preschool Irritability: NIRS Brain Imaging of correlates of clinical irritability

Susan B. Perlman<sup>1</sup>, Theodore Huppert<sup>2,3</sup>

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2. University of Pittsburgh, Radiology, Pittsburgh, PA, United States
3. University of Pittsburgh, Bioengineering, Pittsburgh, PA, United States

**Introduction:** NIRS is a portable brain imaging technology that is well suited for studies involving child or infant populations. In this study, NIRS was used during a frustration task to look at the relationship of clinical child frustration metrics and brain activity.



Fig 1: A child plays FETCH on a touch screen computer while his cortical brain activity is monitored via fNIRS

**Methods:** A total of 21 typically developing children (mean age: 4 years 4 months, range 36-70 months) participated in our tasks during fNIRS data collection. Children ranged in parent reported irritable temperament on the Child Behavior Questionnaire (CBQ- anger/frustration subscale) from 1.5-6.3 on a 1-7 scale (mean 4.78). A TechEn Cw6 NIRS system with a bilateral NIRS probe (4source /8 detectors per side) covering frontal, prefrontal, and DLPFC cortices was used. NIRS scanning was done a dedicated child imaging lab with child and parent present. The Frustrative Emotion Task for Children (FETCH) and a second Go/No-Go task was used in this study. NIRS data was collected and analyzed using custom analysis software developed by the Huppert lab. Analysis included the use of a general linear model and image reconstruction methods utilizing a structural MRI from one of the age-matched participants of the previous fMRI study for display and interpretation purposes.

**Results:** The FETCH Task: Preliminary results (Fig 2) indicate increased activity in the bilateral dorsomedial prefrontal cortex during Winning blocks (compared to Frustration blocks), while activation in the bilateral dorsolateral prefrontal cortex was greater for Frustration blocks (compared to Winning Blocks) [ $t(16) = \pm 11.76$ ,  $p < .05$ , corrected]. Similar results were found in the PI's previous fMRI studies (Perlman and Pelphrey 2010; Perlman and Pelphrey 2011). Irritability score was positively correlated with the increase in deoxygenated hemoglobin during Frustration blocks [ $r(15) = .48$ ,  $p = .05$ , two tailed]. These data suggest that children high in irritability may have experienced increased frustration, compared to their low irritability counterparts, requiring increased activation of the DLPFC to regulate emotion for task completion.

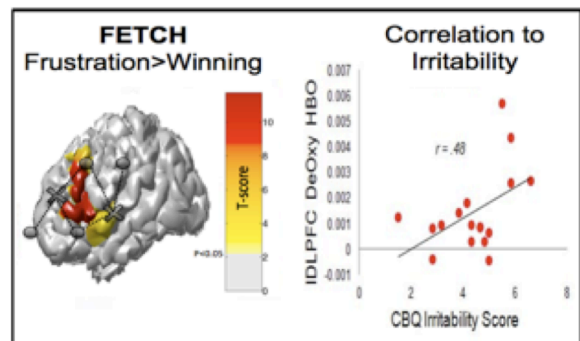


Fig 2: (Left Panel) Increased activity during Frustration in the left DLPFC. (Right Panel) Levels of irritability correlated with increase in deoxygenated hemoglobin in the left DLPFC.

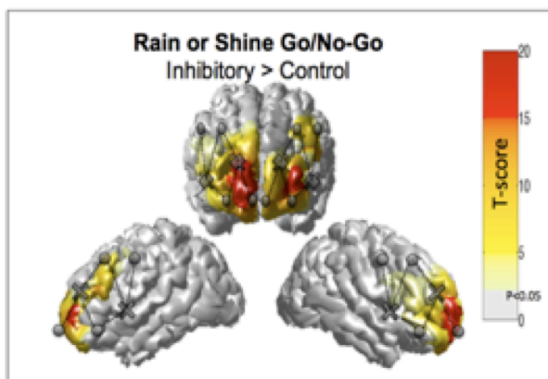


Fig 3: Increased DMPFC activity during inhibitory control.

The Rain or Shine Go/No-Go Task: Preliminary results (Fig 3) indicate decreased activity in the right dorsolateral prefrontal cortex during Inhibitory Control blocks (compared to Motor Control blocks). This effect was right lateralized, with the opposite effect present in the left hemisphere.

**Conclusions:** Results point to evidence for dissociable areas of the prefrontal cortex related to frustration and inhibitory control in preschool children. Future studies are planned to address the nature of neural dysfunction of these areas in child clinical populations.

## Development of a Multimodal Functional Brain Imaging Laboratory for Newborn Infants

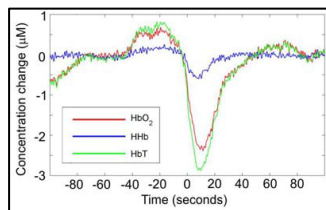
**T Austin**, JC Hebden, AP Gibson, NL Everdell.

*neoLAB – representing Neonatal Intensive Care Unit, Cambridge University Hospitals NHS Foundation Trust & Department of Medical Physics and Bioengineering, University College London.*

**Background** Brain injury in the newborn remains a major cause of death and serious lifelong disability, with a significant number of infants going on to develop cerebral palsy, epilepsy and learning difficulties<sup>1</sup>. Over the past 30 years structural brain imaging has provided a remarkable insight into the nature and extent of perinatal brain injury. However the relationship between brain structure and function is not straightforward. The challenge is to identify functional deficits at an early stage to both assess the benefits of novel neuroprotective strategies as well as initiate remedial therapy during a critical window of brain development.

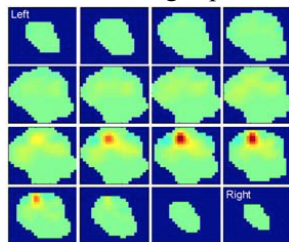
A collaborative group, **neoLAB**, representing clinician scientists in Cambridge, and physicists and engineers at the Biomedical Optics Research Laboratory (BORL), University College London has been formed with the aim of developing and refining optical and electrophysiological systems to study the development of haemodynamic and electrical brain activity in the newborn.

**Optical Topography** BORL has developed a frequency multiplexed optical topography system providing maps of changes in NIR absorption close to the surface of the brain<sup>2</sup>. Recently a commercial electroencephalography (EEG) system has been integrated with the optical topography system to enable simultaneous observation of electrical and haemodynamic activity in the cortex of neurologically compromised newborns at the Rosie Hospital in Cambridge. This pilot study identified previously undocumented transient haemodynamic events in infants with evidence of cerebral injury, not seen in healthy control infants<sup>3</sup>. The underlying cause of these changes is currently unknown and is currently being investigated further.



**Figure 1.** A single-channel example of a haemodynamic event identified in a newborn infant with brain injury, recorded using the UCL optical topography system. It shows a slow increase in oxyhaemoglobin concentration followed by a rapid and profound decrease, before a slow return to baseline. No comparable events were found in any control data sets. The images generated from these data are shown in Cooper et al<sup>3</sup>.

**Optical Tomography** Optical tomography involves acquiring measurements of light transmitted across the full thickness of tissue in order to generate 3D images using sophisticated image reconstruction algorithms. The UCL 32-channel time-resolved optical tomography system uses time-correlated single photon counting (TCSPC) technology to measure the flight times of photons as they are transmitted between points on the surface<sup>4</sup>. Our optical tomography studies on newborn infants represent the first, and so far the only, 3D optical images of the entire brain. Both static images have been obtained in healthy infants and infants with evidence of intraventricular haemorrhage as well as dynamic images, resulting from changes in oxygenation following functional activation of the motor cortex<sup>5,6</sup>.



**Figure 2.** Sagittal slices across a 3D image of absorption change due to arm movement.

**Conclusion** The development of the new generation optical tomography system integrated with EEG will enable studies on neurovascular coupling to be carried out safely in newborn infants.

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Poster Session  
**Hardware Developments**  
Poster #: 1-17

## A non-contact fNIRS scanner: First *in-vivo* tests

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**Introduction:** Non-contact scanning could overcome some limitations of standard fNIRS equipment, in particular (i) poor lateral spatial resolution due to a source-detector separation between 2 cm and 4 cm, (ii) sensor-tissue contact problems. The major obstacle for a scanning approach with zero or small separation between source and detection spot is the huge amount of early photons that are diffusely reflected near the surface and do not carry information about changes in the brain. Recent development of a new measurement method, the Null Source-Detector Separation (NSDS) approach [1, 2], based on fast-gated Single-Photon Avalanche Diodes (SPAD) [3], makes non-contact scanning feasible. The sensitive region for NSDS is much more confined than with separation >2 cm. After proof-of-concept tests on phantoms [4], we here report on first successful *in-vivo* tests.

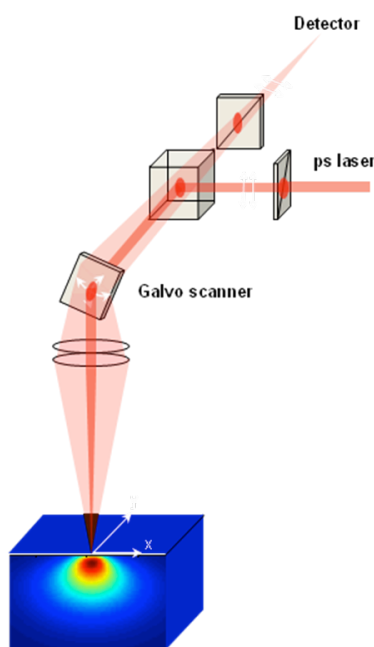


Fig. 1: Optical arrangement

**Methods:** A supercontinuum laser with acousto-optical tunable filter provided ps pulses. A state-of-the-art SPAD was fast gated by a dedicated ultrafast pulser and a delay unit to cut off early arriving photons. Polarization-dependent detection in the optical path suppressed specular reflections. An area of  $4 \times 4 \text{ cm}^2$  was scanned with  $32 \times 32$  pixels at 4 mm source-detector separation. Wavelength was switched line by line between 760 nm and 860 nm. The detected photons were processed by time-correlated single photon counting. Data were analyzed to obtain  $8 \times 8$  pixel images of the time course of changes in oxy- and deoxyhaemoglobin concentrations.

**Results:** Initial tests with venous and arterial inclusion on the arm as well as Valsalva on the forehead of healthy subjects were performed successfully. The results showed the expected behaviour. For a cognitive task (simple math), an activation was observed over the whole area on the left frontal lobe. Motor activation by finger tapping in a bald subject showed a rather localized response near C3, with good signal-to-noise ratio.

**Conclusions:** The feasibility of *in-vivo* non-contact scanning of brain activation was demonstrated. The non-contact scanning approach provides a dense, flexible grid of measurement

positions which allows one to localise brain activation with superior lateral resolution. The method is limited to application in hairless areas.

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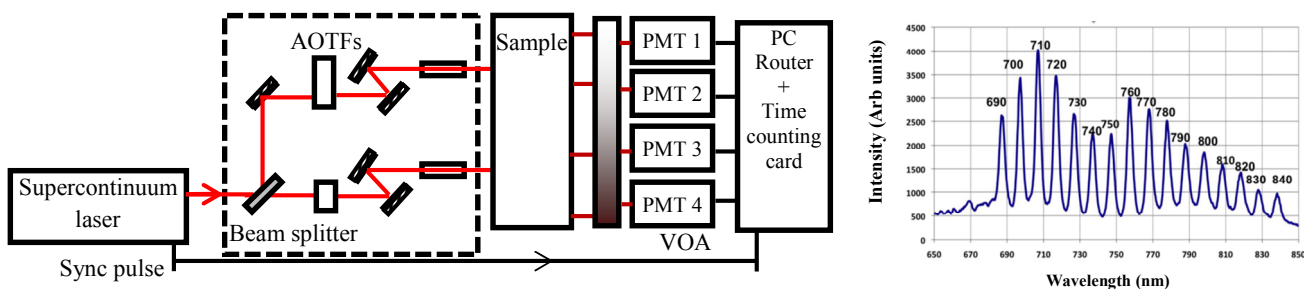
Design of a new fNIRS multi-wavelength, multi-channel time resolved spectrometer using a supercontinuum laser for measuring brain tissue haemodynamics and metabolism

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Medical Physics and Bioengineering, University College London, UK

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**Introduction:** fNIRS is commonly used to measure  $\text{HbO}_2$  and HHb using a small number of wavelengths in both continuous wave and time domain spectrometers. However another strong near-infrared (NIR) light absorber is the terminal electron acceptor of the mitochondrial respiratory chain cytochrome-c-oxidase (CCO), which its absorption spectrum depends on oxygen utilisation[1]. To accurately measure this chromophore a large number and appropriate wavelengths are required as the CCO concentration in the brain is one-tenth of the haemoglobin concentration [1-3]. We propose a new system based in a recent developed supercontinuum laser capable of measuring the absorption ( $\mu_a$ ) and scattering ( $\mu_s'$ ) independently for up to 16 wavelengths. **Hardware** (see Fig 1): We use a supercontinuum laser source (Fianium) producing 6W of power over a broadband spectrum in short ps pulses at 60MHz. The light is passed through an optical fibre to a dual filter system where the light is split in a polarising beam splitter and directed through two Acousto-Optic Tunable Filters (AOTF) mounted at  $90^\circ$  to each other. The filters consist of piezo-electric transducers bonded to a birefringent quartz crystal that create a standing wave at a driven frequency which modulates the refractive index of the crystal creating a phase grating. The white light light from the supercontinuum laser is that split into different diffraction orders. A narrow bandwidth of light (1-2nm) is therefore diffracted by a small angle from the main beam and collected and focussed into an optical source fibre. By varying the radio frequency of the transducer the wave length of light selected can be easily switched. In this system the AOTF fast switches through up to 16 channels at 1kHz allowing multi-wavelength time domain measurements of any combination between 650-890nm due to the sensitivity range of our PMTs. Two source fibres are simultaneously used when the detectors are on either hemisphere of the adult head, however the two sources can be interleaved if crosstalk occurs. The detection of light is achieved using 4 Hamamatsu H7442-50P photon counting photomultiplier tubes (PMT) each protected against over exposure by individual variable optical attenuators. The arrival time of each photon is measured using a Becker and Hickl SPC-130 EM module by timing the difference between the electric pulse from the PMT to a synchronisation pulse produced by the laser. A temporal point spread function measured is then fitted using greens functions calculating  $\mu_a$  and  $\mu_s'$ . **Discussion:** We present a novel time domain fNIRS system capable of measuring  $\mu_a$  and  $\mu_s'$  for up to 16 user defined wavelengths and over four channels; allowing us to resolve and quantify both absolute haemodynamic and oxygenation changes ( $\text{HbO}_2$  and HHb) and mitochondrial metabolism through quantification of the oxidation state of CCO.



**Fig 1:** Schematic of new time resolved system and example of wavelength selection with our supercontinuum laser source.

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## Multiple short separation measurements for removal of systemic oscillation in NIRS data

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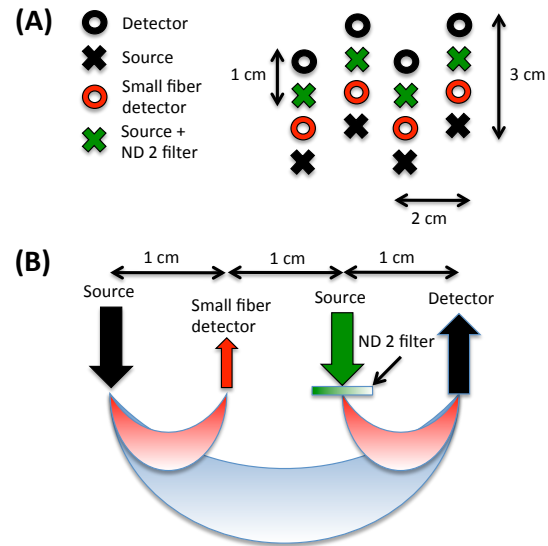
[email: lgagnon@nmr.mgh.harvard.edu](mailto:lgagnon@nmr.mgh.harvard.edu)

Near-Infrared Spectroscopy (NIRS) is a non-invasive technique to measure the hemodynamic changes associated with evoked brain activity. The NIRS signal is contaminated by systemic physiology occurring both in the brain and in the superficial layers of the head. The back-reflexion geometry of the NIRS measurement makes the signal strongly contaminated by systemic physiology of superficial layers origins.

A recent technique to remove this interference has been the use of short optode separation recordings (SOSR) which are sensitive to superficial layers only, including the scalp and the skull. These SOSRs are used as regressors during the post-processing of the NIRS signal and improves the detection of evoked brain activity using NIRS. In our previous paper, we have shown that the systemic interference measured in NIRS is inhomogeneous across the surface of the scalp. Therefore, the SOSR must be located close to the standard 3 cm NIRS channel from which the brain activity is to be detected.

Since the standard 3 cm NIRS measurements integrate the signal through the entire path of the light in the tissue, it is possible that the signal contains interference from two different locations. Therefore, it was reasonable to investigate the effect of using multiple SOSRs, one located close to the source optode and one close to the detector optode, to maximize the performance of SOSR to remove systemic interference in the 3 cm channel.

In this regards, we designed a NIRS probe containing a SOSR located close to each source and each detector optode. Our simulations performed over real NIRS baseline data showed that the multi-SOSR approach results in more accurate recoveries of the evoked hemodynamic response (in terms of MSE) and lower noise in the recovered response. Functional NIRS was also recorded during a 5-sec finger tapping task. Multiple SOSR resulted in a more spatially localized hemodynamic response, lower noise in the baseline signal between individual trials as well as lower inter-trial variability.



# A wireless, self-calibrating sensor for fNIRS studies in preterm infants.

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## Introduction:

It is a common practice at Neonatal Intensive Care Units (NICUs) that both nurses and parents, if health permits, take the preterm infants out of the incubator to hug, stroke and show them fondness and care. It is assumed that the close contact with the infants increases their well-being and helps the infant overcoming health problems. But it is not known how the emotional reaction on the infant is generated. The long term aim is to investigate this by determining the concentration of oxy- and deoxyhaemoglobin ([O<sub>2</sub>Hb], [HHb]) in the brain as an indication of neuronal activation in response to handling.

For this type of study it is important that the fNIRS system does not cause any discomfort, e.g. physical discomfort by cables or psychological discomfort by a large obtrusive size (Wolf et al., 2007). The short term aim therefore was to design and build such an fNIRS instrument.

## Methods:

The fNIRS system should feature a high time and spatial resolution and a low noise level to be able to detect small signals changes. To maximize the comfort of patients and parents, the device should be small, portable and wireless.

Such an instrument called OxyPrem was designed and developed specifically for preterm and term neonates.

## Results:

OxyPrem incorporates a self-calibrating sensor geometry, which is not sensitive to the coupling errors and thus is expected to provide a substantially higher precision. It is miniaturized and wireless fNIRS device and thus enables a higher comfort and an enhanced applicability.

The OxyPrem consists of four LED emitters each of three wavelengths (760, 805 and 870 mm) and two photodetectors. A total of 24 channels (from each emitter there are two paths to the detector: a short and a long one). The time resolution is 35Hz.

The instrument has been tested successfully in phantoms and adults.

## Conclusion:

A wireless, miniaturized fNIRS instrument specifically designed for preterm infants was successfully developed. We plan to employ it to assess well-being of preterm infants.



# Development of new fNIRS-EEG system for seamless whole brain study

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## 1. Introduction

Functional near-infrared spectroscopy (fNIRS) is a versatile functional neuroimaging technology with non-invasive method of monitoring of brain activity. Recently, there is one of the hot topics to explore the wide area network in the brain such as functional connectivity or spontaneous brain activity functions. fNIRS has high potentials for such research topics according to the high temporal/spatial resolution compare to fMRI or EEG. On the other hand, some researches has been pointed out the importance of improvement of reliability of fNIRS signals such as to reduce the effects of skin blood flow<sup>[1]</sup> or improve the spatial resolution<sup>[2]</sup>. In order to achieve the research requirement we developed a new fNIRS-EEG system which allows seamless whole-brain measurement of the surface of the human brain, high spatial resolution measurement, multi-distance measurement, and high temporal resolution measurement. We evaluated the performances of the new system by a phantom and a healthy subject.

## 2. System Description

**2-1. Overall System Parameters:** Figure1 shows the new fNIRS system named “LABNIRS” which developed with CW system using laser diodes as light sources and photomultiplier tubes (PMT) as detectors. LABNIRS has maximum 40 sources and 40 detectors which covers a whole brain (the maximum logical channels is 142). The data analysis relies on the Modified Beer-Lambert Law (MBLL) assuming spatially homogeneous absorption changes in extra cerebral tissues. To improve accuracy, we use three- wavelength (780, 805 and 830nm) and bundled optical fibers for source. We controlled the irradiation with 1ms interval for each wavelength, and the maximum sampling rate is 250 Hz.

**2-2. Optode Holder:** We implemented double density fNIRS (and EEG) holder from flexible adjustable surface holder (FLASH)<sup>[3]</sup> (Figure2). The double density<sup>[2]</sup> needs twice arrangement of the conventional method, the other arrangement is shifted at half of the optode distance from the origin. In grillage construction, electrode holders were put in the midpoint of slides of FLASH to row direction and fNIRS optodes were put in the midpoint of slides of FLASH to column direction. The holder can be also use for multi-distance measurement according to the PMT and flexible fiber settings.

## 3. Experiment and Results

In the experiment, we measured the fNIRS signals during a finger tapping task. We used 128 channels of fNIRS covering the whole brain with the double density method. The subject performed 5 trials which consists 20s rest, 20s task and 20s rest for one trial. Figure3 shows the topographical image of the average of the oxy-Hb change at 20s after starting of the right-finger-tapping task. The results indicated the task-related activity in oxy-Hb. Using the double density method, spatial resolution of image was improved than conventional method to focus the activation area.

## 4. Conclusion

In this study, we developed a new fNIRS-EEG system as a non-invasive brain functional measurement system whole surface of human brain. The new fNIRS allows high performance measurement with high spatial / temporal resolution using seamless measurement techniques, double density techniques, multi-distance measurement techniques and high sampling rate system. The functional data which has highly-spatial resolution and wide field of view would contribute to improve the accuracy of the brain signals, and high temporal resolution supports functional connectivity or spontaneous brain activity function research.

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Figure1

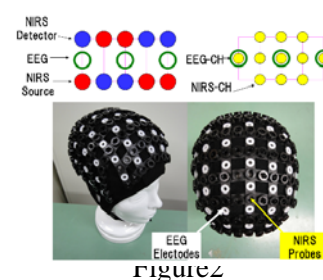


Figure2

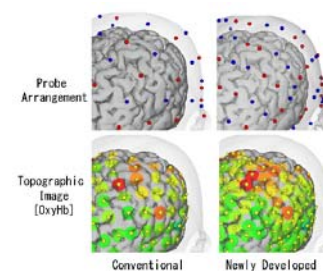


Figure3

## DOCNEURO: Towards pre-commercial, clinical prototype development of hybrid diffuse correlation spectroscopy (DCS) and frequency domain diffuse optical spectroscopy (DOS) for bed-side neuromonitoring.

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**Abstract:** The application of diffuse correlation spectroscopy (DCS) in non-invasive measurements of microvascular cerebral blood flow is a promising candidate for combination with NIRS for bedside, non-invasive, continuous neuromonitoring. Since present devices are designed for scientific use, they pose a barrier against effective translation into clinical use. Here we present our project (DOCNEURO) on the development of a professional system designed according to the medical device norms and usability standards.

**OCIS codes:** 170.1610 Clinical applications;170.5280 Photon migration

Diffuse correlation spectroscopy has been used in non-invasive measurement of cerebral blood flow (CBF) in human brain, in human muscles and during cancer therapy monitoring [1, 2]. By combining DCS with simultaneous diffuse optical spectroscopy (DOS), cerebral blood flow (CBF), oxy-hemoglobin ( $\text{HbO}_2$ ) and deoxy-hemoglobin (Hb) concentrations and total hemoglobin concentration (THC) are accessed which enables to measure changes in cerebral metabolic rate of oxygen ( $\text{CMRO}_2$ ). In order to offer these parameters in a user friendly way, special attention was paid to the graphics interface and data representation features as well as a design concept in accordance to hospital standards (see figure).

The current version (DOCNEURO V0.5) implements the DCS concept and the main software back-bone. The final system will include a frequency domain DOS system [3]. Furthermore, the device/software can readily be interfaced with other commercial and research DOS systems. We will present the current status of the system with examples and our vision for the future.

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## A Wearable Multi-channel NIRS Imaging System for Brain Imaging in Freely Moving Subjects

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Although (f)NIRS has often been cited as portable and suitable for unconstrained experimental settings, probably most of the NIRS setups employed in neuroscientific research still offer a restrained setting. Typically, the subject is tethered by not very flexible or lightweight fiberoptic cables to a more or less stationary instrument<sup>1</sup>. While restrained settings with a portable but stationary instrument might be well feasible for bedside monitoring, they hamper imaging in a more natural environment, e.g. during sports or physical therapy, or when imaging children. Developments towards miniaturized probe arrays or instruments have been reported before, however, usually at the cost of limited measurement channels or restricted specific portions of the head<sup>2-4</sup>. We here present a new, miniaturized, portable diffuse optical NIR tomography system that allows brain imaging in freely moving subjects. The performance of the instrument is demonstrated on N=7 subjects in a hand gripping motor paradigm on a bicycle performed during three conditions: (i) outdoor bicycle riding, (ii) indoor stationary paddling and (iii) rest.

NIRS imager and controlling notebook computer were contained in a backpack worn by the subjects. Eight sources and eight detectors were arranged in two groups around positions C3 and C4 of the extended international EEG 10-20 system to ensure coverage of the primary motor areas of both hemispheres. The paradigm during biking consisted of 10 repetitions of 20 s of self-paced (approx. 1 Hz) left-hand clamping followed by 40 s of rest.

Results show a significant relative HbR decrease over the contra lateral sensory motor cortex in each condition revealing a clear focal activation to left hand clenching. The observed time courses show the prototypical increase in HbO and decrease in HbR in response to neural activation. The HbR decrease is largest in the outdoor cycling condition and lowest at rest

To the best of our knowledge, this is the first outdoor demonstration of NIRS brain imaging on freely moving subjects. A truly portable and miniaturized NIRS technique opens new perspectives to study sensory or cognitive paradigms in realistic environments and furthermore promise clinical uses as a monitoring tool in neuro-rehabilitation and intensive care units.

### Acknowledgements

Part of the work was funded by the Berlin BernsteinFocus: Neuro Technology program of the German Federal Ministry for Education and Research (BMBF).

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# Silicon Photomultipliers bear Potential for fNIRS Instrumentation

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To date, photomultiplier tubes (PMTs) or avalanche photodiodes (APDs) are considered the gold standard for detectors in fNIRS [1]. However, PMTs are sensitive to overexposure, operate at very high voltages, and are bulky. APDs benefit from being solid state devices, but have reduced sensitivity and also need rather high operating voltages. Silicon photomultipliers (SiPMs) are alternative detectors, essentially consisting of an array of parallel connected tiny APDs operating in Geiger mode [2]. They have a high sensitivity and gain, and operate at lower voltages, while performing comparable to PMTs [3]. Here we propose the employment of SiPMs for fNIRS instrumentation and report on experimental evidence that they bear great potential for this purpose.

**METHODS:** fNIRS modules (27x27 mm<sup>2</sup> footprint) consisting of an SiPM with 3x3 mm<sup>2</sup> active area (KETEK GmbH, Germany), two LEDs (680 and 850 nm, 5 mW optical power) and an onboard preamplifier stage were built. During periods of 10 ms, both LEDs were consecutively switched on for 3.3 ms. A digital oscilloscope (sampling at 100 kHz) was used to record the SiPM signal. Samples at  $f_s=100$  Hz were obtained by averaging the data points belonging to 50-90% of the LED-on periods and subtracting the backlight level (determined analogously). A silicone phantom emulating a human head ( $\mu_a=0.1$  cm<sup>-1</sup>,  $\mu_s'=11$  cm<sup>-1</sup>) was used to acquire 50 such samples in order to determine the signal-to-noise ratio (SNR=mean/SD). The source-detector-separation (SDS) was varied from 20 to 60 mm, and the SNR was determined 10 times each. For an SDS of 20 to 30 mm, the LED intensities were adjusted to prevent amplifier saturation. Furthermore, for 20 mm SDS, data were picked up directly at the transimpedance amplifier's output. A measurement with an SDS of 60 mm was furthermore recorded from one of the authors forehead, with the 680 nm LED being constantly on. These raw oscilloscope data were smoothed offline with a digital 10 Hz low-pass filter.

**RESULTS:** For 20 to 40 mm SDS, the SNR was approx. 60 dB. For larger SDS, SNR decreased (Fig. 1A). Theoretical considerations suggested that the SNR was mainly limited by shot- and dark noise [3], as determined based on modeled values for the reflectance [4] for 850 nm and the SiPM specification (grey area in Fig. 1A). The pulsation is clearly visible for an SDS of 60 mm (Fig. 1B).

**DISCUSSION:** The adjustment of the LED light to prevent from detector saturation resulted in plateauing of the SNR for small distances. Assuming signal changes of approx. 1% due to altered brain activity, we considered an SNR of 50 dB a lower bound for reliable measurements. Under this constraint and at  $f_s=100$  Hz, an SDS of up to 45 mm was feasible. The usage of SiPMs in fNIRS instrumentation hence has the potential to allow for highly accurate measurements with miniaturized modules and increased SDS.

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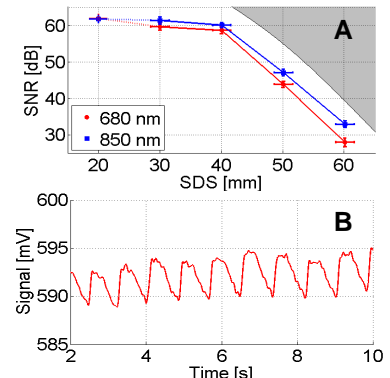


Figure 1: SNR vs. SDS. Error bars indicate SD of 10 measurements and estimated 1.5mm positioning uncertainty, respectively (A). Forehead pulsation (SDS: 60 mm, wavelength: 680 nm) (B).

## New Techniques for Advanced Optical Topography

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Two techniques that improve fNIRS instruments are introduced.

One is a prototype of wearable optical topography developed for observing brain activity noninvasively including regions covered by hair [1]. An avalanche photo diode (APD) whose sensitivity was 30 times higher than the usual Si photodiode was used because the optical transmittance in the region covered by hair is low. The APD, high voltage DC-DC converter, and preamplifier were placed in an electrically shielded case to be safely mounted on the head. Rubber teeth and a glass rod were prepared to clear away hair and reach the scalp. The system will be a useful tool for observing activation in motor, visual, and auditory cortices in daily situations, for example, rehabilitation.

The other is a MD-ICA (multi-distance independent component analysis) technique for separating signals in the scalp [2]. The waves observed with multi-distance probes are divided into components by ICA. When the hemodynamic change in scalp blood is the same as that in cerebral blood, the ICA component includes both of them. The amplitude of the component in the scalp is independent of the source-detector (SD) distance, and the amplitude of components in the deeper region linearly increase when the SD distance increases. Each mixing ratio of scalp signal and deeper region signal in each component can be calculated by observing the SD distance dependency of the component amplitude. Each ICA component was divided into two sub-components according to each mixing ratio. Then, both of scalp and deeper region waves were reconstructed by using the sub-components. This technique was validated by experiments with a phantom. The c-NIRS and conventional ICA technique extract the waves whose shapes are different from the scalp ones. In contrast, MD-ICA provides the cerebral blood volume including the systemic change because the waves are separated by depth. Also the systemic component can be removed by reducing the scalp components. MD-ICA will be applicable to a wide range of situations.

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## Development of multichannel fNIRS system with transcranial pulse oximetry function using CDMA technique

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fNIRS data contains various kinds of physiological fluctuation. Although the fluctuation has been thought to degrade the precision of fNIRS signal, these are expected to give subject's physiological information during the measurement. [1] The main fluctuation component in the signal is heart beat pulsation which strongly reflects the physiological and psychological state. In this study we have developed a multichannel fNIRS system which can extract and present the pulsation component and calculate the oxygen saturation ratio (SpO<sub>2</sub>) using pulse oximeter technique. [2]

### METHODS

Developed is multichannel system with 6 irradiation (wave length: 740nm and 830nm) and 6 detection probes, which measure 16 channel NIRS signals using CDMA(Code Division Multiple Access) modulation technique. The sampling rate is 12.3cycle/sec. Oxy and deoxy hemoglobin's pulsation waveform and frequency power spectrum were calculated and displayed simultaneously. [fig1] The oscillation component originated from heart beat is assigned automatically and used for the calculations.

### RESULT

We measured volunteer's fNIRS signal during mental tasks. Pulsation component was around 0.8-1.2 Hz and the frequency increased during the task. Although the fNIRS signal changed during the task, calculated SpO<sub>2</sub> ratio was stable around 90%.

Developed system can measure the change of heart beat pulsation useful for fNIRS measurement.

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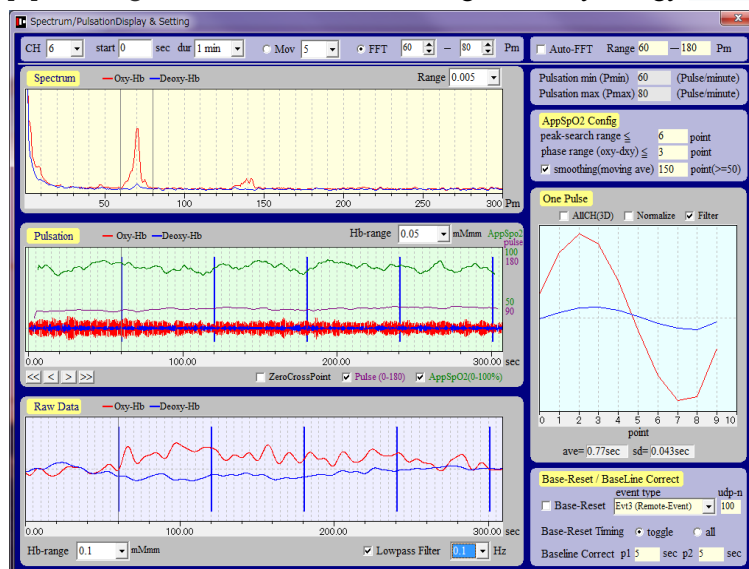


fig. 1

## Head probe for combined near-infrared spectroscopy and electroencephalography

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We present a novel head probe that integrates near-infrared spectroscopy (NIRS) and electroencephalography (EEG) to enable simultaneous measurements of neural electrophysiology and vascular hemodynamics over the whole head for research and clinical studies. The simultaneous NIRS and EEG measurements permit the observation of the temporal and spatial relationships between neural and vascular signals for studies of neurovascular coupling. The probe's design accommodates normal head shape variations and a wide range of head sizes. The current design contains 65 electrodes and 64 optodes. A flexible linkage system (black components in figure 1) follow the primary contours of the scalp by expanding or contracting to fit the desired head size while maintaining equidistant spacing between electrodes. An elastomeric web (orange) supplies uniform pressure over the scalp and holds the probe in place. Clinically relevant scalp positions and positional accuracy is ensured by locating the corners of the probe on standard scalp fiducial positions (inion, nasion, preauricular, and central). The linkage system of the probe then mechanically follows the 10-20 coordinate system and the web holds NIRS optodes and additional electrodes on the 10-10 and some 10-5 positions.

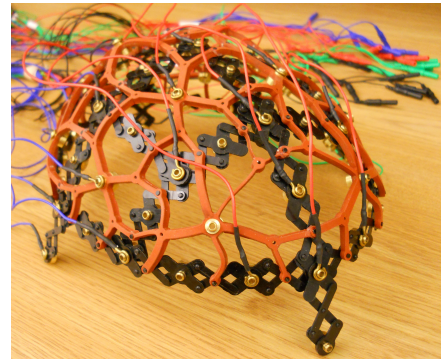


Figure 1 - NIRS-EEG Probe

The purpose of the present study is to evaluate the positional accuracy and precision in the sensor placement. The probe was placed 3 times on 10 subjects and then electrode locations were digitized with a 3D scanner. This was repeated for the commercial EEG cap ANT WaveGuard 32<sup>1</sup>. Precision was computed as the standard

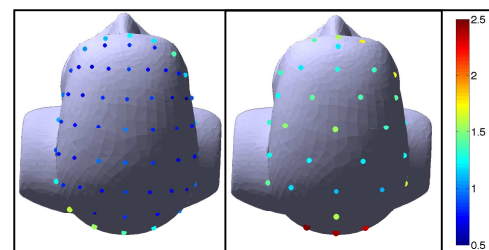


Figure 2 - Precision test results [mm] of NIRS-EEG probe (left) and ANT cap (right)

deviation of each electrode location from the mean position in mm. Accuracy was determined as the root-mean-squared error for each line segment as a percent error of the total arc-length. We are additionally evaluating the uniformity of the scalp pressure applied by the web. A force sensor is being used to measure the force of each position as it is pulled discrete distances away from the scalp.

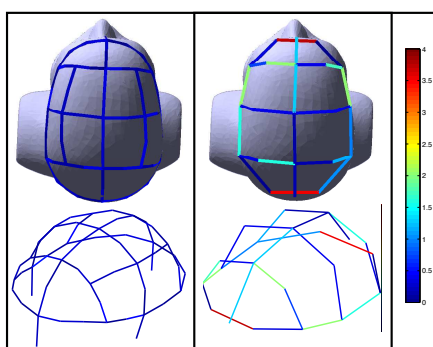


Figure 3 - Accuracy test results [% of total arc length] of NIRS-EEG probe (left) and ANT cap (right)

Accuracy ( $0.89 \pm 0.23$  - NIRS-EEG and  $1.47 \pm 0.36$  mm - ANT [mm]) and precision ( $0.19 \pm 0.15$  NIRS-EEG and  $1.13 \pm 1.02$  - ANT [% of total arc length]) results of the sensor placement are shown in figures 2 and 3 respectively. The web force testing is currently underway.

Accuracy and precision in the sensor location is important in establishing the correspondence of the signals measured from the scalp to the underlying brain anatomy and for the interpretation of scientific or clinical results. Uniformity in the pressure exerted by the optodes on the scalp maximizes optical coupling, stabilizes the probe during head movements, and improves comfort. The NIRS-EEG probe is intended to benefit multimodal data quality, repeatability, and ease of use.

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## **A low cost NIRS spectrometer for monitoring global physiological hemodynamic fluctuations.**

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**Introduction:** Low frequency hemodynamic oscillations have been shown to propagate throughout the body, and are a major confound to hemodynamic based functional imaging methods, such as fNIRS and fMRI. Global NIRS waveforms (with appropriate delay) have shown utility for characterizing and removing physiological confounds from functional imaging data [1-3]. We present a simple device to record these waveforms without requiring a high end research NIRS device.

**Methods:** To speed development time and reduce cost, the spectrometer was constructed using primarily commodity components. The core of the device is an Olimex MOD-PULSE pulse oximeter development board (Olimex, LTD, Plovdiva Bulgaria), which implements Texas Instruments' reference design for a Nellcor-compatible single chip pulse oximeter [4] using a TI MSP430FG437 MCU. It was attached to a Nellcor type fingertip pulse oximeter probe, which measures transmission through the fingertip at 660 and 940nm. This board displays heartrate and blood oxygenation on an LCD screen. Continuous gain and baseline offset adjustment keep the cardiac signal within a limited range to simplify heartbeat detection, which distorts the NIRS waveform in a nonlinear manner and eliminates all information below a few tenths of a Hz. In its default state, the device cannot be used to measure LFOs. However, the firmware of the 'FG437 can be rewritten to provide new capabilities.

The MOD-PULSE ADC has a two stage input amplifier. A low gain primary stage allows offset adjustment to keep the signal with a given range, and a high gain second stage boosts the high frequency signal before digitization. Rather than directly digitizing the second stage, as was done in the Olimex firmware, the 'FG437 was reprogrammed to perform a rapid, closed loop offset adjustment of the first stage to keep the digitized signal at a target value. The 660 and 940nm signals are sampled at 512Hz each while dithering the target value. The offsets are then filtered and downsampled by a factor of 16. Through this process the 'FG437 achieves 14 effective bits of dynamic range at 32 Hz with a flat frequency response (DC to 16Hz) with a 12-bit ADC, sufficient to digitize the all NIRS components of interest. Sample pairs are sent at 32 Hz over a serial channel to an Olimexino-STM32 (an Arduino-compatible development board with a 72 MHz ARM processor) for further signal processing and transmission over USB to a laptop (in this case a MacBook Pro). A Python process on the laptop converts raw NIRS data to oxy- (HbO), deoxy- (HbR) and total hemoglobin (tHb) waveforms, separates them into frequency bands of interest, displays them and stores the data.

The total cost of components excluding the case and the probe is ~\$65 (\$32 for the MOD-PULSE board, \$27 for the Olimexino-STM32, and \$5 for cabling). Reusable Nellcor probes cost between \$100-200 (although compatible probes are available for as little as \$10). Unit costs including case and probe would range from ~\$75 to \$300. Reflashing the MOD-PULSE firmware requires a JTAG programmer, which costs ~\$75; the Olimexino-STM32 can be programmed through the USB port. All software tools used in this project are open source: MSP430 development was done using the msp430-gcc toolchain; Olimexino development uses the Maple IDE, and postprocessing and display are performed in Python 2.6.

**Results:** 700 seconds of data were simultaneously recorded from two fingers on the left hand; the new oximeter recorded from the pointer finger, while a fiberoptic optical probe on the index finger was attached to an ISS Imagent system (690 and 830nm) recording at 12.5 Hz. In both the time and frequency domain, the data from the two spectrometers are indistinguishable.

**Discussion:** Commodity development boards can be used to build inexpensive, high quality NIRS spectrometers for specialized purposes which can be used in place of more complex, expensive instruments, and provide data of equivalent quality.

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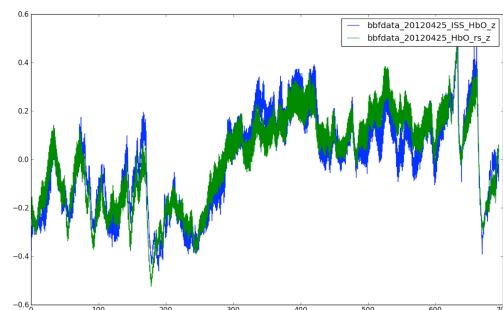


Figure 1 – Comparison of data from homebuilt spectrometer and ISS Imagent.



Improved light injection and detection methods for fNIRS headgear for use in avionics and astronautics

Authors: Jeffrey R. Mackey<sup>1</sup>, Grigory Adamovsky<sup>2</sup>, Padetha Tin<sup>3</sup>, Bertram M. Floyd<sup>4</sup>, **Angela R. Harrivel<sup>5</sup>**

Measuring hemoglobin concentration changes in the brain with Functional Near Infrared Spectroscopy (fNIRS) is a promising technique for monitoring cognitive state and optimizing human performance during both aviation and space operations. Advances in optical instrumentation for fNIRS have been conceptualized, prototyped and integrated into several new headgear designs suitable for use by commercial or military aircraft personnel and astronauts. Despite the continuing improvement of various research laboratory-based and commercial instrumentation, hardware currently used to attach optical fibers to and couple optical signals to the scalp for fNIRS behind the hairline is bulky, uncomfortable to painful, susceptible to motion artifact and interference from the hair, not expeditiously self-applicable and not readily integrated with existing environments (for example, cockpits and pilot headsets). Reducing such difficulties consistently encountered by those in both industry and academia is a design-driven aim. The success of these efforts to produce “next generation” fNIRS headgear will bring the benefits of the fNIRS technique out of the controlled laboratory and into clinical and operational environments. The full-up instrumentation that was tested in this research includes optical, electronic, custom headgear and medical grade phantom components.

This paper addresses the optical design, analysis, characterization and testing of the light delivery and detection systems in a terrestrial laboratory and aboard the Zero-G B727 aircraft during reduced and hyper gravity segments of flight. In particular, the embedded light delivery systems included the coupling of two different wavelength (690 nm and 830 nm) fiber pigtailed diode lasers, the addition of Gradient-index (GRIN) lenses to aid the focus of light through the scalp, skull and cerebral-spinal fluid layer, and the design of custom ferrules and fiber sleeves for use with the multi-mode silica fiber encased in a 900-micrometer tight tube buffer for protection and flexibility. Optical modeling is planned to investigate the effect of the GRIN lenses on the sensitivity profile in the tissue.

The light detection optical components were also embedded into the custom headgear using several GRIN lenses at strategically placed locations along comb-shaped parts. Custom sleeves and ferrules were also used to couple scattered light into multi-mode silica fibers that were part of a 12-count fiber distribution cable. In this manner, several detection locations may be integrated to a single low light-level detector such a photomultiplier tube. The ac- and dc-signal components were measured.

The fibers and optical components were housed securely in rapid-prototyped rigid headbands. These were designed in-house at the NASA Glenn Research Center with comb shapes (LEW-18280-1) to allow efficient self-application in the field by parting the hair upon application to maximize optic-skin coupling. Overall headband design parameters to be optimized for operational use include optical throughput, mechanical stability, self-applicability, comfort, safety and manufacturability.

Headgear testing was accomplished using gray matter phantom material embedded in life-sized phantom heads. Contact loads and accelerations were measured in conjunction with fNIRS signals to determine the optical coupling efficiencies as functions of g-level, pain threshold/level, and index matching media. Motion artifacts were characterized at varying headgear tension levels.

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<sup>1</sup> Vantage Partners, LLC

<sup>2</sup> NASA Glenn Research Center, Optical Instrumentation and NDE Branch

<sup>3</sup> National Center for Space Exploration Research, also acknowledging Daniel Gotti

<sup>4</sup> Sierra Lobo, Inc.

<sup>5</sup> NASA Glenn Research Center, Bioscience and Technology Branch, [angela.r.harrivel@nasa.gov](mailto:angela.r.harrivel@nasa.gov)

## Advances in Customized Headgear and Optode-Hair Penetration

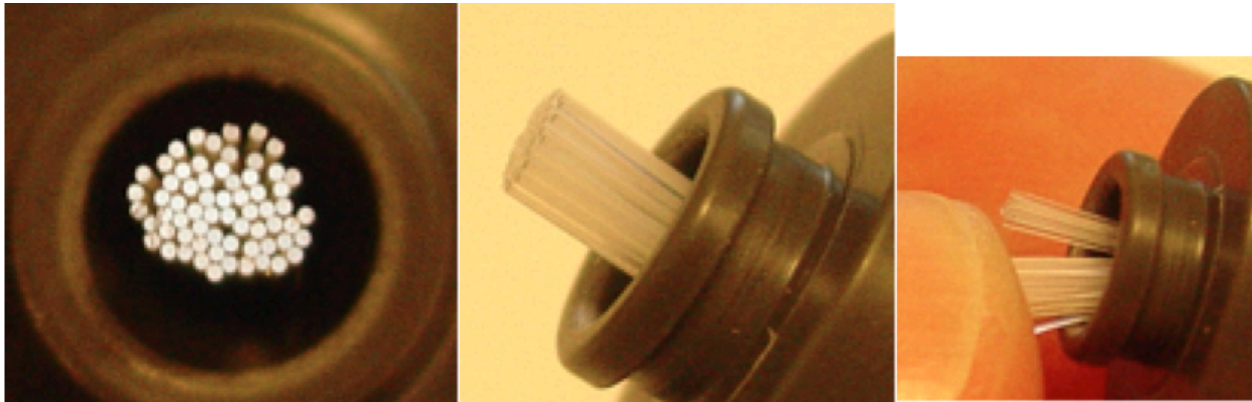
A collaboration between MRRA Inc., University of Texas at Arlington and University of Texas at Dallas developed a hair-penetrating optode producing 10x increases in SNR for fNIRS signals. Additional work by MRRA Inc. is presented utilizing rapid prototyping technology to produce custom headgear. This 3d printing method enables creation of headgear quickly and inexpensively, enabling customization at the single subject, single experiment level. [www.mrrainc.com](http://www.mrrainc.com)

**Chester Wildey, Ph.D., MRRA Inc., [wildey@mrrainc.com](mailto:wildey@mrrainc.com)**

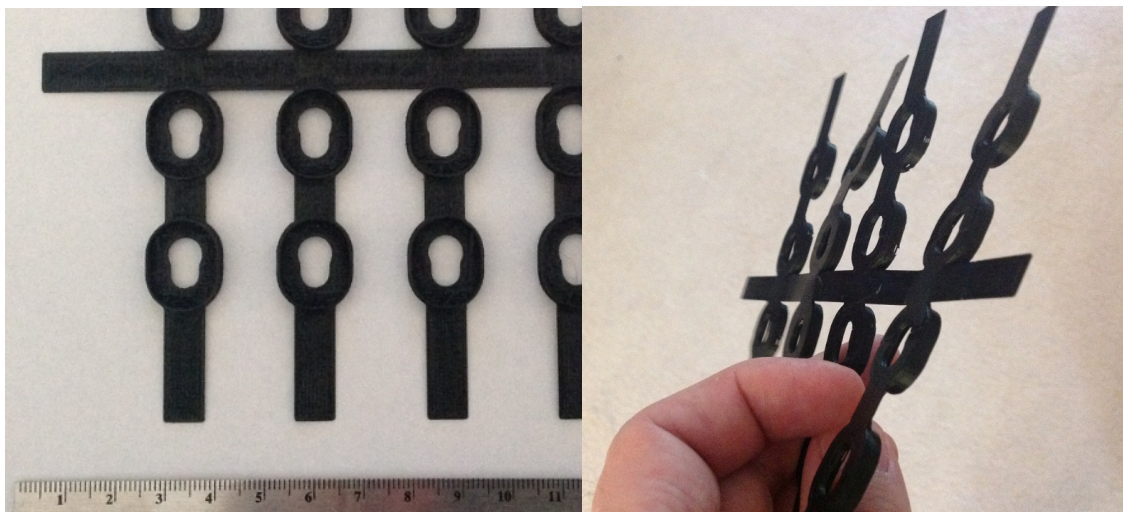
Bilal Khan, University of Texas at Arlington

George Alexandrakis, Ph.D., University of Texas at Arlington

Duncan MacFarlane, Ph.D., University of Texas at Dallas



Figures above show brush optode for penetration through hair. Figures below show 3d printed headgear. The optode layout and design may be adjusted on a per-experiment basis.



## Towards a device capable of detecting the fast optical signal and its application to stroke rehabilitation

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### Abstract:

Subsequent to a stroke, functional reorganization responsible for the recovery, proceed according to a range of strategies [4], which are not fully understood. This reorganization can to some extent be steered by means of therapies involving repetitive exercising. The study of therapy induced neuroplastic changes will benefit from a neuroimaging modality moderately robust to body movement, such as fNIRS [5]. We have very recently been granted funds to undertake this research. The goals of the new born project include (i) the development of a 4-channel frequency-domain fNIRS apparatus to measure the fast optical signal, and (ii) to use this apparatus to in-vivo in-situ observe the therapy induced functional reorganization associated to a virtual reality-based motor rehabilitation therapy [8]. A range of NIRS equipment based on different NIRS modalities is available [1]. In our case, illumination will follow a chirped frequency comb [3]. Signal detection will be achieved using chirp signal correlation. Initially, we plan to base our image reconstruction in differential measurement, although reconstruction from absolute optical data [2] will be considered at a later stage. In vivo measurement of the fast optical signal still poses many challenges [6, 7]. We expect our approach to enhance its detection reliability. This is one of the initial efforts on fNIRS research in Mexico, together with the incipient work with infants of the group led by Dr. Harmony and Dr. Marroquín who have long worked with EEG.

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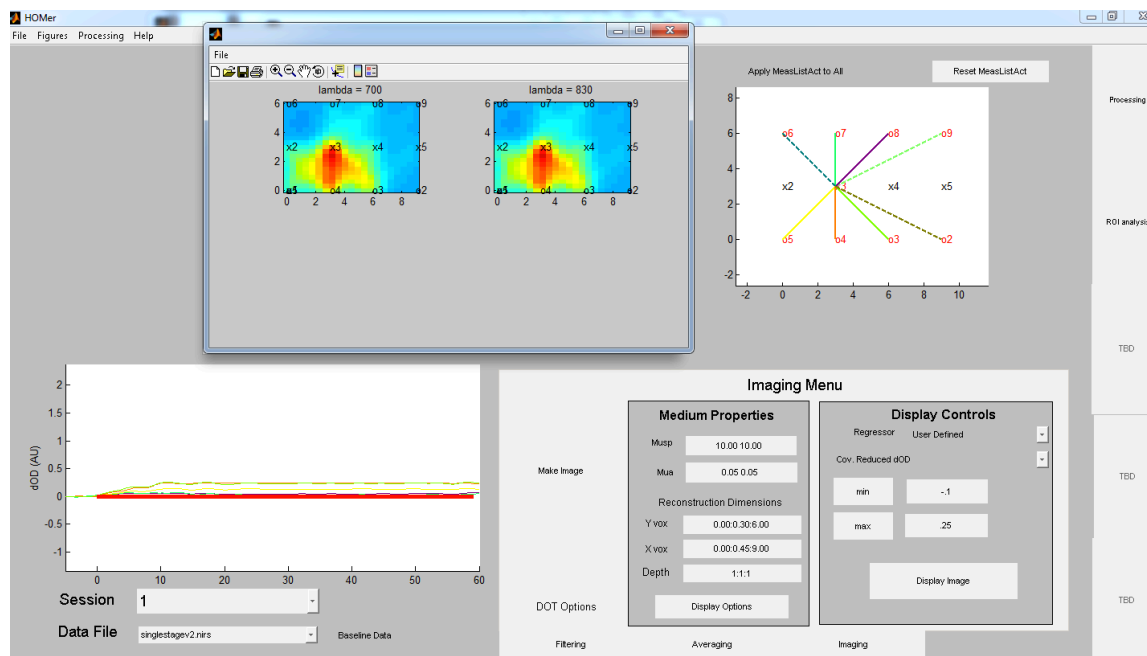
## Smaller, lighter, cheaper. A new fNIRS system from MRRA Inc.

Hair penetrating optodes and advanced digital modulation methods enable high sensitivity fNIRS measurements using PDs in place of APDs. This significantly reduces temperature-induced drift while also decreasing system size and cost. One 48-optode system occupies 1 liter of volume (excluding battery pack) and transmits data wirelessly to a receiver PC. The advanced digital modulation method allows 50% transmit optode duty cycle and is designed to enable real-time demodulation of individual fNIRS signals. Design overview and performance measures are presented. [www.mrrainc.com](http://www.mrrainc.com)

Chester Wildey, Ph.D., MRRA Inc., [wildey@mrrainc.com](mailto:wildey@mrrainc.com)



Figures above show 48 optode fNIRS system occupying 1 liter volume. Figure below shows results of dynamic liquid phantom testing of the system.



## TechEn: Advancing fNIRS Technology for Results

TechEn is a leader in fNIRS technology development, offering the CW6 continuous-wave system. Since 1998, we have collaborated with Dr. David Boas and his Photonics Lab at Massachusetts General Hospital in Boston, Mass., innovating and advancing every aspect of fNIRS systems, including instrumentation, software, head caps, custom accessories and support services.

We offer a variety of systems to meet different research needs and budgets. They range from small, portable systems to much larger ones; our largest includes 96 lasers with multiple wavelengths, 32 avalanche photodiode (APD) detectors and more than 2,000 data measurement channels. Flexible configurations enable partial as well as whole-head coverage.

Our latest advances include expansion of the CW6 systems for breast imaging and other complex studies.

Other recent developments include a new head cap system designed for localization, comfort and performance, and new optical fibers with optodes that facilitate comfortable and consistent contact with the scalp, even through long hair – traditionally a problem with fNIRS monitoring. The lightweight fibers and optodes are designed for use with head caps, head bands, helmets or patches.

TechEn systems integrate seamlessly with the HOMER and HOMER2 packages, and with most other post-processing software. In fact, Dr. Boas recently developed HOMER2 to advance CW6 and fNIRS data analysis capabilities – incorporating a suite of new add-on modules. For example, the user friendly software includes advanced stim mark control, group analysis and principle component analysis.

Researchers choose CW6 systems because key advances and capabilities described herein lead to successful results. The excellent data are made possible by the flexible yet high-performance CW6 instrument; a comfortable head cap and fiber optode system; and ease of use of the HOMER2 software. Other advantages of the systems include:

- Ease of use for set-up and data acquisition
- Real-time display
- Highest performance for signal-to-noise
- Dedicated ongoing support services
- Support for data analysis
- Expert and friendly lab training

Finally, we are very proud of the role our CW6 system has played in pioneering multi-modal studies, including CW6 and EEG especially in epilepsy studies, CW6 and fMRI for brain mapping, CW6 and IMPACT software for TBI, CW6 and TMS for addiction, and CW6 and tDCS for addiction.

Arthur “Buzz” DiMartino TechEn, Inc. email: [AAD@techen.com](mailto:AAD@techen.com) [www.nirsOptix.com](http://www.nirsOptix.com) Poster for fNIRS Conference at UC L



Poster Session  
**Multi-Modal Monitoring**  
Poster #: 18-24

## Multimodal investigation of neural-vascular coupling during somatosensory stimulation and resting state using concurrent MEG-NIRS and MRI-NIRS.

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### Introduction

In this study, multi-channel functional near-infrared spectroscopy (NIRS) signals were recorded from the primary and secondary somatosensory cortex during concurrent magnetoencephalography (MEG) and functional MRI. A pulsed-pair median nerve stimulus was used to probe the relationships of the neural and vascular responses. Concurrent neural and vascular data was also recorded during resting state fluctuations.

### Methods

A total of 15 subjects were scanned on two sessions with concurrent MEG-NIRS and fMRI-NIRS at 3T. A pulsed pair median nerve stimulus was used with 7 conditions of inter-pulse intervals between 50ms-500ms were used to probe the dynamics of the neural refractory period during unilateral stimulation. Unilateral median nerve stimulation was conducted using a computer controlled GRASS S88X stimulator. A stimulating bar electrode was positioned on the right median nerve and adjusted a voltage matching the motor threshold as judged by twitching of the thumb on the stimulated hand. A functional localizer task consisting of repeated 10-second blocks of stimulation at 4Hz with a 20second inter-block rest period was administered. Five-minute scans of event-related pulsed-pair stimulation were then given. The pulsed pair condition consisted of a pair of two median nerve pulses separated by an inter-stimulus interval of 50, 100, 150, 200, 300, 400, or 500ms. The stimulus conditions were presented in randomized order with a minimum spacing of 12-18 seconds between events to avoid potential non-linearities in the hemodynamic response. A TechEn CW6 NIRS system was used to record in both concurrent MRI and MEG sessions. Session dedicated MRI or MEG fiber optics were used. Registration of the NIRS probe was done via both vitamin E markers (for MRI) and HPI positioning coils (for MEG), which were both mounted on the NIRS head cap.

### Results

Concurrent NIRS-MEG and NIRS-MRI showed similar activation areas within S1 (Fig 1). Both MEG and MRI showed additional activations within the secondary sensory area (S2), which was below the spatial resolution of NIRS. Regions-of-interest from the area of S1 were examined as a function of the inter-pulse interval. The NIRS and MRI data both showed a U-shaped response profile indicating a minima in the response at 75-150ms corresponding to the neural refractory period (fig 2). The ratio of the amplitude of the second to first pulse measured via MEG showed a similar response profile.

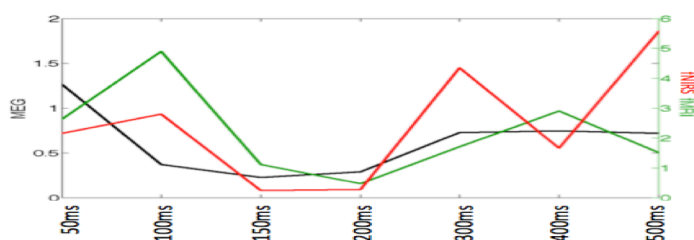


Fig 2. The amplitude of the NIRS, MEG, and fMRI amplitudes were extracted for the 7 pulsed pair conditions based on a region-of-interest defined by the localizer task for each modality.

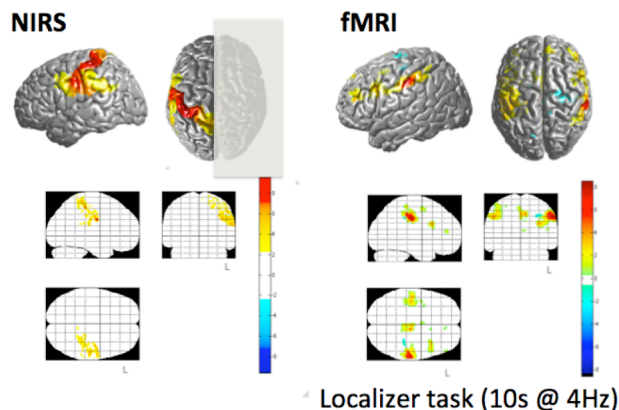


Fig 1. Concurrent NIRS (left) and fMRI (right) recordings of median nerve stimulation showed similar spatial localization. The NIRS was only recorded on the left (contralateral) hemisphere due to the space constraints of the MEG scanner.

### Conclusion

Concurrent MEG-NIRS and MRI-NIRS results show tight coupling of the neural and vascular signals.

## Investigation of brain tissue oxygenation, cytochrome-c-oxidase and intracellular metabolites during perinatal cerebral hypoxia-ischaemia

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**Background:** Hypoxic-ischaemia (HI) neonatal encephalopathy is associated with high mortality and morbidity rates worldwide. In this study we investigate brain oxygenation, cytochrome-c-oxidase (CCO) and energy-resource changes during transient HI and recovery using simultaneous broadband near-infrared spectroscopy (NIRS) and phosphorus (<sup>31</sup>P) magnetic resonance spectroscopy (MRS) in the piglet.

**Methods:** 22 healthy piglets (aged <24 hr) were anaesthetised and physiologically monitored. Transient cerebral HI (duration 20 minutes) was induced by reducing the inspired oxygenation and reversibly inflating bilateral carotid artery occluders. Using <sup>31</sup>P MRS we measured inorganic phosphate (Pi)/epp, phosphocreatine (PCr)/epp, and nucleotide triphosphate (NTP)/epp (epp=exchangeable phosphate pool=Pi+PCr+3NTP). NIRS measured cerebral concentration changes of oxy-haemoglobin (HbO<sub>2</sub>) and deoxy-haemoglobin (HHb), and cytochrome-c-oxidase oxidation state changes ( $\Delta[\text{oxCCO}]$ ).

**Results:** Simultaneous <sup>31</sup>P-MRS and NIRS results are shown in Figure 1. HI rapidly reduced brain oxygenation as shown by changes in haemoglobin difference ( $\Delta[\text{Hbdiff}] = \Delta[\text{HbO}_2] - \Delta[\text{HHb}]$ ) closely followed by a fall in  $\Delta[\text{oxCCO}]$ . PCr/epp fell, and Pi/epp rose, quickly while NTP/epp was buffered initially and only declined when  $\Delta[\text{oxCCO}]$  was significantly lowered. During recovery, metabolic markers for piglet 175 returned to baseline (Figure 1(a)); but they did not for piglet 183 (Figure 1(b)).

**Discussion:** During transient HI, CCO becomes reduced due to oxygen depletion; adenosine triphosphate levels are initially preserved by the creatine kinase reaction leading to PCr decline whereas energy utilisation without oxidative phosphorylation leads to increased Pi. During recovery we have observed high association between the NIRS measurement of  $\Delta[\text{oxCCO}]$  and <sup>31</sup>P-MRS. Complementary MRS and NIRS enable better understanding of the cerebral metabolic response to HI and can help evaluate early interventional therapies.

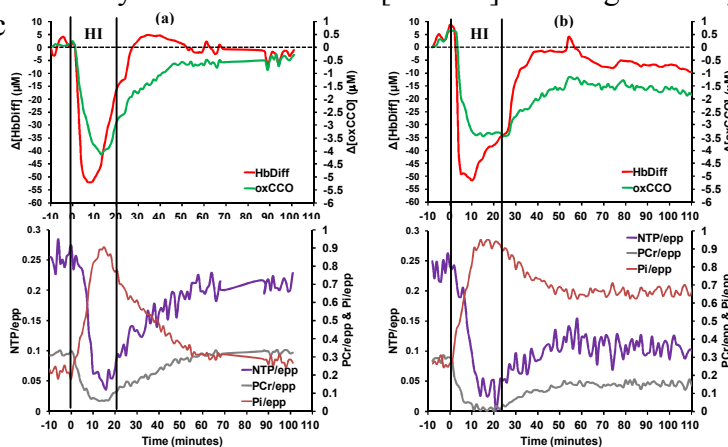


Figure 1. <sup>31</sup>P-MRS and NIRS during HI and recovery; (a) piglet 175; (b) piglet 183.



## Multimodal correlation analysis between fNIRS, fMRI and EEG during motor tasks

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**Introduction.** Investigating human brain function requires a multimodal neuroimaging approach. The combination of different electrophysiological (electroencephalography, EEG) and haemodynamic (functional magnetic resonance imaging, fMRI and functional near-infrared spectroscopy, fNIRS) modalities to measure brain activity complements each other's limitations. EEG measures brain activity directly by placing EEG electrodes over the scalp and measuring the electrical potential at each electrode. fMRI measures brain activity indirectly via changes in the blood oxygenation level-dependent (BOLD) contrast signal, which is related to an increase in cerebral oxygen delivery subsequent to increased neuronal activity (i.e., neurovascular coupling). Similarly, fNIRS measures several physiological parameters related to cerebral oxygenation including measurements of concentration changes in oxygenated (O<sub>2</sub>Hb) and deoxygenated (HHb) hemoglobin. Unlike fMRI, EEG offers good temporal resolution but has very limited spatial resolution, while fNIRS has better temporal resolution than fMRI but lower than EEG, and lower spatial resolution than fMRI but better than EEG. Previous studies have simultaneously measured combinations of two out of the three neuroimaging modalities, but to the best of our knowledge no previous study has measured all three modalities simultaneously, which is usually due to technical limitations. Therefore the aim of the study was to determine the correlation between cortical activation measured with fNIRS, fMRI and EEG during different motor tasks. **Methods.** Five healthy subjects (26y) performed three different motor tasks with their right hand (finger tapping [FT], simple finger sequence [SFS], and complex finger sequence [CFS]) in a block design (10 repetitions with 30-s task and 30-s rest). The experimental setup consisted of fMRI-compatible EEG (256 channels, GEO300, EGI, USA) and fNIRS (24 channels, Oxymon MkIII, AMS, the Netherlands) systems. Four fNIRS probes were placed in the EEG cap around the contralateral motor cortex (CMC) region of the subjects scalp. Subjects were then placed in a supine position inside a 3T MRI scanner (Philips Achieva, Philips, the Netherlands). fMRI (BOLD) time series data from the CMC was extracted, and fNIRS (O<sub>2</sub>Hb and HHb) time series data from all 4 channels were down-sampled to the fMRI time series providing 240 time points for comparison. To determine the relationship between fMRI and fNIRS time series over the 10 blocks during each of the 3 motor tasks, Spearman's correlation was calculated. Scalp EEG electrodes surrounding the CMC were chosen for analysis and their dynamical coherence with the right hand electromyography (EMG) signals was calculated with overlapping windows. This scalp coherence vector (240 time points) was used to calculate its relationship with fNIRS and fMRI time series using Spearman's correlation. Afterwards, dynamic imaging of coherent sources analysis was used to extract the source level EEG from the CMC and then its dynamical coherence with EMG signals was also correlated against fNIRS and fMRI time series using Spearman's correlation. **Results & Discussion.** fNIRS was significantly correlated with fMRI during FT (O<sub>2</sub>Hb:  $r=-0.22$ ,  $P=0.00075$ ; HHb:  $r=0.36$ ,  $P=0.0001$ ), SFS (O<sub>2</sub>Hb:  $r=-0.47$ ,  $P=0.00001$ ; HHb:  $r=0.47$ ,  $P=0.0088$ ), and CFS (O<sub>2</sub>Hb:  $r=-0.39$ ,  $P=0.0001$ ; HHb:  $r=0.15$ ,  $P=0.0182$ ). The scalp coherence vector showed a significant correlation with fNIRS ( $r=0.61$ ,  $P=0.0001$ ) and fMRI ( $r=0.59$ ,  $P=0.0001$ ) only during FT. The EEG source coherence vector showed a significant correlation with fNIRS (O<sub>2</sub>Hb:  $r=0.38$ ,  $P=0.00001$ ; HHb:  $r=0.54$ ,  $P=0.0001$ ) and fMRI ( $r=0.168$ ,  $P=0.009$ ) during all three motor tasks. This indicates that EEG source analysis is better than EEG scalp analysis to determine CMC activation during all three motor tasks. In conclusion, our initial findings show strong temporal correlations between fNIRS, fMRI and EEG data collected simultaneously during three motor tasks. Future effort should implement these novel approaches to increase the significance and the homogeneity of these results in the search of a more complete understanding of the dynamics and the physiology of the neurovascular coupling.

## A Study of Executive Control during Intracorporeal Minimally Invasive Suturing (ICS)

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**Introduction:** The introduction of minimal invasive surgery (MIS) has allowed surgeons to perform complex surgeries through smaller incisions leading to faster patient recovery. Due to the loss of depth perception, lack of tactile feedback and the fulcrum effect MIS is more technically demanding to perform. Of MIS manoeuvres intra-corporeal suturing (ICS) and knot tying are arguably the most challenging and limit the capability of the surgeon to perform advanced surgery<sup>1</sup>. A more detailed appreciation of the cortical response to complex tasks such as ICS is necessary in order to determine which sub-tasks demand most cognitive resources and therefore which episodes need focused additional training time and /or technological assistance. We aimed to assess which aspect ICS evoked most pre-frontal cortex (PFC) activation amongst novices. We hypothesized that the technically more challenging aspect of ICS, namely the *double throw knot* would evoke the greatest PFC excitation.

**Methods:** 15 right-handed laparoscopically naïve medical students (mean age of 21.6±1.3 years SD) were recruited to perform ICS. Each subject initially observed a video tutorial and later trained for two hours on a box trainer, with guidance from a trainer. The task involved of placing three interrupted IC sutures across an enterotomy (laceration in bowel) The ICS task was divided into three subcomponents performed sequentially as follows: insertion of needle (task A), double throw knot (task B) and a pair of single throw knots (task C)<sup>2</sup>. A block design experiment was conducted involving 9 blocks, which comprised of alternate ‘rest’ (40s) and ‘task’ periods (variable time). Primary outcome measures were relative changes in oxygenated and deoxygenated haemoglobin ( $\Delta\text{HbO}_2$  and  $\Delta\text{HHb}$  respectively) in the PFC captured by a 24 channels Optical Topography device (ETG-4000, Hitachi Medical Corp., Japan). Secondary outcome measures were task performance measures (time and validated objective score)<sup>3</sup>.

**Results:** 12 of 15 participants completed the task after a single training session. The remaining three participants were invited for an additional two hours training period before undergoing the assessment. Averaged group data across all PFC channels revealed that Task A evoked a greater change in  $\Delta\text{HbO}_2$  (average of  $\text{HbO}_2$  task- average of  $\text{HbO}_2$  baseline) compared to Task B and C (median values 22.48, 2.80 and 6.61  $\mu\text{Mxcm}$  respectively) which was found to be statistically significant ( $P<0.001$ ). The three subjects who required remedial training demonstrated a greater change rise in  $\Delta\text{HbO}_2$  (average of  $\text{HbO}_2$  task- average of  $\text{HbO}_2$  baseline) across all stimuli than the remaining cohort (remedial group = 29.37, 21.67 and 19.73  $\mu\text{Mxcm}$  for task A, B and C respectively versus 19.26, 0.58 and 5.26  $\mu\text{Mxcm}$  for the residual cohort).

**Discussion:** The PFC is recruited when motor performance is unrefined and attention demands are high<sup>4</sup>. Contrary to published literature<sup>5</sup>, the current study suggests that for novice surgeons there are aspects of intra-corporeal knot-tying that demand attention and executive control. Contrary to our hypothesis, the most attention-demanding manoeuvre appeared to be that of needle insertion instead of double knot-articulation. Interestingly the subjects who required remedial training recruited a greater amount of their cognitive resources across all subtasks. In order to understand this a further longitudinal study is required to examine the pattern of changes in brain behaviour that are associated with improvements in technical skill and amelioration of cognitive load with learning.

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Simultaneous (Q)EEG and NIRS measurements during eyes open and eyes closed resting state conditions in healthy volunteers

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The analysis of resting state brain activity is a common phenomenon in quantitative EEG (QEEG) and gaining more popularity in fMRI research. In the field of NIRS it is however not common to be interested in resting state activity. From EEG and QEEG research we know that during a resting state condition with closed eyes alpha wave activity occurs on the occipital cortex. Upon opening the eyes this alpha wave subsides. Moosman et al. (2003) investigated changes in the occipital EEG alpha rhythm together with changes in fMRI and NIRS. In their study the combination of alpha and Deoxy-Hb (N=4) resulted in a strong positive correlation at a delay of about 8 seconds. As an extension of their work this study explored the difference in resting state activity of the occipital cortex between eyes open and eyes closed in a sample of 38 healthy adults. Changes in alpha wave activity were compared to changes in Oxy-Hb as well as Deoxy-Hb concentrations.

Subjects (N=38) were fitted with electrodes over the O1 and O2 position of the international 10-20 system. Over each location a transmitter and receiver were placed in order to be able to measure brain activity from corresponding brain areas in both modalities. A continuous measurement of 5 minutes was conducted in which subjects were asked every 30 seconds to change from eyes open to eyes closed and vice versa. The starting condition was assigned randomly, assuring an even distribution of the two paradigms.

Pairs were formed within each minute, containing one block of eyes open data and one block of eyes closed data. The average alpha power and concentration of Oxy-Hb and Deoxy-Hb were calculated for every second half of each block in order to avoid transient features and to ensure steady state values were taken into account. After removing outlying data, paired samples t-tests were conducted.

The t-tests revealed significant differences between eyes open and eyes closed conditions for alpha magnitude (mean difference 14.92  $\mu$ V,  $p < 0.0001$ ) as well as Oxy-Hb (mean difference 0.624 mmol,  $p < 0.01$ ) and Deoxy-Hb (mean difference 0.117 mmol,  $p < 0.05$ ) concentrations. During eyes closed conditions more alpha wave activity and higher Deoxy-Hb concentration is found and lower Oxy-Hb concentration compared to eyes open conditions. Subsequently a correlation analysis was conducted in order to establish correlations between the averaged data. This analysis did not reveal any significant correlations leading us to believe that the relationship between resting state NIRS activity and alpha wave activity needs to be sought in time series analysis rather than static analysis of block averages.

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## Comparison of NIRS, EEG and MEG sensitivity to spatial scale of brain activity

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*Introduction:* Functional near-infrared spectroscopy (NIRS), electroencephalography (EEG) and magnetoencephalography (MEG) are functional brain imaging methods that require inverse solutions to localize brain activity. All three methods have spatial resolution as measured by localization error on the order of a centimeter [1, 2]. Despite these similarities, differences in how brain activity is propagated to the sensors means that the imaging methods may be sensitive to different spatial scales of brain activity.

*Methods:* Brain activity was simulated on a realistic cortical surface reconstructed from a T1-weighted MRI using Freesurfer [3]. Different spatial scales of brain activity were generated using spatially filtered white noise on the spherical representation of the cortical surface. Forward models were calculated for all brain imaging modalities using a whole-head probe based on the 10-5 system [4] with 286 electrodes for EEG and 482 source-detector pairs with separations from 2-3 cm were used for NIRS. The Elekta VectorView 306 channel instrument was used as the sensor array for MEG. Brain activity was simulated at 9 different spatial scales, representing spatial activity scales from  $0.026 \text{ cm}^2$  to  $1100 \text{ cm}^2$ . The root-mean-square (RMS) of the simulated brain activity at each sensor was calculated over 500 sample brain activation patterns as a measure of the sensitivity to brain activity at each spatial scale.

### Results and Discussion:

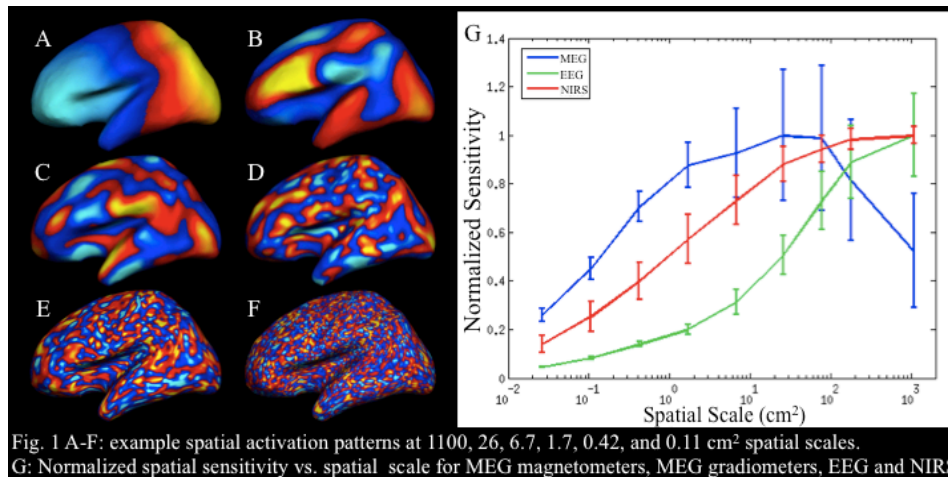


Fig. 1 A-F: example spatial activation patterns at 1100, 26, 6.7, 1.7, 0.42, and 0.11  $\text{cm}^2$  spatial scales.

G: Normalized spatial sensitivity vs. spatial scale for MEG magnetometers, MEG gradiometers, EEG and NIRS.

Larger RMS indicates that the modality is more sensitive to variability in brain activity on that spatial scale. Sensitivity was normalized to the maximum RMS value for each modality. MEG was most sensitive to activity on the 30-80  $\text{cm}^2$  spatial scale. NIRS is most sensitive to the largest spatial scale

activations. EEG is also most sensitive at large spatial scales, and its sensitivity declines more quickly as the spatial scale decreases, indicating that EEG may be less sensitive than NIRS for discerning small-scale activation patterns.

*Conclusion:* MEG, EEG, and NIRS have different sensitivities to the spatial structure of brain activity. This finding indicates that multimodal brain imaging using these methods may measure different spatial scales of activation patterns of the brain, even if similar probe designs are used between modalities.

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## Effect of Visuomotor rotation in Laparoscopic Surgery on the Prefrontal Cortex (PFC)

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**Introduction:** ‘Neuroergonomics’ seeks to study the effects of technologies on the human brain and has recently been applied to evaluate surgical instrumentation<sup>1</sup>. Laparoscopic (keyhole) surgery accelerates recovery, improves cosmesis but is more challenging to perform due to the effects of visuomotor rotation (VMR), loss of depth perception (projection of 3D operative field onto a 2D screen) and lack of tactile feedback. During operative procedures VMR occurs when the laparoscope is unintentionally rotated over its long axis resulting to disoriented images of the operative site. Confusing spatial transformations result in misalignment between visual perception and motor control<sup>2</sup>, degrading performance<sup>2, 3</sup> and theoretically increasing cognitive load. Here we evaluate the impact of VMR on bilateral excitation across the prefrontal cortex (PFC). Given the role of the PFC in attention to actions, visuospatial working memory and performance monitoring; critical for complex skill acquisition<sup>4</sup> it was hypothesised that VMR would evoke greater PFC excitation.

**Methods:** Eight right-handed laparoscopically naive medical students (mean age  $\pm$  SD = 20.4  $\pm$  1.6 years) were recruited to perform peg transfer task requiring peg manipulations between laparoscopic instruments operated by either hand and placed onto a pin board. The task was performed under normal view or with the view rotated by 90° (order randomised). A block design experiment was conducted involving six blocks comprising alternating ‘rest’ (30s) and ‘task’ periods (variable time). Primary outcome measures were relative changes in oxygenated and deoxygenated haemoglobin ( $\Delta$ HbO<sub>2</sub> and  $\Delta$ HHb respectively) in the PFC captured by a 24 channels Optical Topography device (ETG-4000, Hitachi Medical Corp., Japan). Secondary outcome measures were task performance measures (time and validated objective score)<sup>3, 5</sup>.

**Results:** Group average performance was better under the normal view versus the rotated view for time (mean 138.29 s vs. 296 s,  $p < 0.001$ ) and objective score (mean 162.13 vs. -16.3,  $p < 0.001$ ). Across all channels, for all subjects on all trials a greater change in  $\Delta$ HbO<sub>2</sub> (average of HbO<sub>2</sub> task- average of HbO<sub>2</sub> baseline) was observed under the normal view versus rotated view ( $p = 0.022$ ). A greater change in group  $\Delta$ HbO<sub>2</sub> (normal vs rotated view) was observed in all channels overlying the right PFC ( $p = 0.009$ ) and left PFC ( $p = 0.038$ ). Similarly across all channels for all subjects and trials a greater change in  $\Delta$ HHb (average of HHb task – average of HHb baseline) was observed under the normal versus rotated view ( $p$  value  $< 0.001$ ).

**Discussion:** VMR results in poorer technical performance compared to normal view laparoscopy in task naïve subjects. Contrary to the hypothesis normal view laparoscopy resulted in greater PFC responses than VMR. It is conceivable that VMR is so challenging that subjects are unable to engage an appropriate PFC dependent cognitive strategy, or cognitively disengage as a result of task complexity<sup>7</sup>. Further longitudinal studies are required to evaluate the effects of repeated practice under VMR on the evolution in PFC cortical haemodynamics.

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Poster Session  
**Data Analysis**  
Poster #: 25-54

## High frequency content in blood volume signal is predictive of migraine without aura

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Migraine is proposed to be a neurovascular coupling disorder where the neuronal activity-induced metabolic demand, such as oxygen or glucose, is unmet by vascular supply. Based on this suggestion and the findings of our group and the others we attempt to cluster patients and controls by using fNIRS-derived Blood Volume (BV) signals. To this aim, 16-channel fNIRS data were collected from 13 healthy controls and 18 patients with migraine during Stroop interference task (ARGES Cerebro, Hemosoft Inc., Ankara Turkey). As preprocessing steps, BV signals (HbO<sub>2</sub>+Hb) were first band-pass filtered at 0.01-0.8Hz to remove the baseline drift. Then an independent component analysis (ICA) based analysis procedure is applied to the 16 channels [1]. In this procedure, components which are extracted by ICA algorithm from each subject are used to create a feature set. This feature set consists of weights of the ICA components in individual's BV signals. Then, significant features are determined by using a correlation based feature selection algorithm [2]. These features were then used to cluster our experimental groups. We used two unsupervised clustering algorithms which are K-means and Expectation Maximization (EM). As seen in Table-1, both algorithms give similar results in our database. We observed that the selected features mostly correspond to the channels located on right prefrontal cortex. These features are related with ICA components which have relatively high frequency characteristics (Figure.1). In general, fNIRS analysis is restricted to the very limited low frequency band and its high frequency content is considered as a noise and discarded. But our results show that high frequency signals might be important in the evaluation of hemodynamic regulation in patients with migraine. This frequency range does not correspond to any of the defined physiological phenomenon detectable by fNIRS systems. Thus, further studies with simultaneous physiological measurements are needed to understand the origin of this high frequency response. Although in our previous study, we did not find any difference in fNIRS signals between patients with migraine and healthy controls [3], the procedure that we used in the present study is able to cluster the two subject groups successfully. This method could be used in clinical settings to classify migraine from different types of headache, after our results are supported by further studies.

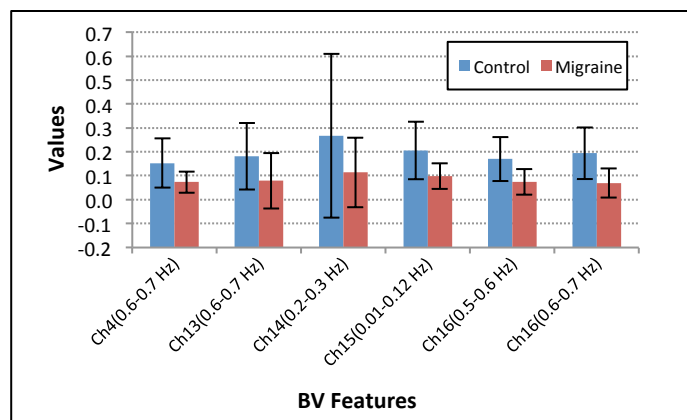
**Table 1.** Clustering results of K-means and EM algorithms.

	Sensitivity	Specificity	Success Rate
K-means	0.89	0.84	0.87
EM	0.78	0.85	0.81

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**Figure 1.** BV features that differentiate controls from patients with migraine. Channel 4 (Ch4) is located over left prefrontal region and the other channels (Ch13, Ch14, Ch15, and Ch16) correspond to the right prefrontal region.



## Haemodynamic Responses to Moving Sinusoidal Gratings

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**Purpose:** To record the changes in oxy (HbO) and de-oxyhemoglobin (Hb) concentrations over the occipito-parietal and occipito-temporal cortex in response to dynamic visual stimuli using functional near infrared spectroscopy (fNIRS).

**Methods:** Data were collected on a two-channel oximeter that used the Frequency Domain Multi-Distance (FDMD) method. Stimuli consisted of static and dynamic sinusoidal annuli presented at 90% contrast and subtending 15 degrees of arc. The spatial frequency of the sinusoidal gratings was 0.33 cpd and the temporal frequency was 0.625 Hz. The gratings alternated between moving centripetally and centrifugally for each trial. Responses to a grey field of equal mean luminance to both static and moving annuli were collected at the start of each trial for 30 seconds to ensure steady baselines levels of HbO and Hb concentration. In accordance with the local ethical committee guidelines, recordings were made from five normal participants (aged 18-32 years) over scalp locations using a modified version of the 10-20 electrode-placement system that corresponded roughly to primary visual and motion sensitive areas of cortex (O1, O2, P03, P04, P07 and P08). Recordings were made in response to the grey screen for 30 seconds at each location prior to the start of each trial. Data were analysed offline applying the kernelized Distributed Lag Model (written in R). kDLM allows simultaneous measurement of the HRF and estimation of the fNIRS response waveform (the response is the convolution of the HRF and the stimulus waveform).

**Results:** As expected, regardless of cortical location, the largest increase in HbO concentration occurred on presentation of the moving sinusoidal annuli after presentation of the grey screen. This coincided with the largest decrease in deoxygenated haemoglobin. HbO concentration fell upon presentation of static sinusoidal grating with a consequent increase in Hb. Applying DLM to the data revealed an HRF having a peak at a lag of 30 seconds, and showed that there was no difference in the responses to the expanding and contracting gratings.

**Conclusions:** This study demonstrated that absolute concentrations of haemoglobin in the visual cortex changed with presentation of a moving stimulus. HbO rose while Hb decreased when moving sinusoidal gratings were stimulating the cortex.



## A new approach to extract stimulus-evoked hemodynamic responses in fNIRS signals using Ensemble Empirical Mode Decomposition

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**Abstract:** Functional near-infrared spectroscopy (fNIRS) enables the measurement of hemodynamic responses (HRs) of the brain evoked by different stimuli. The stimulus-evoked HRs are characterized by a specific change in concentrations of oxyhemoglobin ( $[O_2Hb]$ ), deoxyhemoglobin ( $[HHb]$ ) and total hemoglobin ( $[tHb]$ ) which can be non-invasively measured using fNIRS. Usually, stimulus-evoked HRs are extracted from fNIRS signals (i.e.  $[O_2Hb]$ ,  $[HHb]$  and  $[tHb]$ ) by band-pass filtering with predefined cutoff-frequencies, and subsequent averaging of all trials. Since the choosing of cutoff-frequencies and type of band-pass filter used has an influence on the detectability and characteristic of the stimulus-evoked HR extracted, the goal was to develop an approach that circumvents the need for the (subjective) choosing of cutoff-frequencies and filter-types. In the present paper we present such an approach that enables to extract the stimulus-evoked HRs using a completely data-driven method. This method comprises two main signal processing steps: (i) decomposing of the specific fNIRS signal (i.e.  $[O_2Hb]$ ,  $[HHb]$  or  $[tHb]$ ) into intrinsic mode functions (IMFs) using Ensemble Empirical Mode Decomposition (EEMD) with different added noise levels; (ii) finding all IMFs with the strongest component that is related to the stimulus-evoked HR by using a statistical test; and (iii) performing a block average over all detected HRs in the signal. At the meeting, this new method of stimulus-evoked HR extraction will be explained in detail and application examples will be given. The advantages of the proposed method in comparison to the conventional approach (i.e. completely data-driven analysis of fNIRS signals) will be discussed. In conclusion, we developed a method that improves the detection of stimulus-evoked HR by an automatically data-driven optimization of the band-pass-filtering based on EEMD. Preliminary results show that the extracted stimulus-evoked HR have higher signal-to-noise ratio than those resulting from conventional fNIRS signal processing.

## Development and utilisation of computational models for tomographic fNIRS imaging and co-registration with multi-modal data

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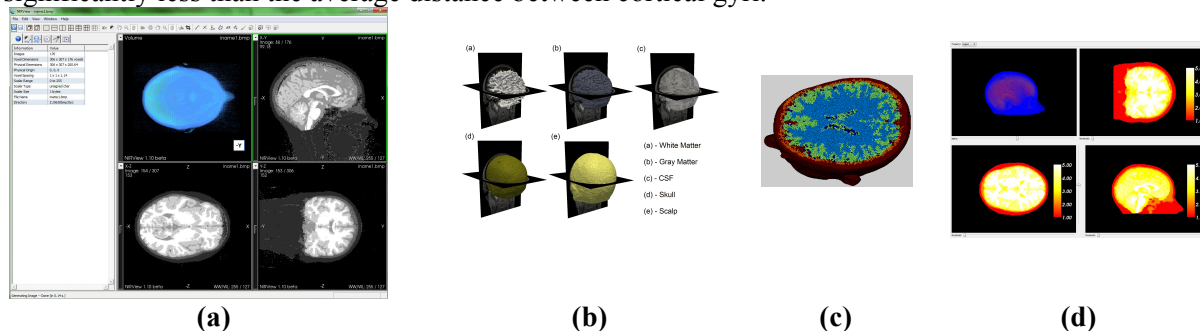
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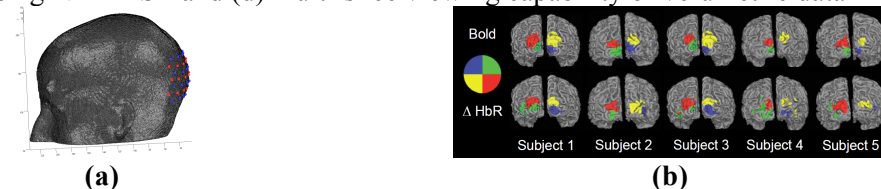
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We have developed a set of open-source GUI driven applications (NIRFAST and Nirview [1,2]) that allow seamless generation of numerical models for utilization in model-based tomographic reconstruction in diffuse optical functional near-infrared spectroscopy (fNIRS). Using multi-modality data, such as MRI, it is possible to segment tissue types using manual and semi-automated segmentation techniques, such as simple thresholding or k-means classification followed by a random markov field refinement. Based on the segmented tissue masks it is a seamless operation to generate a multi-layered volumetric finite element model that can be used to simulate light propagation within the geometry using NIRFAST which also additionally contains easy to follow and computationally efficient reconstruction algorithms to allow tomographic imaging, Figure 1. In this paper, we will outline the key features of this set of software and demonstrate its capabilities by providing a quantitative spatial comparison of high-density diffuse optical tomography (HD-DOT) and fMRI cortical mapping [3], Figure 2. The analysis is performed within the visual cortex using matched visual stimulation protocols in a single group of subjects ( $n=5$ ) during separate HD-DOT and fMRI scanning sessions. To attain the needed voxel-to-voxel co-registration between HD-DOT and fMRI image spaces, we implemented subject-specific head modeling that incorporated MRI anatomy, detailed segmentation, and alignment of source and detector positions. Comparisons of the visual responses found an average localization error between HD-DOT and fMRI of  $4.4\pm 1$  mm, significantly less than the average distance between cortical gyri.



**Figure 1.** (a) A snapshot of Nirview that allows the segmentation of tissue types, (b) rendered surfaces of different tissues within a human head, (c) volumetric finite element model of the human head generated using NIRFAST and (d) multi-slice viewing capability of volumetric data in NIRFAST.



**Figure 2.** (a) Surface rendered model outlining the location of optical sources and detectors on the visual cortex. (b) Quadrant activations for five subjects; all fNIRS quadrants are  $\Delta\text{HbR}$  contrast. Note that for all subjects, there is qualitative agreement between fNIRS and fMRI activations both in location as well as extent.

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## Comparison of Denoising Algorithms in fNIRS

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In this study, we compared the effectiveness of two denoising algorithms: wavelet based and band pass filtering. fNIRS data were collected by a continuous wave near-infrared spectroscopy device (NIROXCOPE 301), which was built in the Neuro-Optical Imaging Laboratory of Bogazici University. This device can sample 16 different channels on the prefrontal cortex using 10 detectors and 4 LEDs [2]. Several types of noise including systemic artifacts like blood pressure oscillations, respiration related, cardiac pulsation, and motion artifacts are known to be included in the fNIRS signal. Systemic artifacts generally correspond to frequencies higher than 0.08Hz while neuronal activity related signals in fNIRS data occupy the frequency range of 0.003-0.08Hz. Data set was obtained from 12 healthy subjects during performance of a Stroop task [1]. Two techniques were used to denoise [3] the fNIRS signal. Since the sampling rate of our data is 1.7 Hz the available frequency range is 0 to 850 mHz, We chose a decomposition tree for the discrete wavelet transform (DWT) with 8 levels. According to the frequency band of interest (0.003-0.08Hz), the details at levels 1, 2, 3 and the approximation at level 8 must be zero. As the band pass filter a 6<sup>th</sup> order butterworth filter was implemented in MATLAB<sup>®</sup> via the use of the built-in “butter” command with the pass band as (0.003-0.08Hz). We used signal to noise ratio (SNR) and normalized mean-squared error (NMSE) as criteria to evaluate the performance of these two methods [3]. We found that the SNR is higher and NMSE is lower in data denoised by wavelet method in comparison to band pass filtered data. The results of Daubechies 5 (db5) wavelet are shown in Table 1. Thus, band pass filtering should be avoided since it might compromise the phase response within the pass band. Wavelet algorithm seems to be a promising tool to eliminate the artifacts in fNIRS data while preserving the temporal dynamics of the hemodynamic response. Furthermore, DWT denoising seems not to favor any channels as observed from the coefficient of variation (COV) that is much lower for DWT. Hence DWT based denoising should be adapted as a standard preprocessing step for fNIRS data analysis.

Table1: The comparison of results between DWT and band pass filter

Method		SNR		NMSE		Method		SNR		NMSE	
		Band Pass Filter	DWT	Band Pass Filter	DWT			Band Pass Filter	DWT	Band Pass Filter	DWT
Channels	Ch.01	-2.21	4.42	0.11	-4.86	Channels	Ch.09	-0.50	8.08	-0.48	-6.80
	Ch.02	-4.05	1.53	-0.33	-3.25		Ch.10	-1.54	5.89	-0.33	-5.48
	Ch.03	-2.00	5.34	0.41	-4.83		Ch.11	-1.53	5.74	0.02	-5.43
	Ch.04	-1.34	5.85	-0.23	-5.51		Ch.12	-1.32	5.42	-0.27	-5.48
	Ch.05	-1.58	5.79	0.10	-5.23		Ch.13	-2.66	3.98	0.47	-4.43
	Ch.06	-0.68	7.01	-0.51	-6.28		Ch.14	-1.75	5.76	0.11	-5.75
	Ch.07	-0.43	8.22	-0.57	-6.67		Ch.15	-1.24	5.71	-0.24	-5.07
	Ch.08	-0.36	7.74	-0.67	-6.24		Ch.16	-0.99	6.39	-0.47	-5.93
Mean of the All Channels		-1.51 ±0.94	5.80 ±1.64	-0.18 ±0.35	-5.45 ±0.89						
		COV= 0.62	COV=0.28	COV=1.94	COV=0.16						

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## Wavelet Cross Correlation for Identification of Interference between Systemic Physiological Processes and Brain Haemodynamics measured by Time-Domain fNIRS during Frontal Lobe Activation.

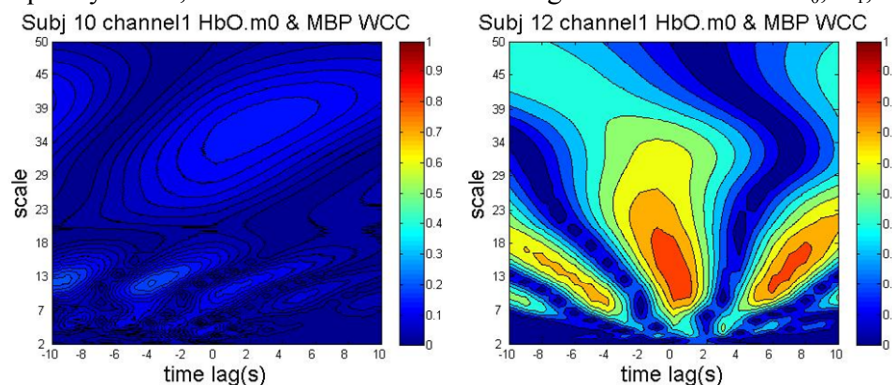
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**Background:** fNIRS is widely used to monitor brain activation, however the measured haemodynamic signals might not reflect the true cortical activation due to systemic signal fluctuations such as mean blood pressure (MBP), heart rate (HR) and skin blood flow (SBF) that can occur during the activation paradigm leading to false positive [1, 2]. In this study we utilise wavelet cross correlation (WCC) techniques to investigate the interrelationships between fNIRS and systemic signals during frontal lobe activation. **Method:** fNIRS concentration changes in oxy- and deoxy-haemoglobin (HbO, HbR) for four channels covering the frontal lobe and systemic signals (MBP, HR, SBF) were measured synchronously on 15 healthy subjects during continuous performance tasks. Changes in HbO and HbR were measured using a time-resolved system (PTB) [3] and analysing (i) the integral  $m_0$ , (ii) the mean time of flight of photons  $m_1$  and (iii) the variance  $V$  of distributions of time of flight of photons [3, 4]. **Results:** Subjects showed significant changes in systemic variables that correlated with the haemodynamic response and the activation. WCC demonstrated a large individual variability (see figure); however group analysis revealed that (i) the strongest WCC was observed in the Mayer wave band; (ii) the highest WCC was between HbO and MBP; (iii) there was a statistically significant difference in WCC between the channels over the left (ch. 1, 2) and the right (ch. 3, 4) frontal lobe; and (iv) the lowest WCC was observed in the fNIRS haemodynamic changes as estimated using the variance signal. **Discussion:** We demonstrated using WCC that systemic changes correlate with the fNIRS haemodynamic changes during brain activation and that this will be different between subjects, frequency bands, channel location and fNIRS signals obtained from  $m_0$ ,  $m_1$ ,  $V$ .



**Fig. 2.** WCC of HbO (m0) vs. MBP for the same forehead position in two representative subjects. The colour shows the correlation (0 to 1).

Note: R wave band:  $2 < \text{scale} \leq 7$  ( $0.15\text{Hz} < f < 0.4\text{Hz}$ ); M wave band:  $7 < \text{scale} \leq 17$  ( $0.06\text{Hz} < f < 0.15\text{Hz}$ ); Activation band:  $17 < \text{scale} \leq 45$  ( $0.022\text{Hz} < f < 0.06\text{Hz}$ ).

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# Influence of static and dynamic physiological parameters on the measurement of neural activation with functional near-infrared spectroscopy (fNIRS)

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## Abstract

We have conducted a simulation study in which we found a strong connection between fNIRS sensitivity and scalp-cortex distance (SCD). By simulating NIR light scattering and absorption in human head tissue models it could be shown that a high SCD leads to a decreased volume of light absorbing gray matter and therefore the sensitivity of fNIRS to measure hemodynamic changes in the cortex is decreased, while it is increased in the scalp. The head circumference, an easily assessable parameter, was positively correlated with SCD. [1]

We used the simulated volumes of light absorbing scalp ( $V_{\text{scalp}}$ ) and gray brain matter ( $V_{\text{gray}}$ ) to examine the feasibility of fNIRS to measure low frequency oscillations usually observed within resting state paradigms. We found the signal-to-noise ratio of fNIRS within a frequency window of [0.01, 0.02] Hz to be significantly correlated with  $V_{\text{scalp}}$  and within [0.02, 0.05] to be significantly correlated with  $V_{\text{gray}}$ . These findings suggest that fNIRS is feasible for resting state paradigms, but also that not the whole range of the low frequency window is accessible.

We also conducted a simultaneous fNIRS-fMRI study in which participants performed a working memory paradigm. We found the SCD to decrease the amplitude of hemodynamic responses to stimuli as measured by fNIRS. Beyond that, we observed a different impact of extracranial hemodynamics (as measured by fMRI) on fNIRS-signals. The signal that maps concentration changes of oxygenated hemoglobin (oxy-signal), was severely impacted by skin blood flow, whereas the deoxy-signal was hardly affected.

By conducting a simultaneous fNIRS-fMRI session during an inter-temporal choice paradigm, we found an interesting correlation between brain activation as measured by fMRI and a personality trait of the participating subjects. In contrast, this correlation could not be found with fNIRS. The influence of task-evoked extracranial signals impairing especially the oxy-signal may have been the limiting factor.

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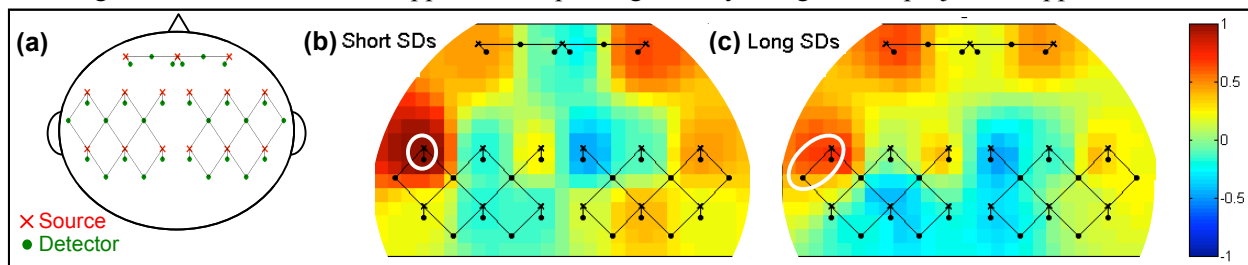
## Contamination of NIRS functional connectivity maps by superficial vasculature symmetries

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Resting-state functional connectivity is a relatively novel approach to study the brain functional networks, which relies on cortical spontaneous activity at rest rather than on activation tasks. The work originated in the fMRI BOLD community [1], but a growing number of studies over the past few years have shown NIRS imaging of functional connectivity [2,3]. A major difficulty of functional connectivity studies is the contamination by physiological signals not arising from neuronal origin [4]. The issue may be even stronger with NIRS because its surface measurements are highly sensitive to extra-cerebral physiological fluctuations. The use of short source-detector (SD) channels has proven a useful way to regress out superficial contamination in functional NIRS. Here we try to assess the contribution of superficial signals in NIRS functional connectivity maps by looking at short and long SD correlation patterns.

We developed a large symmetrical probe of 15 sources (690 and 830 nm) and 28 detectors that covers frontal, temporal and parietal regions, and that consists of both short (8mm) and long (30mm) SD channels (Fig.1a). We recorded resting state data for 20 minutes continuously on one volunteer. Raw intensities in each channel were converted into relative changes of oxy-(HbO), deoxy-(HbR) and total (HbT) hemoglobin concentrations using the modified Beer-Lambert law. Hemoglobin time traces were then band-pass filtered between 0.009 and 0.08 Hz. To minimize the effect of systemic effects, we regressed out from each short (or long) channel a common-mode signal obtained by averaging all short (or long) SD signals. We then created correlation maps of long channels only or short channels only, using the seed approach: the cross-correlation between one seed short channel and the rest of the short channels (fig1b), and one seed long channel and the rest of the long channels (fig1c) were computed. The resulting cross-correlations are mapped on the probe geometry using a back-projection approach.



**Figure 1.** (a) Probe geometry. (b) Correlation maps for short and (c) long SDs. The seed channel is indicated by a circle.

Figure 1 shows the correlation maps for HbT obtained with the short only and long only SDs with a nearby seed. The correlation maps are similar to the functional connectivity maps previously published in the NIRS literature. Interestingly, the short SD correlation map strongly resembles the maps for long SDs. In particular, homologous short channels are highly correlated, even though correlation within one hemisphere decreases with distance. We hypothesize that these strong correlations between homologous short channels result from symmetrical skin vasculature. This result suggests that NIRS-derived “functional connectivity” maps at least partly reflect superficial physiology. It further raises the issue of how to remove this contribution from the long SD correlation maps.

We will present results on more subjects and discuss the contamination of the functional connectivity maps by superficial systemic physiology, as well as possible approaches to detangle them.

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## Kernel distributed lag model applied to fNIRS recordings from visual cortex

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**Purpose.** A standard approach for analysing fMRI time series is to convolve the stimulus on-off waveform with an assumed haemodynamic response function (HRF), and then to perform a linear regression of the observed BOLD signal against the convolved stimulus. The same approach could be used for fNIRS, but it has been shown that the functions for HbO and HbR can have peaks at different times, and that the functions vary between observers. Ideally, besides the size and significance of the response to the stimulus, we would like to measure the HRF. We used the kernel distributed lag model (kDLM) to do precisely that. Using the kDLM permitted estimates of the HRF using a few components, smoothing the resulting HRF estimate in the process, and gave estimates of the strength of the relationship between stimulus and response.

**Methods.** Flickering bullseye gratings were presented in an on-off paradigm. The optode was placed over O1, and an ISS Oxiplex measured HbO and HbR responses. Almon (1965) proposed the original polynomial distributed lag model. We generalised this method to use kernels other than polynomials, including splines and discrete cosine transform components. The method was implemented in the statistical scripting language R.

**Results.** The distributed lag model using several kernels was applied to the data, yielding estimates of the kernel components and the statistical significance of each, and as well giving measures of the strength and significance of the relation between stimulus and response. Estimated HRFs were in line with those in the literature, but varied according to condition, subject, and chromophore, as was expected.

**Conclusions.** The kernel distributed lag model is a simple and effective way to simultaneously measure the HRF and the strength of association between the stimulus and fNIRS responses.

## Analysis of Task-Dependent Scalp Signal Contribution in fNIRS by Use of Reciprocal Information from fMRI

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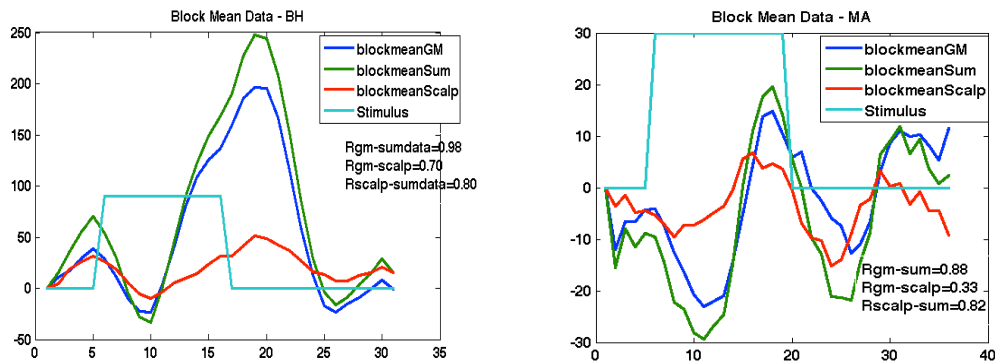
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**Introduction:** We aim to explore the contribution of the scalp layer signal to surface fNIRS measurements via the use of scalp and gray matter fMRI measurements. To this end we introduce an optically weighted spatial average of the fMRI BOLD signal for characterizing the scalp signal contribution to fNIRS measurements. We present two studies where spatially weighted BOLD signal from the superficial scalp tissue and gray matter (GM) tissues are compared for two different tasks to test the task dependence of this systemic contribution that is known to modulate the hemodynamic brain response.

**Method:** fMRI data were collected from 20 healthy subjects during 2 different protocols involving a breath-hold (BH) and a mental arithmetic (MA) task. Given the anatomical structure of the head from MRI, photon-migration theory and Monte Carlo techniques are used to calculate the Green's function describing the optical sensitivity profile to absorption changes in the underlying structures of the head. The overlap of this optical sensitivity profile with the MR images provides a means of predicting the relative contribution of each voxel to the surface fNIRS signal. Hence, the fMRI correlate of an fNIRS signal for a source-detector pair can be calculated as a “summed” signal as follows:  $y_i(t) = \sum_j A_s s_j(t) + \sum_k A_{GM} g_k(t)$  where  $y_i(t)$  represents the fMRI derived fNIRS signal with contributions from the “j” scalp voxels’ fMRI BOLD signals ( $s_j(t)$ ) weighted by a fixed  $A_s$  value (0.92) and “k” GM voxels’ fMRI BOLD signals ( $g_k(t)$ ) weighted by a fixed  $A_{GM}$  value (0.08). The raw fMRI signals were first preprocessed (realignment, slice timing correction, co-registration of the segmented anatomical image to the mean functional image) using SPM8 software and then subjected to a summation operation. Data are block averaged for four consecutive BH and MA sessions.

**Results and Discussion:** Average of 16 GM, 16 scalp and 16 “summed” signals are shown for two different tasks (BH and MA). GM signal change is larger (at least 10 folds) for the BH task compared to MA task as expected while scalp fMRI only has about two folds of increase in favor of BH task.



*Fig1.* Block mean of optically weighted sum, Gray Matter and Scalp data during i) BH and ii) MA task. X-axis is the scan number with 3 seconds of interval between each scan.

Correlations between the summed, scalp and GM signals elucidate the fact that no matter what the task is, correlation between scalp and summed signal is about 80%. Lower correlation between scalp and GM signal observed during MA task ( $R = 0.33$ ,  $p < 0.05$ ) in comparison to BH task ( $R = 0.70$ ,  $p < 0.05$ ), suggests that systemic contribution to the GM signal during MA task is relatively low compared to the contribution during BH task. This finding supports the hypothesis that systemic fluctuations have a task dependent influence on the hemodynamic response measured from GM.



Using Variable Hemodynamic Response Functions  
to Optimize Differential Temporal Information of Hemodynamics  
in Functional Near-Infrared Spectroscopy

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**Abstract:**

It has been nearly twenty years since functional near-infrared spectroscopy (fNIRS) was first applied to assessing human brain functions. It has now become widely accepted as a common functional imaging modality with more than 100 publications of fNIRS-related scientific literature annually. However, universal analytical methods for fNIRS data have yet to be established. Although not frequently mentioned, temporal analysis of fNIRS data also poses a technical challenge: how oxygenated and deoxygenated hemoglobin (Hb) signals should be treated. With its analogy to fMRI, a general linear model (GLM) with regression to a canonical hemodynamic response function (HRF) has often been used. However, the Hb parameters do not necessarily follow the same behavior as the BOLD signal: rather, we often encounter different temporal profiles for the two Hb signals. Here we introduce adaptive methods to find the optimal HRF for temporal analysis of fNIRS data.

In this study, application of the GLM with regression to temporally variable HRFs was applied to the fNIRS activation data during two different linguistic tasks: a Naming Task (NMT) and a Verbal Fluency Task (VFT). A variable HRF having the highest averaged  $t$  value was adopted as the most suitable for activation mapping. The optimal HRF revealed different temporal structures for oxy-Hb and deoxy-Hb signals, with the latter having substantial temporal delay for each linguistic task's data. In addition, optimized HRF for VFT data reflected increased diachronic load. However, when the temporally optimized HRF was used, the variable HRF parameters yielded reasonably compatible activation patterns including activation in classical language-related areas of the left hemisphere. These results suggest the potential use of the GLM with regression to an adaptive HRF to fully utilize temporal information of both Hb parameters.

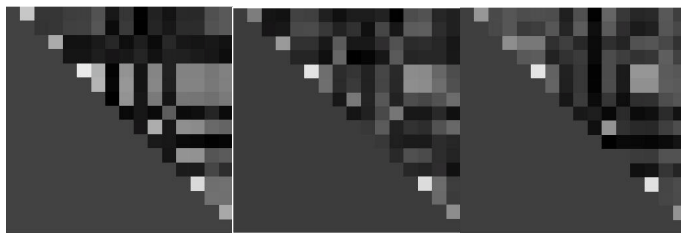
## Consistency of Functional Connectivity Maps

Mehmet Ufuk Dalmış<sup>1</sup>, Yasemin Keskin-Ergen<sup>1</sup>, Haluk Bingöl<sup>2</sup>, **Ata Akin<sup>1</sup>**

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Network analysis and study of statistical relations between activations of different brain regions has gained a considerable popularity in the last years. Functional connectivity is the term used to refer to statistical relations between activations of different regions in brain. Mostly weighted functional connectivity maps (graphs) are the initial results of functional connectivity studies. In this study, fNIRS signals are measured from the prefrontal cortex (PFC) region of 12 healthy subjects during a Stroop interference task via a 16 channel CW-fNIRS device (ARGES Cerebro, Hemosoft Inc., Ankara Turkey). This task consists of three different stimulus conditions: Neutral (N), Congruent (C) and Incongruent (IC). Mutual Information<sup>1</sup> (MI) between each channel is calculated for each type of stimulus to obtain the functional connectivity maps. A metric of “consistency” based on a 2D cross correlation (Equation 1) value is defined to indicate average similarity of different functional connectivity maps computed for a subject for the three conditions. It is found that average intra-subject consistency show high values ( $0.70 \pm 0.11$ ) while average inter-subject consistency is low ( $0.32 \pm 0.16$ ). This implies that the functional connectivity maps computed for subjects are characteristic per subject. In other words, each subject has their own connectivity pattern in PFC. High intra-subject consistency suggests that a fixed/stable PFC connectivity pattern exists for a Stroop task, which is substantially preserved throughout the recording session. The low inter-subject similarity (correlation) among the maps might be due to a mere different wiring patterns among subjects or systemic error since there is a lack of co-registration algorithm of probe placement on each subject.



**Figure 1.** Functional connectivity maps of a subject who has 0.71 consistency (The maps of 16X16 channels correspond to Neutral, Congruent and Incongruent stimulus conditions respectively).

$$r = \frac{\sum_m \sum_n (A_{mn} - \bar{A})(B_{mn} - \bar{B})}{\sqrt{\left( \sum_m \sum_n (A_{mn} - \bar{A})^2 \right) \left( \sum_m \sum_n (B_{mn} - \bar{B})^2 \right)}}$$

**Equation 1.** 2D Correlation of 2 rectangular images (FC maps). Diagonal and symmetric lower triangular entries are replaced with mean value of the upper triangle, in order to eliminate correlation bias introduced by them.

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Title: Enhancement of Hemodynamic Contrast in the Cancerous Breast by Carbogen Inspiration

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Hallmarks of the tumor phenotype include increased stiffness [1], enhanced angiogenesis with sluggish perfusion [2], increased vascular leakiness leading to increased interstitial pressures [3], and increased metabolic demand [2]. Separately, it is known that the vascular autoregulation mechanism normally achieves a tight coupling between the vascular supply and prevailing metabolic demand, but that the fidelity of vascular autoregulation may be attenuated in tumor tissue as a consequence of alterations in the vascular endothelium and surrounding vascular smooth muscle [2]. One consequence of this is that many tumor types operate on the brink of hypoxemia, suggesting that the otherwise enhanced supply actually is limited, perhaps as a consequence of disturbances in hydrostatic pressures caused by vascular leakiness and changes to the interstitium scaffolding [1].

Based on the preceding considerations, we hypothesized that manipulations of the oxygen supply-demand balance may produce responses that differ markedly between the tumor and surrounding healthy tissue. One approach that has recently been explored is the inspiration of carbogen [4]. While the carbogen response is tissue-specific, the most commonly seen response is vasodilation as a consequence of the effects of elevated CO<sub>2</sub> (elevated oxygen levels *per se* typically cause vasoconstriction) [4]. Here we explore the response of the healthy and tumor-bearing breast to a carbogen mixture consisting of 98% O<sub>2</sub> and 2% CO<sub>2</sub>, as a basis for producing additional modulation on the oxygen supply-demand balance.

Simultaneous bilateral breast imaging was performed using an imaging system recently described by Al abdi *et al.* [5], which provides for high optode-density dynamic fNIRS imaging, at rest and in response to physiological manipulations. Collection of measurements from both breasts simultaneously allows for subsequent use of paired difference analyses that cannot be considered using other fNIRS breast imaging systems. After giving informed consent and providing a brief medical history, research participants were seated and the sensing heads were adjusted to make good contact with both breasts. Following a five-minute baseline scan while room air was breathed, a facemask was applied and subjects breathed the carbogen mixture for an additional five minutes. Optical data were analyzed offline: application of a low-pass filter with a 0.2-Hz cutoff frequency was followed by use of the Normalized Difference Method to reconstruct tissue oxygen saturation (HbSat) and blood volume (HbT) images [6].

Imaging results obtained from 48 subjects (16 breast cancer, 18 benign pathology, 14 healthy control) are consistent with the hypothesis that carbogen and room air have different impact on microvasculature in healthy and tumor tissue, comparable to a previously reported effect seen when comparing pure oxygen and carbogen [4]. In particular, we have found that tumor tissue shows a larger drop in HbT and concomitant rise in HbSat in comparison to healthy tissue. Also noteworthy is the finding that image contrast is substantially improved by transforming the (HbSat, HbT) image values to a measure of the statistical extremeness (i.e., the Mahalanobis distance [7]) for each pixel. Furthermore, the preceding effect is enhanced by referencing the image-pixel data of one breast to the distribution of image values for the contralateral breast. This is a concrete demonstration of the above-mentioned utility of the simultaneous dual-breast measurement approach. Thus we have demonstrated that controlled manipulation of the tissue oxygen supply-demand balance can enhance the detectability of breast cancer by exploiting known physiological abnormalities of tumor tissue.

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Region-Specific Cortico-Cortical Synchronization and Desynchronization of Hemodynamic Changes during Auditory Processing in Young Infants

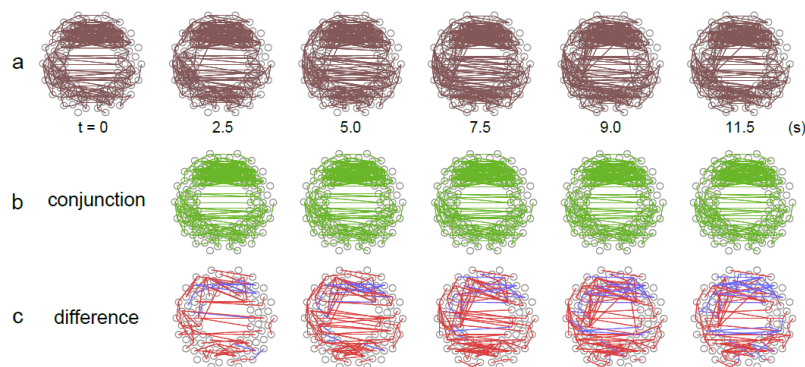
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Several near-infrared spectroscopy (NIRS) studies on cortical hemodynamic responses to auditory stimuli in sleeping infants have shown that averaged signals over trials exhibit significant responses not only in the auditory area but also in diverse cortical regions. In contrast, studies focusing on the sleeping state of young infants have shown spontaneous fluctuations of hemodynamic changes throughout the cortical regions even when no stimuli were presented. However, little is known about the interactions between stimulus-induced responses and spontaneous activities.

In the current study, we measured oxy-Hb signals of 19 infants by using a 94-channel NIRS instrument. The measurements were performed while the infants were asleep. We used a 1-s buzzer sound as the stimulus, and it was presented 20 times. The measured signals were band-pass filtered (0.05 – 0.1 Hz). First, the filtered time course signals were split into blocks of 25 s. By averaging the changes in the oxy-Hb signals over the data blocks for all infants, we obtained hemodynamic responses for each measurement channel. Second, we decomposed the hemodynamic signals into instantaneous amplitudes and phases, and assessed phase synchronizations among cortical regions to examine the influence of the stimulus on phase synchronization properties.

The averaged oxy-Hb signals were in agreement with those reported in previous studies that showed increases in oxy-Hb signals in infants' brain in response to auditory stimuli over broad regions, including the frontal, temporal, and occipital cortices. On decomposing the signals into amplitude and phase, we found that the amplitude of the signals increased in almost all regions, whereas phase synchronization index increased only in some parts of the temporal and occipital regions. These results suggest that the major determinant for the response to the auditory stimulus was an increase in the amplitude of signals in broad regions of the infants' cortex. Furthermore, auditory stimulus temporally induced synchronization among diverse regions and desynchronization within frontal regions. This result indicates that external inputs modify the resting-state cortical network for generating spontaneous activity.



**Fig. a:** Time evolution of highly synchronized connections. **b,c:** Unchanged and changed synchronized connections. Conjunction and difference were calculated by comparing connections between two time points: the time of stimulus onset (0 s) and each time point (2.5, 5.0, 7.5, 9.0, 11.5 s). The green line shows synchronized connections at both time points (b, conjunction). The red and blue lines show induced synchronization and desynchronization, respectively (c, difference).

## The importance of motion artifacts correction in cognitive studies

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Motion artifacts are a significant source of noise in many fNIRS measurements, particularly when infants or patients with particular diseases (for example stroke) are under examination. Motion artifacts are also common when healthy subjects are the participants of the experiment. Motion artifacts can have different shapes and duration and their presence can compromise the quality of the signal acquired. During cognitive experiments, moreover, they can compromise the hemodynamic response estimation, leading to incorrect results. One solution would be to disregard the data around the motion artifact; however, in situation where the number of trials available is already low, its further reduction could be problematic. Many methods for motion artifact correction have been proposed in the literature during recent years, such as Kalman filtering [1], Wavelet analysis [2], spline interpolation [3], and Correlation Based Signal Improvement (CBSI) [4] but also more general methods have been used for the purpose, for example principal component analysis (PCA) [5]. Cooper et al. [6] have recently validated these motion artifact correction methods on synthetic data generated by adding a simulated hemodynamic response to real resting state NIRS data.

Here, we have applied a number of motion correction algorithms proposed in the literature to real NIRS data acquired during a cognitive study. The paradigm was an event-related change-detection task, where the participants read aloud the colour of words presented on a screen. The movement of the jaws during speech resulted in motion artifacts which were temporally correlated with the stimulation. In order to reduce motion artifacts, we applied to this dataset PCA, spline interpolation, a combined method composed of PCA followed by the spline interpolation and the CBSI algorithm. We compared the results obtained with these four methods with that obtained both without any motion correction and that obtained by rejecting all the trials where a motion artifact was found.

We will address the utility of each method and discuss whether it is generally applicable or requires a particular type of motion artifact in the data. We will quantify the standard deviation between hemodynamic responses in the computation of the group average mean hemodynamic response and show its reduction in the data where motion artifacts were corrected. We will compute parameters related to the hemodynamic response curve (e.g. AUC (area under the curve)) and show how the hemodynamic response estimated from the motion corrected data results more physiological compared to the one obtained from the data without motion correction.

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## Model enhanced interpretation of NIRS signals in brain injured patients.

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Cerebral hypoxia-ischaemia following acute brain injury is a key concern and focus for therapy in critical care. However prevention, prediction and intervention is problematic. The underlying pathophysiology that results in secondary injury is complex and neuromonitoring only measures indirect surrogates of the processes of interest. Near infrared spectroscopy (NIRS) is a non-invasive optical technique that measures surrogates of cerebral haemodynamics and metabolism and might be a valuable tool if the complexity of the physiology encoded within NIRS signals can be decoded. Previously we have applied a mathematical model [1] to aid interpretation of NIRS signals during oxygenation changes in healthy volunteers and to characterise cerebral autoregulation in brain injured patients. In this work we present a mathematical model of cerebral biomechanics, haemodynamics, oxygenation and metabolism focused on the analysis of NIRS in brain injured patients. Systemic monitoring (blood pressure, carbon dioxide, arterial oxygenation) serve as model inputs producing simulated outputs for a range of neuromonitoring: NIRS, intracranial pressure (ICP) and transcranial Doppler flow velocity in the middle cerebral artery (Vmca). Model parameters reflect pathophysiology and are modified to reproduce measured signals - hence predicting key physiological abnormalities that explain the observed data. Changes in cerebral autoregulation of blood flow, cerebral compliance and metabolic demand are frequently associated with cerebral hypoxia-ischaemia and are represented by model parameters. Figure 1 demonstrates model based interpretation of NIRS ICP and Vmca in a brain injured patient, predicting impaired autoregulation, reduced compliance and reduced metabolic demand. Further clinical examples will be presented which demonstrate a range of complex interactions between these mechanisms which are manifest in NIRS and other neuromonitoring signals. Patient specific physiological modelling has the potential to predict the key biomechanical, haemodynamic and metabolic changes following brain injury in individual patients, and might be used to inform individualised treatment strategies.

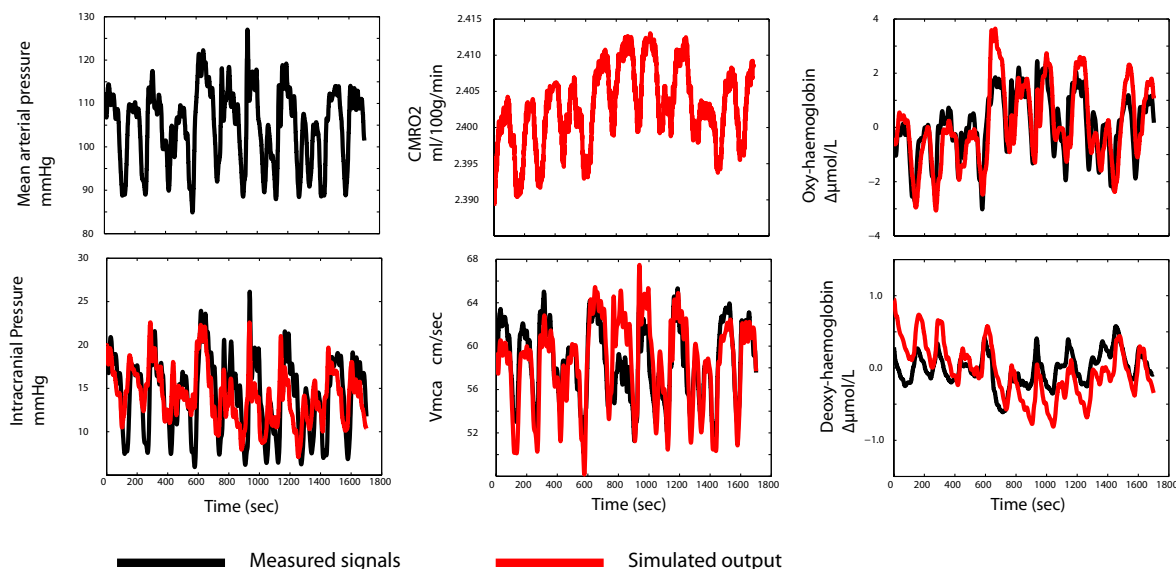


Figure 1. Model based interpretation of NIRS (oxy-haemoglobin, deoxy-haemoglobin), ICP and Vmca in a brain injured patient. Cyclic slow wave activity is seen driven by mean arterial pressure changes. Model parameters suggest pathophysiological changes are required to explain the NIRS, ICP and Vmca signals: reduced autoregulation ( $k_{aut}$ , 7% basal), impaired cerebral compliance (elastance $k_E$ , 35% basal) and reduced cerebral metabolic demand ( $u$ , 17% basal).

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## GLM based detection of fast optical signals in visual cortex

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Fast optical signals (FOS) rely on the hypothesis that electrical activity of single neuron is accompanied by synchronous (at least on the hundred milliseconds scale) changes of NIR light scattering properties of activated neurons. By capitalizing on these changes, Gratton et al. (1995) proposed that fast optical signals - also called Event Related Optical Signals - could localize *in vivo* brain activity with a temporal resolution of 20 ms or less. During the last 15 years, there have been several attempts to record the evoked FOS noninvasively through the scalp and skull in human subjects (see Gratton, 2010, for a review). The results of these studies, however, have been largely controversial because of the very low SNR, which imposes large number of repeated trials for evaluating grand average responses (Steinbrink, 2005).

We propose the use of a GLM approach. Since there is no previously defined Impulse Response Function (IRF) for FOS, we tested the reliability of the method by adopting an on-off square IRF, with a variable onset delay after the stimulus delivery. We first ran simulated experiments to evaluate the reliability of applying GLM to FOS. Then, we applied GLM to both FOS and standard hemoglobin signals (HS) obtained during a hemi-field visual stimulation, both kinds of signals being recorded by means of a frequency-domain optical system. Through the analysis of the simulated data, we demonstrated the feasibility of applying GLM analysis to FOS in order to properly recover the expected cortical activations. In particular, the method performed better than the grand average event-related approach for measurements characterized by typical SNR for *in-vivo* phase measurements and as low as 0.07. For SNR = 0.05, GLM correlation value with the simulated activation channel scheme was as high as 0.9.

Ten healthy volunteers (age: 25-40 years, mean: 26) were enrolled in the *in vivo* experiments. The stimulus was a canonical reversing black and white checkerboard. We used a commercial frequency-domain 20-channels oximeter. Our experiments showed that the contralateral activation of visual cortex, easily proved by using GLM method to HS, could be also highlighted by applying GLM to FOS, pending the assumption of rectangular IRF, lasting 30 ms with 80- 100 ms delay with respect to the stimulus onset.

Our FOS values reported time delays of optical signal quantitatively in agreement with previous studies on occipital cortex during visual stimulation for both order of magnitude (i.e., few picoseconds) and time delay signal peak after visual stimulation (Gratton, 2010).

Application of GLM to FOS seemed to perform better than other method so far used for processing FOS, especially grand average approaches and frequency domain analysis. The method appeared reliable even in the disadvantageous conditions of low SNR, still being capable of identifying visual activation in single subject analysis.

The results from our study seem to confirm that optical local properties, and particularly diffusion properties through the scattering coefficient, present variations on a temporal scale of a few tens of milliseconds, likely associated with neural activity.

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## Continuous correction of differential path length factor in near-infrared spectroscopy

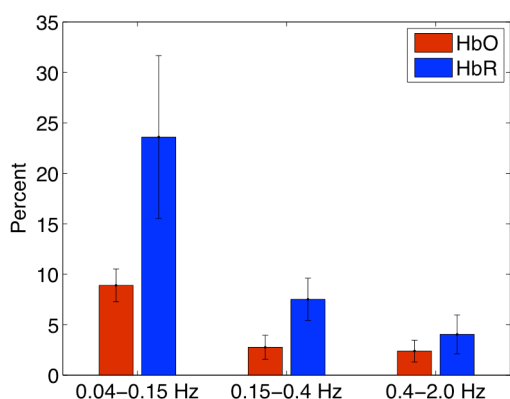
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In continuous wave near-infrared spectroscopy (CW-NIRS), changes in the concentration of oxyhemoglobin ( $\Delta HbO$ ) and deoxyhemoglobin ( $\Delta HbR$ ) can be calculated by solving the modified Beer-Lambert Law (MBLL) (Cope et al. 1988). Application of MBLL in CW-NIRS requires prior knowledge of the wavelength dependent differential path length factor (DPF), which rescales the geometric distance between source and detector optodes to the mean photon path length. Accurate DPF values are important if quantitative estimates of  $\Delta HbO$  and  $\Delta HbR$  are desired. Furthermore, systematic errors in the selection of DPF can introduce crosstalk between  $\Delta HbO$  and  $\Delta HbR$  estimates (Strangman et al. 2003). DPF values cannot be directly measured with CW-NIRS and can vary by wavelength and across subjects due to differences in anatomical structure and tissue composition of the head. In the present study, we introduce an application of the extended Kalman filter (EKF) to continuously estimate a DPF correction term in CW-NIRS. We show using simulated and experimental four-wavelength NIRS data that this approach compensates for inaccurately assumed DPF values and corrects the crosstalk that would otherwise enter  $\Delta HbO$  and  $\Delta HbR$  estimates.

Our EKF model has state variables for  $\Delta HbO$  and  $\Delta HbR$  and a nonlinear DPF correction term. EKF filter parameters were tuned using simulated NIRS by minimizing the residual error between known and estimated  $\Delta HbO$  and  $\Delta HbR$  from correcting relative changes in DPF values ( $\Delta DPF$ ) at three wavelengths (690 nm, 785 nm and 830 nm) with respect to the DPF value at 808 nm. The tuned EKF



**Fig 1.** Cross-talk error corrections in  $\Delta HbO$  and  $\Delta HbR$  from the application of the proposed EKF algorithm. Mean percent correction and standard error shown for three frequency bands.

was then applied to experimental NIRS data collected from 3 human subjects. The results are compared with the solution obtained using a weighted least squares (WLSQ) technique (Huppert et al. 2009). Residuals for the EKF and WLSQ methods are compared in 3 frequency bands (0.04-0.15 Hz, 0.15-0.4 Hz and 0.4-2.0 Hz). Cross-correlation coefficients between residuals at different wavelengths are evaluated as an indication of crosstalk. We also quantify the mean percent deviation of the EKF hemodynamic signals from the WLSQ hemodynamic signals (Fig. 1), which indicates how much correction the EKF contributes in reducing cross-talk error in  $\Delta HbO$  and  $\Delta HbR$ . Results indicate that the mean cross correlation in residuals is lower in EKF compared to WLSQ (ANOVA,  $p < 0.001$ ). The average reduction in cross-talk error over all frequency bands was 4.7% for  $\Delta HbO$  and 11.7% for  $\Delta HbR$ . The proposed EKF algorithm is able to provide more reliable estimates of hemodynamics and reduce cross-talk errors that may arise in spectroscopic calculations from using wrongly assumed differential path length factors.

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## Segmentation of magnetic resonance images for individual head models for DOT

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In diffuse optical tomography (DOT), the light propagation analysis in head models is essential to estimate the spatial sensitivity profiles of probe pairs. Recently, the anatomical structure of the head models tends to be based on magnetic resonance (MR) images of the head. Since the details of the geometry of the head structure vary in individuals, it is desirable that the head model for each subject be constructed from their own MR head images. During the construction of the head models, the segmentation of the MR head images is a time consuming process. The fast and automatic segmentation of the MR head image is of interest for the construction of the individual head models.

In this study, we chose the pulse sequences which can acquire adequate MR images to segment different types of tissues in the head and construct an individual head model for the light propagation analysis for DOT. All the MR experiments were performed with a 3.0-T clinical MR system (SignaHDx 3.0; GE Healthcare, Milwaukee, WI). Figures 1(a)-1(c) show a slice of the MR images acquired by the different pulse sequences; (a) T1-weighted, (b) fat-saturated proton-density-weighted (FSPDW), and (c) fast imaging employing steady-state acquisition (FIESTA). The individual head model consisted of six types of tissues, such as the scalp, skull, cerebrospinal fluid (CSF), sagittal sinus, grey matter and white matter. The scalp and skull regions were segmented from the FSPDW images, and the CSF region was segmented from the FIESTA images. The boundary between the grey matter and white matter was extracted from the T1-weighted images. The sagittal sinus was segmented from the images of the MR angiography shown in Fig. 2. During the segmentation process, the images were binarised by the region-growing approach. After the binarisation, the noises in the binarised images were removed by morphological processes. All the segmentation processes were semi-automatically conducted. The individual head model for the light propagation analysis for DOT constructed from the MR images is shown in Fig. 3.

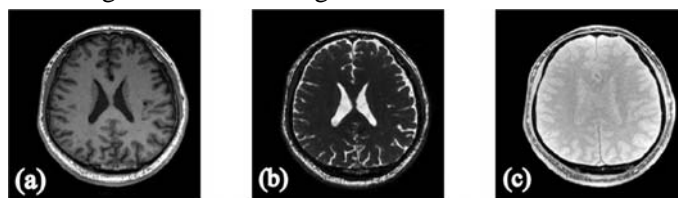


Fig. 1 A slice of MR images acquired with (a) T1-weighted, (b) FSPDW and (c) FIESTA.

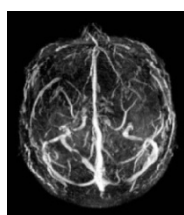


Fig. 2 Image of MR angiography.

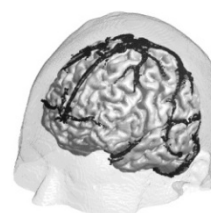


Fig. 3 Head model constructed from MR images.

## Development of a flexible neurofeedback system for brain-machine interface using fNIRS

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<sup>2</sup> Hitachi, Ltd., Advanced Research Laboratory, Japan

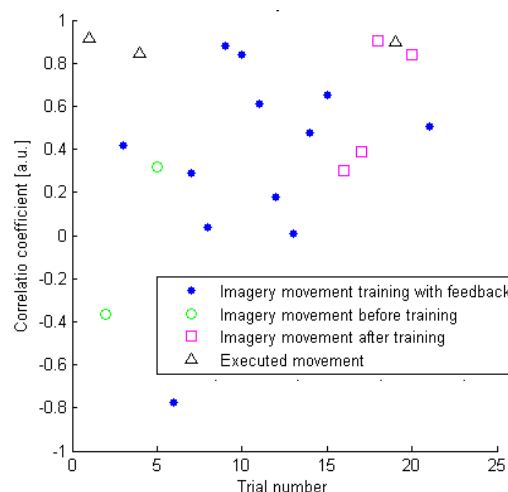
**Introduction:** Brain-Machine Interface (BMI) allows users to communicate with external devices through thought processes alone. There is an increasing interest in the use of fNIRS for BMI as a tool to detect both brain conscious activation and enhance neurofeedback. fNIRS measures the haemodynamic and oxygenation response secondary to brain electrical activation and as such the signal can also be affected by brain physiological changes due to systemic physiological fluctuations [1]. Here we present a new signal analysis method that will improve identification of activation and provide real time feedback to the subject to enhance neurofeedback. The system is designed as a plug-in for the Platform for Optical Topography Analysis Tools (POTATo) [2] implemented in MATLAB.

**Methods:** The analysis consists of two stages aimed at identifying inter-channel hemodynamic correlation and then testing the neurofeedback performance. The first experiment identifies the desired activation area followed by a no-task experiment aimed at measuring inter-channel correlation during systemic changes. Using the identified channel pairing a more accurate activation signal is obtained while accounting for systemic changes. The selected activation channels are then used for visual feedback during training experiment. The validity of the procedure is assessed by comparing fNIRS signals during executed movement and imagery movement.

**Results:** The correlation coefficient of the measured signal during experiment trials and the measured signal in the sensorimotor channels during executed movement for one of the subjects is presented in the figure. In the presented data the learning effect can be observed with the motor imagery trials at the end of the experiment show higher correlation with executed movement than initial motor imagery trials.

**Discussion:** Off-line analysis shows task related signal improvement in all subjects during the feedback sessions both in terms of magnitude and correlation.

The experimental results are in agreement with previously published papers showing enhanced motor imagery related haemodynamic cortical activation [3].



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Artifact removal for assessment of cross-network anticorrelation with fNIRS

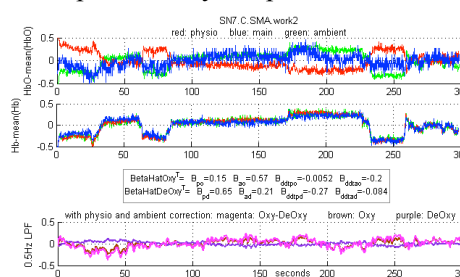
Authors: **Angela Harrivel**<sup>1</sup>, Luis Hernandez-Garcia<sup>2</sup>, Scott Peltier<sup>2</sup>, Douglas Noll<sup>2</sup>

The end goal of this project is to detect potentially hazardous resting states during attention-demanding tasks in near real time with Functional Near Infrared Spectroscopy (fNIRS) using probes placed at superficial nodes of the attentional (ATN) and default mode networks (DMN). Functionally-connected networks in the resting state have been detected with fNIRS (White, 2009; Sasai, 2012). It may be possible to detect cross-network anticorrelation as well, using only single point measurements made at network nodes. We propose that an increase in anticorrelation between the default network and the attentional network may be a powerful indicator of reduced attention to task. However, correlation measures can be compromised by motion artifact and masked by local physiological contributions. Hence, operational or ambulatory application requires the application of algorithms and filters for the removal of unwanted signal. Here we introduce a computationally simple correction method for ambient and physiological signal component reduction prior to correlation assessment.

Data were collected at 6.25Hz (Imagent, ISS, Inc.) from consented subjects resting 8 minutes with eyes open. Probes were placed at the dorsolateral prefrontal cortex (dlPFC), supplementary motor area (SMA), medial frontal gyrus (MFG) and angular gyrus (AngG) using the I10-20 system for localization. The signal processing steps are as follows.

*First*, all traces were normalized and mean centered.

*Second*, the traces from a detector channel with no source (e.g. above in green) and their time derivatives were used to model and remove unwanted contributions to the signal of interest due to probe motion and ambient light exposure using standard linear regression (output in lowest panel above). *Third*, traces from a secondary source close to and in line with that probe's detector, which only sampled superficial tissue (above in red), were used to measure physiological fluctuations. As a first-order correction, the physiological traces were subtracted (as in Zhang, 2007, eq. 5) from the hemoglobin traces of interest (above in blue). *Fourth*, the result was filtered to include 0.01Hz to 0.08Hz using an equiripple FIR zero-phase filter to examine frequencies corresponding to the hemodynamic response. *Fifth*, correlation coefficients (CC) for same-species trace pairs over the full time course were computed, and averaged over 6 subjects to identify anticorrelation.



Results are presented in the table below. The CC for the oxygenated hemoglobin (HbO) trace pairs were positive for all within-network pairs, and negative for half of the between-network pairs. The deoxygenated hemoglobin (Hb) trace pairs showed in network correlation and cross-network anticorrelation for one probe on each network. CC for traces without physiological correction were all positive, showing no network-consistent patterns.

CC, N=6	DMN:	DMN:	ATN:	DMN:	DMN:	ATN:
	rMFG, HbO	rAngG, HbO	lSMA, HbO	rMFG, Hb	rAngG, Hb	lSMA, Hb
rDMN: AngG	0.19±0.46			-0.028±0.35		
lATN: SMA	-0.28±0.41	-0.20±0.44		-0.204±0.33	0.128±0.45	
rATN: dlPFC	0.13±0.35	-0.06±0.31	0.16±0.45	-0.082±0.41	0.186±0.30	0.270±0.42

We conclude it may be possible to detect cross-network anticorrelation, but physiological contributions to the measurements are dynamic, and static removal is not universally effective (Zhang, 2009). Thus, the implementation of an adaptive physiological filter is planned to improve state detection accuracy and network correlation measures to support this ongoing human subject study.

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Title: A Computing Environment for Multimodal Integration of EEG and fNIRS

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Following the brain's own tendency to integrate multiple sensory modalities (visual, auditory, somatosensory, etc.), multimodal integration of neuroimaging techniques has been a recurring theme in the field. Here, the combination of electroencephalography (EEG) and functional near infrared spectroscopy (fNIRS) is considered. A principal reason for the interest in EEG-fNIRS is the expectation that evaluation of neurovascular coupling can have practical utility in, e.g., studies of the alpha rhythm [1], or of epilepsy [2]. In addition, noninvasive detection of an fast optical signal (FOS), having a time course similar to an event-related potential (ERP) and resulting from changes of scattering properties in neural tissue [3], has been a topic of considerable interest [4], but also of controversy owing to its low signal-to-noise ratio [5]. However, a recent report used simultaneous ERP and fNIRS measurements to demonstrate that concurrent EEG may facilitate FOS detection [6].

A requirement for integration of EEG and fNIRS, which depend on different physical properties (EEG – conductivities; fNIRS – absorption and scattering coefficients) of the same head tissues, is forward models that can be used for estimation of neuroelectric sources or cerebral hemodynamic states in a common anatomical space (e.g., derived from structural MRI). To address this need, we have introduced NAVI [7,8], a MATLAB-based environment that supports many of the principal data transformations common to evaluation of bioelectric and hemodynamic studies, and is geared mainly toward supporting atlas-based parametric mapping with full 3D tomographic capabilities. The package includes modules for image formation, display and analysis; an electronic ledger that automatically records metadata associated with the various data transformation resources; and a number of utilities modeled principally after strategies supported by SPM8 [9,10]: GLM-based parametric mapping of detected hemodynamic response functions; atlas-based mapping of image findings onto identified brain regions, with an automated anatomical labeling functionality; and examination of effective connectivity via strategies such as dynamic causal modeling [11]. The data analysis environment also includes the EMSE Suite (Source Signal Imaging, Inc.), which comprises software modules for integrating EEG with structural MRI [12]: spatial mapping of sensor positions and MRI co-registration; review of EEG data, with various spatial and temporal filters for treating artifacts; mapping signal-space measures topographically onto the head surface; computing and displaying solutions to the cortical current-density inverse-problem; display of MRI data, with tissue segmentation capabilities; mesh generation based on segmented MRIs; and statistical nonparametric mapping, via randomization of experimental conditions, in either signal space or source space.

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## Group level analysis methods in NIRS

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**Introduction:** We have developed new analysis methods for statistical inference, image reconstruction, and group level analysis for NIRS imaging. This analysis pipeline extends from methods previously introduced in the fields of fMRI and EEG/MEG analysis of functional imaging data. The key steps of our analysis pipeline are outlined in figure 1.

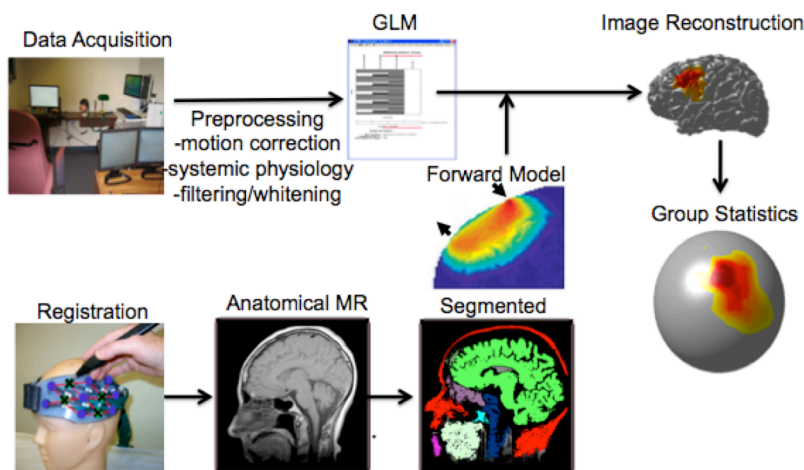


Fig 1. Overview of the steps of NIRS analysis.

register the NIRS cap to anatomical volumes. These NIRS tools make use of several existing similar tools developed for EEG and MEG registration.

- Once registered to anatomical volumes, finite element or monte carlo methods are applied to generate the optical forward model. Registration and segmentation tools from MRI and EEG/MEG from FreeSurfer and the MNE pipeline have been interfaced for NIRS analysis.
- Tools for tessellation and wavelet representation of the structural MRI are implemented as part of the image reconstruction method.

### Preprocessing

- New methods for motion correction based on combined wavelet and independent component analysis (ICA) have been developed to deal with both spike and shift types of NIRS artifacts
- A new approach based on single-channel ICA analysis has been used to characterize and remove physiological noise in NIRS data.
- Data-basing tools for management of NIRS subject and study information (including multimodal data) have been developed.
- A new GUI called NIRSviewer was built to allow visualization of the NIRS data (fig 2).

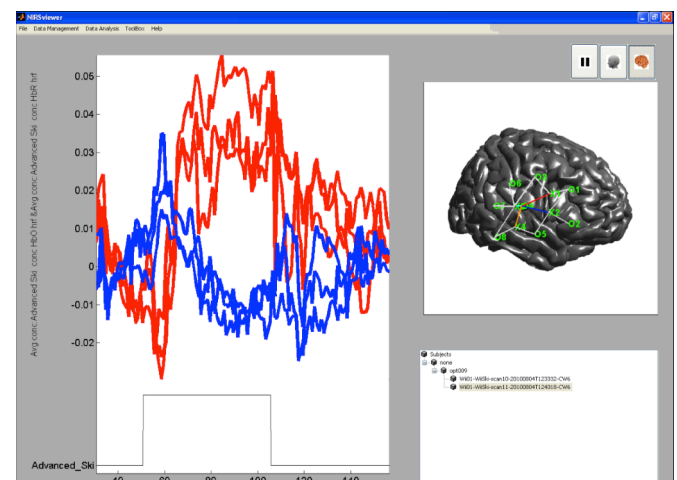


Fig 2. Screen shot from the new NIRSviewer

## Morphological modification of brain structure for optical brain activation imaging

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The inverse problem in optical brain activation imaging is normally ill posed and the solution is not unique. A priori information of the anatomical structure of the head is incorporated into the inverse problem to improve the accuracy of the image reconstruction. In this study, the adequate geometry of the brain surface in the head model to predict the spatial sensitivity profile for the inverse problem is investigated in order to improve the optical brain activation imaging.

Figure 1(a) shows the geometry of the brain surface segmented from the magnetic resonance (MR) head images. The longitudinal fissure and sulcus structure are clearly observed in the brain surface. The spatial sensitivity profile for the source-detector pair shown in Fig. 1(a) was predicted by a Monte Carlo simulation and is shown in Fig. 2(a). The spatial sensitivity profile in the model with a simple geometry, such as a homogeneous model, is symmetrically distributed with respect to the line connecting the source and detector while the spatial sensitivity profile shown in Fig. 1(a) is distorted by the uneven thickness of the superficial tissues and the geometry of the brain surface. The spatial sensitivity significantly decreases around the sulci and the sulcus structure is clearly observed in Fig. 2(a). The measurement points in the common imaging systems are sparsely distributed and they cannot resolve the spatial frequency of the spatial sensitivity profile including the sulcus structure. The high frequency component may cause errors in the reconstructed images. The geometry of the brain surface smoothed by a morphological close operation is shown in Fig. 1(b). The sulci are plugged, however, the primary geometry of the brain surface still remains in the model. The spatial sensitivity profile estimated from the model including the smoothed brain is shown in Fig. 2(b). The high frequency component in the spatial sensitivity profile around the sulcus structure is removed while the distortion caused by the anatomical structure of the head remains in the spatial sensitivity profile.

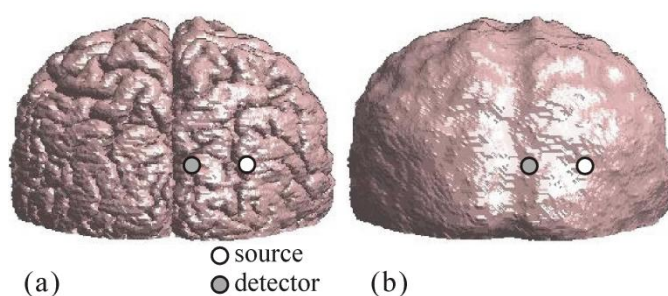


Fig. 1 Geometry of brain surface.  
(a) precise, (b) smoothed.

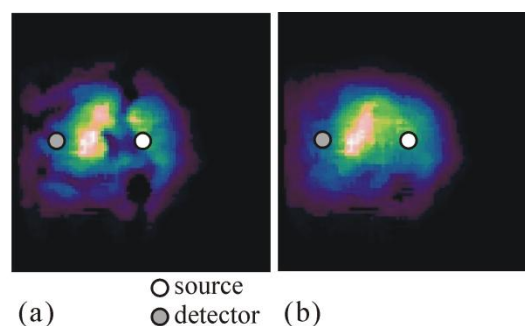


Fig. 2 Spatial sensitivity profile obtained by  
(a) precise model, (b) smoothed model.

## Correlation based signal improvement (CBSI) combined with Motion artifact removal algorithm (MARA) for enhancing synthetic fNIRS signals

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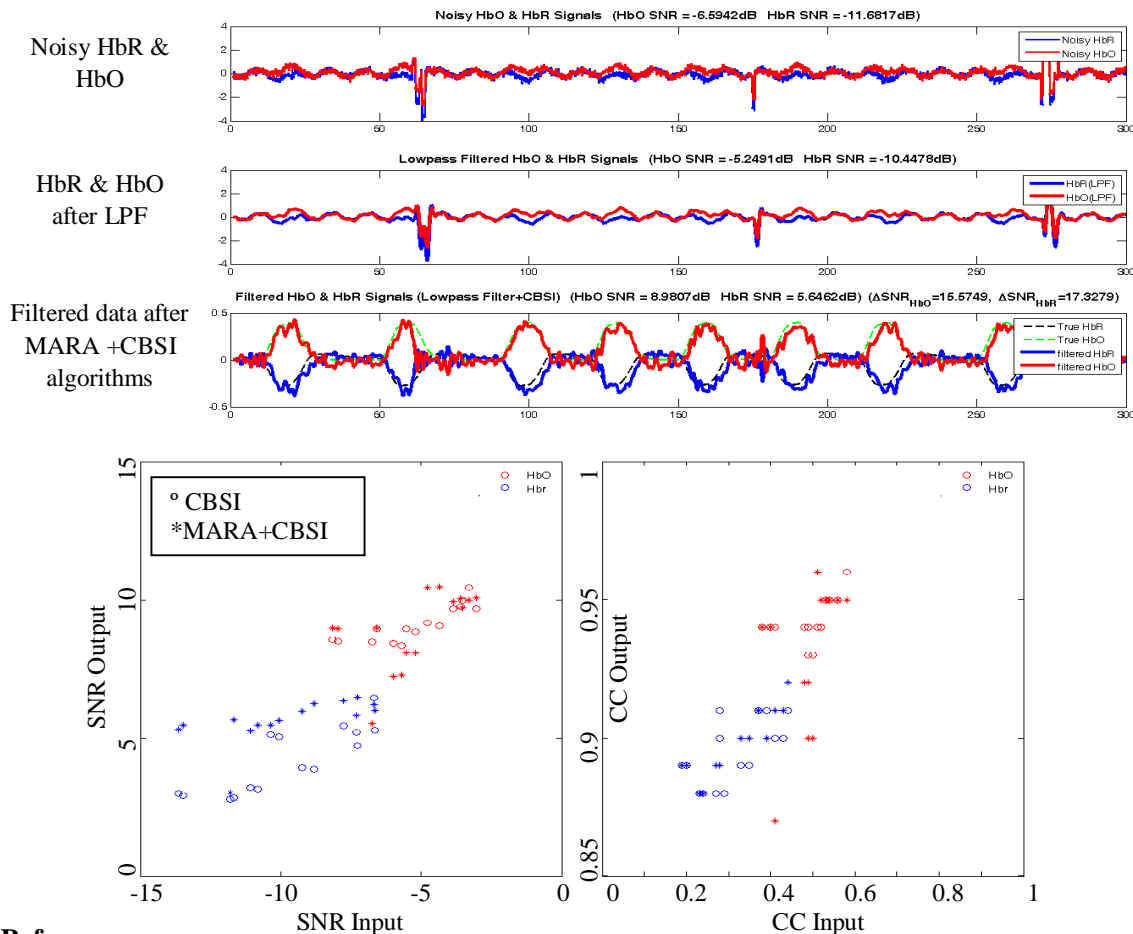
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**Abstract:** A growing number of algorithms are being developed for fNIRS noise reduction and signal improvement. Correlation based signal improvement (CBSI) algorithm has been developed by Cui et al [1] based on the hypothesis that oxy-deoxy Hb are negatively correlated during neural activation. In this study we combine CBSI with motion artifact removal algorithm (MARA) [2] and test this modified algorithm on synthetic fNIRS signals.

### Material and Methods:

We used the balloon model to simulate true oxy-deoxy Hb signals without noise and then add instrument, physiological and experimental errors to generate synthetic fNIRS data.

**Results and Conclusion:** results show that by combining MARA and CBSI algorithms we can reach a higher SNR for HbR signal when correlation coefficient (CC) of the output signal remains constant in contrast to using only CBSI algorithm.



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## Quantitative indexes of artifacts for NIRS signals

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**Introduction:** The modified Beer-Lambert law (MBLL) is used to describe the changes in light attenuation in scattering media. The differential form of MBLL (dMBLL) is widely used in near-infrared spectroscopy (NIRS). By solving its simultaneous equations, NIRS signals (changes of the product of the hemoglobin concentration and the partial path length during functional activation of the cerebral cortex) are calculated. The dMBLL is based on some assumptions: (1) the absorbance changes are attributed to the only oxygenated and deoxygenated hemoglobin, (2) the absorbance is linear with the concentration changes, (3) the absorption changes homogeneously, (4) the wavelength dependence of the path length is negligible, (5) the path length is constant, (6) the scattering loss is constant and (7) the absorbance changes caused by changes in coupling between the fibers and the subject's head surfaces (moving, sweat, etc.) is negligible. In the head model, however, the multi-region activations in the multi-layer structure should be considered and these assumptions should be investigated. In this work, we propose some quantitative indexes of artifacts for NIRS signals caused by these assumptions.

**Methods:** We used a continuous NIRS imager with three wavelengths (FORE-3000, Shimadzu) and defined the root-mean-square difference (RMSD) of NIRS signals ( $RMSD = \sqrt{(\Delta X_{1,2} - \Delta X_{2,3})^2} + \sqrt{(\Delta X_{2,3} - \Delta X_{3,1})^2} + \sqrt{(\Delta X_{3,1} - \Delta X_{1,2})^2}$ , where  $\Delta X$  means oxygenated or deoxygenated hemoglobin changes). These indexes reflect the differences (discrepancy) among solutions which satisfy combination of any two dMBLL simultaneous equations out of three. Firstly, we calculated RMSD by simulating various wavelength-dependent absorbance changes due to any other causes than hemoglobin concentration changes. Then we estimated RMSD experimentally under some conditions, such as changing an angle of a light guide on a phantom surface, dropping oil into the space between a phantom surface and a light guide and a subject's head movement.

**Results:** RMSD calculated by simulating absorbance changes due to any other causes than hemoglobin concentration changes changed largely, though the NIRS signals were typical for brain activation (Fig.1). In the experiments of changing the angle of the light guide, dropping oil and the subject's head movement, significant changes in RMSD were observed (data not shown).

**Conclusions:** RMSD are useful as quantitative indexes of artifacts for NIRS signals caused by some assumptions of the dMBLL.

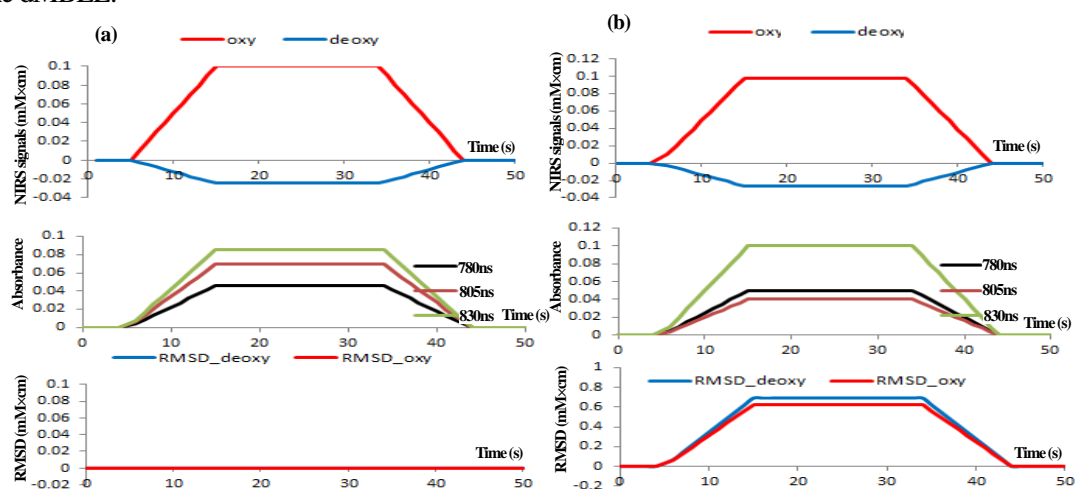


Fig.1 Examples of NIRS signals and RMSD calculated by simulating absorbance changes due to (a) hemoglobin concentration changes and (b) any other causes than them.



## Head phantom including multiple absorption inclusions for near infrared topography

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Head phantoms are important in order to estimate the nonuniform spatial sensitivity of near-infrared (NIR) topography, to optimise the probe arrangements and to evaluate the image reconstruction algorithm. The peak value and spatial extent of the absorption change in the topographic images depend on the relative position between the absorption inclusion and source-detector pairs. In this study, multiple absorption inclusions in the head phantom were imaged by NIR topography to evaluate the influence of the nonuniform spatial sensitivity on the topographic image of the absorption change.

A picture of the head phantom is shown in Fig. 1. The phantom is a water tank filled with an intralipid solution and green ink mimicking brain tissue. The bottom wall consists of two layers mimicking superficial tissue (scalp and skull) and cerebrospinal fluid (CSF). Multiple absorption rods are able to be inserted in the intralipid solution to realise the absorption change caused by the brain activation. The source and detector probes were attached to the bottom of the tank to detect the change in intensity caused by the absorption rods. Figure 2(a) shows the measurement points, which are the midpoint of the source-detector pair, and the positions of the absorption inclusions. The distance between the source and detector for all the source-detector pairs was 30 mm. The change in intensity detected by each probe pairs caused by the absorption inclusions was mapped at the corresponding measurement point and is spatially interpolated to obtain the topographic images. The topographic images of the two inclusions are shown in Fig. 2(b). The solid lines in the images indicate the position of the absorption inclusions. The diameter of the absorption inclusion at position (A) is 15 mm while that at position (B) is 10 mm (b1) or 20 mm (b2). The absorption coefficient of the inclusions at positions (A) and (B) are the same. Although the absorption coefficient of the inclusion is the same, the peak values of the absorption changes in the image obviously varied with the size of the absorption inclusion. This result indicated that the change in the size of the absorption inclusion at (B) rather more affects the peak value than the spatial extent of the absorption change in the topographic image calculated by the simple mapping method.

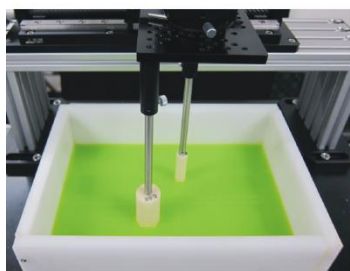


Fig. 1 The head phantom.

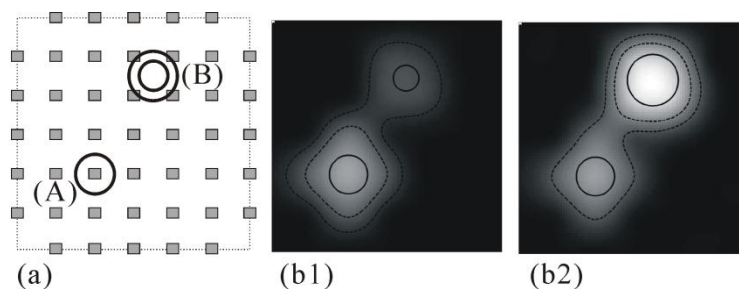


Fig. 2 (a) Measurement points of NIR topography.

(b) Topographic images of absorption inclusions.

## Depth-compensated tomography (DC-Tomo) based on standard brain atlas

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**Introduction:** In diffuse optical tomography (DOT), researchers often face challenges to accurately recover the depth and size of the reconstructed objects. Recently we developed a depth compensation algorithm (DCA) to improve the depth specificity in DOT [1,2]. We also demonstrated that DCA could be combined with L1-norm regularization to solve the over-smoothing problem that degrades the spatial resolution [3]. However, all of these studies were based on a semi-infinite, homogeneous brain model which deviated from the realistic human brain anatomy. In the present work, we have implemented the depth-compensated tomography (DC-Tomo) onto a standard brain atlas and further investigated how reconstructed images are affected by (1) heterogeneity of the brain, (2) sparsity of the optode geometry, and (3) selectivity of source-detector distances. Computer simulations and human experiments were conducted to evaluate the brain atlas-based DC-Tomo. At last, the tomographic images were also compared with the topographic images generated by a toolbox that we developed recently (“EasyTopo”).

**Methods:** Two-layer finite element mesh of a standard brain atlas (ICBM 152) was generated using the iso2mesh toolbox. Then DC-Tomo was implemented using the following procedures: (1) probabilistic registration to localize DOT measurements on the brain mesh by digitizing the coordinates of optodes along with five cranial landmarks; (2) NIRFAST, which is based on the diffusion approximation to solve the forward problem; (3) DCA to compensate the node-wise sensitivity along depth; (4) regularized inversion to reconstruct the 3D tomographic images; and (5) node-wise statistical analysis based on the general linear model (GLM). Human motor activation by a finger tapping task was acquired using high-density optode geometry. To investigate how the sparsity of the optode geometry affects the image quality, this high-density geometry was converted to a sparse geometry by removing part of source-detector pairs.

**Results:** The heterogeneity of the brain does not affect DC-Tomo significantly. DC-Tomo can recover the correct depth of an imaged object (e.g., an embedded absorber or activated motor cortex) using either high-density or sparse geometry. Including the 1<sup>st</sup> nearest source-detector neighbors (~1.6 cm) appears to degrade the spatial resolution. Figure 1 shows the results of human motor activation by using high-density geometry (with 2<sup>nd</sup> nearest source-detector neighbors only). Node-wise GLM analysis provides regions of interest (ROIs) consistent with those in reconstructed hemodynamic (or oxy-hemoglobin) images. Moreover, the tomographic images agree with the topographic images generated by EasyTopo, while the former is always better (see Fig. 2).

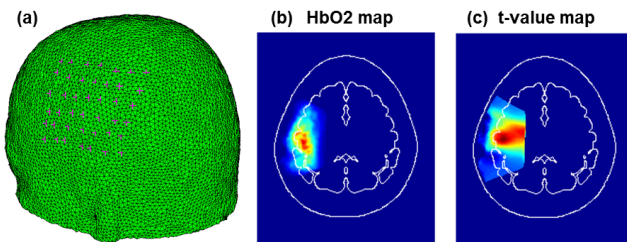


Fig 1. (a) Brain mesh and optode geometry; (b) reconstructed HbO2 image; (c) t-value image attained from node-wise GLM.

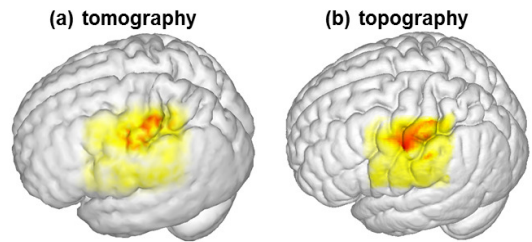


Fig 2. (a) Tomographic HbO2 image; (b) Topographic HbO2 image.

**Future work:** We will combine DC-Tomo with L1-norm regularization to improve the spatial resolution.

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1. F Tian, H Niu, ZJ Lin and H Liu. Optics Letters 35(3), 429-431, (2010).
2. F Tian, H Niu, S Khadka, ZJ Lin, and H Liu. Biomed. Opt. Express 1, 441-452 (2010).
3. VC Kavuri, ZJ Lin, F Tian, and H Liu. Biomed. Opt. Express 3(5), 943-957 (2012).

## fNIRS data analysis by Slope: an alternative method to distinguish the level of cortical activation pattern during functional tasks.

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Keywords: fNIRS, data analysis, quantitative method, linear regression.

More and more investigations in the field of Life Sciences are issues from growing interest for the functional near-infrared spectroscopy (fNIRS) application. A large fNIRS literature seeks (i) to assess the level of brain involvement in daily human movement and (ii) to depict fNIRS real-time signal biomarkers. While the fNIRS signals are strongly well-known to reflect several hemodynamic processes (i.e., changes in blood volume and in the hemoglobin oxygenation state), no real consensus does still exist on how to perform the fNIRS data analyzes for obtaining a suitable assessment of cortical activation. Different fNIRS analysis methods have been proposed to estimate the largeness of the amplitude on the cortical activation pattern. Commonly, the significance of data changes (i.e., pre-stimulation vs. stimulation) is based on the magnitude of the activation level. Currently, the variables of interest calculated to depict the fNIRS activation pattern are the: differential signals change (i.e., the difference of oxy-Hb and deoxy-Hb so-called diff-Hb); additive signals change (i.e., the sum of oxy-Hb and deoxy-Hb so-called tot-Hb); area under the curve (AUC); Z-score; time-to-peak (TTP, i.e., temporal mismatch to achieve the maximum positive or negative values in oxy- and deoxy-Hb, respectively); amplitude response for oxy-Hb; etc. But such approaches introduce difficulties to discriminate a low response of activation. Therefore, we propose a new fNIRS analysis routine aiming to investigate the degree of cortical activation pattern. In the present study we adopted a simple approach based on the use of a linear regression technique over a sufficient time window of stimulation and the calculation of the slope coefficient (Figure below). Although the data (activation period + plateau period) cannot be fitted perfectly by linear regression it is clear that the slope discriminates the cortical activation pattern with respect to some aforementioned methods.

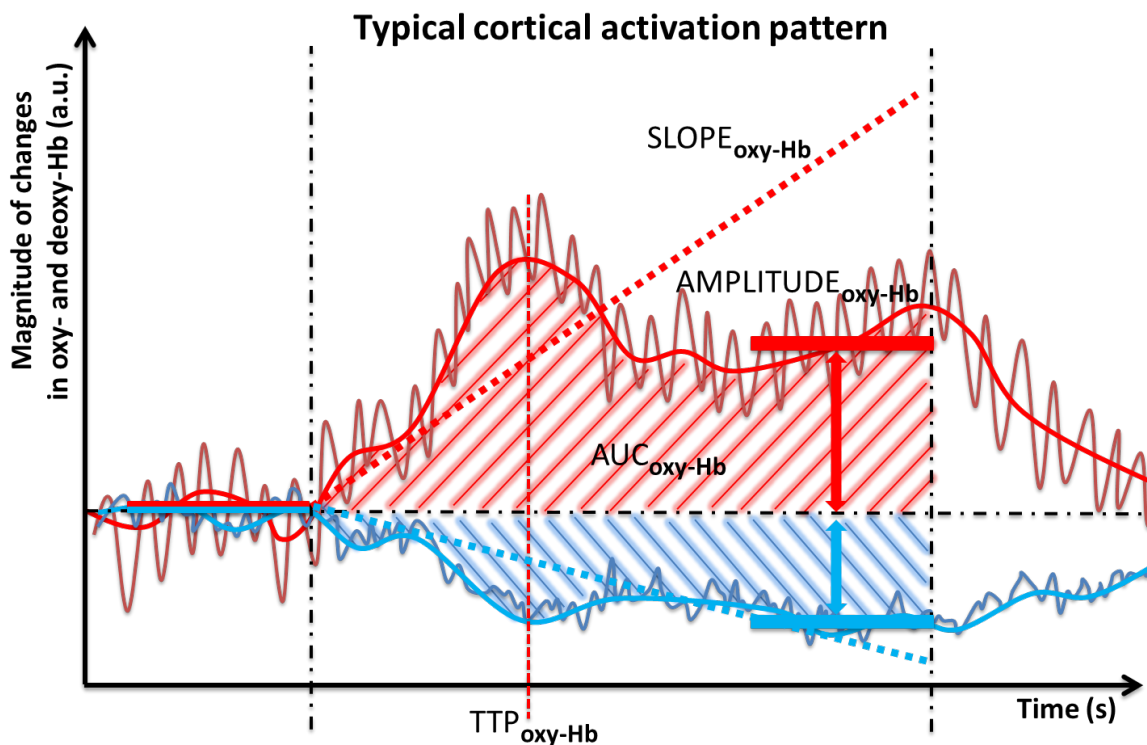


Fig. Current methods and Slope approach using linear regression to analyze the typical fNIRS hemodynamic changes response during functional task.

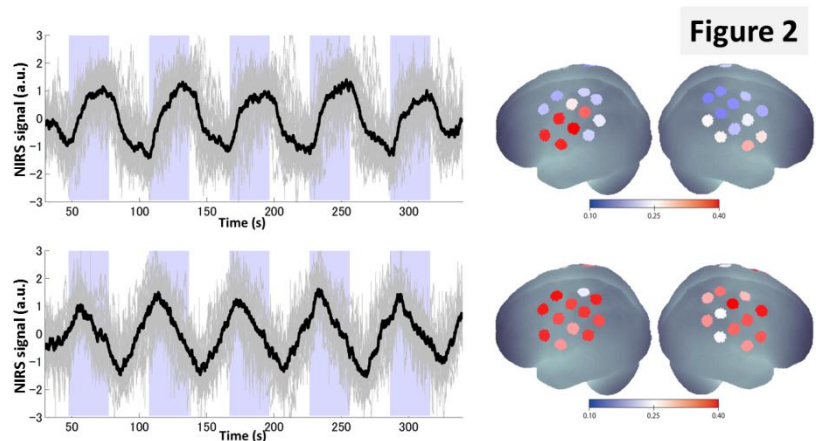
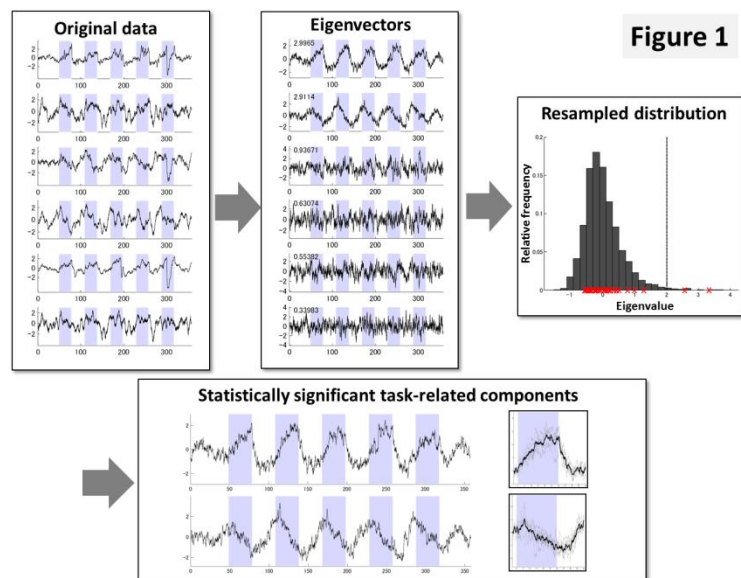
## Task-Related Component Analysis for Functional Neuroimaging and Application to Near-Infrared Spectroscopy Data

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Reproducibility of experimental results lies at the heart of scientific disciplines. Here we propose a signal processing method that extracts task-related components by maximizing the reproducibility during task periods from neuroimaging data. Unlike hypothesis-driven methods such as general linear models, no specific time courses are presumed, and unlike data-driven approaches such as independent component analysis, no arbitrary interpretation of components is needed. Task-related components are constructed by a linear, weighted sum of multiple time courses, and its weights are optimized so as to maximize inter-block correlations (CorrMax) or covariances (CovMax). Our analysis method is referred to as task-related component analysis (TRCA). The covariance maximization is formulated as a Rayleigh-Ritz eigenvalue problem, and corresponding eigenvectors give candidates of task-related components. In addition, a

systematic statistical test based on eigenvalues is proposed, so task-related and task-unrelated components are classified objectively and automatically (Fig. 1). The proposed test of statistical significance is found to be independent of the degree of autocorrelation in data if the task duration is sufficiently longer than the temporal scale of autocorrelation, so TRCA can be applied to data with autocorrelation without any modification. We demonstrate that simple extensions of TRCA can provide most distinctive signals for two tasks and can integrate multiple modalities of information to remove task-unrelated artifacts. TRCA was successfully applied to synthetic data as well as near-infrared spectroscopy (NIRS) data of finger tapping. There were two statistically significant task-related components (Fig. 2): one was a hemodynamic response, and another was a piecewise linear time course. In summary, we conclude that TRCA has a wide range of applications in multi-channel biophysical and behavioral measurements. This study will be published in NeuroImage.



Poster Session  
Neurodevelopment (I) and (II)  
Poster #: 55-70

## Fronto-posterior connectivity during phonological processing in the infant brain

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Infants produce language-specific speech sounds at approximately 10 months of age but can discriminate phonological contrasts from birth. The neural foundation of the linkage between perceiving and producing speech sounds is unclear in the infant brain. We investigated whether the cortical regions related to speech production in infants show functional connectivity with the posterior temporal and parietal regions when processing speech sounds; 25 three-month-old infants (age range, 104-119 days) were assessed during natural sleep. We used 94-channel near-infrared spectroscopy (ETG-7000, Hitachi Medical Corporation) to examine cortical activation on perceiving speech sounds for the repetition (/ban/-/ban/), consonant change (/ban/-/pan/), and pitch change (/ban/ for standard pitch and /ban/ for higher pitch) conditions. We evaluated changes in oxygenated hemoglobin (oxy-Hb) and deoxygenated hemoglobin (deoxy-Hb) signals for each measurement channel. Furthermore, we calculated the temporal correlations between the oxy-Hb signals by using all of the continuous data [1]. Analysis of variance of oxy-Hb signal data for all 3 conditions indicated that the anterior temporal regions on both sides and the precentral regions of the left hemisphere showed greater activation under the consonant-change condition than under the other conditions. Correlation analyses revealed that the correlation between the oxy-Hb signals of the precentral regions and the oxy-Hb signals of the posterior temporal and parietal regions in the left hemisphere was higher than the correlation between the oxy-Hb signals of the anterior temporal regions and the posterior regions. Analyses of phase synchronization [2] confirmed this tendency. Our results show that phonological processing in infants is subserved by the temporal regions and the precentral regions. The fronto-posterior connectivity in the left hemisphere may be the basis of the dorsal stream connecting the perceptual and articulatory networks during speech processing in infants.

[1] Homae F, Watanabe H, Nakano T, Taga G (2011) Large-scale networks underlying language acquisition in early infancy. *Front Psychol* 2:93.

[2] Taga G, Watanabe H, Homae F (2011) Spatiotemporal properties of cortical hemodynamic response to auditory stimuli in sleeping infants revealed by multi-channel NIRS. *Phil Trans R Soc A* 369:4495-4511.

PRELEXICAL CUES IN FIRST LANGUAGE ACQUISITION: TRAINING INDUCED CHANGES IN THE PROCESSING OF PHONOTACTICALLY LEGAL AND ILLEGAL CONSONANT CLUSTERS.

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**Background:** Speech comprehension requires the rapid mapping of an incoming auditory signal onto meaningful mental representations. Since natural connected speech does not provide bottom-up auditory cues (e.g., pauses) to indicate word boundaries segmentation of the auditory stream must rely on top-down linguistic knowledge. Prelexical regularities, such as phonotactics, support this task. For example in English (and German) the succession of the two phonemes /t/ and /k/ signals a boundary between two words, particles, or syllables because no existing word in these languages starts or ends with this consonant cluster. The combinatorial rules in a given language constrain ‘legal’ clusters at the onset, within, and at the coda of words. Phonotactic rules are language specific and must be acquired during first language acquisition or modified, when learning a second language later in life. In a number of experiments we inquired into the neuronal mechanisms underlying the processing of phonotactic properties. We could show that even in the absence of any semantic information the adult brain differentially processes pseudowords with legal compared to illegal onset clusters (Rossi et al., 2011). Moreover a short 3 day training scheme can modulate the response to ‘illegal’ pseudowords (Rossi et al., *subm.*). Using a cross sectional approach in infants we find evidence for a relatively early sensitivity to phonotactic rules at 3 months. Our data support the notion that an initially bilateral response to familiar versus unfamiliar onset clusters evolves into a more linguistic processing with a left lateralized response in adults. The ongoing project presented here goes one step further and addresses the question how a short intervention alters the processing of phonotactically legal vs. illegal pseudowords.

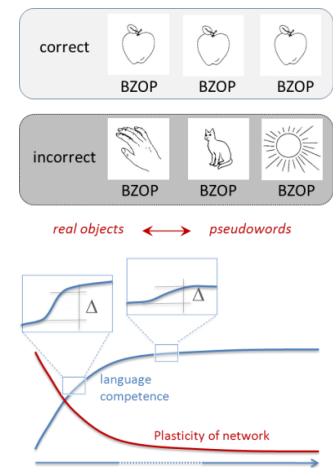
**Methods:** Infants of different age groups (6 & 18 months) undergo a 3 day training scheme. During training they are exposed to legal (e.g., /BRÖP/) and illegal (e.g., /BZOP/) pseudowords. Changes in neuronal processing are assessed prior to and after training using simultaneous EEG and fNIRS. 3 different training schemes are tested: (i) passive familiarization,

(ii) statistical learning of pairings between pseudowords and real objects and (iii) statistical learning using pseudoobjects. **Results:** in 38 6-month-olds the complete 3-day training using statistical learning with real objects (upper fig.) was performed. EEG data suggest a training induced modulation of legal and illegal pseudowords while preliminary fNIRS results seem to confirm a differential processing of legal and illegal pseudowords but analysis of training induced modulations needs to be finalized in order to get a clearer picture.

**Conclusion and Perspective:** This study on a longitudinal 3-day training in infants demonstrates that combined EEG-fNIRS assessment of plasticity in response to an intervention can be investigated in very young infants. For the case of prelexical properties of speech the project taps into the more general question how plasticity changes during development are related to the emerging linguistic competence (lower fig).

ROSSI, S., HARTMÜLLER, T., VIGNOTTO, M. & OBRIG, H. *submitted*. Modulation of lexical processing by repetitive exposure to foreign phonotactic rules.

ROSSI, S., JURGENSON, I. B., HANULIKOVA, A., TELKEMEYER, S., WARTENBURGER, I. & OBRIG, H. 2011. Implicit processing of phonotactic cues: evidence from electrophysiological and vascular responses. *J Cogn Neurosci*, 23, 1752-64.

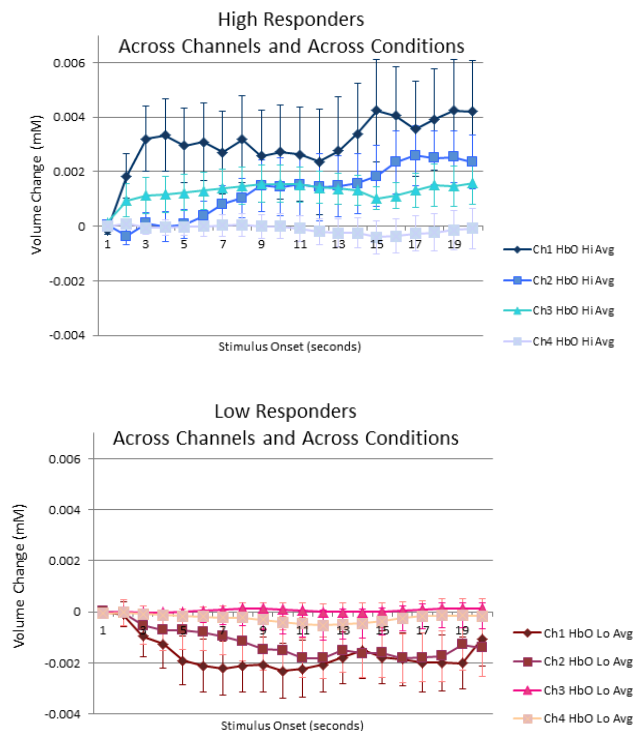


## Classifying Hemodynamic Responses to Auditory Input in Preverbal Infants

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Numerous studies have provided clues about the ontogeny of lateralization of auditory processing in humans, but most have employed specific subtypes of stimuli and/or have assessed responses in discrete temporal windows. The present study used near-infrared spectroscopy (NIRS) to establish changes in hemodynamic activity in the neocortex of preverbal infants (aged 4-11 months) while they were exposed to two distinct types of complex auditory stimuli (full sentences and musical phrases). Measurements were taken from bilateral temporal regions, including both anterior and posterior superior temporal gyri/sulci. When the infant sample was treated as a homogenous group, no significant effects emerged, nor were any effects detected when infants were subgrouped by age. However, when infants' hemodynamic responses were categorized according to their overall changes in volume, two very clear neurophysiological patterns emerged. Infants with high-volume hemodynamic responses (the *high responder* group) showed a pattern of early and increasing activation, primarily in the left hemisphere, similar to that observed in comparable studies with adults. In contrast, infants with low-volume hemodynamic responses (the *low responder* group) showed a pattern of gradually *decreases in* activation over time. These differences (focusing on HbO<sub>2</sub>) are highlighted in the two figures below. Notably, no significant differences emerged for type of auditory input (speech versus music), suggesting that the high versus low responder characterization generalizes across classes of auditory stimuli. These results highlight a new way to conceptualize the variability frequently observed across infant participants, with hemodynamic response volumes potentially serving as an early indicator of developmental changes in auditory sensitivity. We are currently examining the relationship between hemodynamic response volume/direction and infants' performance on a battery of standardized perceptual measures.





## Six-month-olds' brains respond more to highly frequent vowels

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Functional Near InfraRed Spectroscopy (fNIRS) has provided unprecedented insight into the emergence of language networks in the infant brain. A number of studies have shown that, in infants 6-20 months, discrimination of vowels that are present in the native language evokes larger and/or more left-lateralized responses than discrimination of comparable stimuli which are absent from the infants' ambient language (Minagawa -Kawai et al, 2007). The relative contributions of maturation and exposure in the emergence of networks specialized in the ambient language is, however, poorly understood. Previous evidence suggests that maturation is a *necessary* precondition for some linguistic abilities (Pena et al., 2010). But is maturation *sufficient*, or must infants further have sufficient exposure to a given sound contrast in order to display language-specific responses to it? To answer this question, we assessed 5-7 month old Dutch infants' brain responses to contrasts between a pair of highly frequent (/I/ - /eI/) and a pair of highly infrequent (/Y/ - /ø/) native vowels. Both of the vowel contrasts were native to the infants and additionally matched on acoustic and perceptual characteristics. However, they differed markedly in their frequency of occurrence in Dutch. As a result, at any given age, infants will have had greater exposure to the high frequency than the low frequency vowels. A difference in processing of the two contrasts would indicate that exposure plays a role beyond maturation.

Standard artifact detection and detrending were applied, followed by GLM analyses on oxygenated hemoglobin. A ROI was defined by 5 channels above perisylvian regions, which were activated ( $p$  uncorr < .05) at one or both conditions, in the left or right hemispheres (see Fig. 1). The resulting average  $\beta$  for the ROI was entered into an ANOVA with Condition (high Frequency, low Frequency) and Hemisphere (left, right) as factors. Results revealed a main effect of frequency [ $F(1,21) = 3.94$ ,  $p = .06$ ] with a higher  $\beta$  for the frequent compared to the infrequent contrast (Fig. 2), with no main effect of hemisphere and no interaction between the factors.

These results strongly suggest that frequency of exposure modulates brain responses to native language contrasts at around six months of age. Such a finding is most compatible within an interactional view of the emergence of language networks in the human brain, according to which such specialized responses rely crucially on *both maturation and experience*.



Figure 1: Channels constituting ROI

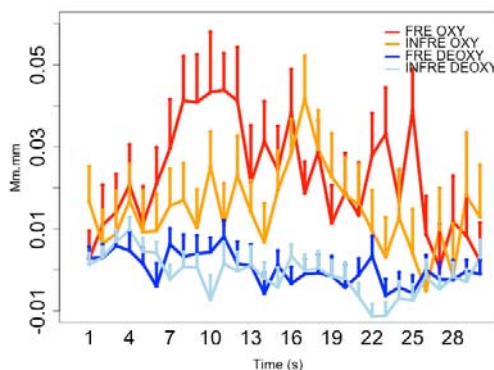


Figure 2: HRF over ROI channels

### Vowels and Consonants at Birth: a NIRS study

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Our main goal is to investigate the perception of Vowels (Vs) and Consonants (Cs) in newborns. Cs and Vs are functionally asymmetric: Cs weigh more in lexical tasks, whereas Vs carry more information at the structural levels: prosody, morphology and syntax (consonantal & vocalic biases respectively, Nespor, Peña, & Mehler, 2003). Both biases have been observed in adults, infants, and recently before 12 months (Hochmann et al., 2011, Nishibayashi & Nazzi, 2012). If this “division of labor” started at birth, it would constitute a significant learning bias towards the acquisition of lexical and structural levels of language. However a certain amount of exposure to speech may be necessary before infants use this Cs/Vs functional asymmetry. For instance in a lexical task 6-month-olds exhibit a bias for Vs (Hochmann, 2010) contradicting Nespor et al. (2003)’s predictions. In order to directly investigate the starting point of the C/V functional asymmetry, the current study measured the responses of the newborn brain using NIRS, to speech signals which according to the division of labor hypothesis, should elicit a vocalic bias under one experimental condition (*extraction of regularity*), and a consonantal bias under another (*item-based learning*).

Gervain et al. (2008) found a differential response in temporal and left frontal areas between ABB and ABC in CVCVCV sequences (e.g. “mubaba” vs. “mubage”, respectively). This extraction of a repetition rule over syllables is important for acquiring linguistic structures (Marcus et al., 1999). The current study uses Gervain et al. (2008)’s paradigm, with 3 different patterns: the ABC rule (e.g. “mulevi”) and two different ABB rules: ABBc with repetition of Cs, e.g. “muleli”, and ABBv with repetition of Vs, e.g. “muleve”. The 3 patterns are presented in 2 block designs:

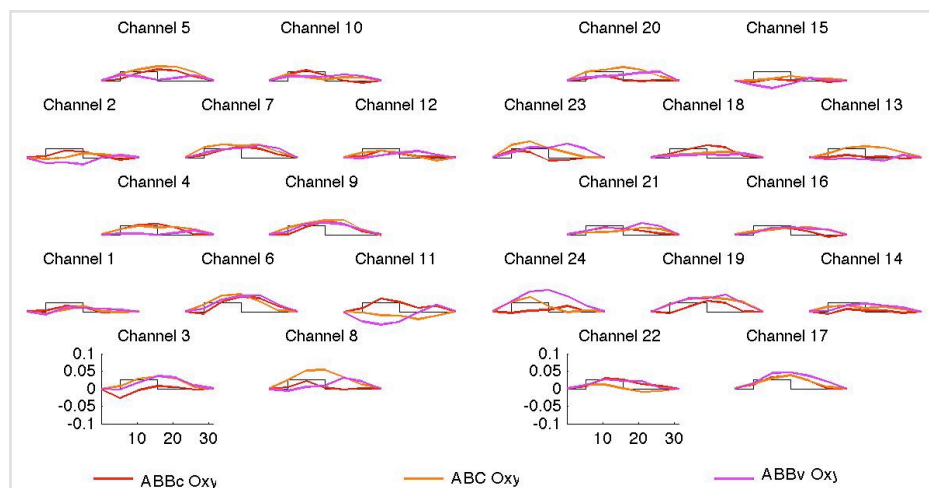
- Exp. 1 *extraction of regularity*: heterogeneous blocks of 6 different items;
- Exp. 2 *item-based learning*: homogeneous blocks of 6 repetitions of the same word;

The “division of labor” hypothesis predicts that Exp. 1 encouraging rule detection, should favor the ABBv over ABBc sequences; whereas, Exp. 2 encouraging identification of a repeated unit, this resembles ‘lexical’ processing that should favor ABBc over ABBv sequences. Both experiments used the same material: 36 CVCVCV synthesized with MBROLA, with minimized acoustic differences between Cs and Vs.

So far 16 newborns have been kept for the analysis in Exp.1 (cf. Fig.1). Comparing ABC and ABBv yielded a significantly greater activation for ABC in channels 2 ( $P = .01$ ) and 5 ( $P = .02$ ) (paired sample t-test, p values are uncorrected) indicating that ABC and ABBv are distinguished in the left frontal area. Comparing ABBc and ABBv yielded a significantly greater activation for ABBc in channel 4 ( $P = .03$ ), indicating that ABBc and ABBv are distinguished in the left temporal area. Comparing ABC and ABBc yielded no significant differences. Overall these preliminary results suggest, first, a stronger involvement of the LH for all 3 patterns; and secondly, a repetition suppression effect occurring for the ABBv pattern. This confirms the predicted vocalic bias in bias in a context favoring the *extraction of regularity*.

Testing of Exp. 1 & 2 will be completed before the conference.

**Figure 1.** Grand average oxyHb changes evoked by ABC, ABBc & ABBv in Exp. 1. The x-axis represents time in seconds; the y-axis shows concentration in mmol-mm. The rectangle along the x-axis indicates time of stimulation.



Experience-Dependent Changes in Infant Brain and Behavior: The Case of Color Priming  
Teresa Wilcox, Texas A&M University (twilcox@tamu.edu)

One notable property of the immature brain is the remarkable capacity for experience-dependent changes in structure and function. Most research has focused on the extent to which repeated and extensive experience helps shape the development of our perceptual and cognitive systems. The current research explores the extent to which limited and selective experience can alter brain and behavior in the infant.

Previous behavioral studies have revealed that prior to 11.5 months infants do not spontaneously use color information to individuate objects. However, select experiences can prime younger infants to do so (Wilcox & Chapa, 2004). For example, if 9.5-month-olds are first shown events in which color predicts object function (Fig. 1a) they showed prolonged looking to a green ball-red ball test event (Fig. 2). This is taken as evidence that infants individuated the objects (they interpreted the event as involving two objects and recognized that both objects could not fit behind the narrow screen). Infants aged 9.5 months do not typically individuate-by-color (do not show prolonged looking to the this event). If the pretest events involve distinct motions but the motions are not functionally relevant (Fig. 1b) priming is not observed. It is the linking of color to an object property to which infants are already sensitive – object function – that leads to increased sensitivity to color information, which is then carried forward to the subsequent test event. The current research investigated whether experience-dependent changes in object processing are accompanied by changes in patterns of neural activation. That is, does color priming alter functional activation of the infant cortex?

**Method:** Infants first viewed either a function or motion event (Fig. 1). Next, infants' capacity to individuate-by-color was assessed using the narrow-screen test event (Fig. 2). Infants saw 4 20 s test trials. Each trial was preceded by a 10 s baseline event in which a curtain was lowered over the front of the apparatus and infants were given no auditory or visual stimulation. NIRS data were collected at 9 channels localized over four cortical areas (Fig 3): anterior temporal (T3), posterior temporal (T5), posterior parietal (P3), and primary visual (O1) cortex. Changes in HbO, compared to baseline, were averaged over trials and participants to obtain a grand average for each group. Previous research implicates neural activation at T3 as important to individuation-by-feature in the infant (Wilcox et al., 2011). Looking time data were collected and averaged.

**Results:** The infants in the function but not the motion condition showed prolonged looking to the narrow-screen test event, indicating that only the former group individuated-by-color. This is consistent with previous reports that viewing function but not motion events leads to increased sensitivity to color information in a subsequent individuation task. Different patterns of activation were also obtained in response to the function and motion events. Whereas both groups showed activation at V1 and T5, only the function group showed activation at T3. An additional group of infants saw the test event without first seeing pretest events: they showed behavioral and neural responses similar to those of the infants in the motion group. These results reveal experience-dependent changes in cortical activation in infants after limited and selective exposure to pretest events. The neural mechanisms that support such plasticity in the immature brain are speculated upon.

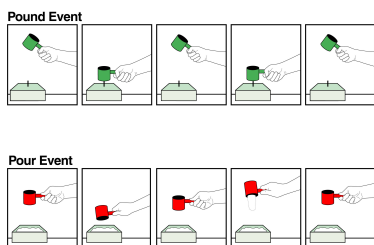


Fig. 1a. Function Event

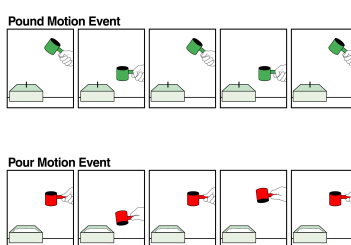


Fig. 1b. Motion Event

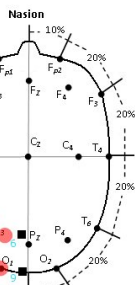
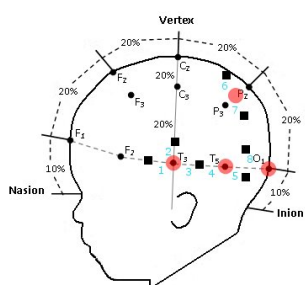


Fig. 3. Placement of sources (red circles) and detectors

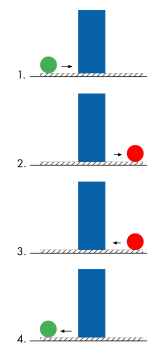


Fig. 2. Narrow-screen test event

Randomized, double blind, placebo controlled, crossover design to evaluate MPH effect in ADHD children using fNIRS monitoring during Go/NoGo task

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### 【Objective】

Functional neuroimaging data on ADHD in children is sparse compared to those of adults, whose less activation was revealed at prefrontal cortex (PFC) during attention and inhibition tasks. Developing feasible test to assess the brain dysfunction of ADHD in children is of value for the early and objective diagnosis and the evaluation of the treatment. We applied fNIRS to assess the activity of PFC and the effect of methylphenidate (MPH) during Go/NoGo tasks for ADHD in children.

### 【Methods】

Sixteen patients (12 boys, 4 girls; mean age, 8.6 years; range, 6-13 years) with ADHD fulfilling DSM-IV criteria were enrolled after obtaining informed consent from the parents. All patients were right-handed with IQ > 70. As controls, 16 healthy children were recruited. Sixteen ADHD and control subjects were matched in gender and age. Randomized, double blind, placebo-controlled, crossover design was conducted to evaluate MPH effect in ADHD children using fNIRS monitoring during Go/NoGo task. After the first examination, patients took MPH (18-45 mg) or placebo, and repeated the similar measurement 1.5 h after medication. The control subjects undertook fNIRS measurement only once without taking medication.

### 【Results】

Before MPH administration, patients showed no significant activation in the right ventrolateral PFC (R-VLPFC) ( $p < 0.05$ ) compared with controls. MPH significantly increased brain activation in the R-VLPFC compared to the placebo ( $p < 0.05$ ). The degree of brain activation after the administration of MPH was comparable to that in controls.

### 【Conclusion】

This fNIRS-based research presents the first neuropharmacological evidence of the MPH effect in ADHD children. Attention and inhibition control in ADHD was related to the R-VLPFC. fNIRS effectively showed the biological effects of MPH.

Different Patterns of Activation in Temporal Cortex to Function vs. Non-Function Events  
**Teresa Wilcox, Amy Hirshkowitz, Laura Hawkins**  
 Texas A&M University

Over the last several decades a great deal of research has been conducted to explore the neural basis of object motion processing in the human. Existent literature suggests that human infants use motion-carried information to distinguish between broad categories of objects (e.g., biological vs. non-biological; artifacts vs. natural kinds) and events (function vs. non-function; goal directed vs. non-goal directed). In addition, the adult cortex contains specialized systems for processing these broad categories. For example, distinct cortical areas involved in processing of biological vs. non-biological motion (Pelphrey et al., 2003; Peuskens et al., 2005) and different patterns of activation are observed in response to social vs. mechanical events (Chao et al., 1999; Moore & Price, 1999; Martin & Weisberg, 2003). However, little is known about the origins and development of these specialized systems. One common finding is that the superior temporal sulcus (STS) is involved in processing of meaningful and/or biologically relevant object motion. There is some evidence that the infant cortex may be organized in ways similar to that of the adult (Lloyd-Fox et al., 2011; Shimada & Hiraki 2006), which suggests early developmental specialization. The present research explored the extent to which category-specific differences are observed in neural response to function versus non-function events.

Infants mean age 9.5 months viewed one of two events live in a puppet-stage apparatus: function (n=21) or non-function (n=19). In the function event, infants saw a green or red object either pound a nail or scoop and pour salt, respectively, on alternating trials (Fig. 1). In the non-function event, the objects underwent similar motions but to the side of the nail-box or salt-box. Hence, the function and non-function events were perceptually similar but differed in whether the actions were functionally relevant. Each trial was 30 s in duration and preceded (and followed) by a 10 s baseline event in which a curtain was lowered over the front of the apparatus, without auditory or visual stimulation. Optical imaging (fNIRS) data using a NIRS 8x8 (TechEn) were collected at 9 channels localized over four cortical areas (Fig 2): visual anterior temporal cortex (1,2,3), posterior temporal cortex (4,5), posterior parietal cortex (6,7) and visual cortex (8,9) (Figure 2). Changes in HbO, compared to baseline, were averaged over 4 test trials and participants in each group. Different patterns of activation were obtained in response to the function and non-function events (Fig 3). Most importantly, activation was obtained in anterior temporal cortex in response to the function events and in posterior temporal cortex in response to the non-function events. These results reveal that some of the same category-specific patterns of activation that have been observed in adults are also observed in infants.

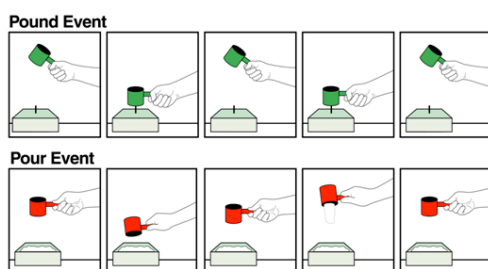


Figure 1. Wilcox & Chapa (2004). *Cognition*.

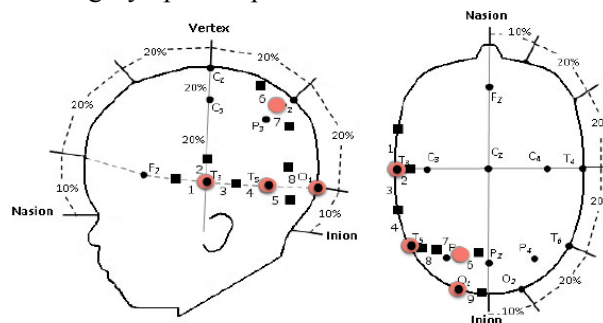


Figure 2. Headgear placements and channels.

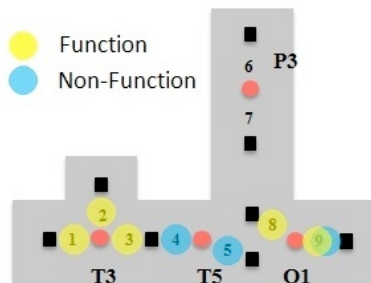


Figure 3. Significant activations for function and non-function events.

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### Hemodynamic Correlates of Ratio-Based Numerical Discrimination in Infancy: An fNIRS Study

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Studies on pre-verbal infants and non-human primates have demonstrated evidence of an early nonverbal cognitive system for representing number (see Carey, 2009; Dehaene, 1997; Feigenson, Dehaene, & Spelke, 2004; Gallistel, 1993 for reviews). One key behavioral signature seen across populations and species is sensitivity to the ratio between two numerical quantities to be compared (see Feigenson et al., 2004 for a review). That is, the ability to discriminate between any two numerical quantities seems to be a function of the ratio between them, with discrimination becoming harder as the ratio approaches 1. The behavioral observance of the ratio signature suggests that this system is present from birth, and shared with a variety of non-human animals. Furthermore, recent work suggests that this primitive number system may form the basis for the later acquisition of symbolic and mathematical concepts (e.g. Halberda et al., 2008; Gilmore et al., 2010). Despite its importance, relatively little is known about the neural basis of this system early in development.

Several studies using event-related potentials (ERPs) suggest that infants and adults show common functional brain signatures to ratio-based numerical changes. However, the functional neuroanatomy of these signals cannot be confidently determined through these methods (Hyde & Spelke, 2011; Izard et al., 2008; Libertus et al., 2010). One previous study has employed fNIRS to study the mechanisms of numerical processing in infancy (Hyde et al., 2010). While this study reports sensitivity and selectivity for number changes in the right parietal lobe, its findings are limited given the small number of parietal and occipital sites from which the researchers were able to record.

The current study aimed to expand on previous fNIRS work on numerical processing in infancy by estimating the hemodynamic response using NIRS over a wider range of posterior scalp sites, and by employing a potentially more powerful number alternation block design. Specifically, using a Hitachi ETG-4000 NIRS system, we presented 6-month-old infants with dot arrays either differing in a 1:2 ratio or showing no change (1:1 ratio). Two 3 x 3 chevron arrays of emitter and detector optical probes were placed over occipital and parietal regions of both hemispheres. Changes in oxy- and deoxyhemoglobin were monitored as infants passively viewed up to 20 blocks of quantity stimuli. Each block contained 10 stimulus images which remained onscreen for 500ms each. The first block (and all subsequent odd-numbered blocks) contained a series of 10 unique arrays of 8 dots; the second block (and all subsequent even-numbered blocks) contained a series of alternating arrays of 8 dots and 16 dots. Fifteen infants with at least three useable blocks of each type were included in subsequent analyses.

We observed a significant difference in the concentration of oxyhemoglobin to the left parietal region during viewing of alternating displays of 8 and 16 dots, compared to viewing only 8 dot displays ( $p = 0.05$ ). This finding is consistent with previous work using fMRI to examine numerical processing in school-aged children and adults (Ansari & Dhital, 2006; Isaacs et al., 2001), though it is in contrast to Hyde et al. (2010), who observed only a right parietal response to number changes using an adaptation design with infants. The employment of additional parietal recording sites and a different experimental design may have allowed us to detect left parietal sensitivity where others found none in infants. Nevertheless, these findings taken together suggest that infants show neural sensitivity to viewing numerical changes despite the absence of spoken language or number words. Continued work will further elucidate the neural mechanisms for numerical processing in pre-verbal infants, how these mechanisms change over development, and how these changes relate to conceptual numerical development.

## DBIfNIRS: A community-augmented online DataBase of Infant functional Near InfraRed Spectroscopy studies

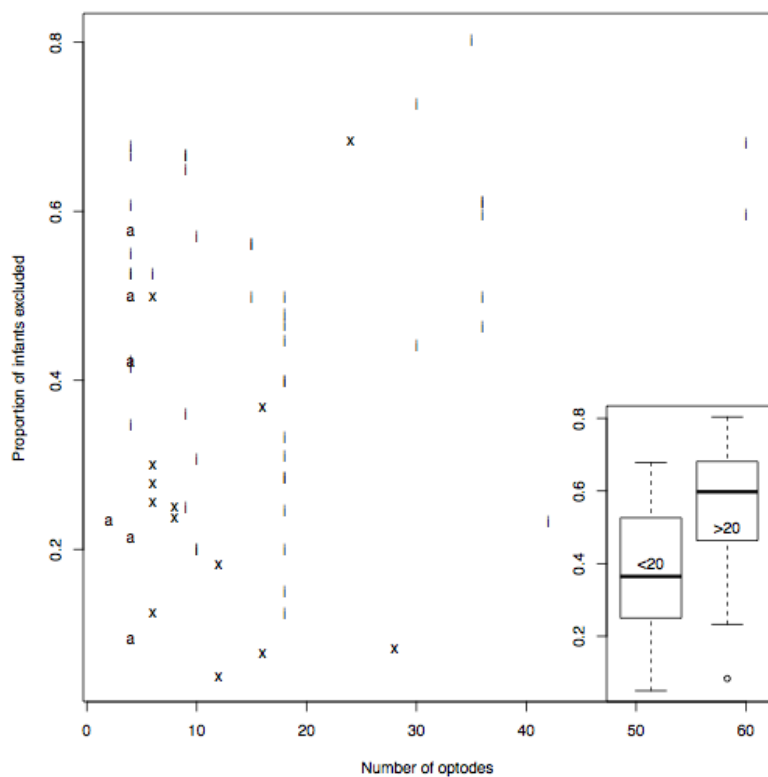
Alejandrina Cristia,<sup>1,\*</sup> Emmanuel Dupoux,<sup>2</sup> Yoko Hakuno,<sup>3</sup> Sarah Lloyd-Fox,<sup>4</sup> José Kivits,<sup>1</sup> Manuela Schuetze,<sup>1</sup> Tomas Bergvelt,<sup>1</sup> Marjolijn van Gelder,<sup>1</sup> and Yasuyo Minagawa-Kawai<sup>3</sup>

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Until recently, neuroimaging the infant brain was extremely challenging. However, this seemed to change with the advent of fNIRS, a technique that is becoming increasingly common in the study of infant motor, perceptual, and cognitive development. In such an emergent field, it is particularly important to share methodological knowledge that will allow replicable and robust results. We present DBIfNIRS, a community-augmented database that facilitates precisely this exchange. We tabulated 76 articles and theses published between 1998 and 2012 reporting 109 experiments on infants below 3 years of age along several methodological dimensions. The resulting spreadsheet was uploaded in a format allowing individuals to both continue to contribute their new results, and download the most recent version from the nucleating website, <https://sites.google.com/site/dbifnirs/>. We illustrate the usefulness of the database by revealing a number of factors affecting 2 key variables: infant attrition, and the reliability of oxygenated and deoxygenated responses. For example, we find that attrition rates vary nonlinearly with infant age within the first year (~ 20% at 0-2 months, >50% at 4-3 months and over 9 months, ~35% at 5-8 months); and attrition rates increase with the number of optodes on the headgear (see Figure 1). Finally, we summarize general strengths and weaknesses of the DBIfNIRS, and outline future developments.



**Figure 1:** *Proportion of infants excluded as a function of number of optodes.* Number of optodes is totaled over sources and detectors. Each letter indicates an entry, coding for the system: “i” stands for Hitachi, “a” for Hamamatsu, and “x” for all other systems. The boxplot on the right bottom panel represents the exact same data, collapsing into two categories: less than 20 optodes, and more than 20 optodes.

## Perception of rhythmic grouping: An optical imaging study

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The goal of the present study was to test whether neonates' early brain specialization for language is driven exclusively by a universal preparation for language, or whether there is influence from prenatal language experience. To do so, we tested the perception of the iambic/trochaic law (ITL) in newborns. The ITL claims that elements contrasting in duration naturally form rhythmic groupings with final prominence (Short-Long), whereas elements contrasting in intensity/pitch form groupings with initial prominence (Strong/High-Weak/Low) (Woodrow, 1909; Hayes, 1995; Nespor et al., 2008).

It has been hypothesized that ITL can be modulated by language experience in adults and infants (Yoshida et al 2010, Bion et al 2011, Iversen et al 2008, Bhatara et al 2012). These findings are in opposition to Hay and Diehl (2007), who found that linguistic rhythm perception relies on general auditory mechanisms rather than being influenced by the linguistic environment, and thus perceptual grouping would not be culturally dependent.

Languages differ in their typical stress patterns. According to the ITL, languages that are predominantly iambic would rely on durational contrasts and predominantly trochaic languages would rely mainly on pitch and intensity contrasts, both at the levels of words and phonological phrases. Young infants develop preferences for particular stress patterns in speech depending on the stress pattern of their native language (Höhle, Bijeljac-Babic, Herold, Weissenborn, & Nazzi, 2009; Jusczyk, Cutler, & Redanz, 1993).

When does this sensitivity to prosodic prominence/grouping first emerge and is it influenced by early, possibly even prenatal, experience?

To answer this question, we used near-infrared spectroscopy (NIRS) to measure neonates' brain responses to tone sequences that varied in duration or pitch. These stimuli followed the ITL-predicted grouping patterns (short-long or high-low) or the non-predicted grouping pattern (long-short or low-high) or did not provide any grouping cues (equal duration and pitch).

We conducted two experiments: one where tones sequences varied only in duration (Experiment 1) or in pitch (Experiment 2). In each experiment, we compared neural responses to iambic sequences (short-long or low-high), trochaic sequences (long-short or high-low) and neutral ones (short-short/long-long or low-low/high-high).

Results from Experiment 1 (n= 10) showed that healthy, full-term newborns (exposed to French in utero) had significantly greater brain response to the iambic sequences (short-long) than to the trochaic sequences (long-short), in particular in the auditory areas of the left hemisphere.

Experiment 2 is ongoing.

Experiment 1 thus suggests that the ITL might be in place very early on, possibly at birth. However, Experiment 2 will provide crucial evidence, as the newborns tested in Exp 1 were mostly exposed to French, an iambic language. Therefore, only Exp 2, using a contrast not present in the infants' prenatal experience, can provide definitely conclusions.



Age-related Changes in the Functional Organization of Object Processing Pathways  
 Teresa Wilcox, Amy Hirshkowitz, and Laura Hawkins  
 Texas A&M University

Previous studies conducted in our lab suggest that different patterns of neural activation are obtained when infants individuate-by-feature than when they fail to do so. Furthermore, there are age-related changes in patterns of neural activation obtained during individuation-by-feature. The goal of the current research was to identify when this re-organization occurs and the extent to which it is seen when infants individuate-by-spatiotemporal information. We investigated age-related changes in functional activation to a shape-difference and a speed-discontinuity occlusion event. Behavioral studies have demonstrated that 4.5- and 11.5-month-olds interpret the shape-difference event as involving two objects. Infants aged 4.5 months (11.5-month-olds have not yet been tested) interpret a speed-discontinuity event as involving two objects.

**Method:** Infants aged 4.5, 7.5, and 11.5 months viewed one of three events on a puppet-stage apparatus (Fig. 1). Infants saw the event appropriate for their condition on four consecutive 24 s trials. Each trial was preceded (and followed) by a 10 s baseline (the curtain was closed over the front of the apparatus). NIRS data were collected at 9 channels localized over four cortical areas (Fig 2): anterior temporal (T3), posterior temporal (T5), posterior parietal (P3), and primary visual (O1) cortex. Changes in HbO, compared to baseline, were averaged over trials and participants to obtain a grand average for each group. Previous research implicates neural activation at T3 as important to individuation-by-feature (Wilcox et al., 2011).

**Results:** Patterns of activation at each of the nine channels, for each of the three age groups are displayed in Fig 3. Three main findings emerged. First, at all three ages activation was observed at V1, T5, and T3 in response to the shape difference event. However, the younger infants also showed activation in P3, indicating that analysis of shape differences in young infants draws on the dorsal system. Furthermore, patterns of activation observed at T5 were less robust in the 7.5- and 11.5month-olds (and did not differ significantly from control). Second, at all three ages activation was observed at V1 and P3 in response to the speed-discontinuity event. However, only the 4.5- and 7.5-month-olds also evidence activation in T5 and T3. This suggests that all three ages detected the speed discontinuity, but only the two younger groups used the speed discontinuity to individuate the objects. Looking time data supports this conclusion: only the two younger groups found the speed-discontinuity event surprising. Finally, the 7.5- and 11.5-month-olds showed less activation in V1 and T3 to the control event. Overall, these results suggest paring down of pathways and/or structures involved in object processing during the first year of life, starting at least by 7.5 months.

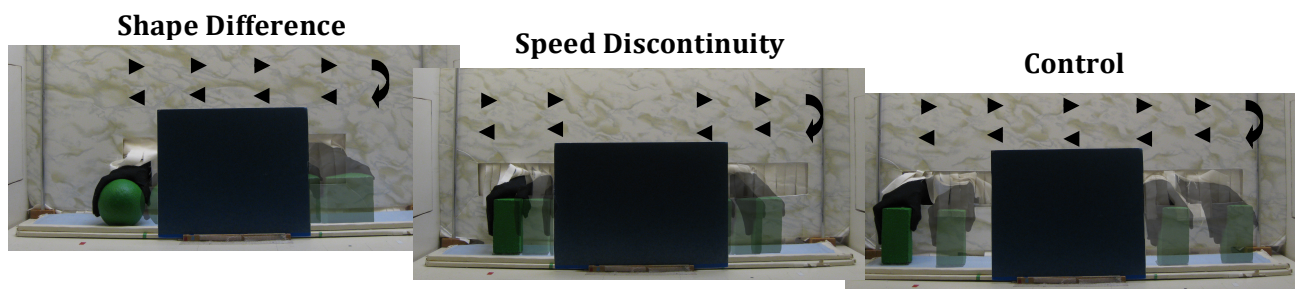


Fig. 1. Test events

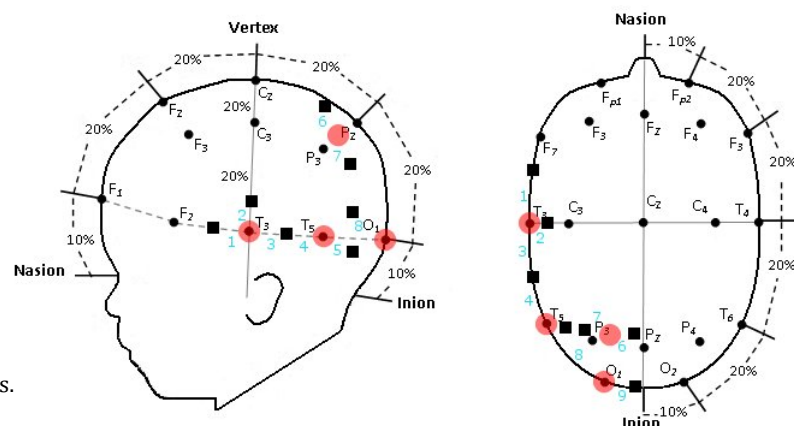


Fig. 2. Placement of sources (red circles) and detectors (black squares) and the corresponding nine channels.

## Multimodal EEG-NIRS studies of noxious and sensory stimulation in newborn infants

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**Aim:** To simultaneously measure electrophysiological and haemodynamic responses to innocuous and noxious sensory stimuli in newborn infants.

**Introduction:** Previous EEG studies<sup>1</sup> have shown a changing pattern of cortical responses to pain and touch in early development, with a transition from a temporal to central location at approx. 35-37 weeks gestational age (GA). The purpose of this study was to measure haemodynamic correlates to this electrophysiological activity.

**Methods:** Participants were healthy infants (34 – 41 weeks GA) studied at 0 – 3 days of age (n=10).

Noxious stimulation was a clinically required heel lance. Group 1 received the heel lance, a sham (the auditory and tactile components without the lance), and an auditory click stimulus. Group 2 received calibrated touch to the heel with a customised tendon hammer.

Brain activity was monitored with simultaneous and synchronised EEG and NIRS recordings. EEG electrodes were placed according to the international 10:20 system. Haemodynamic responses (concentration changes in  $\mu\text{mol/L}$ ) were obtained at contralateral central (C3/C4) regions, as described previously<sup>2</sup>, and in temporal (T3/T4) regions using the NIRO-200NX (Hamamatsu Photonics K.K.).

**Results:** To date we have successfully obtained data from 10 infants; 5 heel lance studies and 5 innocuous stimulation studies.

**Table 1: Mean (range) concentration change ( $\mu\text{mol/L}$ ) per stimulus type and optode location.**

	C3/C4 Optode			T3/T4 Optode		
	HbO	HHb	HbT	HbO	HHb	HbT
Lance	<b>5.0</b> (1.4-8.5)	<b>2.5</b> (1.5-4.4)	<b>5.2</b> (2.3-9.3)	<b>1.9</b> (0.1-5.0)	<b>3.5</b> (.1-10.1)	<b>3.2</b> (0.0-9.1)
Sham	<b>2.2</b> (1.7-2.5)	<b>2.6</b> (1.7-3.3)	<b>2.6</b> (1.1-4.3)	<b>2.0</b> (1.5-2.9)	<b>0.7</b> (0.2-0.9)	<b>1.8</b> (1.4-2.5)
Auditory	<b>3.4</b> (1.1-6.6)	<b>2.2</b> (0.4-4.6)	<b>4.0</b> (1.0-8.0)	<b>3.9</b> (1.2-6.2)	<b>0.5</b> (0.1-1.0)	<b>4.0</b> (1.2-5.9)
Touch	<b>0.9</b> (-.1-2.0)	<b>0.6</b> (0.2-1.1)	<b>1.0</b> (-.5-2.3)	<b>0.9</b> (0.2-1.4)	<b>0.3</b> (0.0-0.6)	<b>0.8</b> (-.5-1.5)

Concurrent EEG measurements were consistent with previous work which differentiated noxious and touch components<sup>1</sup>.

**Conclusion:** We have demonstrated that it is possible to measure simultaneously electrophysiological and haemodynamic responses from both central and temporal regions in newborn infants.

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## Integrating Behavioral and Neural Dynamics over Development in the Dimensional Change Card Sort (DCCS) Task

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We use fNIRS to test a hemodynamic prediction of Dynamic Field Theory (DFT) with 3- and 4-year-olds in the Dimensional Change Card Sort (DCCS) task. The DCCS requires children to switch between shape and color rules when sorting cards. Three-year-olds typically perseverate, while 4-year-olds switch rules. Between these ages, frontal activation also becomes stronger, suggesting that frontal activation is necessary for rule-switching. However, 3-year-olds can reliably switch rules when visual conflict is absent (No-Conflict version) during the pre-switch phase. If frontal activation is necessary for rule switching, then how are 3-year-olds with an immature frontal cortex able to switch rules at all?

In previous work, we used DFT to capture children's behavioral performance in the DCCS task in quantitative detail. Here, we examined whether we could use this neuro-dynamic model to generate hemodynamic predictions which we could test using fNIRS. Model simulations predict that 3-year-olds who perseverate in the standard task should show stronger frontal activation when they switch rules in a No-Conflict version. This is driven by the fronto-parietal connectivity in the model. When no-conflict test cards are used during the pre-switch phase, memories about the task and the current inputs for the posterior system spatially overlap. This overlap sends strong inputs to the frontal cortex, which increases frontal activation via reciprocal fronto-parietal loops. We successfully tested this prediction using fNIRS with 3- and 4-year-olds: Perseverators showed stronger frontal activation when switching in the No-Conflict version of the task compared to when they perseverated in the standard task.

Neural responses to point-light displays of biological motion in the first year of life: a functional near-infrared study

Anderson, L.C., Bennett, R.H., Bolling, D.Z., Pelphrey, K.A., Kaiser, M.D.

From birth, human infants preferentially attend to point-light displays (PLDs) of biological motion over scrambled motion (Simion, Regolin, & Bulf, 2008). The posterior superior temporal sulcus is involved in biological motion processing in typical children and adults (Kaiser et al., 2010). Yet, the early development of brain mechanisms for biological motion processing is not well understood. Functional near-infrared spectroscopy (fNIRS), which measures of oxygenated (oxy-Hb) and deoxygenated hemoglobin concentrations in cortical brain regions, is ideally suited to measure correlates of brain activity in awake infants.

fNIRS studies of biological motion processing in infants have been limited to a narrow age range (Lloyd-Fox et al., 2009, 2011) and have not included PLDs of full body motion (Ichikawa et al., 2010). Thus, the purpose of the current study was to track the typical development of the neural underpinnings of biological motion processing, *per se*, across the first year of life. We monitored regional cerebral blood volume changes using a 24-channel NIRS apparatus over bilateral temporal regions to measure brain activity while infants viewed 10s video clips of PLDs of biological and scrambled motion for 7 minutes.

To date, we have data from 6 infants ranging from 3.5-13.2 months ( $M = 9.5$ ,  $SD = 3.8$ ). We calculated changes in oxy-Hb in each channel for integrated blocks of biological and scrambled trials. We then examined average oxy-Hb levels within a time window of 5-12s post-stimulus onset and identified channels with a differential response to biological and scrambled motion greater than  $0.1 \text{ m[mmol/l]*mm}$ . Three contiguous channels in the left posterior temporal region met this criterion. Within this region, oxy-Hb concentration changes to biological motion stimuli trended towards being greater than those to scrambled motion stimuli. As a control, we performed the same analysis within a 3-channel region in the left anterior temporal region. Here, we found equivalent oxy-Hb values for biological and scrambled motion. We expect this pattern to reach significance with a larger sample.

We identified a left posterior temporal response to PLDs of biological motion in 6 infants, consistent with several fMRI studies that have found posterior temporal lobe involvement in typical children and adults. This suggests that within the first year of life, this region already plays a role in this type of processing. Future work will include a larger sample, assessed longitudinally, with the goal of charting the development of brain systems involved in biological motion processing in both typical infants and in those at risk for developing autism.

## Location, Location, Location – Where Are We in the Brain?

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Functional Near Infrared Spectroscopy (fNIRS) exhibits many advantages over other neuroimaging technologies: it is child-friendly, quiet, and easily compatible with other imaging methods and medical devices. Precise **spatial localization** of brain activation, within approximately 3 cm., is one of its most important capabilities. However this spatial precision may be called into question by the fact that, unlike fMRI, fNIRS does not allow researchers to see brain anatomy beneath the skull. Furthermore, unlike ERP, its probe distances are inflexible and caps of different sizes may then situate the probes atop different spatial locations within the brain. Traditional solutions to the fNIRS spatial localization dilemma have involved co-registration with the ERP 10-20 coordinate system using fMRI scans with vitamin-E probes, and 3D tracking devices. Here we propose the importance of an additional solution: **functional localizers**. fMRI researchers frequently use these “functional localizer” tasks to more accurately define within individual subjects the region specific to the relevant brain function, since the exact location of this functional specificity may vary (see Saxe, Brett & Kanwisher, 2006). We propose that the use of functional localizers is an important step towards improving the fNIRS research method. In our study we explore different functional localizer tasks for use in the study of various language functions (phonology, semantics, and grammar), and will present the efficacy of these tasks in localizing brain regions specific to language function, using fNIRS. The goal of the present work is to improve the fNIRS imaging method and to foster a forum for creating and standardizing functional localizer tasks for various aspects of cognition and perception in various age groups.

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Poster Session  
**Applications: Adult (I)**  
Poster #: 71-83

## **Assessment of hemodynamic activity modulations: investigating visual short-term memory mechanisms through fNIRS and EEG**

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### **Introduction:**

Functional near-infrared spectroscopy (fNIRS) is a neuroimaging technique capable of monitoring hemodynamic activity within human head in a low cost and noninvasive manner. A proper analysis of the so-called stimulus-evoked hemodynamic response (HR) is crucial to interpret the functional activity of the brain. Unfortunately, the estimation of HR from fNIRS signal is difficult because of the presence of random noise and some other physiological components. The assessment of HR is challenging above all in event-related paradigms, in which the HR elicited by a single briefly presented stimulus is completely hidden by noisy components. However, event-related paradigms are essential in the studies of cognitive mechanisms, as in the investigation of visual short-term memory (VSTM). The hypothesis that the bilateral increase of BOLD response in the parietal cortex found in functional magnetic resonance imaging (fMRI) studies [Robitaille et al., *Neuroimage*, 2010], and contralateral parietal increases in event-related negativity, found in electrophysiological works [Luria et al., *Journal of Cognitive Neuroscience*, 2010], might be different reflections of the same underlying neural/functional processing is here investigated in a synchronous recording of event-related potential (ERP) and fNIRS signals. Given the lack of a standard method for fNIRS signal processing, a new method to estimate stimulus-evoked HR from fNIRS measurements within an event-related paradigm is proposed.

### **Material and Methods:**

The signal is acquired in EEG-fNIRS co-registration sessions from three subjects performing a variant of the change-detection task proposed in a previous study [Cutini et al., *Neuropsychologia*, 2011], which was based only on fNIRS recordings. A new filtering technique for HR estimation is developed, based on the exploitation of a “reference” channel characterized by a source-detector distance less than 1 cm. Signal from the reference-channel is exploited to estimate a parametric model of the physiological noise, which is then used to correct the recordings from the remnant “standard” channels (with source-detector distance of 3 cm). Then residual random noise is reduced by adopting a Bayesian filtering approach, designed on a single-trial basis [Scarpa et al., *Optics Express*, 2010].

### **Results and Conclusions:**

As expected, results from EEG data show that maintenance of unilaterally encoded objects elicits unilateral (contralateral) an increase in event-related negativity in parietal cortex which is proportional to the number of objects retained in visual short-term memory. Results from fNIRS data show that maintenance of bilaterally encoded objects elicits bilateral increases of hemodynamic activation in IPS-IOS cortex, proportional to the number of objects retained in visual short-term memory, with increased hemodynamic activity in the contralateral IPS–IOS relative to the ipsilateral condition. The present findings suggest that EEG and fMRI/fNIRS techniques reveal distinct neural signatures of the mechanisms supporting visual short-term memory.

fNIRS results are obtained with the previously described filtering technique and are in agreement with recent findings [Cutini et al., *Neuropsychologia*, 2011]. On the contrary, results obtained with the standard block-average technique do not show an increased hemodynamic activity proportional to the number of objects retained in visual short-term memory, whereas such increase is instead found in fMRI studies [Robitaille et al., *Neuroimage*, 2010]. This suggests that the proposed filtering technique leads to a more correct estimation of the hemodynamic response with respect to standard methods.

## Measurements of Hemoglobin Concentration of the Deep Brain Tissue Using Near-Infrared Time-Resolved Spectroscopy

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### 1. Objective

In near-infrared time-resolved spectroscopy (NIR-TRS), we found that an optical pulse irradiated to an ear canal could be detected safely at the other ear canal by the means of a highly sensitive photon counting technique. The temporal profiles could also be obtained by a time-correlated single photon counting (TCSPC) method. It is expected that these profiles contain the hemodynamic information of the deep brain area including the brain stem which is responsible for human life-sustaining. Using a highly sensitive TRS system, improved version of TRS-10 [1], we have tested fifty healthy adult volunteers to estimate the hemoglobin information of the deep brain based on photon diffusion theory.

### 2. Method

We developed a highly sensitive TRS system with high-power light source called “Nanosecond Light Pulsers (NLPs)”. NLPs emit light pulses at 760nm, 800nm and 830nm, with a total average power of 3mW. We also employed a detection fiber which raised photon collection efficiency (numerical aperture was 0.56) and a highly-sensitive photomultiplier tube with a GaAs photocathode.

Fifty adult volunteers (mean age  $40.2 \pm 11.4$  years, range: 23 to 61 years old; 41 men and 9 women) were studied. To measure the hemodynamics of the deep brain in the resting state, the NIR pulsed light was irradiated to the right ear canal and the photons that passed through the brain tissue were collected at the left ear canal. The subjects themselves adjusted the position and the direction of the fiber so that the signal intensity was maximized.

### 3. Results

Optical signals with sufficient intensity were successfully obtained from 46 persons of the fifty volunteers. The mean of the optical path-length was  $40.8 \pm 3.9$  cm at 800nm. The theoretical curves derived from the photon diffusion equation [2] were fitted to the measured temporal profiles in order to determine the reduced scattering and absorption coefficients at each wavelength. Then oxyhemoglobin ( $\text{HbO}_2$ ), deoxyhemoglobin (Hb), total hemoglobin (tHb) and tissue oxygen saturation ( $\text{SO}_2$ ) were calculated. The average values of  $\text{HbO}_2$ , Hb, tHb and  $\text{SO}_2$  were  $26.3 \pm 5.0 \mu\text{M}$ ,  $18.8 \pm 2.2 \mu\text{M}$ ,  $45.1 \pm 6.8 \mu\text{M}$  and  $58.0 \pm 3.5\%$ , respectively.  $\text{SO}_2$  values of the deep brain were on average  $10.1 \pm 2.4\%$  lower in contrast to the results at the forehead (correlation coefficient:  $r=0.73$ ). Moreover, tHb values of the deep brain were always lower than the forehead results.

### 4. Conclusion

We have developed a highly sensitive TRS system and performed hemodynamic measurements of the deep brain area in fifty adult volunteers. The results demonstrated a potential applicability of this system to examine deep inside the brain.

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## Brain Response to Painful versus Non-Painful Electrical Stimuli

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Awareness under general anesthesia can have significant consequences including the development of posttraumatic stress disorder. Inadequate surgical anesthesia leading to chronic pain is a common and late sequelae of surgical incisions affecting approximately 30% of all surgical patients. Therefore, there is a need for a robust and objective measure of pain sensation to guide surgical anesthesia to reduce the occurrence of post-operative sequelae. Previous studies using noxious and innocuous heat stimulation show that it is possible to discern painful stimuli from non-painful stimuli based on the temporal and spatial characteristics of the response in somatosensory cortex and frontal brain areas. Based on these studies, noxious stimuli produce a prolonged or biphasic response whereas innocuous stimuli produce a response similar to other evoked hemodynamic response. In this study, we sought to detect the hemodynamic response in somatosensory cortex and in frontal brain areas to innocuous and noxious electrical stimulation using diffuse optical tomography (DOT) in healthy volunteers. We wanted to see whether the noxious electrical stimulus also produces a biphasic response similar to noxious thermal stimulus. We have integrated in the optical fibers into an elastic cap from EasyCap using custom designed optode ring holders that greatly facilitates placement of the fibers on the head and adjustment of any hair obscuring the optical signal. Moreover, to filter out the global physiological changes, we included a short separation detector next to each source in addition to the long distance detectors. We performed measurements at 690 and 830 nm to obtain sensitivity to changes in oxygenated, deoxygenated hemoglobin and total blood volume changes on 5 healthy volunteers. Our results show that the response to noxious electrical stimuli is highly subject dependent, however it is clearly more pronounced compared to innocuous stimuli. The addition of short separation detectors helped improve the localization of the response.

## An exploratory fNIRS study with immersive virtual reality

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**Introduction.** Virtual Reality (VR) is a useful instrument in several fields and has reached a considerable value in medical, psychological, and neuropsychological treatments (e.g., Tomikawa et al., 2010). Nevertheless, neuroimaging techniques might be very helpful in supporting the VR usefulness in these research fields. Nowadays, functional magnetic resonance imaging (fMRI) is the most commonly used brain imaging technique; fMRI monitors brain activity by using blood oxygen level dependent (BOLD) responses. A major obstacle with fMRI to study the neural correlates of VR experiences regards the “immersion” within the artificial environment. Huge machinery dimensions, disturbing noise, the horizontal and unnatural position of the participant during brain scan, constitute some of the most limiting factors in the use of fMRI with VR. Crucially, functional near-infrared spectroscopy (fNIRS) is cheap, portable and allows the easy use of an adapted Head Mounted Display (HMD) to grant a full immersion into the virtual environment. In the present study we investigated the possibility to implement fNIRS while participants experienced immersive VR. The aim of the study was to investigate whether a modified HMD helmet is suitable for correct signal acquisition with fNIRS in an immersive environment during a visuo-spatial task, such as line bisection.

**Method.** Eight right-handed participants (7 males; 27.6 years: 24–36) participated in the experiment after providing their informed consent. Bilateral hemodynamic activity of the parieto-occipital was recorded with a multi-channel frequency-domain fNIRS (ISS Imagent™, Champaign, IL), equipped with 32 laser diodes (16 emitting light at 690 nm, and 16 at 830nm) modulated at 110MHz, and 4 detectors. Optodes were placed using a recent probe placement method (Cutini et al., 2011). Participants viewed the virtual environment through an adapted V8 Research HMD attached to a modified bike helmet (provided of an intersense tracker) and an fNIRS holder, in order to reach brain areas from the fNIRS optical fibers. The virtual environment was created using 3DStudioMax 8.0 (for the development of three-dimensional objects) and Virtools 3.5 (for the interaction with them). A virtual room was created with a “wooden” table in the center: above and aligned with the table’s center, there was a white panel (50×50 cm) for displaying horizontal lines. There were two viewer-line distances: 60 cm and 120 cm. The lines to be bisected were 4–8 cm-long at the distance of 60 cm, and 8–16 cm-long at the distance of 120cm. Participants bisected the lines using a Nintendo Wiimote® controller (simulating a laser pointer). The Wiimote moved a 2.5mm red dot as a simulation of the same one represented by a real laser pointer. The ‘A’ button on the Wiimote served to memorize the response (i.e., the last point of contact over the line) and to switch to another line and/or distance.

**Results.** We observed statistically significant oxygenated hemoglobin (HbO) activity in most of the occipital and parietal channels. In particular, a pronounced HbO activation was observed in a right parietal channel (PR1) during virtual line bisection. To provide a solid proof in regard to the reliability of the hemodynamic response observed in channel PR1, we compared its activity with that of the symmetrical channel on the left hemisphere (PL1). Interestingly, we observed a marginally significant difference between PR1 and PL1 activities ( $p = .077$ ,  $t(6) = 1.628$ , one tailed t-test).

**Discussion.** Results indicated the involvement of the parietal and occipital lobes during line bisection, with a predominance of the right parietal cortex. These results are consistent with previous investigations, which have found parietal activation right hemisphere predominance during attention, space perception and visuo-spatial tasks, such as line bisection (e.g., Fink et al., 2000). In conclusion, the present findings provide solid evidence that fNIRS can be efficiently used during the exploration of virtual immersive environments and can provide a valuable support to VR applications.

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## Examining Resting State Functional Activity in the Medial Prefrontal Cortex Using fNIRS: A “Proof-of-Concept” Study

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### ABSTRACT

The use of functional near-infrared spectroscopy (fNIRS) to examine functional connectivity among cortical regions has become a focus of recent fNIRS research (e.g., Medvedev et al., 2011; Sasai et al., 2011; Sasai et al., 2012). The proposed poster will present the results of a “proof-of-concept” analysis of the feasibility of using fNIRS to conduct resting state functional connectivity analyses in the prefrontal cortex. Specifically, the results of an analysis of resting state connectivity of medial prefrontal cortical areas across hemispheres will be presented.

Data obtained from a study using fNIRS to examine characteristics of diurnal cerebral blood flow during routine daily activities (Brinckman et al., manuscript in preparation) were analyzed to determine whether patterns of functional connectivity could be detected during the resting state. In the original study, changes in oxygenated hemoglobin (oxy-Hb) and deoxygenated hemoglobin (deoxy-Hb) concentrations during alternating 5-minute rest and 25-minute low cognitive demand activity periods were observed over the course of an eight-hour day. A 16-channel continuous wave NIRS system, provided by the Optical Brain Imaging Group of the School of Biomedical Engineering at Drexel University, was used to measure the time course of hemoglobin concentration change within and across study conditions. Data obtained from four healthy, non-smoking, English-speaking, right-handed female participants during rest were analyzed in the current study. Rest sessions in which at least three of four prefrontal medial voxels in each hemisphere (voxels 5-8 in the left hemisphere and 9-12 in the right) yielded interpretable signals were chosen for analysis. Average bivariate correlation coefficients for both oxy-Hb and deoxy-Hb within and across hemispheric voxel groups were calculated in order to examine both intra- and interhemispheric connectivity. Strong average intercorrelations ( $r=0.72-0.80$ ) were found for oxy-Hb, both within each hemisphere and across hemispheres; similarly, moderate to strong average intercorrelations ( $r=0.41-0.59$ ) were found for deoxy-Hb within each hemisphere and across hemispheres. Limitations and directions for future research will be discussed in the proposed poster presentation.

Driving errors and cerebral hemodynamics during simulated driving with and without hands-free telecommunication: It's not about where your hands are, it's about where your mind is

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**Background:** Technological advancements during the last two decades have led to a tremendous increase in the use of hands-free telecommunication devices during automobile use. Handling distractions while driving increases the cognitive load which is evident by an increase in neuronal activation in the prefrontal cortex. Near infrared Spectroscopy (NIRS) directly measures neuronal activation, which is evident by an increase in the concentration of oxy- hemoglobin (HbO<sub>2</sub>) and a concomitant decrease in the concentration of deoxy-hemoglobin (HHb). **Purpose:** In order to gain a better understanding of neural mechanisms during distracted driving, the changes in the acute cerebral hemodynamics need to be investigated. The aims of the study were to examine the: (1) behavioral effects of hands-free telecommunication use during simulated driving, (2) reliability of cerebral NIRS variables during this task, and (3) relationship between the number of driving related errors during distracted driving with the changes in the NIRS variables. **Methods:** 26 male participants drove in a simulated urban scenario (VS500M, Virage Simulation, Canada), without (4 minutes) and with (2 minutes) naturalistic conversation using a hands-free earpiece on two separate occasions. The cerebral hemodynamic responses were recorded by dual-wave NIRS from the left prefrontal lobe using a dual wave instrument (Oxymon Mk III, Artinis Medical Systems, The Netherlands). Driving errors were counted under both conditions and the delta values of the NIRS data were computed. **Results:** Driving with hands-free telecommunication led to a 175% increase in driving errors. During the telecommunication conversation, two distinct trends were observed in the NIRS responses: (1) increased neuronal activation as evidenced by a systematic increase in HbO<sub>2</sub> with a concomitant decrease in HHb in 64% of the participants, and (2) decreased neuronal activation (ie. deactivation) as evidenced by a significant decline in HbO<sub>2</sub> with a concomitant increase in HHb in 12% of the participants. Driving related errors, NIRS variables, between the two trials were highly reproducible (ICC between 0.44 and 0.64). There were no significant correlations ('r' values between -0.24 and 0.33) between the incidence of driving responses and the changes in the NIRS variables. **Conclusions:** NIRS is a suitable technique to reliably measure the acute changes in the cerebral hemodynamic responses during functional tasks. The increased incidence of errors during hands free telecommunication under simulated driving conditions does not seem to be associated with specific changes in the cerebral hemodynamics due to the large inter-individual variability amongst the participants.

The Neural Correlates of the Face Attractiveness Aftereffect:  
A Functional Near-infrared Spectroscopy (fNIRS) Study

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Adults' expertise in recognizing individual faces has been attributed to norm-based coding, a process by which individual faces are compared to a prototypical face that represents the average of all faces previously encountered. Extensive behavioral evidence shows that our internal representation of faces, or face prototype, can be dynamically updated by immediate experience. This is illustrated by the robust attractiveness aftereffect phenomenon whereby originally unattractive faces (e.g., faces with compressed features) become attractive after we are exposed to a set of similarly unattractive faces. Although behavioral evidence suggests this effect to have a strong neural basis, little neuroimaging evidence in fact exists. Here we used functional near-infrared spectroscopy methodology (fNIRS) to bridge this gap. In the pre-test, participants rated the attractiveness of three sets of faces: normal and undistorted faces, compressed faces (the internal features and the distances between them were compressed), and expanded faces (the internal features and the distances between them were expanded). We then showed participants a new set of compressed faces for 5 minutes, a process called adaptation, after which participants judged the same three sets of faces in the post-test. After adaptation, participants rated compressed faces as more attractive and both undistorted and expanded faces as less attractive, replicating the robust adaption aftereffect. fNIRS results showed that short-term exposure to compressed faces led to significant decreases in [oxy-Hb] activities to undistorted faces in the extended network of cortical regions in the frontal and occipital cortexes. In contrast, significant decreases in [oxy-Hb] activities were only observed in the right middle frontal gyrus to the compressed faces and the left middle frontal gyrus to the expanded faces. These differential responses to the three sets of faces suggest that the attractiveness face adaption effect for the three sets of faces may have different neural bases. The greater involvement of cortical regions in the adaptation of the undistorted faces suggests that adaption may have the greatest impact on the normative face prototype. Functional connectivity analyses further revealed that in response to the undistorted faces, changes in [oxy-Hb] activities to the undistorted faces in the right inferior frontal regions were bi-directional and mutually affecting each other. Taking together, the present findings suggest that the face attractiveness aftereffect mainly reflects the neural representation of the face prototype in response to recent exposures to new face exemplars.

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## Cerebral &amp; Muscle Hemodynamics during Unilateral Knee Extensions at Different Loads &amp; Velocities

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**Background:** Muscle fatigue is a transient phenomenon which is task dependent and can originate centrally and/or peripherally (Gandevia et al., 2001). Currently the physiological factors implicated in fatigue during resistance exercise are poorly understood. Near infrared spectroscopy (NIRS) is a valid and reliable non-invasive optical technique that is used to measure central neuronal activation (Huppert et al., 2006) and muscle oxygen extraction (Mancini et al., 1994) during exercise. **Purpose:** The current study used NIRS to examine the relationship between fatigue during dominant knee extensions (KE) at two different loads (60% and 80% of predetermined 1RM) and velocities ( $25^{\circ}\cdot s^{-1}$  and  $80^{\circ}\cdot s^{-1}$ ) and the alterations in cerebral and muscle oxygenation (Cox, Mox) and blood volume (Cbv, Mbv) in healthy volunteers. **Methods:** Six males and 3 females ( $35.8\pm 10.8$  yrs;  $74.2\pm 16.7$  kg;  $171.0\pm 10.0$  cm) completed one set of KE to task failure with the dominant leg at each load and velocity in random order in one testing session. NIRS measurements were recorded simultaneously from the contralateral prefrontal lobe and dominant vastus lateralis during 2 min rest, KE to fatigue, and 3 min recovery as previously described (Gomes et al., 2012). Delta and Range in Cox, Cbv, Mox and Mbv were computed for each load and velocity. **Results:** Total work index (TWi, calculated as the product of load and number of repetitions) was significantly greater at  $25^{\circ}\cdot s^{-1}$  compared to  $80^{\circ}\cdot s^{-1}$  for each load. During the contractions, *Cox and Cbv increased systematically* until task failure with no signs of attenuation or plateau. In contrast, *Mox and Mbv demonstrated a rapid decline* followed by a plateau or slight increase until task failure. No significant ( $P > .05$ ) correlations were observed between TWi and Delta Cbv or Mbv when the loads and velocities pooled ( $N = 18$ ). The correlation coefficients between TWi and Delta Cox and Delta Mox for the pooled data are summarized below.

Method	Delta Cox	Probability	Delta Mox	Probability
Loads pooled at $25^{\circ}\cdot s^{-1}$	0.48	> .05	<b>0.55</b>	< .05
Loads pooled at $80^{\circ}\cdot s^{-1}$	<b>0.52</b>	> .05	<b>0.63</b>	< .05
Velocities Pooled at 60% 1RM	0.42	> .05	0.39	> .05
Velocities pooled at 80% 1RM	0.41	> .05	<b>0.59</b>	< .05

**Conclusions:** These findings suggest that fatigue during unilateral KE is more closely correlated with the decline in muscle oxygen utilization and not by a reduction in central neuronal activation. The decline in Mox is attributed to the decrease in Mbv (an indirect measure of blood flow) to the exercising muscle which results in a reduction in oxygen availability and utilization.

## Verbal and visual working memory investigated by multi-channel time-resolved functional near-infrared spectroscopy

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**Introduction.** Working memory (WM) is a core component of human cognition and it is fundamental for a number of different cognitive processes. WM allows the short-term maintenance and manipulation of the information selected by attentional processes. Some of the most common neuropsychological tests for evaluating the WM abilities are the forward and backward digit span (DF and DB, respectively), and the symbol span (SS) tasks [1]. In DF the maintenance of the verbal information entering the phonological loop is demanded, whereas DB requires the manipulation of the information contained in verbal WM [2]. Brain imaging studies suggested that the neural substrates of WM reside in the prefrontal cortex (PFC) [3, 4]. More specifically, the ventrolateral PFC (VLPFC) (Brodmann Areas, BA: 44/45/47) and the dorsolateral PFC (DLPFC) (BA: 9/46) are believed to be involved in active manipulation of information while the BA10 and 11 are thought to be responsible for the maintenance of information. Indeed, an fMRI investigation of WM revealed a greater right activation of BA10 during the DF, and a greater activation of BA 9/46 during the DB [5]. Similarly, in a study performed with time-resolved fNIRS, a strong activation of DLPFC (i.e., increase of oxy-haemoglobin, O<sub>2</sub>Hb) was observed during the DB [3].

**Aim.** The goal of this study was to examine by time-resolved fNIRS the neural correlates of the verbal and visual WM during DF, DB and SS tasks. A neural dissociation was hypothesised between maintenance and manipulation processes. In particular, a DLPFC/VLPFC recruitment was expected during the DB task, whilst a lateralised involvement of BA10 was expected during the execution of the DF task.

**Methods.** Thirteen subjects were monitored by an 18-channel, dual wavelength (690 and 829 nm) time-resolved fNIRS system (sampling time: 1 Hz) developed at Politecnico di Milano [6]. The optodes were positioned according to the international 10-10 system. The experiment included three blocks (one for each task: DF, DB and SS) counterbalanced across participants. The DB and DF protocols lasted 3 min, while the SS protocol 4 min. During the DF or DB task, participants repeated a series of digits in the same or reverse order of presentation. The digit sequences started with a span of 3 (for DF) or 2 digits (for DB), and increased in steps of 1 digit until the participants failed 2 sequences within the same span level. During the SS task, the participants memorized a series of stylized and uncommon images of increasing number (from 3 to 7 images) until they failed 2 series within the same span level. The participants' memory span (calculated for each task) corresponded to the highest level in which at least one sequence out of two was correctly reproduced.

**Results.** The mean span level for DF, DB and SS was  $6 \pm 1.1$ ,  $6 \pm 1.3$  and  $5 \pm 1.3$  elements, respectively. No correlation was found between the span level and the heart rate data (monitored by pulse oximetry). As expected, DB elicited a broad activated area (measured as O<sub>2</sub>Hb increase) in the bilateral VLPFC and the right DLPFC, whereas a more localized activation was observed over the right hemisphere during either DF (BA10) or SS (BA10 and BA44).

**Discussion.** The results of the present study confirm those of previous studies in which right DLPFC was found particularly activated during DB [3, 5]. The activation of the PFC in the 3 tasks is related to cognitive processing and maintenance of the information. The robust involvement of the DLPFC during DB, compared to DF, is compatible with previous findings [3-5, 7] and with the key role of the central executive in manipulating processes.

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### **Being social: a NIRS study on the Social Simon effect**

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Cognitive neuroscientists have predominantly studied individual brains in isolation. Recently, however, it has been argued for the need of taking a social perspective on cognitive activities. The aim of the present study is to investigate the neuronal underpinnings of sharing a task in a proper social context.

We recorded cortical activity by means of near-infrared spectroscopy, while participants performed a joint Simon task. At the behavioural level, we found faster RTs to compatible as compared to incompatible trials, albeit each participant was actually performing a go/no-go task. This result suggests participants integrated the potential action of their co-actor in their own action. Regarding the neural activity, we found higher activation in the left ventral premotor cortex and left inferior parietal lobule while processing incompatible as compared to compatible trials referring to one’s own action alternative. Strikingly, when participant was not responding, because it was the turn of the other member of the pair, the same inferior parietal activation was stronger to incompatible as compared to compatible trials while the left ventral premotor cortex was not activated. These findings suggest that the joint Simon effect relies more on shared attentional mechanisms rather than a proper mapping of the other’s motor response.



## Cerebral hemodynamic responses during carbon dioxide rebreathing, aerobic exercise and cognitive activity

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Cerebrovascular reactivity to  $\text{CO}_2$  ( $\text{CvCO}_2$ ) is the dilatory response of brain circulation to the  $\text{CO}_2$  stimulus. It may represent a marker of individual response to physical and cognitive load.  $\text{CvCO}_2$  at different levels of activity and fitness has not been studied. Neither has there been a consistent indication of the relationship between cognitive function and  $\text{CvCO}_2$ . Further, no studies to date have directly investigated the relationship between cerebral hemodynamic changes in response to rebreathing  $\text{CO}_2$ , cognitive activity and varying fitness levels. Knowledge of the nature of these relationships may clarify how these various aspects of cerebral hemodynamic function operate at various stages of health and disease.

**Purpose:** This study investigated changes in concentration of oxyhemoglobin [ $\text{O}_2\text{Hb}$ ], deoxyhemoglobin [ $\text{HHb}$ ] and total hemoglobin [ $\text{tHb}$ ] during  $\text{CO}_2$  rebreathing, aerobic exercise and cognitive testing in healthy males. It was hypothesized that the changes in [ $\text{tHb}$ ] and [ $\text{O}_2\text{Hb}$ ] during  $\text{CO}_2$  rebreathing will be positively correlated with these same hemodynamic measures obtained during tasks of attention and memory, and sub maximal aerobic exercise.

**Methods:** Informed consent was obtained from eleven males (20-58yrs, predicted  $\text{V}\text{O}_{2\text{max}} = 35.06 \pm 8.5 \text{ml/kg/min}$ ;  $\text{BMI} = 22.10 - 28.73$ ) with high school to university graduate level education. Participants performed three procedures in random order up to two weeks apart. The procedures included rebreathing 5% $\text{CO}_2$  for up to 90 seconds in an upright seated position, seated cycling at a sub maximal level for 6 – 8 minutes on an electronically-braked cycle ergometer, and completing a digit span test (a three part test of working short term memory). Single channel near infrared spectroscopy (NIRS) was used to measure hemodynamic responses over the left prefrontal lobe (PFC) during the three procedures. Delta (peak minus baseline) values of [ $\text{tHb}$ ], [ $\text{O}_2\text{Hb}$ ] and [ $\text{HHb}$ ] were used for statistical analysis.

**Results:** NIRS trends for all three test conditions demonstrated hemodynamic changes that were indicative of enhanced neuronal activation: increase in [ $\text{O}_2\text{Hb}$ ] with a concomitant decrease in [ $\text{HHb}$ ]. Delta values of [ $\text{O}_2\text{Hb}$ ], [ $\text{HHb}$ ], and [ $\text{tHb}$ ], measured during  $\text{CO}_2$  rebreathing and sub maximal cycling, were not significantly correlated ( $P > .05$ ). For Delta [ $\text{O}_2\text{Hb}$ ], there was a significant negative correlation ( $P < .05$ ) between  $\text{CO}_2$  rebreathing and two portions of cognitive testing; namely, digit span forward ( $r = -0.555$ ) and digit span sequencing ( $r = -0.770$ ). There were also significant negative correlations between sub maximal cycling and these two cognitive measures for Delta [ $\text{O}_2\text{Hb}$ ]. Delta [ $\text{tHb}$ ] was significantly negatively correlated for cycling and digit span forward ( $r = -0.788$ ). Additionally, significant correlations were noted on measures of Delta [ $\text{HHb}$ ] for sub maximal cycling and digit span forward ( $r = 0.641$ ) and digit span sequencing ( $r = 0.701$ ).

**Conclusion:** The significant negative correlations between Delta [ $\text{O}_2\text{Hb}$ ] during  $\text{CO}_2$  rebreathing and parts of digit span testing were inconsistent with our hypothesis. This was also the case for hemodynamic changes in  $\text{CO}_2$  rebreathing and cycling. Negative correlations between cycling and cognitive testing, along with positive correlations with [ $\text{HHb}$ ], suggest that oxygenation changes during these three experimental conditions may be operating under different physiological mechanisms. The use of a single channel NIRS procedure and a heterogeneous sample are notable limitations associated with this study.

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**Prefrontal cortex is not activated by observation of disgusting and pleasant pictures:  
a multi-channel time-resolved functional near-infrared spectroscopy study in healthy subjects**

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**Introduction.** The disgust is one of the basic emotions with a central role not only in the social environment, but also in the manifestation of psychiatric disorders. The DSM IV [1] includes the horror in the diagnostic criteria of the Post-Traumatic Stress Disorder (PTSD) defining it as one of the feelings that occur following to a traumatic event (such as the earthquake that occurred in 2009 at L'Aquila town - Italy). Although disgust perception has been mainly investigated in patients by passive viewing of emotional pictures related to trauma or disorder [2], a limited number of studies has investigated the neural circuits involved in healthy individuals. An important role in the cognitive control of affective responses is played by the prefrontal cortex (PFC) [3]. Although there is evidence that the PFC is activated in response to emotional visual stimuli [4], few studies have confirmed the role of the PFC in the disgust perception [5]. So far, only few fNIRS studies have investigated the brain activation of healthy subjects during the perception and the imagery of neutral, happy, and disgusting stimuli. However, these studies examined the occipital and parietal cortex only [6, 7].

**Aim.** The goal of this study was to evaluate by fNIRS the role of the PFC in the disgust perception of healthy subjects during the exposure to disgusting, pleasant and neutral stimuli. A different activation pattern over the PFC is expected in response to the three conditions.

**Methods.** Nineteen healthy males subjects (29.7±4.1 y.o.; high level of education) were monitored by an 18-channel, dual-wavelength (690 and 829 nm) time-resolved fNIRS (sampling time: 1 Hz) developed at the “Politecnico di Milano”. The optodes were positioned over the frontal cortex according to the international 10-10 system. The heart rate was monitored by a pulse oximeter. The stimuli were divided into six blocks of five disgusting, pleasant or neutral images (two blocks for each condition). The 30 different images were taken from International Affective Picture System (IAPS) [8] and presented in a random order. Each block was presented for 30-sec and was separated by the others by a 1-min inter-block interval. Optical recording started 2-min before the onset of the first picture and ended 1-min after the offset of the last picture (protocol duration: 11-min). At the end of the study the subjects were administered with a questionnaire regarding the perception of the images. The participants rated each image on a scale from 1 to 7 (where 1 indicated a high level of repulsion toward the stimulus, 4 indicated indifference toward the stimulus, and 7 indicated high level of attraction toward the stimulus).

**Results.** The mean values attributed to the disgusting, neutral and pleasant images were: 2.2±0.7; 4.2±0.2; 5.6±0.4, respectively. In contrast with the behavioural data, the different emotional valence of the images did not significantly affect the haemodynamic response patterns observed in the PFC. Finally, the heart rate did not change significantly between the baseline and task period.

**Conclusions.** Although the images were perceived as disgusting, neutral and pleasant, no PFC modulation in response to the different images was found by time-resolved fNIRS on healthy subjects. Despite the lack of positive results, a PFC activation during passive viewing of disgusting images cannot be excluded in PTSD patients or in those affected by other psychiatric disorders.

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## Quantification of Cerebral Hemoglobin in Adult Brain Using Near-Infrared Spectroscopy

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## INTRODUCTION

Historically quantification of total hemoglobin (tHb) has been a challenge for near-infrared spectroscopy (NIRS), however success in quantification would allow us to compare between subjects for parameters such as tissue saturation and microvascular oxygenation<sup>1</sup>. This would be widely applicable in for monitoring brain hypoxia in conditions such as stroke or diseases of aging.

Quantification is possible using frequency-domain NIRS systems<sup>2</sup>. Our objective was to determine if consistent quantified levels of cerebral hemoglobin can be measured with NIRS.

## METHODS

Measurements were taken using the OxiplexTs (ISS), a frequency domain NIR system, which measures absolute tissue oxygen saturation (StO<sub>2</sub>) as well as THb, oxyhemoglobin (OHb) and deoxyhemoglobin (HHb) concentrations. Each optode has one light detector and eight emitters, four emitting light at 834nm and four emitting light at 692nm at varying distances between the source detectors.

Seven subjects were included (2 male, 5 females; age 37.9± 13.2 years, mean±SD). This study used a repeated measures design. Each participant was required to undergo six study sessions on six different days. Frontal lobe measurements were taken for one minute on each hemisphere, under quiet and dark conditions. Analysis included descriptive statistics, between-subjects one-way ANOVAs and paired t-tests to compare between hemispheres.

## RESULTS and DISCUSSION

The average between-subject coefficient of variation for the right frontal lobe was 1.42% for StO<sub>2</sub>, 1.13% for tHb, 2.3% for OHb and 1.88% for HHb. Slightly greater variation was found for the left frontal lobe. The dataset includes variations when measuring the same subject over time, and when comparing a normal patient population.

These results show that very consistent values can be obtained both between subjects and when comparing the same subject over time when quantifying using the Oxypex, time domain system. Such a system allows for applications such as determining if an acute stroke patient differs in saturation from that of an age matched control population.

Right Frontal Lobe				Left Frontal Lobe			
StO <sub>2</sub> (% ±SD)	tHb (μM ±SD)	OHb (μM ±SD)	HHb (μM ±SD)	StO <sub>2</sub> (% ±SD)	tHb (μM ±SD)	OHb (μM ±SD)	HHb (μM ±SD)
63.3 ±0.9	41.2 ±0.5	26.2 ± 0.6	15.0 ± 0.3	63.5 ±1.0	38.0 ±0.6	24.2 ± 0.7	13.7 ± 0.3

**Table 1.** Values indicate overall average values for each parameter, with data from all subjects combined. Results are comparable with values reported in the literature by one different study using similar methodology<sup>2</sup>. Measurements were also take for OHb and HHB but are not presented here.

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Poster Session  
**Applications: Adult (II)**  
Poster #: 84-103

## Cerebral Hemodynamics at Altitude: Effects of Hyperventilation and Acclimatization on Cerebral Blood Flow and Oxygenation

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**Introduction:** High altitude has profound cerebrovascular effects on those that work, live, or are stationed at greater than 2400 m. For them, high altitude cerebral edema is a common cause of death, and the only currently used treatment is immediate descent.

We hypothesize that we can use methods proven to successfully treat brain-injured patients to help those with altitude illness without having to descend. The simplest example is hyperventilation, which can be used to decrease cerebral blood flow and, therefore, intracranial pressure.

Diffuse correlation spectroscopy (DCS) could provide a non-bulky, fairly lightweight instrument to probe changes in blood flow at altitude. The aim of this study is to test the feasibility of using DCS as a monitor of relative cerebral blood flow (rCBF) at high altitude during hyperventilation.

**Materials and Methods:** We used a house-built, two-channel DCS module. Source-detector separation used was 2.5 cm, with relative cerebral blood flow (rCBF) data being taken every 3 seconds. A commercial near-infrared spectroscopy (NIRS) device, the Fore-sight Absolute Cerebral Oximeter, measured cerebral tissue oxygen saturation (StO<sub>2</sub>). A transcranial Doppler ultrasound (TCD) instrument to measure peak systolic velocity (PSV) and a capnograph for end-tidal CO<sub>2</sub> were also used.

The twelve otherwise healthy subjects ranged in age from 22 to 80. None had travelled to altitude during the previous three months, nor had any history of cardiovascular, respiratory or neurological disease.

A hyperventilation protocol was repeated on the same subjects at three different time-points: 1) 75 m above sea level, 2) 4559 m above sea-level after 2 days of being at altitude, 3) 4559 m above sea-level after 7 days of being at altitude. Subjects ascended to the Capanna Regina Margherita in the Italian Alps by cable car and on foot, with 2 days spent acclimatizing at 3611 m.

Subjects were positioned supine, and probes for DCS, TCD, and NIRS were attached to their forehead. Baseline data were taken for 5 minutes. Then subjects were asked to hyperventilate to 50% of their baseline end-tidal CO<sub>2</sub>, and asked to maintain this level for 3 minutes. A mixed effects model was used to test relevant hypotheses.

**Results:** Out of 12 initial subjects, data were collected on 9 after two days at altitude, and on 7 after seven days at altitude. Subjects dropped out for reasons such as altitude mountain sickness.

DCS revealed a decrease in rCBF of -20.9% (95% CI, -31.3, -10.3) following hyperventilation at sea level, -24.5% (-36.7, -12.4) following hyperventilation after 2 days at altitude and -37.6% (-51.3, -23.8) following 7 days at altitude. There was a trend towards more pronounced decreases in CBF with hyperventilation with increasing time at altitude that approached, but did not reach, statistical significance ( $p = 0.051$  between sea-level and altitude day 7). PSV also decreased with hyperventilation at all three time-points ( $p < 0.001$ )

StO<sub>2</sub> decreased with hyperventilation at sea level ( $p < 0.001$ ), but increased after 2 days at altitude ( $p = 0.001$ ). After 7 days, there was no significant difference with hyperventilation.

**Conclusion:** Hyperventilation induced lowered rCBF and PSV both at sea-level and at altitude. DCS was shown to be a promising technology with the potential to increase our understanding of changes in cerebral blood flow at altitude. Larger studies and further refinements in technique are necessary to reduce inter-subject variability.

## Reduction of Cytochrome *c* Oxidase During Vasovagal Hypoxia-Ischaemia in Human Adult Brain: a Case Study

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Near infrared spectroscopy (NIRS)-derived measurement of oxidised cytochrome *c* oxidase concentration ([oxCCO]) has been used as an assessment of the adequacy of cerebral oxygen delivery. We report a case in which changes in conscious level were associated with changes in [oxCCO].

Hypoxaemia was induced in a 31 year-old, healthy male subject by delivery of a hypoxic inspired gas mix; this was part of an on-going clinical study. NIRS monitoring was performed with the hybrid optical spectrometer (pHOS), which comprises multidistance broadband and frequency domain spectrometers and is described elsewhere<sup>1</sup>. The pHOS measured changes in [oxCCO], oxyhaemoglobin and deoxyhaemoglobin ([HbO<sub>2</sub>] and [HHb], respectively) at four different source-detector separations (35/30/25/20mm) and optical scattering at four discrete wavelengths (690/750/790/850nm). The haemoglobin difference ([HbDiff] = [HbO<sub>2</sub>] – [HHb]), was calculated. Other monitoring included transcranial Doppler ultrasound measurement of ipsilateral middle cerebral artery flow velocity (Vmca), pulse oximetry to measure arterial oxygen saturation (SpO<sub>2</sub>), and continuous non-invasive arterial blood pressure (ABP); the latter two variables were used to calculate estimated changes in cerebral oxygen delivery ( $\Delta ecDO_2 = \Delta SpO_2 \times \Delta Vmca$ )<sup>2</sup>.

Midway through the hypoxaemic challenge, the subject experienced an unexpected vasovagal event with bradycardia, hypotension and reduction in cerebral blood flow and *ecDO*<sub>2</sub> (Figure 1). An associated decrease in [oxCCO] was observed at 35mm (-1.6  $\mu$ M), but only minimal change (-0.1  $\mu$ M) at 20mm source-detector separation (Figure 2). A change in optical scattering was observed, but pathlength remained unchanged. This unexpected physiological event provides an unusual example of a severe reduction in cerebral oxygen delivery and is the first report correlating change in clinical status with changes in [oxCCO].

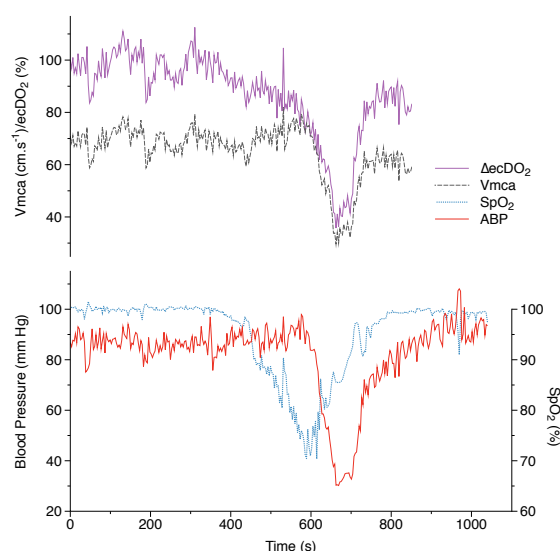


Figure 1: change in ABP, SpO<sub>2</sub> and consequent reductions in Vmca and *ecDO*<sub>2</sub> observed during vasovagal event.

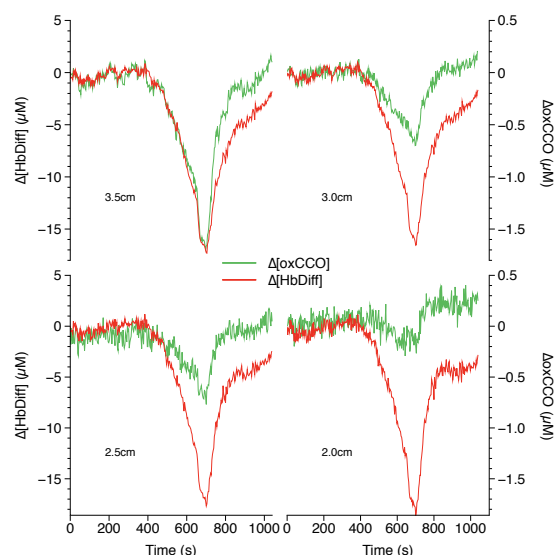


Figure 2: changes in [oxCCO] and [HbDiff] observed at four source-detector separations during vasovagal event.

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## Longitudinal fNIRS Stroop Study of Adult Traumatic Brain Injured Patients in Post-Acute Treatment

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Traumatic brain injury (TBI) and stroke are the leading causes of adult disability and death worldwide<sup>1</sup>. The Stroop test is used to determine the selective attention of subjects. TBI patients, one year post injury, undergoing Stroop studies with functional Magnetic Resonance Imaging (fMRI) show increased activation of left dorsolateral prefrontal (DLPFC) and left posterior parietal cortices<sup>2</sup>. Also functional Near-Infrared Spectroscopy (fNIRS) of healthy subjects after exercise in comparison to control groups for interference tasks shows significant left DLPFC activity<sup>3</sup>. To determine the effects of TBI on the inhibitory response to distraction within one year of injury, a two part Stroop task was performed by patients receiving multidisciplinary therapy at a post-acute treatment facility.

A Hitachi ETG-4000 fNIRS system with a 3x11 array was used to image the frontal cortex of 16 patients and 14 controls. For Task A the subject spoke the color of a presented dot. For Task B the subject spoke the font color of an incongruent word. Each run started with a 10 s rest followed by an ABBABA task pattern with 25 images per block at a rate of 1 image/s, and a rest period of 30 s. Subjects repeated the run two weeks, and four weeks after the original run.

NIRS-SPM version 4 with wavelet-MDL and hemodynamic response functions were used for analysis. Individual false positives improved with Euler characteristics<sup>4</sup>, but group analysis with no correction limited false negatives. Figure 1 shows subtraction of Task B from A to reveal activity which is specific to interference task. Over a one month period, the control group shows a decrease in frontopolar cortex activity while the patient group shows an increase in left DLPFC activity. The lack of significant activity shown in patient group run 1 is possibly a result of saturation during Task A for patients with significant dispersed activity and may indicate a lack of inhibitory response. Run 3 is consistent with patient studies one year after injury. Therefore, left DLPFC increased activity may be an indicator of gradual return to normal brain function from receiving multidisciplinary therapy.

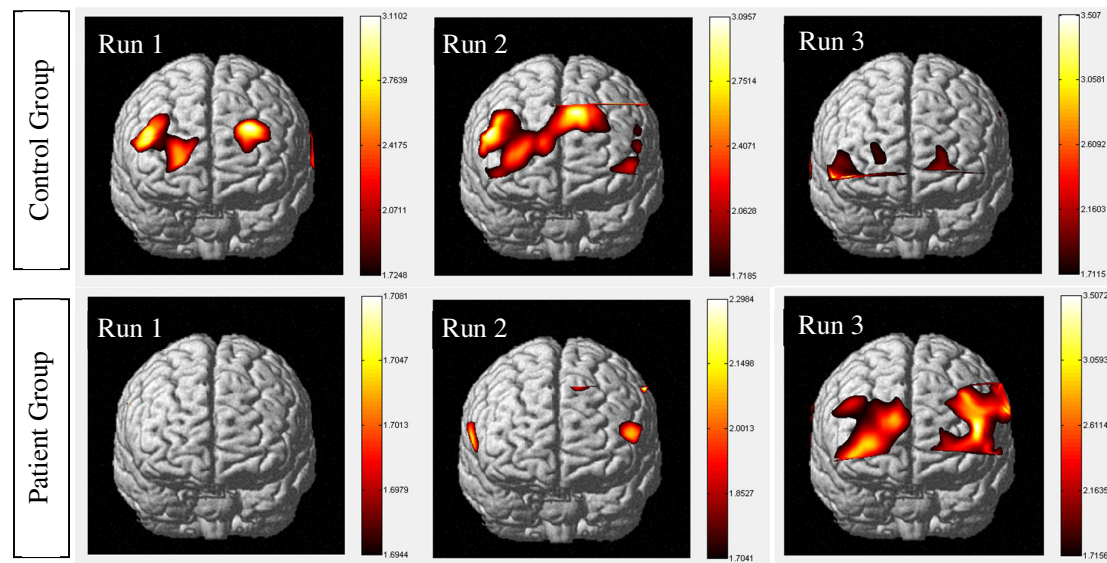


Fig 1) Interference task minus simple task (B-A) p-value=0.05, no correction;  
 Control Group (n=14, 13, 13); Patient Group (n=16, 14, 16)

<sup>1</sup>U.S. Centers for Disease Control and Prevention

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Presurgical diagnosis of the epileptogenic focus using near-infrared spectroscopy mapping

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**Purpose:** An accurate diagnosis of the epileptogenic focus is inevitable in order to get good outcome in a surgical intervention for drug resistant epilepsy. The purpose of our study is to investigate the feasibility of ictal near-infrared spectroscopy (NIRS) recording.

**Method:** We used 48-channel NIRS system in a conventional mode and also in a double density mode. Thirty three patients with drug resistant epilepsy admitted for the presurgical evaluation of epilepsy surgery were enrolled in this study. Ictal recording using NIRS has been applied simultaneously with long term scalp video-EEG monitoring. Inter-ictal IMZ SPECT and FDG-PET were also applied.

**Results:** Ictal NIRS showed increase of regional blood flow in the focus area at the beginning of epilepsy seizures. We utilized this phenomenon to identify the focus location. Ictal NIRS diagnosed laterality of the epileptogenic focus correctly in 80% of patients which was superior to IMZ SPECT (diagnostic in 47.8%) and FDG PET (diagnostic in 50%). Ictal NIRS showed also higher specificity than that of IMZ SPECT (80% and 47.8% respectively), and higher sensitivity than that of FDG PET (80% and 50% respectively). These results were much more prominent in patients with neocortical epilepsy, as ictal NIRS diagnosed laterality of the epileptogenic focus correctly in all patients (100%) with a specificity and sensitivity of 100%, while IMZ SPECT was diagnostic in 50% of patients with a specificity of 50%, and FDG PET was diagnostic in 33.3% of patients with a sensitivity of 33.3%. Ictal NIRS has been shown also to be superior to IMZ SPECT and FDG PET in the diagnosis of laterality of the epileptogenic focus in patients with normal MRI results (non-lesional epilepsy), as they were diagnostic in 100%, 44.4% and 40% respectively.

**Conclusion:** These results augment our previous results that ictal NIRS is a valuable and reliable method to diagnose laterality of the epileptogenic focus especially in patients with neocortical epilepsy and patients with non-lesional epilepsy.



Title: Enhancement of Hemodynamic Contrast in the Cancerous Breast by a Controlled Articulation

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Details of blood delivery to tissue and bulk fluid redistribution among the various tissue compartments frequently are impacted by disease or trauma. For example, derangements in hemodynamic states, accompanied by increased tissue stiffness and local edema, is a common breast cancer phenotype [1]. Accordingly, we have hypothesized that externally applied mechanical forces can produce distinct dynamic responses between diseased and healthy tissue fractions, thereby enhancing diagnostic image contrast. Additional evidence for this sort of contrast-enhancing effect comes from recently reported correspondences that we have observed, between fNIRS-based hemodynamic image data and results of computed estimates of internal mechanical stress and pressure distributions, as a function of various applied articulation maneuvers [2]. The reported concurrences suggest that spatial distributions of hemodynamic variables in the fNIRS images represent redistributions of blood in response to changes in the internal stress.

To evaluate the hypothesis that image contrast between breast tumors and surrounding healthy tissue may be enhanced via controlled articulation maneuvers, we have conducted a pre-clinical study using a recently developed an fNIRS-based breast imaging system [3]. A principal technological element of the imager is concurrent bilateral measurements of the viscoelastic and hemodynamic properties of the breast, in response to a wide range of controlled articulation maneuvers. After giving informed consent and providing a brief medical history, research participants were seated and the sensing heads were adjusted to make good contact with both breasts. Following a five-minute baseline scan, the skin-optode contact pressure was rapidly ( $\sim 2$  s) increased to a level of either 4.4 N or 7.1 N, and data collection continued during the subsequent period of stress relaxation (60-120 s). Optical data were analyzed offline: application of a low-pass filter with a 0.2-Hz cutoff frequency was followed by use of the Normalized Difference Method to reconstruct images of oxygenated and deoxygenated hemoglobin (HbO, HbD), tissue oxygen saturation (HbSat), and blood volume (HbT) [4].

Imaging results obtained from 61 subjects (17 breast cancer, 21 benign pathology, 23 healthy control) are consistent with the hypothesis that the articulation maneuvers enhance the contrast between tumor and healthy tissue. Also noteworthy is the finding that image contrast is further improved by transforming pairs of co-varying image-values [i.e., (HbD,HbSat), (HbD,HbT), or (HbSat,HbT)] to measures of the statistical extremeness (i.e., the Mahalanobis distance [5]) for each pixel. The magnitude of the preceding effect is maximized by referencing the image-pixel data of one breast to the distribution of image values for the contralateral breast. In the final analysis, the paired difference between the numbers of image pixels identified as abnormal is greater for subjects with breast cancer than for either of the other sub-groups, by a statistically highly significant amount ( $p \leq 0.007$ , unequal variance t-test). In addition, diagnostic accuracies for breast cancer of 80-90% (ROC analysis [6]) are achieved. This is a concrete demonstration of the utility of the simultaneous dual-breast measurement approach; of the fNIRS-based breast imagers reported to date, to our knowledge this strategy has been implemented only in the instrument described in Ref. 3. Thus we have demonstrated that controlled manipulation of the internal force distribution of breast tissue can enhance the detectability of cancer, by exploiting a known tumor phenotype.

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## Validation of the time-resolved optical measurement combined with ICG-bolus tracking in assessment of brain perfusion in posttraumatic brain injury patients

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It was reported recently, that monitoring of time-resolved diffuse reflectance and fluorescence on the surface of the head during indocyanine green (ICG) bolus injection may be useful in assessment of brain perfusion (Liebert, Wabnitz et al. 2005; Liebert, Wabnitz et al. 2006; Steinkellner, Gruber et al. 2010; Gerega, Milej et al. 2012; Jelzow, Wabnitz et al. 2012). We will show results of time-resolved measurements carried out in patients after posttraumatic brain injuries and comparison of this data with results obtained in healthy subjects. The measurements were carried out with an in-home build instrument allowing for simultaneous multichannel acquisition of distributions of times of flight of diffusely reflected photons (DTOFs) and distributions of times of arrival (DTAs) of fluorescence photons excited in the dye circulating in the brain. Data analysis algorithms were developed for evaluation of brain perfusion disorders in patients treated in Intensive Care Unit after brain hemorrhage or brain edema resulting from traumatic brain injury. Analysis of optical signals recorded during inflow and washout of optical contrast agent ICG was carried out in order to determine delays in arrival of ICG bolus in the investigated tissues and to compare usefulness of DTOFs and DTAs in such analysis.

The assumptions of the proposed methodology are based on our observations of large time shifts between the signals of statistical moments of DTOFs and DTAs (number of photons, mean time of flight/arrival, and variance of DTOF or DTA) measured in healthy volunteers and much smaller time shifts observed in posttraumatic brain injury patients. Statistical analysis of the time shifts of bolus arrival related to the signals of different moments of the DTOFs and DTAs obtained in healthy volunteers and groups of patients was carried out. Results of this analysis showed that the most useful parameter for differentiation of the studied groups is the delay between bolus appearance obtained from signals of variance of the DTOFs and signals of number of diffusely reflected photons. It was also found that the absolute amplitude of change in variance of the DTOF is significantly lower in healthy subjects than in patients with severe posttraumatic disorders. It was confirmed that the method based on ICG injection and time-resolved optical monitoring of inflow of the dye provides information on blood perfusion of the brain. Temporal parameters of the time-resolved signals obtained in patients with blood perfusion reduced by brain edema and in patients with cessation of cerebral blood flow showed statistically significant difference in comparison to the parameters obtained in healthy volunteers.

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## Differential cortical mechanisms of tool use related gesture production

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*Introduction:* Studies of patients with left hemispheric damage or callosal disconnection suggest that both hemispheres are competent to perform tool use demonstrations, while only the left hemisphere is specialized for pantomiming tool use [1,2]. De Renzi et al. (1982) also reported opposite findings of patients with a preserved pantomime but an impaired tool demonstration [3]. Furthermore, split-brain patients, who had a left hand apraxia for pantomimes, were able to perform body-part-as-object (BPO) demonstrations with the left hand [2]. Accordingly, in an fMRI differences in hemispheric activation were found for BPO as compared to pantomime [4]. To solve this controversy, in the present study we investigate if the cerebral hemodynamic response patterns of tool use demonstration, tool use pantomime, and BPO of tool use differ between the left and right hemisphere. *Methods:* A randomized block design was developed including tool use demonstration, pantomime of tool use, and BPO of tool use. Each condition was executed with the right and left hand. Cerebral oxygenation changes were recorded by Near-Infrared Spectroscopy (Device: DYNOT Imaging System, NIRx Tech.). 30 optodes were placed over the Primary, Pre- and Supplementary Motor Cortex and the Somatosensory Cortex above each hemisphere resulting in 60 channels of measurement. Data were analyzed using the NIRS-SPM toolbox. *Results:* First results show significant interaction effects of *condition\*hand\*hemisphere* ( $F(2,177)=4.287$ ,  $p<0.05$ ). Post hoc pairwise comparisons reveal highest changes of oxygenation during pantomime of tool use. Tool use demonstration and pantomime of tool use show a left lateralized hemodynamic response for either hand whereas BPO activates contralateral cortices only. *Discussion:* This is the first fNIRS study to provide evidence for different oxygenation changes of tool use related gesture production. Pantomiming tool use seems to demand a wide range of cortical networks leading to greatest oxygenation changes among the three conditions. This finding is line with the proposition that performing the pantomime of tool use without having the tool in hand or integrated (BPO) requires abstract thinking and higher cognitive abilities [2]. The present data further support previous findings demonstrating a left hemispheric specialization for tool use demonstration and tool use pantomime. However, contrary to previous studies, our study suggests that the competence to perform BPO of tool use is represented in both hemispheres.

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### **Very-low-frequency oscillations of cerebral hemodynamics and blood pressure are influenced by aging and cognitive activation**

**Objectives:** The origin of spontaneous slow oscillations in cerebral hemodynamics is controversial, but they may represent autoregulatory processes. Very-low-frequency oscillations (VLFOs, 0.02-0.07 Hz) are hypothesized to result from neurogenic activity, whereas low-frequency oscillations (LFOs, 0.07-0.20 Hz) are possibly caused by activity in microvascular smooth muscle cells. High-frequency oscillations (HFOs, 0.20-0.35 Hz) are due to respiratory activity. The influence of blood pressure oscillations is however frequently neglected. Evidence exists that aging is accompanied by a degeneration of the vascular system and changes in neurovascular coupling, which may have consequences for regional cerebral blood flow and cognitive performance. Therefore, we aimed to establish the dependency of slow oscillations in cerebral hemodynamics and blood pressure on the factors age and cognitive activation, by using functional Near-Infrared Spectroscopy.

**Methods:** In this study, 14 healthy young (23-32 years) and 14 older adults (64-78 years, MMSE=29.1±0.9) performed a verbal n-back working-memory task. Oxygenated ([O<sub>2</sub>Hb]) and deoxygenated hemoglobin ([HHb]) concentration changes, as indices of brain activation, were registered by two fNIRS channels located over left and right prefrontal cortex. Concentration changes in total hemoglobin ([tHb]) are used as an indicator of alterations in total blood volume. Blood pressure (BP) was measured in the finger by photoplethysmography (Finapres).

**Results:** [O<sub>2</sub>Hb] increased in both groups under influence of cognitive activation. In comparison to baseline measurements, BP increased slightly under high working-memory load (2-back) in young (4.3±4.4 mmHg) and older adults (5.9±5.0 mmHg), but the increase did not differ between groups. Power spectral density analysis showed that VLFOs of BP, [O<sub>2</sub>Hb], and [tHb] are influenced by both age and working-memory load. In the control condition (0-back), VLFOs of BP were equal in power for young and older adults. However, high working-memory load resulted in declined VLFOs of BP (-24.0%) in young adults, while in older adults the VLFOs did not change. VLFOs of [O<sub>2</sub>Hb] and [tHb] were stronger in young adults in comparison to older adults during the control condition. However, under high working-memory load, in young adults the VLFOs of [O<sub>2</sub>Hb] (-23.4%) and [tHb] (-22.5%) were reduced and became similar to those in older adults. LFOs and HFOs of [O<sub>2</sub>Hb], [HHb], [tHb], and LFOs of BP were not influenced by working-memory load, but declined with age. Transfer function analysis indicated that the relationship between BP and [O<sub>2</sub>Hb] oscillations does not change under influence of age and cognitive activation.

**Conclusions:** Our study shows that VLFOs, LFOs and HFOs in cerebral hemodynamics decline with age. VLFOs are influenced by intensity of cognitive activation, but only in young adults. This age-dependency may indicate age-related changes in neurovascular coupling. Moreover, our results on BP oscillations show that not only local vasoregulatory processes, but also systemic processes influence the cerebral hemodynamic signals. To conclude, the effects of age and BP should be taken into account in the interpretation of neuroimaging studies that rely on blood oxygen levels.

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## Functional Near-Infrared Spectroscopy shows altered functional connectivity in the brain of patients with multiple sclerosis

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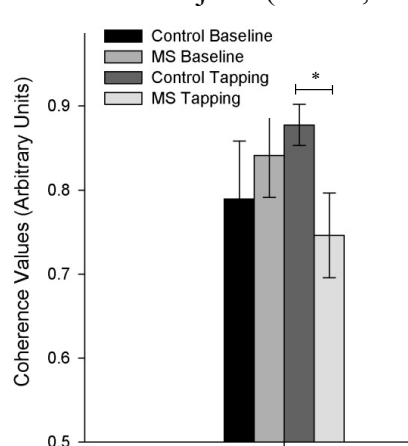
### INTRODUCTION

Multiple sclerosis (MS) is associated with demyelination of white matter tracts<sup>1</sup>, which is likely to be a major factor in the reduction of brain function in MS. Functional near-infrared (NIR) spectroscopy based optical imaging or fNIRS can be used to measure the changes in oxygenated and deoxygenated microvascular hemoglobin, markers of brain activation<sup>2</sup>.

Coherence analysis coupled with fNIRS technology may be able to establish a metric with which to determine disease progression<sup>3</sup>. The corpus callosum is a large white matter tract that connects the two brain hemispheres, and reduction in size occurs in MS<sup>4</sup>. We hypothesized that changes in coherence will provide a quantitative index of white matter degeneration in MS.

### METHODS

Control subjects (6 male, 2 females; age  $42.5 \pm 12.6$  years, mean  $\pm$  SD) and MS patients (5



male, 3 female; age  $53.7 \pm 8.1$  years, mean  $\pm$  SD) were studied. MS patients were recruited through the MS Clinic at Foothills Medical Centre (Calgary, Alberta, Canada).

We used a continuous wave (CW) optical mapping system (CW5, TechEn, MA, USA)<sup>5</sup>. There were 4 transmitters and 8 detectors in each of 2 pads, with the sources operating at 690 nm and 830 nm. The area imaged on each motor cortex was  $5.6 \times 6.0$  cm<sup>2</sup>. Baseline was recorded for 300 seconds. The motor function consisted of 15s of tapping, followed by 30s of rest, repeated for 7 rest and 6 tapping periods. Coherence maps were generated by an in-house program using MATLAB.

Fig. 1. Coherence values between left and right motor cortex. Resting state coherence is not significantly different between controls and MS patients. The coherence values were reduced in the MS patients during finger tapping compared with controls ( $p = 0.035$ , mean  $\pm$  S.D. ).

### RESULTS and DISCUSSION

The coherence in the contralateral motor cortex of MS patients was significantly lower compared to controls when measured during finger tapping, which may be due to reduced function of white matter tracks. When studying coherence, it may be that further differentiation of some disorders can be achieved by differentiating the resting state from functional state. This work shows that fNIRS detects dysfunction in MS patients.

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## Cortical response during motor task in adult volunteers and epileptic patients with movement disorders: a multimodality fNIRS-EEG, fMRI-EEG and TMS clinical study

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Integration of functional magnetic resonance imaging (fMRI) or functional near infrared spectroscopy (fNIRS) with electroencephalography (EEG) has the potentiality to monitor neuronal and vascular response [1-3]. Recently, also transcranial magnetic stimulation (TMS) has been used to study the motor system and higher brain functions in healthy and diseased states (e.g. multiple sclerosis, motor neuron disease, stroke, epilepsy, and movement disorders) [4]. In this work we present a multimodality approach based on fNIRS-EEG, fMRI-EEG and TMS on adult volunteers and epileptic patients with movement disorders during motor task. The work is performed within the European project nEUROpt [5] aiming at assessing the potentiality of time domain fNIRS for noninvasive imaging of brain function and disease by pulsed light.

fNIRS-EEG and fMRI-EEG data were recorded in two successive experiments from 14 volunteers and 11 patients (Unverricht-Lundborg disease genetically assessed) performing a motor task (clutching a soft ball at 2Hz; 40s initial rest period, 10 trials alternating 20s task and 20s rest, then 50s recovery; 3 paradigms: right hand vs. rest, left hand vs. rest, left hand vs. right hand; total duration 24 minutes). A multi-channel dual-wavelength medical device for time domain fNIRS [6] measured oxy- and deoxygenated hemoglobin (O<sub>2</sub>Hb, HHb) changes in the cortical region at 1Hz from 30 independent channels centered on C3 and C4. Activation maps were estimated by the NIRS-SPM software [7]. MR images were acquired with a 1.5T MR scanner and fMRI data were analyzed using the SPM8 software [8] to calculate activation maps. From EEG data Event-Related Desynchronization/Synchronization (ERD/ERS) analysis (time course and scalp topography) was performed. Single subject and group analysis was carried out for all imaging modalities. Finally TMS-based mapping of primary motor cortex of the hand, associated to real-time frameless neuronavigation system, was performed. Calculation of center of gravity of the TMS motor maps for each hemisphere was used as the most accurate estimation of the location of the represented muscle in the motor cortex.

As general outcome results of individual and group analyses on volunteers agree with literature. Functional activation was detected by fNIRS as an increase in O<sub>2</sub>Hb and a corresponding non symmetrical decrease in HHb in the contralateral hemisphere in channels closely located to C3 (or C4). fMRI maps revealed activation in the primary motor area contralateral to the movement and in the supplementary motor area. EEG measurements revealed  $\alpha$ -ERD and  $\beta$ -ERD in central areas during movement execution (more evident in contralateral area),  $\beta$ -ERS in contralateral area immediately after the movement offset. Results are confirmed in group analysis. All centers of gravity lie around C3 and C4 positions, but differences in center of gravity location was observed among subjects. In most of the cases maps obtained by TMS show good correlation with fMRI, EEG and NIRS data. The elicited fNIRS response in patients is generally more limited than in volunteers, both in terms of spatial extension and of intensity of hemodynamic changes. Concerning location of the activation, fNIRS results in patients are however consistent with fMRI and TMS responses. Overall the fMRI and TMS activation maps show no significant difference with volunteers. The ERD/ERS analysis on patients confirmed the absence or reduction of post movement synchronization in  $\beta$  band [9].

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## Methylphenidate-mediated reduction in prefrontal hemodynamic responses to working memory task: A functional near-infrared spectroscopy study

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### INTRODUCTION

Methylphenidate (MP) is a piperidine-derived central nervous system stimulant that acts as a dopamine/norepinephrine agonist by binding to the monamine transporters in the presynaptic membrane and blocking reuptake<sup>1</sup>. It is used in the treatment of attention deficit hyperactive disorder (ADHD), narcolepsy<sup>2</sup>, depression, and co-morbid depression in the medically ill<sup>3</sup>. Functional near infrared spectroscopy (fNIRS) is a non-invasive optical technique for bedside evaluation of cerebral metabolism that has clinical potential for monitoring the efficacy of pharmacological treatment. In this pilot study, we investigated the cognitive effects of methylphenidate (MP) on prefrontal function using fNIRS in healthy subjects.

### METHODS

Thirteen right-handed healthy subjects underwent working memory tasks (0-back, 2-back) after a single oral dose of MP (20 mg) or placebo administered in a double-blind crossover design on two different days separated by 1-3 days. We measured changes in oxyhemoglobin (oxy-Hb) and deoxyhemoglobin (deoxy-Hb) concentrations during the tasks in bilateral prefrontal regions after MP or placebo administration using 2-channel NIRO-200.

### RESULTS AND DISCUSSION

There were significantly more correct responses and fewer missed responses during the 2-back task performance after MP treatment as compared with placebo. Baseline-corrected increase in oxy-Hb was reduced after MP treatment compared with the placebo in the 2-back task in right frontal region, but was not different in the 0-back task. Baseline-corrected deoxy-Hb and total-Hb concentrations were not significant between MP and placebo conditions in either of the cognitive tasks. This data is consistent with previous PET findings of MP-mediated reduction in lateral prefrontal activity<sup>4</sup> accompanied by improved cognitive performance and shows that fNIRS may be useful in assessing responses of brain to cognition altering drugs.

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## Analysis of frequency components in optical signals measured by time-resolved near infrared spectroscopy on adults head: preliminary study

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The aim of the study was to develop a method for assessment of the autoregulation of blood microcirculation in the cerebral cortex in human adults. Hemodynamic of cerebral circulation will be monitored noninvasively at the bedside with the use of the time resolved near-infrared spectroscopy. Frequency analysis methods will be combined with the modern time-resolved optoelectronic measurements in order to analyze components of the signals related to the respiration, as well as heart and vascular activity. It was shown that time-resolved near-infrared spectroscopy allows for separation of changes in hemoglobins concentration in intracerebral tissue from changes related to extracerebral compartments (like a skin, bones of the skull) (Steinbrink, Wabnitz et al. 2001; Liebert, Wabnitz et al. 2004; Kacprzak, Liebert et al. 2010; Kacprzak, Liebert et al. 2012). Proposed methodology may allow for the evaluation of cerebral blood flow autoregulation by frequency analysis of the optical signals and will be applied in the control group of healthy volunteers and in the patients with cerebral blood flow disorders caused by traumatic brain injuries.

The optical signals were acquired in 22 in healthy volunteers during 10 minutes long measurement. The subjects were investigated in rest conditions in supine position with the use of in-home build time-resolved setup which was previously presented in detail (Kacprzak, 2007). The instrument is based on semiconductor lasers, photomultipliers and time-correlated single photon counting electronics.

The results of frequency analysis of the time-resolved signals showed that in most of the subjects all the statistical moments of the measured distributions of times of flight of photons (number of photons, mean time of flight and variance of the distribution) the components from the pulse and breathing can be observed. This observation suggests that the analysis of these frequency components in the time-resolved optical signals can be used to study tissue saturation and in combination with the beat-to-beat pressure measurement the methodology may be used for investigation of brain autoregulation. Furthermore, analysis of respiratory and pulsatile components of the optical signals may be used in estimation of arterial, venous and tissue oxygenation specific for the brain tissue compartment in adult humans.

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## Cerebral vasoreactivity to carbon dioxide and neural activation in schizophrenia: a study with near-infrared time resolved spectroscopy

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**OBJECTIVE:** Hypofrontality has been a major finding obtained from functional neuroimaging studies on schizophrenia. Our previous study<sup>1</sup> has suggested that resting hypofrontality is a chronically developed feature of schizophrenia, and this does not necessarily represent frontal dysfunction, but may anatomical and/or functional changes in frontal microcirculation. To test this possibility, we investigated the cerebral vasoreactivity to carbon dioxide (CO<sub>2</sub>) and neural activation in schizophrenia.

**METHODS:** Thirteen schizophrenic patients with no brain anatomical abnormalities (7 males, 29-68 years) and 11 healthy volunteers (5 males, 23-49 years) participated in this study. A two-channel time-resolved spectroscopy instrument (TRS-20, Hamamatsu) was used to measure Hb concentrations during the performance of a random number generation (RNG) task, hyperventilation (HV) and breathing into a paper bag (PB). The incident and detecting light guides were bilaterally placed on the forehead adjacent to Brodmann area 10. Subjects sat on a chair and were first asked to recite a sequence of random digits between 0 and 9 to a 1-Hz pacing tone. As the control task, they were asked to repeatedly count out softly in order from 0 to 9. They performed each task until a total number of 100 digits were recited. After the cognitive tasks, PB were performed for 2 minutes, which was followed by 2-minute-long HV with an interval of a couple minutes. During the HV and PB tests, end-tidal CO<sub>2</sub> (ETCO<sub>2</sub>) was monitored (Gas Analyzer, AD Instruments). BP, pulse rate and SpO<sub>2</sub> were also monitored continuously. This study was approved by the Ethical Committee of Tokyo Metropolitan Institute of Medical Science.

**RESULTS:** RNG-related increases in oxy-Hb were bilaterally observed in eight patients and 10 control subjects, while four patients and one control subject showed increases in oxy-Hb only on the right side of forehead. The relationship between  $\Delta\text{ETCO}_2/\text{ETCO}_2$  and  $\Delta\text{oxy-Hb}/\text{oxy-Hb}$  in patients was almost the same as that in controls.  $\Delta\text{CMRO}_2/\text{CMRO}_2$  was more tightly correlated to  $\Delta\text{CBF}/\text{CBF}$  during the RNG task than during HV and PB. There were no significant differences in these correlations between patients and control subjects.

**CONCLUSIONS:** These results suggest the possibility that neurovascular coupling and reactivity to CO<sub>2</sub> are not primarily impaired in schizophrenia.

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Abstract for  
 “fNIRS Meeting”, London, October 26<sup>th</sup>-28<sup>th</sup>, 2012

see <http://www.fNIRS.org/fNIRS2012.html>

### **Multi-channel and multi-distance NIRS during neuroangiography: Feasibility and technical aspects**

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#### **Introduction**

Digital Subtraction Angiography (DSA) by its high spatial and temporal resolution is the gold standard in brain vessel imaging. The inherent methodological limitations of DSA are: a) long-time monitoring is impossible because of the limited applicability of X-rays and contrast media, and b) assessment of the hemodynamic state of the brain is restricted to imaging of large vessel collaterals. Non-invasive monitoring of concentration changes of oxygenated and deoxygenated hemoglobin within the outmost millimeters of the brain is possible by NIRS.

#### **Methods**

Multi-channel NIRS was measured during DSA examinations and interventions using the FOIRE-3000 system (Shimadzu, Japan). Absorbance of near infrared light was recorded at three wavelengths (780, 805 and 830nm) and changes of oxygenated and deoxygenated hemoglobin were calculated. The number of channels varied between 4 and 56. Transmitters and receivers were placed on the scalp at 30 and 42mm distance.

#### **Results**

- I) Fibre holders and fibre holder caps of the FOIRE-3000 did not significantly interfere with radiography. But the glass fibres of near infrared transmitters and receivers have high X-ray opacity. Adaption of the positioning of the transmitters and receivers nevertheless allowed simultaneous DSA and multi-channel NIRS measurement.
- II) The first pass of the contrast agent bolus could be recorded by NIRS and corresponded to the injection site.
- III) Compared with the channels spaced at 30mm, the channels at 42mm yield a lower signal-to-noise ratio (SNR) of the raw NIRS signal. Despite this, their SNR was higher for the NIRS response to bolus injections into brain specific vessels, because these channels cover a higher proportion of brain tissue. Repeated measurements from the same site could be used for further improvement of SNR.

#### **Conclusions**

NIRS monitoring during DSA is feasible with the FOIRE-3000 and may provide complimentary information specific to vascular territories. Due to their high X-ray opacity the glass fibres must be placed adequately to avoid restriction of the field of view of the angiographer. Signals measured at optode distance 42mm have larger brain contribution and redundant measurements allow noise reduction.

*Prefrontal cortex activity and H-reflex variability during dual and single task treadmill walking in healthy subjects.*

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### *Introduction*

Walking has been shown to be affected under dual task conditions. The prefrontal cortex is known to be more active during dual tasking, however there has been no research reported on the impact of dual tasking on peripheral reflex responses. Gaining a better understanding of both peripheral and central mechanisms during different walking conditions could increase knowledge and inform the development of more targeted training programs. This study set out to explore prefrontal cortex activity and peripheral reflexes during dual task conditions.

### *Methods*

17 Healthy subjects (7 males, 10 females), aged 22-44, were measured with functional Near-Infrared Spectroscopy (fNIRS) and H-reflex while walking at self selected walking speed (SSWS) and at 20% faster than SSWS. Measurements were taken during treadmill walking (single task) and treadmill walking whilst performing a cognitive distracter task (dual task). NIRS optodes were placed over the prefrontal cortex. H-reflexes were elicited in the right soleus during mid-stance (30% of gait cycle). Subjects were instructed to count backwards in steps of 7 during the cognitive distracter task.

### *Results*

The average walking speed of participants during both dual and single task treadmill walking was  $1.22\text{ms}^{-1} \pm 0.24\text{sd}$  for SSWS and  $1.48\text{ms}^{-1} \pm 0.26\text{sd}$  for 20% faster than SSWS. fNIRS results showed a significant higher concentration of oxy haemoglobin in the right prefrontal cortex and a trend towards significance in the left prefrontal cortex during dual task walking compared to single task treadmill walking during both speeds ( $p = 0.049$ ;  $p = 0.069$ ). Deoxy haemoglobin concentrations did show a trend towards a significant lower concentration in the left prefrontal cortex during dual task treadmill walking compared to single task treadmill walking for both speeds ( $p = 0.085$ ).

A trend was observed in the variability of the amplitude of the H-reflex, measured with the coefficient of variation, during dual task walking compared to single task walking ( $p = 0.088$ ).

### *Conclusion*

The increased concentration of oxy haemoglobin in the prefrontal areas suggest that those areas were more active during dual than single task conditions. This could indicate that the prefrontal cortex was more involved in coordinating the walking movement when the subject was dual tasking. The trend towards an increased variability of the H-reflex suggests that peripheral reflexes may also be affected by dual task conditions. This data may provide more insight in different ways to look at walking control which in future could contribute to specific rehabilitation training programs for neurological populations.

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## fNIRS of auditory, visual and somatosensory responses in normal-hearing individuals

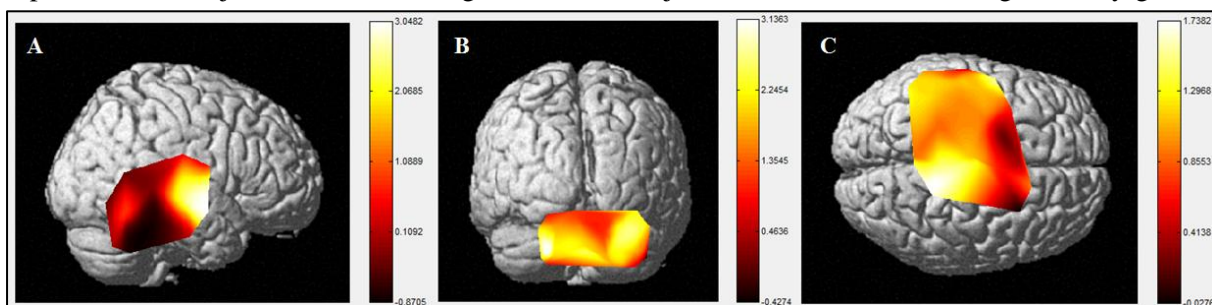
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**Introduction:** The auditory cortex becomes more sensitive to visual and somatosensory stimulation following deafness [1]. Preliminary evidence suggests that this ‘cross-modal’ brain reorganisation may predict outcome of cochlear implant use, as evidenced by electrophysiology and fMRI studies [2]. However, these measures are poorly suited for use with cochlear implant recipients, due to the nature of the implanted device. A recent study by Sevy and colleagues suggests near infra-red spectroscopy is unaffected by the presence of a cochlear implant [3]. Specifically, they measured cortical responses to sounds in cochlear implant recipients. We used NIRS to measure cortical responses to visual, somatosensory and auditory stimulation in normal-hearing adult participants.

**Methods:** Auditory stimuli were presented from a loudspeaker at 80dB SPL. They consisted of sinusoidal amplitude-modulated (10Hz; 100% modulated) or un-modulated broadband noise bursts. Visual stimuli consisted of 1000 white dots on a black background that were randomly flashing or moving coherently. Somatosensory stimuli were low frequency tones at 20Hz or 10Hz, presented using a loudspeaker and propagated across a thin plastic plate. Participants placed the palms of both hands on the plastic plate for the duration of the experiment. Auditory, visual and somatosensory stimuli were all 20s in duration, and repeated five times in a pseudo-random order. Each stimulus was interleaved with a 20s rest period. Deoxy- (HbR), oxy- (HbO) and total (HbT) haemoglobin NIRS responses were acquired using a 24 channel Hitachi ETG4000 system. Optodes were bilaterally applied to the scalp in 3×3 grids over the temporal lobes during auditory stimulation and over the post-central gyrus during somatosensory stimulation. A single 3×5 grid covered the occipital lobe during visual stimulation. NIRS channel positions were obtained using a 3D digitiser. NIRS functional data were pre-processed using wavelet-MDL detrending and a Gaussian low-pass filter with a FWHM of 4s, and statistically analysed with the NIRS-SPM software suite using a GLM of the block design.

**Results & Discussion:** 10 participants (age=33±9 years, n=6 female) were recruited to the pilot study. Cortical responses were successfully recorded in auditory (n=8), visual (n=9) and somatosensory (n=6) modalities. HbT changes in the temporal lobe, occipital lobe and post-central gyrus from a representative subject are shown in Figure 1. Most subjects exhibited areas with significantly greater



**Figure 1:** HbT changes in the temporal (A) and occipital (B) lobes and in the post-central gyrus (C) in response to auditory (AM noise > noise), visual (coherent > randomly moving dots) and vibrotactile (20 Hz > 10 Hz) stimuli respectively, in the same representative subject.

HbT responses ( $p < 0.05$ ; Expected EC correction) to (A) modulated compared with unmodulated noise (6/8 participants), (B) coherent-moving compared with random-flashing dots (6/9 participants), while (C) 20 Hz vibration compared with 10 Hz produced significant differences in half the (3/6) participants. In future studies we will use identical techniques to measure and compare cross-modal activation within the auditory cortex of profoundly deaf subjects with and without a cochlear implant.

**Acknowledgements:** Supported by the MRC and NIHR. **References:** [1] Lomber S.G. et al., 2010. *Nat Neurosci.* 13(11)1421-1429. [2] Rouger J., et al., 2011. *Hum Brain Mapp.* [Ahead of print]. [3] Sevy A.B.G., et al., 2010. *Hear Res.* 270:39-47. **Author’s e-mail:** rebecca.dewey@nottingham.ac.uk

Abstract for  
 “fNIRS Meeting”, London, October 26<sup>th</sup>-28<sup>th</sup>, 2012

see <http://www.fNIRS.org/fNIRS2012.html>

### **NIRS during neuroangiography: First results and potential added value**

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#### **Introduction**

A prerequisite for planning neuro-vascular interventions such as recanalization therapy in acute stroke is Digital Subtraction Angiography (DSA), which enables imaging of large vessel collaterals. NIRS may monitor non-invasively the hemodynamic changes within the outmost millimeters of the brain and might qualify as tool providing complementary information.

#### **Methods**

Temporal changes in oxygenated and deoxygenated hemoglobin concentrations during DSA examinations and interventions were measured using the multi-channel NIRS system FOIRE-3000 (Shimadzu, Japan) with 4 to 56 channels. Recording time varied between 6 and 120 minutes.

#### **Results**

- I) During unilateral temporary balloon occlusion of the internal carotid artery (ICA) the territory of the ipsilateral middle cerebral artery (MCA) and the watershed areas showed measurable changes in oxygenation.
- II) In patients with unilateral high grade stenosis of the ICA the effect of the pulsatile heart rate on the variance of the NIRS signal allowed lateralization of the stenosis.
- III) Brain hyperperfusion due to CO<sub>2</sub> increase during apnea is detectable by NIRS.

#### **Conclusions**

NIRS measurement might offer a non-invasive instrument to monitor the treatment effects of revascularisation therapy and provide additional insights on hemodynamic compromise of the outmost brain layers during DSA. In particular, a compromise of some watershed areas was detectable.

## Abnormal Activation Pattern of Schizophrenia in Performing Tower of London Test

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Function near-infrared spectroscopy (fNIRS) is a recently developed optical method, which characterizes noninvasive in vivo measurements of changes of concentrations of oxygenated (HbO<sub>2</sub>), deoxygenated (HbR) and total hemoglobin (HbT) in brain outer cortex. The hemoglobin oxygenation state is intimately associated with the neuronal activity[1]. So the fNIRS facilitates neuroscientists to explore neuronal activity of subjects. Here we utilized it to recognize abnormal activation pattern of schizophrenia during taking the same test as normal controls, instead of measuring the difference of mean concentrations[2].

We located 28 fNIRS channels on the frontal lobe of subjects, seven normal controls and ten schizophrenia patients. They followed instructions and then performed the Tower of London test of three levels, demanding one, two and three steps to approach targets. Results of concentrations of channels and activation pattern are shown in Fig. 1 and Fig. 2, respectively.

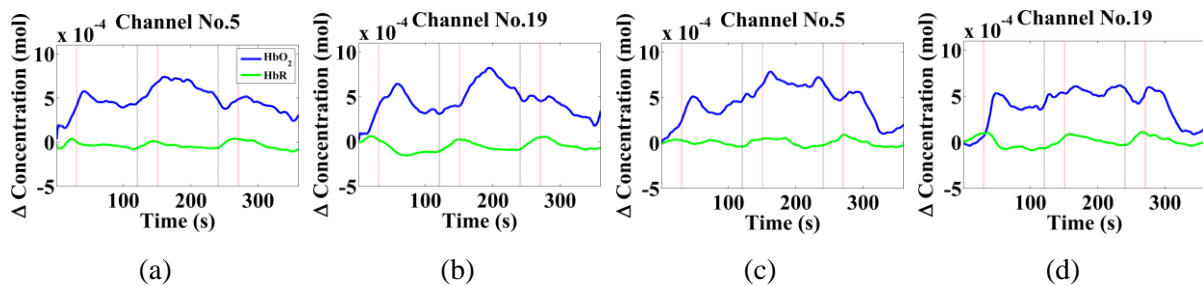


Fig. 1 Concentrations of HbO<sub>2</sub> and HbR at channel 5 and 19 of normal (a, b) and patients (c, d). There were 28 channels to record concentrations of HbO<sub>2</sub>, HbR and HbT at different positions over frontal lobe. Fig. 1 shows two channels, No. 5 and 19 to present variations of HbO<sub>2</sub> and HbR as well as the difference of the same recording position between normal control and schizophrenia patients.

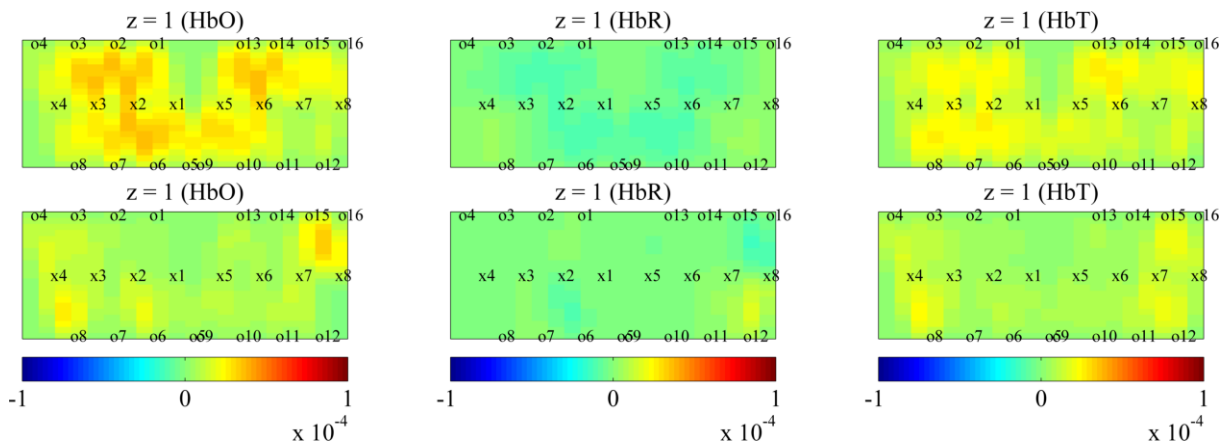


Fig. 2 Reconstruction images of subjects during TOL test. The first row shows HbO<sub>2</sub>, HbR and HbT from normal control, while the second row from patients.

Referring to these results, HbO<sub>2</sub> apparently is more sensitive to brain activities. Schizophrenia patients have less concentration changes from resting state and their frontal lobe is less activated than normal, especially in the medial prefrontal part.

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Title: The rate of deoxy-Hb changes can be used as a neuromarker to detect the emergence from deep to light anesthesia.

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#### Abstract

This presentation focuses on awareness and suppression of consciousness and on the neurophysiological processes mediating consciousness and the memory process involved in loss of consciousness (LOC). Our study involved a group of patients who underwent general anesthesia during surgery. The anesthetics administered were mainly Propofol and Sevoflurane. To monitor depth of anesthesia, we used two systems simultaneously: the BIS<sup>®</sup> monitor (Aspect Medical Systems, Norwood, MA) and the functional near-infrared (fNIR) system (fNIR Devices LLC, Potomac, MD). The BIS utilizes an algorithm combining measurement of patient movements with amplitude and phase information from Fourier-transformed electroencephalogram epochs between 0 and 100, with 40-60 indicating the target for awareness prevention. The fNIR is a non-invasive, minimally intrusive, safe *medical device* which detects the hemodynamic response of brain cortex to cognitive activation. Depth of consciousness was monitored every 8 seconds during induction by using the modified Observer's Assessment of Alertness/Sedation Scales (OAA/S) as the patient transitioned to deep anesthesia. Averaged 15-second deoxygenated hemoglobin (deoxy-Hb) data prior to each marker following wound closure is compared to BIS measurements until each patient's eye opening. Change in deoxy-Hb and BIS measurements are obtained according to wound closure marker point, i.e., deep anesthesia phase for each marker point until eye opening which is marked as light anesthesia phase. Our data shows that there is a significant negative correlation between deoxy-Hb and BIS values ( $r=-0.85$ ). As BIS values increase from deep to light anesthesia, deoxy-Hb values decline to the baseline condition of emergence from deep anesthesia to light anesthesia. Hence, a negative correlation is expected. Working memory and attention are the main cognitive processes involved in consciousness and awareness. Further technical and theoretical implications for operating rooms and hospitals are discussed.

Uncomfortable visual stimulation and the shape of the haemodynamic response.

Sarah Haigh and Arnold Wilkins  
University of Essex

The amplitude of the haemodynamic response measured using NIRS during presentation of a visual grating stimulus varies with the brightness contrast, colour contrast and motion of the component bars of the grating. In general, the grating parameters that increase the amplitude increase the aversiveness of the grating. When discomfort is extreme, as it is when the grating drifts or vibrates at 10Hz, the haemodynamic response is shorter and the response may briefly end below baseline. Recently abnormalities in the haemodynamic response have been observed in patients with migraine. The change in the size and shape of the waveform with increasing aversion provides an interpretation of the abnormalities in migraine as reflecting the greater discomfort experienced by migraineurs. Strong uncomfortable visual stimuli appear to elicit a high-amplitude but relatively brief haemodynamic response.



Poster Session  
Applications: Neonatal and Paediatric  
Poster #: 104-106

## Investigation of resting state and visual evoked functional activity in neonates during concurrent NIRS and MRI.

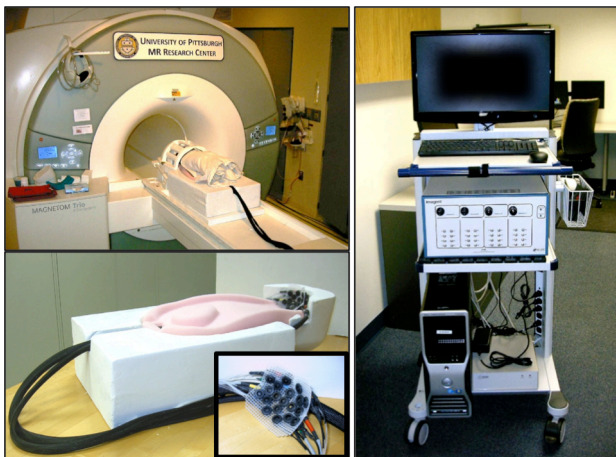
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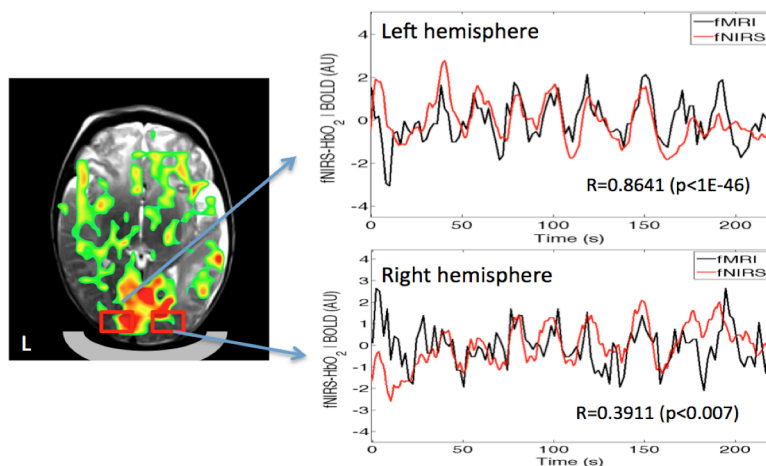
**Introduction:** Approximately 12.1% of all births in the United States are preterm (i.e., occurring before 37 weeks gestational age). Within this group, nearly half of the infants with birth weights <1500 g will later exhibit cognitive and behavioral deficits, including cognitive visual impairment (CVI), necessitating special educational and rehabilitative (physical, occupational, visual and speech) services. Early intervention is optimal for ameliorating cognitive and behavioral deficits, especially CVI, because it maximizes the timing of intervention against critical periods for development and minimizes the impact of these deficits on later academic skills (e.g., reading, mathematics). However, diagnosis of CVI in a neonate is challenging due to the limited number of visual behaviors that may be assessed clinically in an awake infant.

In this study, we performed concurrent frequency-domain NIRS imaging during 3T MRI scanning in neonates in order to compare baseline physiological values (oxygenation and blood volume), resting state fluctuations in brain activity, and functional activation between the optical and MRI modalities.



**Fig 1.** NIRS instrument (right) and MRI-insert head cap for NIRS recordings (left/bottom).

**Methods:** A frequency-domain NIRS system (ISS Imagent) was used to record baseline and functional optical signals. A custom built MRI compatible probe with multi-distance overlapping (tomographic) measurements was used (shown left). MRI scanning was done at 3T using a Siemens TRIO scanner with a 12-channel adult head coil (in order to accommodate the NIRS probe). Vitamin E markers on the probe were used for registration in the MRI structural image. A custom built LED-based lighting system that was mounted on the inside of the MRI bore was used for visual stimulus. Six LED positions (at about 15° spacing) were illuminated under computer control and programmed to flash in unison (at 2Hz) or to sweep sequentially from side to side to produce a moving visual stimulation



**Fig 2.** Concurrent fNIRS-fMRI data was recorded during the resting state in a term infant at 43weeks. The images above show strong (R=0.86 and 0.39) correlations between the fNIRS and BOLD signal for signals from left and right hemispheres. The MRI image shows the effective connectivity map generated from a seed region within the left region-of-interest (occipital).

**Results:** Figure 2 shows the NIRS and MRI time courses from a 43week infant. Strong correlation between the NIRS and fMRI (R=0.86) was observed in the occipital cortex during the resting state scan

**Conclusions:** This study remains ongoing, but our initial data indicate strong correspondence between MRI and NIRS data. This suggests the possibility of using NIRS as a stand-alone (bedside) modality in future studies.

## THE IMPACT OF NEONATAL INTRAVENTRICULAR HEMORRHAGE ON AUDITORY HEMODYNAMIC RESPONSE

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### **Objective**

Children with delays in language and speech development are at high risk for later disorders in reading, spelling, and writing, academic skills which are highly dependent on language abilities. Brain injuries have been found to be associated with language and speech outcomes among children born prematurely. Severe grades of intraventricular hemorrhage (IVH) are risk factors for adverse neurodevelopmental outcomes, including cognitive impairment and cerebral palsy.

### **Method**

Eight healthy and five ill preterm neonates (IVH grade III and IV) (GA:28-32 weeks) participated in an optical topography study designed to assess the specific characteristic of neurovascular coupling to auditory syllabic stimuli in healthy and ill neonate brains. Auditory stimuli consist of two digitized syllables /ba/ and /ga/, naturally produced by a male and a female speaker. Neonates were tested while they slept. We used 16-channel Near-Infrared Spectroscopy (NIRS) device to assess changes in the concentration of deoxyhemoglobin (HBR) and oxyhemoglobin (HBO) in response to auditory syllabic stimuli in the right and left hemispheres.

### **Result**

We found that temporal areas of healthy neonates showed significantly more activation (increase in [HBO], decrease in [HBR]) than ill neonates when were exposed to auditory stimuli.

### **Conclusion**

The present data confirm the existence of neurovascular coupling in healthy premature brain. It also shows that ill premature neonates are unable to process syllabic stimuli, a step for language acquisition ability. The results are in accordance with what we previously described concerning abnormalities of spontaneous neurovascular coupling in pathological EEG discontinuity in ill premature neonates. This inability of pathological brain to adapt to either endogenous or exogenous stimuli by an increase in blood flow can represent a mechanism by which the pathological brain enters in a deleterious pathological loop. This might explain cerebral disabilities observed later in acquisitions throughout the neurodevelopment.

## Concurrent Functional Near-Infrared Spectroscopy and Motion Tracking to Assess Functional Improvement of Children with Cerebral Palsy After Constrained Induced Motion Therapy

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A special interest in functional neuroimaging is to quantify brain plasticity as identified by changes in cortical activation patterns after therapy. In this work we will image cortical plasticity in children with cerebral palsy (CP) after they have undergone occupational therapy. In recent studies<sup>1</sup> we have demonstrated that functional near-infrared (fNIR) imaging is a viable and sensitive method for mapping motor cortex activities in children with CP. FNIR imaging metrics such as Time-to-Peak (TtP), Duration, Laterality Index (LI), and Area of Activation (AoA) were found to be significantly different between CP and age-matched healthy children. In addition to fNIR imaging, quantitative information about the actions performed during imaging can be used to correlate the child's physical improvement to the changes seen in cortical activity. Thus in this study, fNIR imaging and measurements of the movement will be performed concurrently. Additionally, the fNIR imaging field of view will be expanded to include the secondary motor areas (premotor cortex and supplementary motor area), and both tapping and sequential tapping will be performed by the children during the imaging. Both types of tapping will be tracked by a 6-camera motion tracking system which will determine the three dimensional positions of retro-reflective targets placed on the fingers, wrists, and arms of the children. These measurements will be done on four children with CP before and immediately after two weeks of constrained induced motion therapy (CIMT), and on 5 age-matched healthy controls. Improvements in motor performance will then be determined by the changes in motion tracking metrics before and after therapy and these will be correlated to the spatio-temporal changes in cortical activity patterns.

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Keywords: functional imaging, near-infrared, cortical activation, motion tracking, cerebral palsy

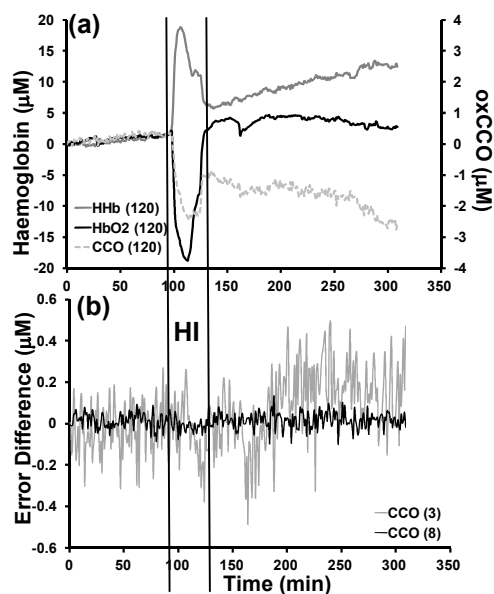
Poster Session  
**Other**  
Poster #: 107-115

## Optimal Wavelength Combinations for Resolving in-vivo Concentration Changes of Haemoglobin and Cytochrome-c-Oxidase with fNIRS.

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**Introduction:** In continuous-wave fNIRS we employ a linear algorithm that relates the changes in optical attenuation (measured in discrete near-infrared wavelengths) with the changes in concentrations of the tissue chromophores of interest - oxy-, deoxy- haemoglobin (HbO<sub>2</sub>, HHb) and oxidised cytochrome-c-oxidase (oxCCO) - scaled with their optical absorption characteristics and the total pathlength of light. This spectroscopic approach has the potential to cause crosstalk between the concentration measurements of the three chromophores. It has been suggested that this can be minimised by utilising a large number of optical wavelengths[1]. Here we investigate the issue of wavelength number versus wavelength combination. **Methods:** We use changes in attenuation measured between 780-900nm with 1nm resolution from the piglet brain with broadband spectrometer during hypoxic-ischaemia (HI) when the haemoglobin and oxCCO changes are large[2]. We then continued to investigate the optimal number and combination of 3, 4, 5, 6, 8 NIR wavelengths out of the 120 that can produce similar estimations for the three chromophores. We chose that wavelength range due to greater availability of discrete laser sources in that range. The possible combinations in that range for example for eight wavelengths out of the 120 wavelengths are 899,749,479,915. Resolving these combinations is computationally unrealistic. To tackle the issue we estimate a normalised root mean square residual for all three chromophores. We then implement a minimisation function based on the use the genetic algorithm (GA); we modified the Matlab built-in function for GA provided in the Global Optimization Toolbox (MathsWork Inc.). GA is a



**Fig 1.** (a) Concentration changes in a piglet study during HI as estimated using broadband (120 wavelengths) NIRS data resolving from 780-900nm ("gold standard"); (b) Absolute difference in  $\mu\text{M}$  of oxCCO concentration changes versus the "gold standard" when resolve for the optimised 3 (790,834,886nm), 8 (784,800,819,842,855,870,879,894nm) wavelengths.

technique that uses heuristic search to solve for solutions to optimisation problems using natural evolution such as selection of population, mutation and crossover. **Results:** Figure 1(a) shows an example from an animal that experienced a severed insult without recovery and Figure 1(b) the difference that wavelength numbers have to the concentration of oxCCO. Using data from 10 animal studies during HI we have identified the optimum wavelength number to be 8 and wavelength combination for these 8 wavelengths to be  $\lambda_1=784$ ,  $\lambda_2=799-804$ ,  $\lambda_3=815-819$ ,  $\lambda_4=829-833$ ,  $\lambda_5=855-859$ ,  $\lambda_6=869-873$ ,  $\lambda_7=878-881$  and  $\lambda_8=894-895\text{nm}$ . **Discussion:** Broadband NIRS provides the optimum solution for resolving the changes in the HbO<sub>2</sub>, HHb and oxCCO however these systems are expensive and not commercially available for medical use. A NIRS system with a discrete number of wavelengths can be a cheaper solution but careful selection of the wavelength combination is needed to minimise any crosstalk effects. Here we suggest possible wavelength combinations based on experimental data and using our novel GA optimisation tool.

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## Performance assessment of time-domain fNIRS instruments in the “nEUROPt” project

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**Introduction:** The European project “nEUROPt” (FP7-HEALTH-2007-201076) was devoted to developments in technology and data analysis for time-domain optical brain imaging and their application in clinical pilot studies. To assess and compare the performance of instruments as well as methods of data analysis, standardized protocols were developed and applied. While the previous “MEDPHOT” protocol [1] was employed to assess photon-migration instruments with respect to their ability to measure the optical properties of homogeneous media, specific tests for optical brain imagers were covered with two new protocols. The “Basic instrumental performance” (BIP) protocol [2] is related to relevant, solely instrumental characteristics. The “nEUROPt” protocol [3] addresses sensitivity, spatial resolution and quantification of absorption changes in the brain by measurements on specific inhomogeneous phantoms.

**Methods:** As part of the BIP protocol, a novel test measures the responsivity of the detection system, i.e. the overall efficiency to collect and detect light emerging from tissue. For this test dedicated, spectrally characterized solid slab phantoms were used. The “nEUROPt” protocol was implemented with liquid phantoms based on Intralipid [4] and ink [5], with black inclusions and, alternatively, in two-layered geometry. Small black cylinders of various sizes were used to mimic small localized variations of the absorption coefficient. Their position was varied in z (depth) and x-y direction to measure contrast and spatial resolution. Two-layered liquid phantoms were used, in particular, to determine depth selectivity, i.e. the ratio of contrasts due to a deep and superficial absorption change of the same magnitude. Measurements were analyzed by methods based on time windows and moments of time-of-flight distributions.

**Results:** Four groups in the “nEUROPt” consortium applied the protocols together with guidelines for their implementation to characterize their time-domain optical brain imagers. Several synthetic descriptors, e.g. for contrast, contrast-to-noise ratio, depth selectivity, were employed to quantitatively compare the various instruments and approaches of data analysis.

**Conclusions:** Most of the tests are not restricted to time-domain methods but are applicable to fNIRS instrumentation in general. With some modification, part of the phantom tests can be adopted for verification purposes in a future fNIRS standard.

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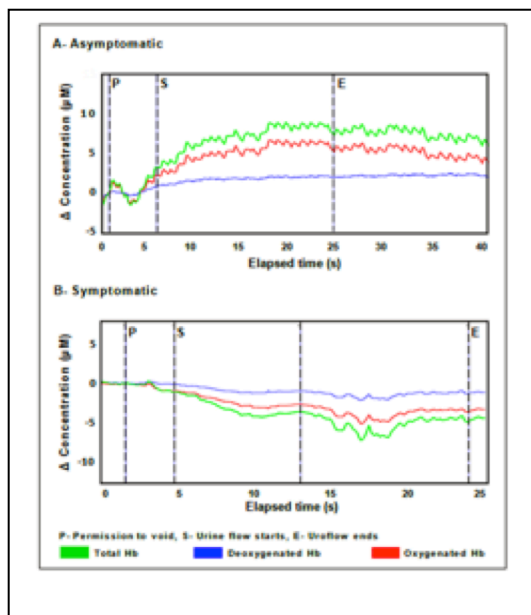
### Near infrared spectroscopy of the bladder to monitor physiologic function in health and disease.

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NIRS applications for bladder studies are recent. The bladder is uniquely vascularised so that the microcirculation can maintain perfusion as the organ contracts and then fills. Various diseases compromise the ability of the microcirculation to maintain perfusion during the spatial changes that occur during filling and emptying, and/or affect the mechanics and physiology of detrusor muscle contraction. As the bladder empties contraction of the detrusor muscle generates changes in oxygenated and deoxygenated haemoglobin concentration which allow variations in the organ's hemodynamics and oxygen supply and demand to be inferred. This information is not available to urologists by other means and their current 'gold standard' test (UDS) used to evaluate all forms of voiding dysfunction is invasive and only measures bladder pressure and urine flow. Consequently non-invasive transcutaneous optical monitoring of the bladder is both relevant and clinically desirable.

The feasibility of various devices has been demonstrated: continuous wave with lasers, single and multi-channel, emitter/detector grid configuration for fNIRS mapping, and a miniaturized self-contained wireless instrument with light emitting diodes (LED) and spatially resolved emitter/detector geometry.

Different trends and patterns of chromophore change are evident from monitoring the voiding cycle in patients in health and disease (figure). Such patterns 'match' NIRS data from other tissues where altered hemodynamics and impaired oxygen supply and demand occur, and hence provide novel insights into the underlying causes of voiding dysfunction, and choice of potential therapeutic interventions. Three different diagnostic algorithms have also been studied; all incorporate elements of bladder NIRS data reflecting differences in detrusor hemodynamics and have comparable discriminant ability, good specificity and sensitivity, and concordance (89%) with 'gold standard' UDS pressure flow data in the diagnosis of bladder outlet obstruction due to prostatic hyperplasia in independent studies.



Confidence that bladder NIRS measures physiologic changes in the detrusor comes from: the physics of penetration, scattering and chromophore absorption of NIR photons; the consistent anatomic position of the bladder and ultrasound evidence that the anterior wall maintains its spatial geometry with a NIRS device on the lower abdominal skin during voiding; and because the changes only occur over the bladder (not control emitter/detectors elsewhere on the abdomen) and in relation to events in the voiding cycle.

The evolution of wireless NIRS methodology for bladder studies is an example of effective clinician researcher collaboration; miniature self-contained devices with LEDs and 'oxygen saturation' capability make monitoring in ambulant subjects straightforward, and studies possible in special populations such as children and patients with spinal cord injury.

Hence, bladder NIRS is an advance of relevance in urology, and wireless devices offer an avenue to expand research and clinical monitoring in this field and a new opportunity to progress further with translation of NIRS into other relevant clinical arenas.



## *In vivo* Time-resolved DOT images of human forearm under exercises

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### 1. Introduction

During the forearm exercise, it is generally understood that the inner muscles work for the task, and the outer muscles work to fix the joints for efficient work of the inner muscles.

Time-resolved diffuse optical tomography (TR-DOT) can provide cross-sectional images of the change in the oxygenation state inside human forearm. *In vivo* measurements using a TR-DOT system were performed for human forearms under the handgrip exercises. The tomographic images of the oxygenation state were reconstructed using the algorithm based on the modified generalized pulsed spectrum technique<sup>[1]</sup>.

### 2. Methods

A 16-channel TR-DOT measurement system was used for the measurements. Total 16 fiber probes were fixed around the forearms of subjects through a circular fiber holder with an equal spacing. One fiber probe working as a source illuminated the forearms with pulsed light, and the other fiber probes detected light transmitted through the forearms. Repeating the measurements by changing the source probe, we acquired a dataset for image reconstruction. Data acquisition time for one DOT image was about 150 sec. Reference data were firstly acquired before exercise. Soon after the reference measurement, the subject was asked to start the handgrip exercise. 30 sec after the start of the exercise, another measurement was performed without changing the system conditions.

Modified generalized pulse spectrum technique (mGPST) was used for the image reconstruction. It is a Newton-Raphson method based technique, which minimizes, in the least-square sense, the error between the featured data and the forward solution of the Laplace-transformed photon diffusion equation by updating the distributions of the optical properties iteratively. The finite element method was employed to solve the photon diffusion equation.

### 3. Results and Summary

Figure 1(a) shows the reconstructed DOT images of the changes in the concentrations of the oxy-Hb&Mb, deoxy-Hb&Mb and total-Hb&Mb by the handgrip exercise when the forearm was placed horizontally on an arm holder. These images are the differential images between the task and reference states. By comparing with the MR-image, the large oxygenation changes appearing inside the forearm are believed to show the activities of the inner muscles.

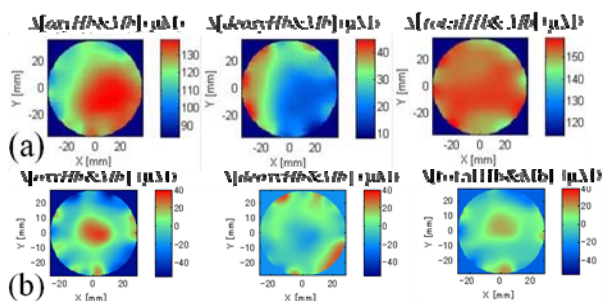
Figure 1(b) shows the reconstructed DOT images when the forearm was hung vertically without an arm holder. Large oxygenation changes also appear inside the forearm. The area of the large oxygenation changes is smaller than in the case of Fig. 1(a). The difference in the images between the cases of horizontal placement and vertical hanging of the forearms may be due to the difference in the types of the active inner/outer muscles.

### 4. Acknowledgement

This work was supported by KAKENHI (22300151).

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Figs. 1 Reconstructed  $\Delta$ Hb&Mb images generated from TR-DOT measurement for handgrip exercises with the two attitudes.

(a) Forearm was placed horizontally.  
(b) Forearm was hung vertically.

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## **Introduction**

Functional near-infrared spectroscopy (fNIRS) is a non-invasive brain imaging method that uses light to record regional changes in cerebral blood oxygenation during functional tasks. In a set of experiments, we have applied fNIRS to study cortical brain activations during vestibular and posturography testing.

## **Methods**

A 32-channel device was used to record brain activation during a series of vestibular experiments.

Caloric stimulation. A bilateral fNIRS probe was used to record brain activity from the frontal and temporal regions of 20 healthy persons: (N=10 young; N=10 older). Brain responses were recorded during warm (44°C) and cool (30°C) caloric irrigations. The older group showed increased bilateral activations of the superior temporal gyrus (STG) compared to the younger population.

Dynamic Posturography. FNIRS was recorded during sensory organization testing (SOT) on an Equitest™ platform in ten young healthy volunteers. Brain areas in STG and frontal cortex (FC) were activated during the SOT conditions.

Rotational testing. A 4-channel wireless fNIRS system was built to allow measurements in STG during earth-vertical axis rotational testing. Bilateral STG/SMG activation was recorded from twenty healthy volunteers (N=10 young; N=10 older) during sinusoidal rotation (0.1 Hz, 60 deg/sec) in the dark.

## **Results**

In each of these experiments, significant changes in the superior temporal gyrus were recorded using fNIRS. This finding is consistent with the role of this part of the brain in cortical processing of secondary vestibular information.

## **Conclusions**

These experiments demonstrate the feasibility of using fNIRS imaging for studying cortical activity during vestibulo-ocular and postural challenges.

**Exploring the effects of Nilvadipine on blood pressure, cerebral blood flow and cerebral autoregulation in patients with mild to moderate Alzheimer's Disease: a NILVAD add-on study**

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**Introduction:** Nilvadipine is a dihydropyridine calcium channel blocker with putative neuroprotective properties. For instance, in comparison with amlodipine, nilvadipine showed favourable effects on cognitive function with stabilization of cognitive decline and reduced conversion to AD in hypertensive patients with mild cognitive impairment (Hanyu et al. 2007). It has a selective effect on the cerebral artery contrary to other calcium channel blockers and it easily penetrates the central nervous system through the blood-brain barrier. In a European phase III trial (the NILVAD study), the efficacy and safety of nilvadipine as a disease course modifying treatment in mild to moderate AD will be investigated, focussing on changes in cognitive function.

As an add-on study to NILVAD, we will investigate the physiological effects of nilvadipine on blood pressure, cerebral autoregulation, cerebral blood flow, and Alzheimer-related cerebral damage in 40 patients who participate in the NILVAD study in Nijmegen (the Netherlands).

**Methods:** In this double-blind randomised controlled study a total of 40 mild to moderate AD patients (MMSE  $\geq 12$  and  $\leq 26$ ) will be enrolled. For 18 months, they will take either nilvadipine (8 mg) or a placebo daily. At baseline, after 24 weeks and 72 weeks participants visit our clinic for measurements. In the week prior to the visits home-based blood pressure will be measured daily, to ensure reliable values on blood pressure and blood pressure variability. The measurements during visits consist of: 1) continuous NIRS measurements (frontal cortical oxygenation); 2) simultaneous Transcranial Doppler and continuous blood pressure monitoring to provide (together with NIRS) insight in the pressure-flow relationship (cerebral autoregulation); and 3) Arterial Spin Labeling MRI, providing information on regional cerebral blood flow. Main outcomes are the changes from baseline to week 24 (and week 72) in these parameters.

**Results:** The enrolment for this study is planned to start in October 2012. Results of baseline measurements are expected in 2014, and completion of the data collection in 2016.

**Hypothesis:** We hypothesize that treatment with nilvadipine will improve blood pressure stability and cerebral perfusion in patients with AD, and that these effects will constitute the basis of the hypothesized beneficial effects of nilvadipine on cognition. Due to cortical atrophy and affected microvessels in patients with AD, cerebral perfusion is declined. Among others, improvement of cerebral perfusion by nilvadipine can be reflected in oxygenation levels measured with NIRS (Claassen and Zhang, 2011; van Beek et al. 2010; van Beek et al. 2012).

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## Hemodynamic cerebral response as a function of the neurovascular coupling to brain activation: NIRS signal changes

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*Keywords: physiological modeling, NIRS signal, neurovascular coupling*

In the brain, coupling of neuronal activity and metabolism with regional blood flow and cerebral blood oxygenation is tight (i.e., the so-called neurovascular coupling). Precisely, it is the mechanism by which focal neuronal activity produces an undue increase of local blood flow in the microvasculature after brain activation. This excessive influx of blood termed “functional hyperemia” was described first by Roy and Sherrington (1890) who postulated that chemical by-products of metabolism (vasoactive substances) affected the vessel wall, altering the arteriole and capillary caliber. It is often assumed that hyperemia serves to sustain neuronal tissue metabolism by adjusting the blood flow to meet energy needs (glucose and oxygen supply). Assessing neuronal activity by non-invasive techniques of functional brain imaging, which are based on the hemodynamic responses, depends totally on the physiological cascade of metabolism and blood flow. At present, blood-oxygen-level dependent functional MRI (BOLD-fMRI) and functional NIRS (fNIRS) are widely used in cognitive neuroscience to depict the hemodynamic response as a function of the neurovascular coupling to brain activation. Due to the high temporal resolution, the NIRS measurement has advantages over BOLD-fMRI in that it is possible to characterize more accurately the transient response of blood volume and oxygenation time courses. However, the lack of a detailed understanding of the underlying physiology did not hinder to interpret correctly the NIRS signal changes. Knowledge of how neurovascular coupling is extracted from NIRS data is crucial for understanding, analyzing and interpreting various NIRS pattern responses in healthy and disease people. Indeed, the output NIRS signals during functional brain activity depend upon many hemodynamic and physiological interrelated parameters like regional cerebral blood flow (rCBF), volume (rCBV), cerebral metabolic rate of oxygen (CMRO<sub>2</sub>), cerebral metabolic rate of glucose (CMRGluc), oxy- and deoxy-hemoglobin concentration changes ( $\Delta[\text{HbO}_2]$  and  $\Delta[\text{HHb}]$ , respectively). We have investigated, reviewed and integrated several recent findings, models and knowledge to provide an original schematic illustration of time courses of  $\Delta[\text{HbO}_2]$  and  $\Delta[\text{HHb}]$  and hemodynamic variables as a function of the neurovascular coupling during brain activation. Accordingly, since the most notable NIRS pattern found in the literature is a localized increase in  $\Delta[\text{HbO}_2]$  with a concomitant drop in  $\Delta[\text{HHb}]$  over an activated brain area, we proposed below this illustration for short (2 s) or long (60 s) functional stimulus application (Figure).

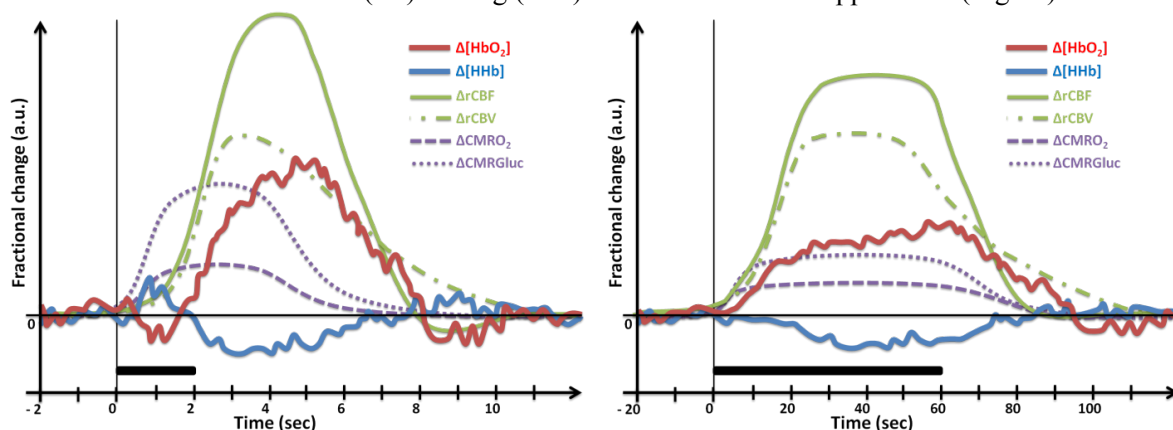


Fig. The typical NIRS signal changes observed during and after short (at the left) or long (at the right) functional stimulation.

## Analysis of Stroop Test fNIRS data by use of Singular Value Decomposition

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**Introduction:** The prefrontal region of brain is composed billions of neurons working in a connected manner. Through fNIRS measurements we can observe only groups of these neurons due to finite resolution of the technique. In this work AR(1) model is used to obtain the connectivity pattern of the prefrontal brain region. An SVD based scheme is exploited to suppress the common mode network and highlight the single channel pairs that are strongly connected.

**Method:** fNIRS data were collected from 12 healthy subjects during Stroop Test. This test is composed of three different question types: neutral, congruent and incongruent (N, C, IC). Subjects respond to 30 questions of each type that are clustered into 5 blocks. The blocks are randomly interchanged for each subject. After each question block there is a 20 second rest. The data is preprocessed by a Hampel filter to eliminate the outliers and band-pass filtered in the interval (0.003-0.08 Hz). The AR(1) model is given as  $Y_{j+1} = AY_j + n_j$  where  $Y_j$  is the time series of the 16 channel fNIRS measurements at “ $j^{\text{th}}$ ” time interval and  $A$  is the AR(1) connectivity matrix.  $A$  matrices are calculated for each question block by use of maximum likelihood estimate and averaged over blocks to obtain the representative  $A$  matrices for each question type for each subject. The connectivity  $A$  matrix is modeled as  $A = A_{CN} + A_{N,C,IC} + A_{RN}$  and decomposed via SVD method where the lower valued eigenvalues stand for the random network (noise) part  $A_{RN}$ , higher eigenvalues stand for the common mode Stroop activity related network  $A_{CN}$ , while the middle part stands for true Stroop test related connectivity:  $A_{N,C,IC}$ .

**Results and Discussion:** ANOVA is applied to 12 subjects for the three question types.  $p < 0.05$  values are thresholded. As a result 13 entries are found to be significant in the Stroop test: (1,14) (2,11) (3,7) (6,13) (6,15) (9,11) (10,11) (11,9) (12,9) (12,11) (12,14) (14,3) (15,1). The second entry means that it exerts influence to the first entry. For example 1,14 means: 14<sup>th</sup> region influences the 1<sup>st</sup> region.

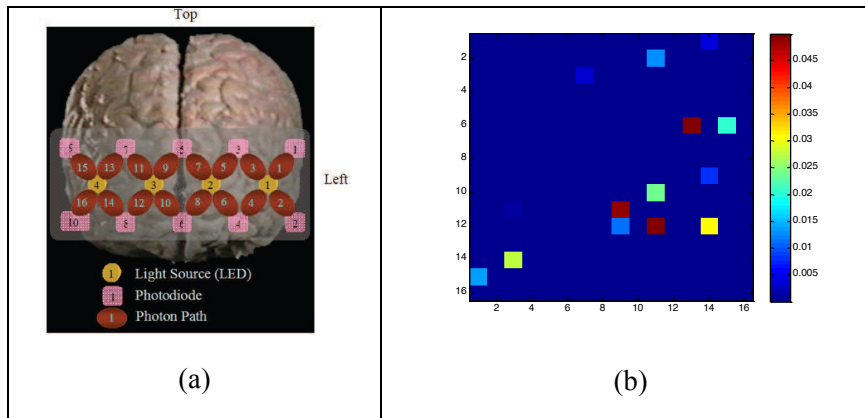


Fig1. (a) Locations of the channels on the forehead and the approximate corresponding PFC sampling area (channels in red) (b) Statistically significant entries in the  $A$  matrix (the right bar is the  $p$  value)

**Conclusion:** Channels 11 and 14 on the right middle PFC seem to influence the rest of the channels with a stronger influence suggesting a right dominance during the stroop activity while Ch 11 seems to be the most influenced. Hence Ch 11 can be a hub for the Stroop activity.

## Cerebral oxygenation measurement with acousto-optics: a simulation study

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In functional near infrared spectroscopy (fNIRS), a widely adopted kind of optical probe consists of a single optical source and a single detector, which measure optical attenuation reflected back from the cortex. The sensitivity profile of this optical probe has a “banana” shape [1]. An example of the sensitivity profile is shown in Figure 1. It is noted that the most sensitivity region is in fact near to the skin, rather than in the brain. This is the reason why in many fNIRS studies, the systemic response, which also manifests itself in the skin, greatly affects the cerebral oxy- and deoxy-hemoglobin signals leading to a high number of false positives [2].

In this work, we consider a new design of optical probe which incorporates focused ultrasound with fNIRS, a technique known as acousto-optics. When diffused photons pass through an ultrasound field, their optical phases are modulated by the ultrasound. The focused ultrasound therefore acts like it were “tagging” the photons. Although ultrasound is highly attenuated by the skull, this technique only requires ultrasound to go one way into the brain (rather than two-ways as in the case of ultrasound imaging), which makes the focusing of ultrasound in the brain feasible.

We have been developing computational models for acousto-optics including Monte Carlo simulations [3, 4] and finite element method (FEM) models. Figures 1 and 2 depict our recent FEM results for an optical probe and an acousto-optic probe. It can be seen that the sensitivity profile of the acousto-optic probe has much higher sensitivity values inside the head model, in comparison to that of the optical probe. These simulations were based on a simple homogenous, circular geometry. In the conference, simulation results based on anatomical head geometries will be presented. This work explores the feasibility of applying acousto-optics to fNIRS which may one day offer a better solution to improve the accuracy of fNIRS studies.

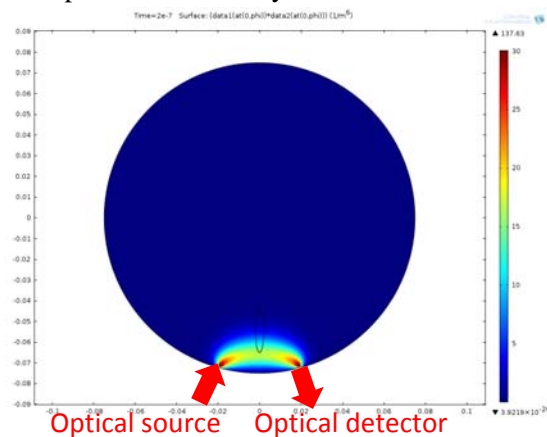


Figure 1 Sensitivity profile of an optical probe (note: red corresponds to higher values)

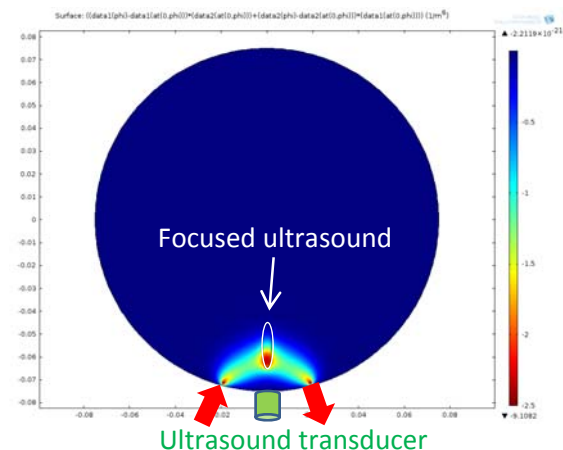


Figure 2 Sensitivity profile of an acousto-optic probe (note: red corresponds to higher values)

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