# **Using Optical Coherence Tomography** to Validate Diffusion MRI

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### Introduction

Diffusion-weighted MRI (DW-MRI) allows us to probe the microstructure of the white matter (WM) by estimating the preferential directions of the diffusion of water molecules at every voxel. Although DW-MRI is now widely used to study WM integrity in health and disease, its validation has been challenging due to the absence of ground truth regarding the true fiber orientations and connectivity of the brain. Tracer studies can be used for this purpose [2]. However, such tracers, like Dil [3], penetrate tissues very slowly, which limits their use in the human brain. Optical imaging, mostly using polarization, has emerged as a promising alternative [1, 7]. Here we propose to image WM fibers using Optical Coherence Tomography (OCT) with the goal of validating DW-MRI in ex vivo samples.

### **Methods and Materials**

**Optical coherence tomography** OCT is an optical technique providing **3D high resolution** images up to several hundreds of microns in depth in biological tissue [4]. This technique avoids cutting, mounting or staining and greatly reduces deformations in the tissue. OCT detects differences in refractive index between tissues types, e.g. cell bodies and myelinated fibers.

Our Set Up [6]

#### **ODF** Examples





Axial resolution : 3.5  $\mu$ m Lateral resolution 3  $\mu$ m Field of View:  $1.5 \times 1.5 \text{ mm}^2$ Maximum Intensity Projection (MIP) over 400  $\mu$ m Stitching

**Tissue Preparations** Fixed temporal lobe samples were used for this study. DW-MRI data was acquired on a 4.7T small-bore Bruker system with a solenoid coil (300  $\mu$ m resolution, 2 lowb images, 20 DW images with b=4028, TE=28ms, TR=320ms, FA=180°). A tensor was fit to the data at every voxel and the primary eigenvector of the tensor was extracted for comparison with the maxima of the OCT-derived ODFs. The samples were then sectioned to collect 50  $\mu$ m thick slices for histological staining. The remaining flat-faced tissue block was imaged with OCT.

Qualitative comparison Fig. 1A shows the MIP of the OCT imaging in a gyrus in the isocortex, where the fibers are clearly visible. Fig. 1B shows the gallyas stain slice of a similar tissue sample, where the fibers are stained in dark.



Fig. 2: ODF reconstructions for A: 1 visible fiber direction, B: 2 visible fiber directions and C: no visible fiber.

The figure shows the ODF for different study cases (A: 1 fiber orientation visible, B: 2 fiber orientations, C: no visible fiber) for different window sizes (1mm typical in vivo resolution, 300  $\mu$ m typical ex vivo resolution and 150 $\mu$ m). The colored circles represent the cut-off frequency of the low-pass filter.

### **Preliminary Results**



Fig. 1: A: MIP of the OCT data on part of isocortex sample, B: Gallyas stain on a similar sample.

### **Orientation Density Function Processing**

The in-plane fiber orientations in the isocortex sample are computed using a windowed Fourier analysis on the MIP images. The process of estimating the Orientation Density Functions (ODF) is described in the following diagram.



Fig. 3: Preferential direction of the fibers for various regions of interest assessed by the Fourier analysis of the MIP image obtained by OCT.

### **Advantages of OCT**

#### ► High resolution

OCT can image individual fibers, which allows the visualization of complex structures (crossing fibers, kissing fibers, grid...)

- ► 3D reconstruction of ODF at high resolution
- ► Cyto- and myelo- architecture obtained simultaneously<sup>1</sup>





. Cytoarchitecture of cortex imaged by Optical Coherence Tomography, poster 3639

## **Conclusion and Future Work**

The high resolution that can be attained by the OCT image processing approach described here makes it a promising tool for the validation of DW-MRI and perhaps for resolving crossing fibers by acquiring OCT data with a  $1\mu$ m resolution. Although we used 2D images in this preliminary study, OCT holds useful information in all 3 dimensions. In the future we will perform 3D reconstruction of a volume of several cm<sup>3</sup> by adding a vibrotome to our setup [5]. We also plan to take advantage of the myelin sheath surrounding the fibers by adding polarization sensitivity to the system. Finally, we intend to explore the use of OCT-derived information as priors for in vivo ODF estimation and tractography.

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