



BrainVision RecView

Software version 1.4.3



Software

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Contents

Contents	iii
List of figures	v
About this manual.....	15
Introduction.....	19
Chapter 1 Installation	23
1.1 Installing RecView under Windows®	24
Chapter 2 Configuring the software	27
2.1 Installing the RecView license	27
2.2 Configuring the Recorder	29
2.3 Configuring RecView.....	31
Chapter 3 Getting started and handling the program	35
3.1 The user interface	35
3.2 Performing a simple session.....	40
3.3 Selecting a master filter.....	44
3.4 Constructing a filter tree	45
3.5 The workspace concept	54
3.6 Command line parameters	56
Chapter 4 Configuring the user settings.....	61
4.1 Configuring the scaling.....	61
4.2 Configuring the axes	63
4.3 Graph display	65
4.4 Representation of the frequency bands.....	66
4.5 Adjusting the electrode positions	67
4.6 Configuring fast access to the parameters dialog	68
Chapter 5 Montages	69
Chapter 6 Basic filters	71
6.1 Average	72
6.2 Band Power Trigger	75
6.3 Bipolar Montage	79
6.4 Bridge Tool	81
6.5 FFT (Fast Fourier Transform)	85
6.6 Frequency Filter.....	88
6.7 Level Trigger.....	90
6.8 Linear Derivation.....	94
6.9 LORETA	97
6.10 Map	104

6.11	R-Peak Trigger	109
6.12	Segmentation	112
Chapter 7	Optional filters	115
7.1	MRI filter	115
7.2	Pulse-artifact filter.....	121
Chapter 8	Programming user-defined filters	127
8.1	Overview.....	127
8.2	Interfaces.....	128
8.3	Programming examples	130
Appendix A	Electrode coordinate system	133
Appendix B	Installing the RecView license from the Brain Products web site	135
Appendix C	How can I find the address of the LPT port?	139
Appendix D	Behavior of TTL pulses in different parameter configurations.....	141
Appendix E	Legal notes	145
	List of abbreviations	147
	Glossary.....	149
	Subject index	151

List of figures

Chapter 1 Installation

- 1-1 RecView screen 27

Chapter 2 Configuring the software

- 2-1 RecView license on the supplied USB data medium 35
- 2-2 Running the license file as administrator under Windows® 7 35
- 2-3 Calling Recorder program information 36
- 2-4 Displaying sub-licenses in the Recorder 36
- 2-5 "Preferences" in the Recorder menu 37
- 2-6 Activating the RDA server in the Recorder 37
- 2-7 Unblocking the Recorder software 38
- 2-8 Entering the server name 39
- 2-9 Calling the dialog box for selecting the Work Files folder 40
- 2-10 Selecting the Work Files folder 40
- 2-11 Calling the dialog box to enter the LPT port address 41
- 2-12 Entering the address of the LPT port 41

Chapter 3 Getting started and handling the program

- 3-1 Menu bar and toolbar 43
- 3-2 RecView interface 46
- 3-3 Tabs for switching between filter windows 47
- 3-4 Scaling bar at the end of the channel list 47
- 3-5 Scaling bar display in front of each channel 47
- 3-6 Markers displayed 48
- 3-7 Starting data viewing/recording in the Recorder 48
- 3-8 Simultaneous data view in the Recorder and RecView 49
- 3-9 Individual channel mode 49
- 3-10 Global deactivation of a channel 50
- 3-11 The VEOG channel has been deactivated globally and the HEOG channel locally 50
- 3-12 Impedance mode in the Recorder and impedance view in RecView 51

- 3-13 Dialog box for selecting the master filter 52
- 3-14 Empty filter tree 53
- 3-15 Adding subnodes to main filter nodes by means of drag-and-drop 54
- 3-16 Invalid filter combination: Frequency filter attached to FFT filter 54
- 3-17 Details on the currently selected filter 56
- 3-18 Context menu for filters 57
- 3-19 Invisible LORETA filter 57
- 3-20 Right-clicking to run RecView as administrator 58
- 3-21 Example error message from the Level Trigger filter if the LPT port address is not specified 58
- 3-22 Data representation with a filter tree 59
- 3-23 Functions for arranging the filter windows 60
- 3-24 Enlarging the data window to show the data correctly 61
- 3-25 Creating a new workspace 62
- 3-26 Saving the new workspace 63
- 3-27 Newly created "BrainVision1" workspace 63
- 3-28 Loading an existing workspace 64
- 3-29 Create shortcut on the Windows-Desktop 64
- 3-30 Open the shortcut properties 65
- 3-31 Editing the command line 66
- 3-32 Verify correct workspace 66

Chapter 4 Configuring the user settings

- 4-1 Calling the "Preferences" dialog box 67
- 4-2 Configuring the scaling parameters 67
- 4-3 Scaling selected channels 68
- 4-4 Configuring the axis parameters 69
- 4-5 Configuring the subdivisions of the axis (tickmarks) 70
- 4-6 Configuring how graphs are displayed 71
- 4-7 Defining frequency bands 72
- 4-8 Selecting the electrode positions 73

- 4-9 Configuring fast access to the filter parameter dialog 74

Chapter 5 Montages

- 5-1 Displaying and selecting montages (A) 75
- 5-2 Displaying and selecting montages (B) 76
- 5-3 Assigning keyboard shortcuts to montages 76

Chapter 6 Basic filters

- 6-1 Software filters active in the Recorder have no effect in RecView 77
- 6-2 Parameters dialog box for the Average filter 78
- 6-3 Average filter 80
- 6-4 Parameters dialog box for the Band Power Trigger filter 81
- 6-5 Band power trigger filter 83
- 6-6 Parameters dialog box for the Bipolar Montage filter 85
- 6-7 Bipolar Montage filter 86
- 6-8 Filter tree with Bridge Tool filter and associated parameters dialog box 87
- 6-9 Displaying gel bridges in the Paired Channel View 89
- 6-10 Parameters dialog box for the FFT filter 91
- 6-11 FFT in the frequency graph view using individual-channel mode 92
- 6-12 FFT in the map view 93
- 6-13 FFT filter without overlap (left) and with overlap (right) 93
- 6-14 Parameters dialog box for the Frequency filter 94
- 6-15 Frequency filter 95
- 6-16 Parameters dialog box for the Level Trigger filter 96
- 6-17 Level Trigger filter 99
- 6-18 Generating the new channel from the combination of the input channels Fp1 and Fp2 100
- 6-19 Parameters dialog box for the Linear Derivation filter 101
- 6-20 Generating new channels using the Linear Derivation filter 102
- 6-21 Parameters dialog box for the LORETA filter 103
- 6-22 Creating an ROI 103

6-23	Adding lobes	104
6-24	Adding a specific position	105
6-25	Adding a block	105
6-26	Part of the LORETA filter dialog box, containing a list of the components of the ROI "Frontal"	106
6-27	Display of the mouse pointer in the cross-section and the information field	107
6-28	Virtual channels "Frontal" and "Frontal_2"	108
6-29	Performing individual scaling of the the ROI channels (A)	109
6-30	Performing individual scaling of the ROI channels (B)	109
6-31	Configuring the Map filter for continuous time data	110
6-32	Map filter for continuous time data	111
6-33	Configuring the Map filter for segmented time data	112
6-34	Map filter for segmented and averaged time data	112
6-35	Configuring the Map filter for frequency data	113
6-36	Map filter for frequency data	114
6-37	Parameters dialog box for the R-Peak Trigger filter	115
6-38	Negative ECG curve (negative polarity) with steep R-peaks	117
6-39	R-Peak Trigger filter	117
6-40	Parameters dialog box for the Segmentation filter	118
6-41	Segmentation filter	119
6-42	Display of the segment number and the "Time Zero" marker	119

Chapter 7 Optional filters

7-1	Parameter dialog box for the MRI artifact filter	124
7-2	Advanced configuration of the MRI artifact filter	125
7-3	MRI artifact filter	127
7-4	Parameters dialog box for the Pulse-artifact filter	129
7-5	R-peak marker and correction of a channel	131

Chapter 8 Programming user-defined filters**Appendix A Electrode coordinate system**

A-1 Coordinate system for electrodes 140

Appendix B Installing the RecView license from the Brain Products web site

B-1 Data entry form for product registration 141

B-2 Login form 142

B-3 Download area for sub-license files 142

B-4 Installing sub-licenses 143

B-5 Displaying sub-licenses in the Recorder 143

Appendix C How can I find the address of the LPT port?

C-1 Displaying the address of the LPT port in the Windows® Device Manager 145

Appendix D Behavior of TTL pulses in different parameter configurations

D-1 Diagrammatic representation of the behavior of TTL pulses 149

Appendix E Legal notes**Installation 23**

RecView screen 24

Configuring the software 27

RecView license on the supplied USB data medium 27

Running the license file as administrator under Windows® 27

Calling Recorder program information 28

Displaying sub-licenses in the Recorder 28

Activating the RDA server in the Recorder 29

Unblocking the Recorder software 30

Entering the server name 31

Calling the dialog box for selecting the Work Files folder 32

Selecting the Work Files folder 32

Calling the dialog box to enter the LPT port address 33

Entering the address of the LPT port 33

Getting started and handling the program 35

Menu bar and toolbar 35

RecView interface 38

Tabs for switching between filter windows 39

Scaling bar at the end of the channel list 39

Scaling bar display in front of each channel 39

Markers displayed 40

Starting data viewing/recording in the Recorder 40

Simultaneous data view in the Recorder and RecView 41

Individual channel mode 41

Global deactivation of a channel 42

The VEOG channel has been deactivated globally and the HEOG channel locally 42

Impedance mode in the Recorder and impedance view in RecView 43

Dialog box for selecting the master filter 44

Empty filter tree 45

Adding subnodes to main filter nodes by means of drag-and-drop 46

Invalid filter combination: Frequency filter attached to FFT filter 46

Details on the currently selected filter 48

Context menu for filters 49

Invisible LORETA filter 49

Right-clicking to run RecView as administrator 50

Example error message from the Level Trigger filter if the LPT port address is not specified 50

Data representation with a filter tree 51

Functions for arranging the filter windows 52

Enlarging the data window to show the data correctly 53

Creating a new workspace 54

Saving the new workspace 55

Newly created "BrainVision1" workspace 55

Loading an existing workspace 56

Create shortcut on the Windows-Desktop 57

Open the shortcut properties 57

Editing the command line 59

Verify correct workspace 59

Configuring the user settings 61

Calling the "Preferences" dialog box 61

Configuring the scaling parameters 61

Scaling selected channels 62

Configuring the axis parameters 63

Configuring the subdivisions of the axis (tickmarks) 64

Configuring how graphs are displayed 65

Defining frequency bands 66

Selecting the electrode positions 67

Configuring fast access to the filter parameter dialog 68

Montages 69

Displaying and selecting montages (A) 69

Displaying and selecting montages (B) 70

Assigning keyboard shortcuts to montages 70

Basic filters 71

Software filters active in the Recorder have no effect in RecView 71

Parameters dialog box for the Average filter 72

Average filter 74

Parameters dialog box for the Band Power Trigger filter 75

Band power trigger filter 77

Parameters dialog box for the Bipolar Montage filter	79
Bipolar Montage filter	80
Filter tree with Bridge Tool filter and associated parameters dialog box	81
Displaying gel bridges in the Paired Channel View	83
Parameters dialog box for the FFT filter	85
FFT in the frequency graph view using individual-channel mode	86
FFT in the map view	87
FFT filter without overlap (left) and with overlap (right)	87
Parameters dialog box for the Frequency filter	88
Frequency filter	89
Parameters dialog box for the Level Trigger filter	90
Level Trigger filter	93
Generating the new channel from the combination of the input channels Fp1 and Fp2	94
Parameters dialog box for the Linear Derivation filter	95
Generating new channels using the Linear Derivation filter	96
Parameters dialog box for the LORETA filter	97
Creating an ROI	97
Adding lobes	98
Adding a specific position	99
Adding a block	99
Part of the LORETA filter dialog box, containing a list of the components of the ROI "Frontal"	100
Display of the mouse pointer in the cross-section and the information field	101
Virtual channels "Frontal" and "Frontal_2"	102
Performing individual scaling of the the ROI channels (A)	103
Performing individual scaling of the ROI channels (B)	103
Configuring the Map filter for continuous time data	104
Map filter for continuous time data	105
Configuring the Map filter for segmented time data	106
Map filter for segmented and averaged time data	106

Configuring the Map filter for frequency data 107

Map filter for frequency data 108

Parameters dialog box for the R-Peak Trigger filter 109

Negative ECG curve (negative polarity) with steep R-peaks 111

R-Peak Trigger filter 111

Parameters dialog box for the Segmentation filter 112

Segmentation filter 113

Display of the segment number and the "Time Zero" marker 113

Optional filters 115

Parameter dialog box for the MRI artifact filter 118

Advanced configuration of the MRI artifact filter 119

MRI artifact filter 121

Parameters dialog box for the Pulse-artifact filter 123

R-peak marker and correction of a channel 125

Programming user-defined filters 127

Electrode coordinate system 133

Coordinate system for electrodes 134

Installing the RecView license from the Brain Products web site 135

Data entry form for product registration 135

Login form 136

Download area for sub-license files 136

Installing sub-licenses 138

Displaying sub-licenses in the Recorder 138

How can I find the address of the LPT port? 139

Displaying the address of the LPT port in the Windows® Device Manager 139

Behavior of TTL pulses in different parameter configurations 141

Diagrammatic representation of the behavior of TTL pulses 143

Legal notes 145



About this manual

This User Manual describes the ExG visualization software BrainVision RecView Version 1.4.3. It is part of the software product.

It is essential to follow the instructions in the manual in order to use the software correctly and as intended.

The structure of the manual

The User Manual has 8 chapters:

- ▶ [Chapter 1](#) contains a description of the individual installation steps.
- ▶ [Chapter 2](#) contains instructions on how to configure RecView and the BrainVision Recorder recording software before you can start viewing and recording data.
- ▶ In [Chapter 3](#) you will learn how to operate RecView.
- ▶ [Chapter 4](#) provides information on configuring the user-specific settings.
- ▶ [Chapter 5](#) describes the use of montages.
- ▶ [Chapter 6](#) and [Chapter 7](#) describe all the filters that are available for RecView.
- ▶ In [Chapter 8](#) you will find information on how to program your own filters.

Who is the manual intended for?

The current User Manual is intended for users in the psychological and neurophysiological research area as well as physicians and medical experts.

Conventions used in the manual

The manual uses the following typographical conventions:

<i>italic</i>	Italic text is used to identify menus, menu commands, dialog boxes, buttons, options and the names of files and folders. Italic font is also used to highlight portions of running text.
<u>underscore</u>	Underscored text indicates a cross-reference or a web address.
monospaced	A monospaced font is used to indicate text or characters to be entered at the keyboard, such as source code and programming examples.
●	The blue dot indicates the end of a chapter.

The manual also uses the following symbols to help you find your way around:



Personal injury: This symbol indicates that incorrect use of the devices may result in a health hazard to the test subject, the user and/or a third-party. Failure to observe the information in these Operating Instructions constitutes incorrect use.



Damage to property: This symbol indicates that incorrect use of the devices may bring about an urgent risk of damage to property.



Stop: This symbol indicates that you should not carry out a particular action.



Cross-reference: This symbol indicates a reference to a related chapter, section or document.



Note: This symbol draws your attention to important information relating to the current topic.



Tip: This symbol draws your attention to recommendations on how to use our products.



New: This symbol indicates that the Operating Instructions have been changed or that new material has been added at this point.

Revision history

Page	Status	Subject
25	modified	Windows XP and Windows Vista are no longer supported.
26	modified	Installation procedure has been updated to remove Windows XP and Vista.
29	modified	BrainVision Application Suite USB replaces the previous DVD version.
30	modified	Screenshot updated.
31	modified	Screenshot updated.
33	modified	Updated to remove references to Windows XP and Vista.
140	modified	Screenshot updated.

Reporting errors and support

You can search for updates of this manual on our Web site under www.brainproducts.com/downloads.php?kid=5&tab=2.

If you require technical support or if you discover a mistake in the manual, the software or during operation, please contact:

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Web site: <http://www.brainproducts.com>

Email: techsup@brainproducts.com

On request, the technical support team will also send you a form to assist in clarifying faults and problems. ●



RecView and its functions

The BrainVision Recording Viewer – referred to below as RecView – is an add-on module for the BrainVision Recorder recording software that allows you to assess the quality of the EEG recording. RecView allows you to process the recorded data in real-time and provides a number of Online processing filters for this purpose.

In addition to traditional signal processing filters such as the Frequency filter or the FFT filter, RecView also provides special filters for correcting scanner and pulse artifacts for data recorded during combined fMRI-EEG measurements.

The Segmentation filter and Average filter allow you the option of viewing your data by segment and carrying out event-related and marker-based analyses. You can use the extended Average filter to calculate weighted averages with various weighting functions in both the time and frequency domains.

The FFT filter possesses configurable window functions to improve the calculation of the frequency spectrum.

The LORETA filter allows you to calculate virtual channels over "regions of interest" and to use the LORETA method to trace signals back to their sources in the various regions of the brain.

The Linear Derivation filter allows you to define new channels as linear combinations of existing channels. Alongside manual configuration, it is also possible to read the coefficient matrix from a text file.

RecView also possesses three filters which can directly address your computer's parallel port: The Level Trigger filter sends signals to the parallel port as a function of the voltage curves, the R-Peak Trigger filter is a variation of the Level Trigger filter which sends signals to the parallel port when ECG peaks are detected. The Band Power Trigger filter sends signals depending on the characteristics of the frequency spectrum.

RecView can not only display the impedance values but also possesses an innovative function for improving the quality of your EEG recordings: The Bridge Tool filter is used to detect gel bridges and assists you to prepare for the acquisition of EEG data using a large number of channels.

You can daisychain filters and introduce branches to create extensive filter trees, thus allowing you, for instance, to take the output data from an MRI artifact correction and use it as the input data for an FFT filter. Or you can implement the Level Trigger filter after the LORETA filter and use the voltage curve from your virtual ROI channel to control a feedback application as part of a BCI experiment.

The modular structure of RecView allows you to expand the software to incorporate additional, user-defined filters in the same way as you can for the transforms of our EEG analysis software BrainVision Analyzer.

You can run RecView on the computer on which the Recorder is installed or on further computers in the network. This networking capability means that you can run up to ten RecView programs simultaneously on different computers in conjunction with just one Recorder.

Intended use

As of September 30th, 2013 and software version 1.4.3, BrainVision RecView is not a medical device anymore and may be used in the context of non-medical applications in order to carry out fundamental or applied research on the basis of neurophysiological methodology and data.

RecView is intended to be used for visualizing and processing electrophysiological signals (e.g. EEG, EMG, ECG, EOG) and/or signals from other approved sensors. RecView allows ExG¹ data to be viewed concurrently while it is being recorded using the ExG recording software Recorder and is only to be used in conjunction with the Recorder.

Use of the RecView for diagnosis, therapy, monitoring of vital life functions (such as cardiovascular functions etc.) or other medical purposes is expressly forbidden.

The user is solely liable for any risks to test subjects associated with the investigation if the software is not used in accordance with the correct use described. Brain Products GmbH provides no guarantee and accepts no liability for the results obtained with RecView.

Correct use

BrainVision RecView is permitted to be used by users in the psychological and neurophysiological research area as well as physicians and medical experts.

BrainVision RecView is not permitted to be used by

- ▶ unqualified persons (e.g. laymen),
- ▶ people who personally cannot read or understand the User Manual (e.g. due to insufficient language knowledge, due to blindness).

BrainVision RecView can be used to view and filter neuro-/electrophysiological signals from healthy and sick adults, children and animals

Irrespective of any liability on our part, the specialist staff must observe the relevant national stipulations for operators and other relevant national legislation.

1. EEG, EOG, ECG, EMG, EDA, etc.

If you record EEG/ExG signals in an MR scanner, the computer must always be positioned and used outside the scanner room.



Personal injury

All versions of BrainVision RecView that have been released into the market as medical products do remain medical products. Brain Products will continue to treat them as medical products (i.e. to perform post market surveillance, for example) until the end of their service life.



The user should be aware that if a former BrainVision RecView version that was a medical product is replaced by a newer version that is not a medical product anymore, the terms and conditions of the new BrainVision RecView version are effective only from then on.



Use together with other products and components

BrainVision RecView is foreseen by the manufacturer to be combined with BrainVision Recorder.





Chapter 1 Installation

Under normal conditions, RecView does not cause any conflicts with other programs that are already installed. Brain Products GmbH, however, only guarantees that programs will interact without problems if the programs concerned have been tested for compatibility. This applies to the EEG analysis software BrainVision Analyzer, BrainVision Recorder and to the Microsoft operating systems, Windows® 7 SP1 (32-bit or 64-bit), Windows® 8.1 (64-bit) and Windows® 10 (64-bit).



To use RecView, you must have installed the recording software BrainVision Recorder Version 1.10 or later on your computer and you must possess a license for RecView.

General conditions

If you are using additional computers, you must ensure that there is a TCP/IP network connection between the computers.

The system has the following hardware and software requirements:

System requirements

- ▶ Operating system: Windows® 7 SP1 (32-bit or 64-bit), Windows® 8.1 (64-bit), Windows® 10 (64-bit).
- ▶ Minimum configuration: Intel Pentium IV, 2 GHz processor or higher, 512 MB of RAM, graphics card with 64 MB of RAM.
- ▶ Minimum 1 GB free hard disk space. Additional storage requirements depend on the extent of the data to be processed.
- ▶ We recommend a monitor with a screen diagonal of at least 17". For more than 32 channels, you should use a 21" monitor.





1.1 Installing RecView under Windows®



Please make sure that you possess the most recent RecView program version – including any updates. You can check whether a more recent version is available on our Web site at <http://www.brainproducts.com/downloads.php?kid=3&tab=1>.



1 Start Windows®.

2 Insert the Application Suite USB into a USB drive.

Open Windows Explorer or My Computer and browse to the location of the Application Suite USB.

3 Double click to open the folder.

4 Double click **Autorun.exe**.

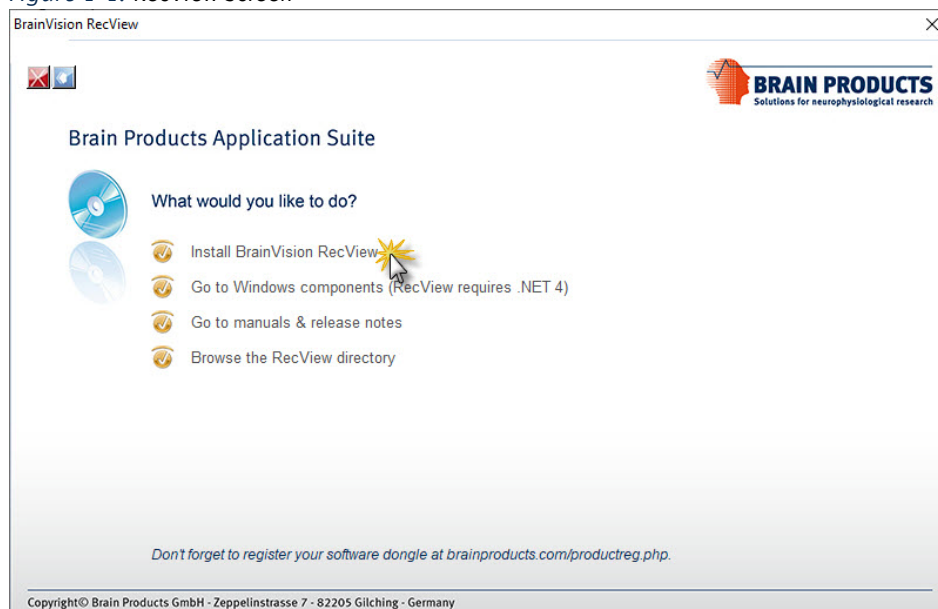
The Welcome screen opens.

5 Click **Install BrainVision RecView**.

The RecView screen opens (Figure 1-1).

You require Microsoft .NET Framework Version 4.0 or later to be able to use RecView. If this runtime environment is not present on your computer, click **Go to Windows components** and install **dotNet4.exe** from the Components folder.


Figure 1-1. RecView screen



6 Click **Install BrainVision RecView**.

The BrainVision RecView 1.4.3 Setup opens.

7 Follow the installation instructions which are now displayed until installation is completed.

Connect the supplied USB license dongle to one of the USB ports of your computer before you start RecView. Start RecView by double-clicking the RecView shortcut  , which you will find on your desktop after installation has been completed successfully.

After successful installation of RecView and the required software components



Chapter 2 Configuring the software

2.1 Installing the RecView license

Install the license for RecView on the computer on which you are running the Recorder.

The license file is on the USB data medium accompanying the BrainVision Application Suite USB (see [Figure 2-1](#)).


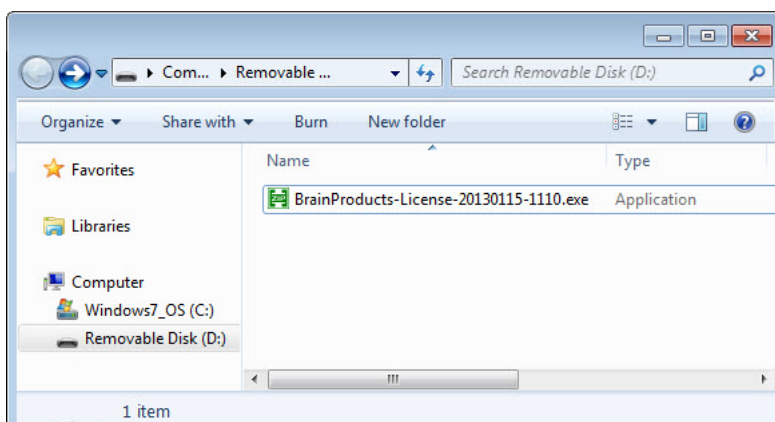
 **Alternatively, you can obtain the most recent license file from the Brain Products Web site. For detailed information, refer to [Appendix B](#) as of page 135.**

Figure 2-1. RecView license on the supplied USB data medium

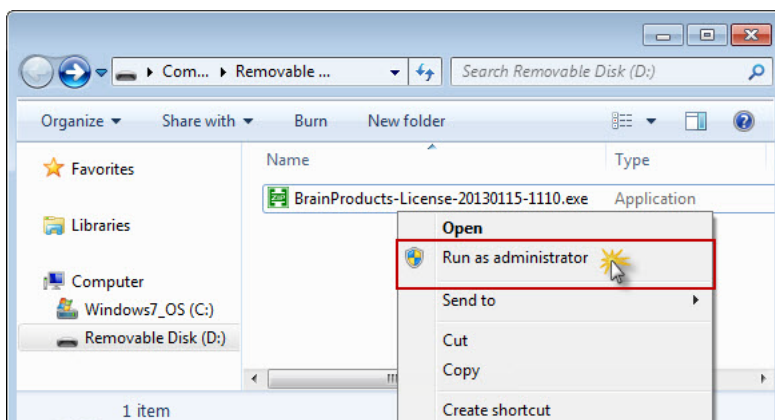


Proceed as follows:

- 1 Unpack the ZIP file *BrainProducts-License-xxxxxxx-xxxx.zip*.
- 2 Run the EXE file *BrainProducts-License-xxxxxxx-xxxx.exe* by double-clicking it. Follow the instructions from the installation program.
On Windows® 7, 8.1, 10, always run the file by right-clicking it and choosing *Run as administrator* (see [Figure 2-2](#)).



Figure 2-2. Running the license file as administrator under Windows®

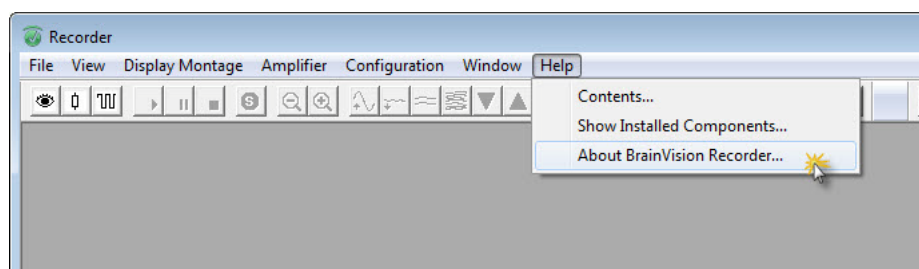


- 3 Then connect the USB license dongle supplied with the BrainVision Application Suite USB to one of the USB ports of your computer.



To check whether you have a dongle with a RecView license, start the Recorder and choose *Help > About BrainVision Recorder...* from the menu (see [Figure 2-3](#)).

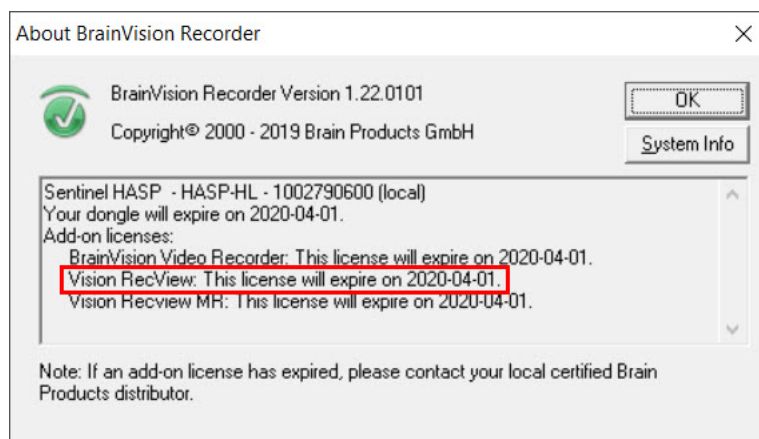
Figure 2-3. Calling Recorder program information



If you have a suitable USB license dongle, the line *Vision RecView* is shown under *Sub-licenses* (see [Figure 2-4](#)).



Figure 2-4. Displaying sub-licenses in the Recorder



2.2 Configuring the Recorder

To start RecView, activate the Remote Data Access server (RDA server) in the Recorder.

- 1 To do this, choose *Configuration > Preferences...* from the menu.
- 2 In the *Preferences* dialog box, open the *Remote Data Access* tab.
- 3 Check the *Enable Remote Data Access* box (see [Figure 2-5](#)).


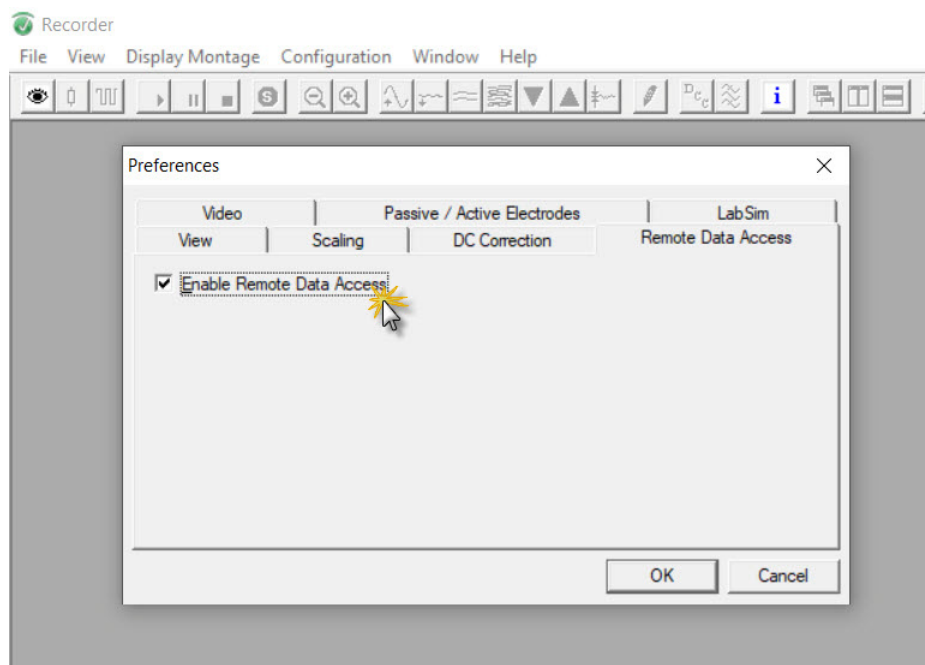
 You will find detailed information on using the Recorder in the associated User Manual.

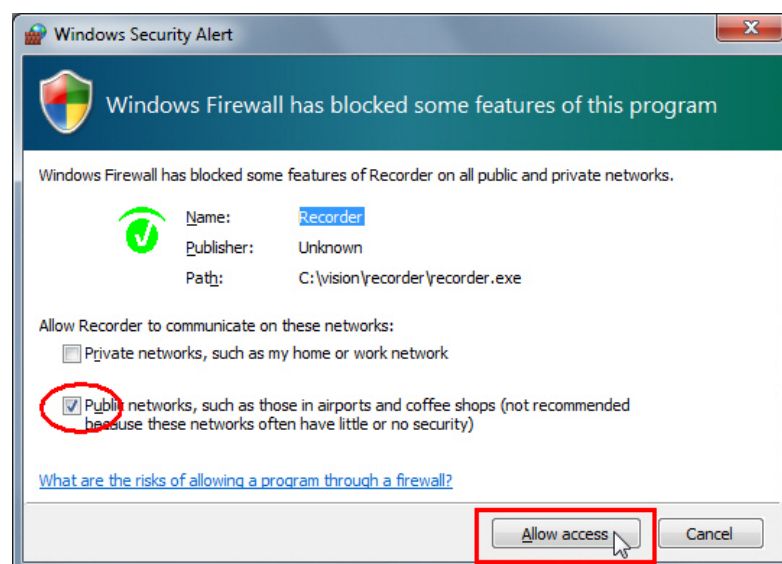
Figure 2-5. Activating the RDA server in the Recorder



While it is being displayed, the EEG data can now be passed via TCP/IP to other programs on the local computer and to computers in a network.



The RDA server of the Recorder uses the TCP/IP ports with the port numbers 51234 and 51244. If you are running a firewall on your computer, it will issue a message when you activate the RDA server. You can specify that the Recorder software should no longer be blocked (see [Figure 2-6](#)). Alternatively, some firewalls allow you to enable TCP/IP ports 51234 and 51244 explicitly. For further details, refer to the user documentation for your firewall software.

Figure 2-6. Unblocking the Recorder software



2.3 Configuring RecView

Proceed as follows to configure RecView for the data view:

- 1 Start RecView by double-clicking the RecView shortcut , which you will find on your desktop after installation has been completed successfully.
Alternatively, you can call RecView from the task bar by choosing *Start > BrainVision RecView* .
- 2 You must now specify what computer in the network the Recorder is running on. To do this, choose *Configuration > Server...* from the RecView menu (see [Figure 2-1](#)). The *Server* dialog box appears.
- 3 Here you enter either the IP address or the computer name (see [Figure 2-7](#)).


 **If the Recorder is on the local computer, enter the IP address 127.0.0.1 or the name "localhost".**

Abbildung 2-1. Calling the "Server" dialog box

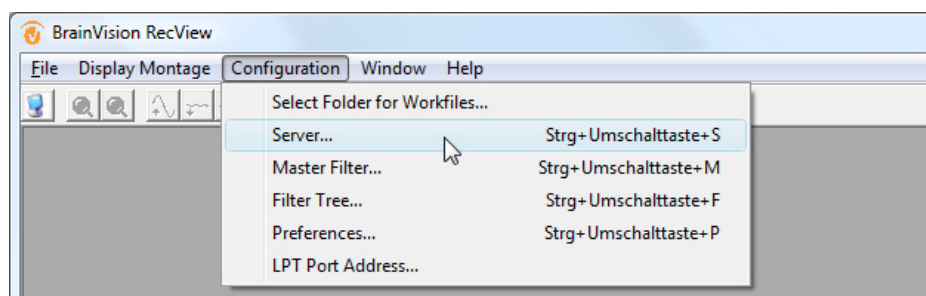
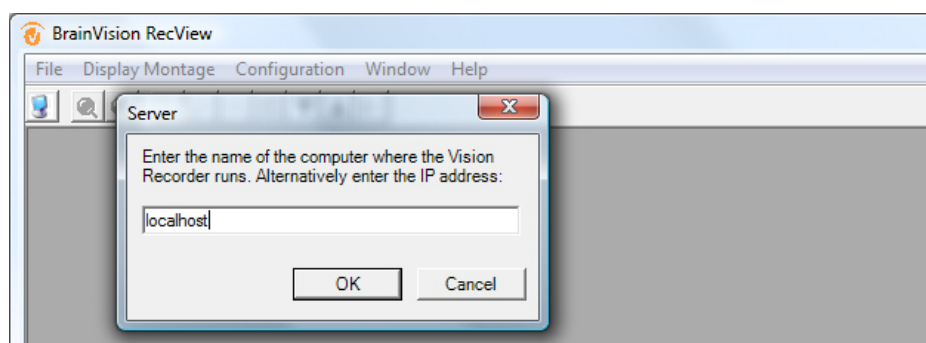


Figure 2-7. Entering the server name



If a version of the Recorder is already installed locally on the computer, RecView takes the folder specified for work files from this installation. This folder is known as the *Work Files folder*. The work files include the workspaces and montages.

Creating a new Work Files folder

To create a new Work Files folder, choose *Configuration > Select Folder for Workfiles...* and then select the required folder (see [Figure 2-8](#) and [Figure 2-9](#)).

Figure 2-8. Calling the dialog box for selecting the Work Files folder

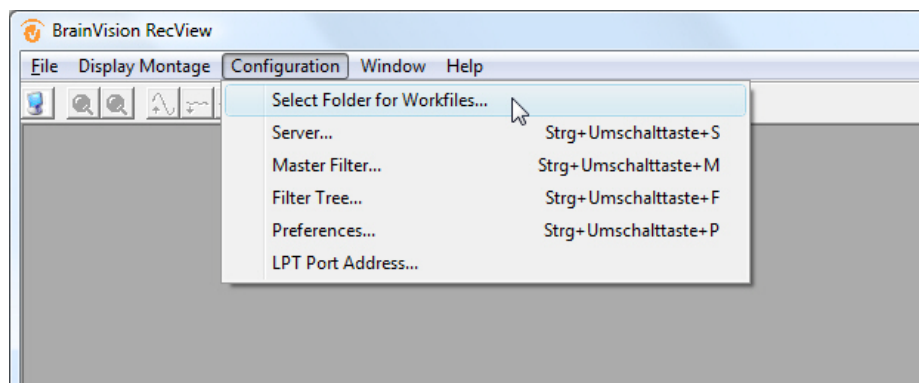
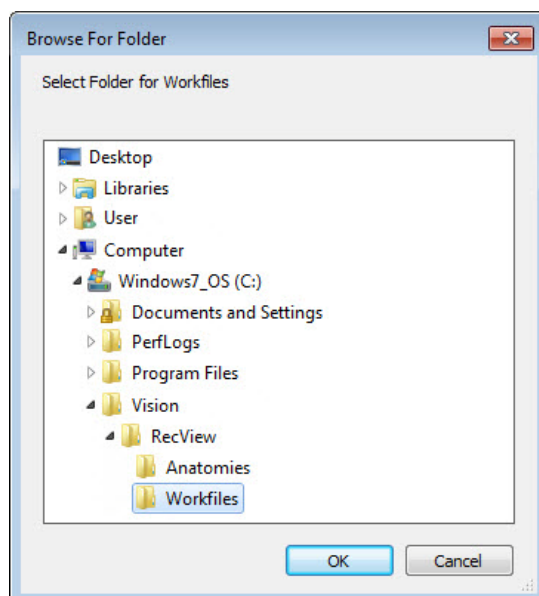


Figure 2-9. Selecting the Work Files folder

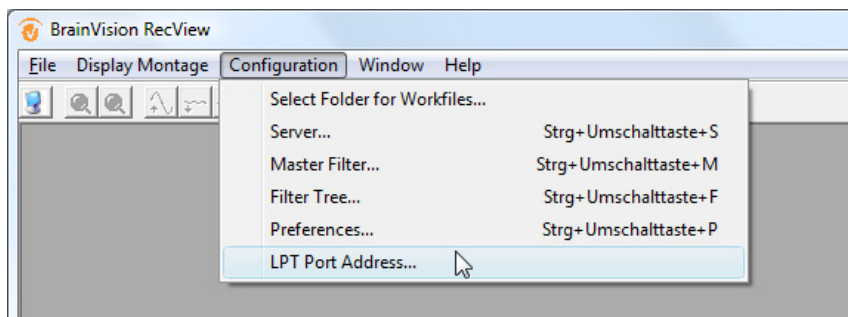


Specifying the LPT port address

If you want to use a filter with parallel port control, you must specify the LPT port address:

- 1 To do this, choose *Configuration > LPT Port Address...* from the menu (refer to [Figure 2-10](#)).
- 2 Enter the LPT port address in the text box *Hardware Address of LPT Port (hex)* (see [Figure 2-11](#)).

Figure 2-10. Calling the dialog box to enter the LPT port address




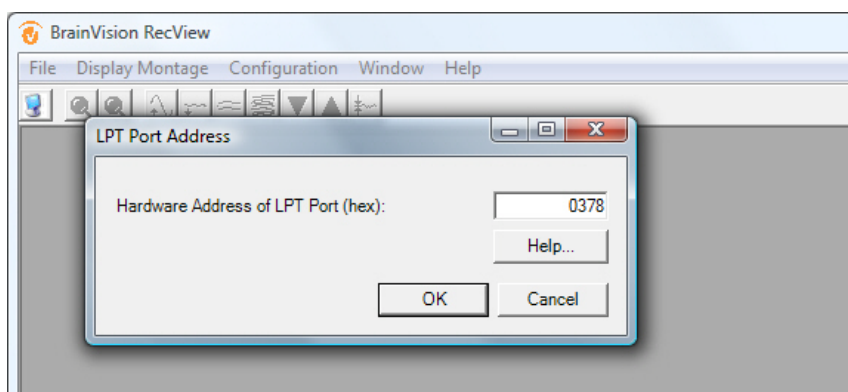
 For information on identifying the LPT port address, refer to [Appendix C on page 139](#).

Figure 2-11. Entering the address of the LPT port



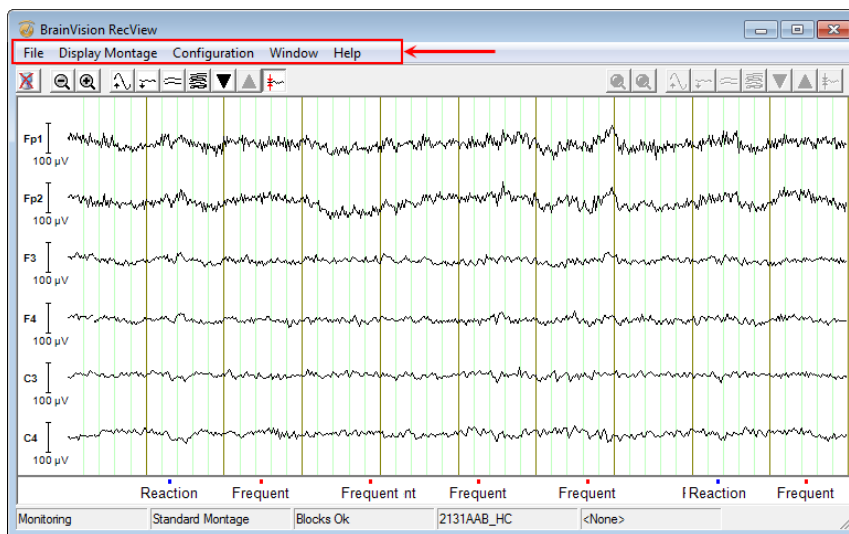


Chapter 3 Getting started and handling the program

3.1 The user interface

The menu bar and the toolbar are located at the top of the RecView window.

Figure 3-1. Menu bar and toolbar



The individual menus have the following functions:














Menu bar

Menu	Description
<i>File</i>	is used to set up, edit and save a workspace.
<i>Display Montage</i>	is used to display the montages.
<i>Configuration</i>	is used to make default settings for the locations used to archive and store the work files and the data and to configure the filters and user settings.
<i>Window</i>	is used to organize the data windows.
<i>Help</i>	is used to display program information and the installed components and to open this User Manual.





The main toolbar is located below the menu bar and allows you to make a number of different settings, including the displayed interval and the number of channels displayed simultaneously.




Toolbar

The labels for the elements in the main toolbar are displayed when you position the mouse pointer over each element. A tool tip appears after a few moments. The main toolbar contains the following elements. They refer to the main window (left-hand window):

Menu	Description
	<i>Connect to Vision Recorder</i> establishes the connection to the Recorder
	<i>Disconnect from Vision Recorder</i> interrupts the connection to the Recorder
	<i>Increase Interval</i> increases the displayed interval (alternatively, use the keyboard shortcut <i>Ctrl + Num -</i>)
	<i>Decrease Interval:</i> decreases the displayed interval (alternatively, use the keyboard shortcut <i>Ctrl + Num +</i>)
	<i>Scale Up</i> increases the scale (alternatively, use <i>Ctrl + arrow up</i>)
	<i>Scale Down</i> decreases the scale (alternatively, use <i>Ctrl + arrow down</i>)
	<i>Decrease Channels</i> decreases the number of channels displayed
	<i>Increase Channels</i> increases the number of channels displayed
	<i>Next Channel Group</i> switches to the next channel group (alternatively, use <i>Ctrl + page down</i>). This function is only available if you have previously reduced the number of channels.
	<i>Previous Channel Group</i> switches to the previous channel group (alternatively, use <i>Ctrl + page up</i>). This function is only available if you have previously reduced the number of channels.
	<i>Baseline Correction in Display</i> activates or deactivates baseline correction. Only the baseline of the display is changed, not the data itself.
	<i>Reset Averaging Templates</i> used to recalculate the correction templates for MRI artifact correction during filtering. This button is only available for MRI artifact correction and is only visible when this filter is active (see also  Section 7.1 as of page 115).

At the top right of the RecView window is another toolbar that applies to the currently active filter window (right-hand window). This contains the following buttons:

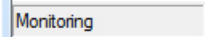
 *Scale Up*,  *Scale Down*,
 *Decrease Channels*,  *Increase Channels*,



 *Next Group*,  *Previous Group* and  *Baseline Correction in Display*.

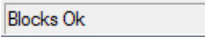
Their functions and keyboard shortcuts are the same as those of the main toolbar. However, note that you have to press the key combination *Ctrl + Shift* rather than just the *Ctrl* key to use the keyboard shortcuts.

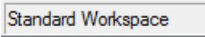

The status bar at the bottom of the RecView window is made up of the following sections:

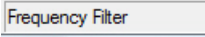

Status bar


 The first section shows the current status of the program (*Not Connected*, *Connected*, *Monitoring*, *Impedance Check*, etc.).

 The second section shows the type of montage used. For further information on montages, refer to  [Chapter 5 as of page 69](#).


 The third section (block indicator) shows whether the data blocks sent to RecView by the Recorder have been completely processed ("Blocks Ok") or whether blocks have been lost during data transfer ("Blocks Lost!"). Data may be lost during transfer if RecView is unable to accept the data in time due to high loads.

 The fourth section contains the name of the current workspace. For further information on workspaces, see  [Section 3.5 as of page 54](#).

 The fifth section shows the employed master filter. If you have not selected a master filter, the status bar displays the entry *<None>* here. For information on selecting a master filter, refer to  [Section 3.3 as of page 44](#).

 If you use a filter with parallel port control (Level Trigger, Band Power Trigger, R-Peak Trigger) then the sixth section of the status bar contains a graphic display of the status of the LPT port's eight data lines. Red stands for the status "high" and black for the status "low". Please note that TTL pulses that are reset immediately are not visible in the status bar.

To be able to use the filter with parallel port control, you must specify the address of the LPT port. To do this, choose *Configuration > LPT Port Address...* from the menu.

 For information on identifying the LPT port address, refer to [Appendix C on page 139](#).

The main window (left) shows the data sent by the Recorder. The filter window (right-hand section of the RecView window) contains the filters selected by the user (see [Figure 3-2](#)). Tabs allow you to switch between the individual filters (see [Figure 3-3](#)).


 You will find detailed information on creating a filter tree in [Section 3.4 as of page 45](#).

Figure 3-2. RecView interface

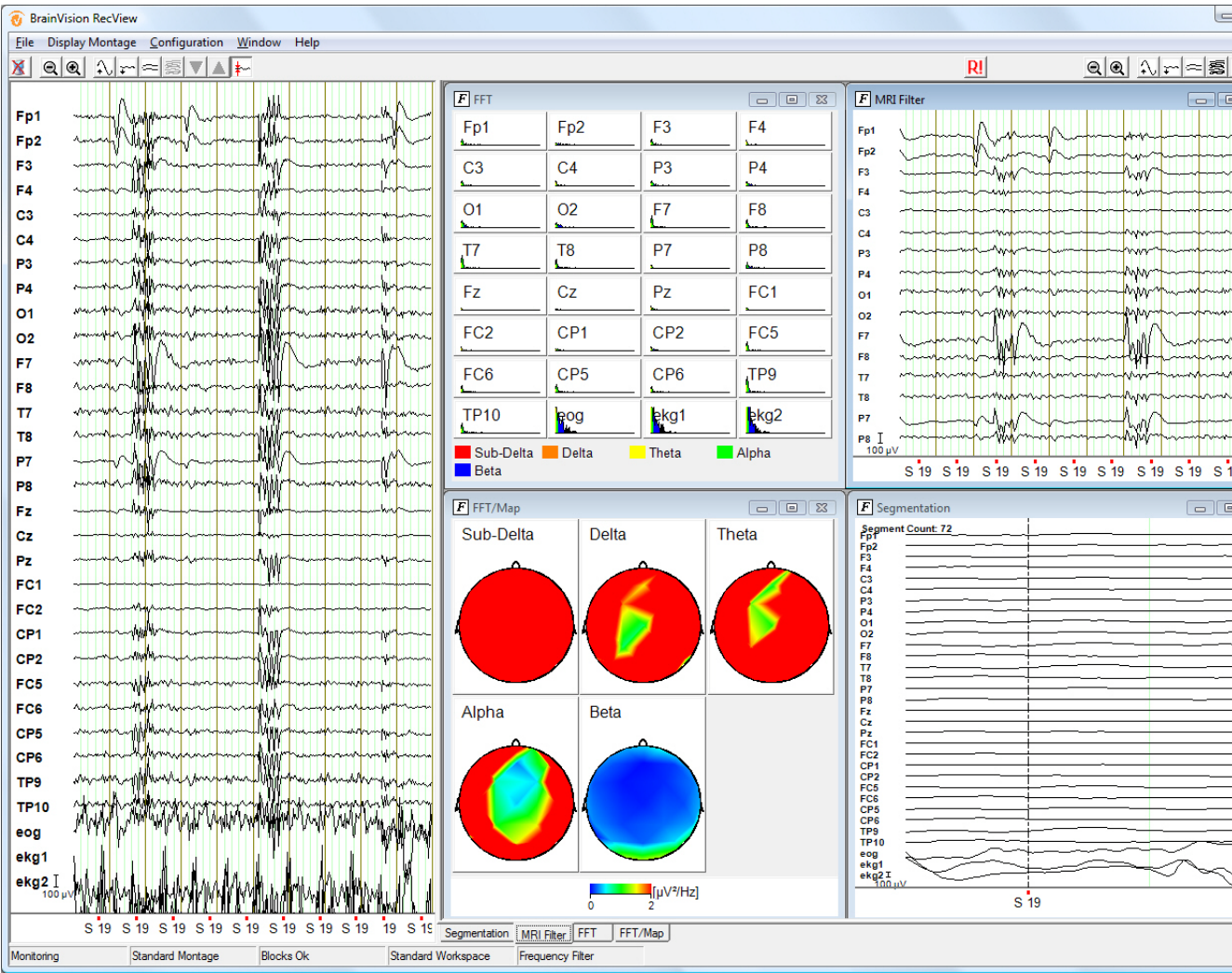
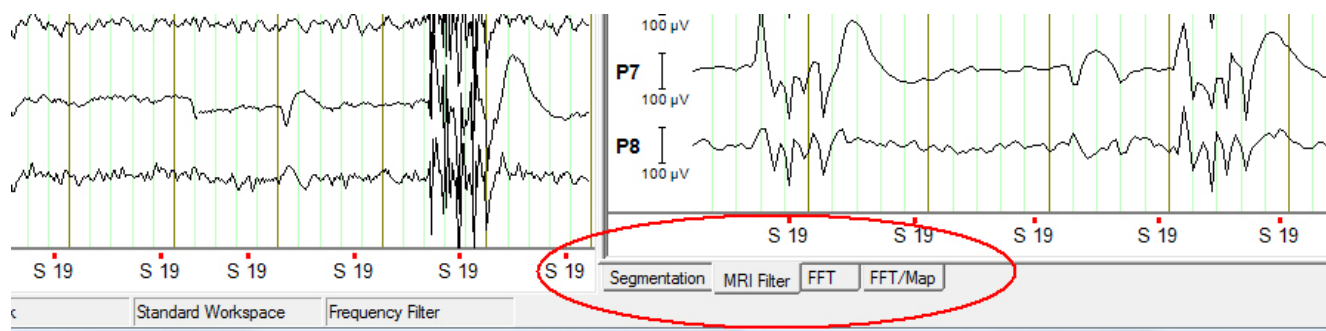


Figure 3-3. Tabs for switching between filter windows



The channel names are shown on the far left of the RecView window. At the end of the channel list, there is a scaling bar (see [Figure 3-4](#)). The scaling bar is used to assess the signal size. If a small number of channels are displayed and there is enough space, a scaling bar is shown in front of every channel (see [Figure 3-5](#)).

Figure 3-4. Scaling bar at the end of the channel list

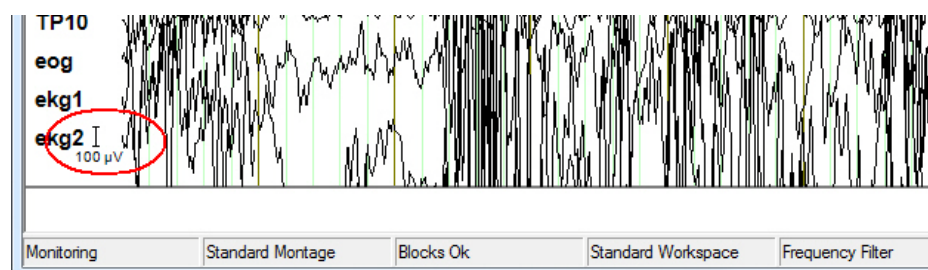
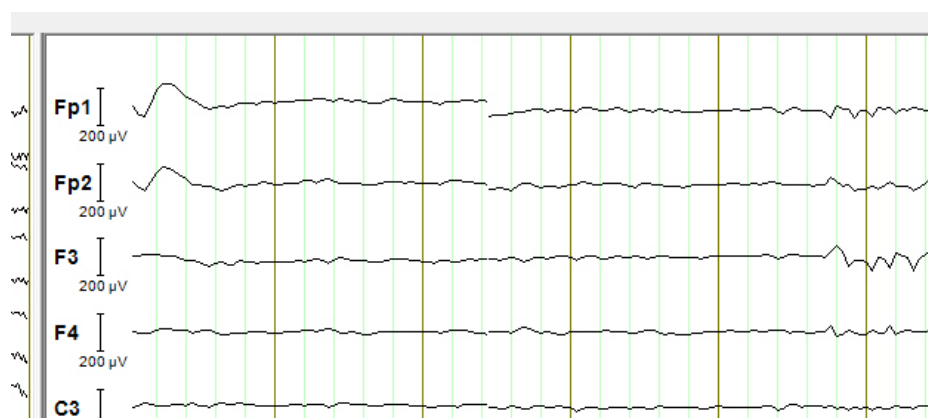


Figure 3-5. Scaling bar display in front of each channel



Beneath the channel list, separated by a gray line, the program displays any markers present in the EEG (see [Figure 3-6](#)).

Figure 3-6. Markers displayed



3.2 Performing a simple session

Proceed as follows to test the basic functionalities of RecView:



- 1 Once it has been successfully installed and configured, start the Recorder.
- 2 Start RecView.
- 3 In the RecView toolbar, click *Connect to Vision Recorder* . This establishes the connection between the Recorder and RecView. If the Recorder is not available, the message: *Waiting for Recorder...* appears in RecView.
- 4 Start the Recorder in monitoring mode by clicking the *Monitor* button  (see [Figure 3-7](#)).
- 5 RecView now also displays the data sent by the Recorder (see [Figure 3-8](#)).

Figure 3-7. Starting data viewing/recording in the Recorder

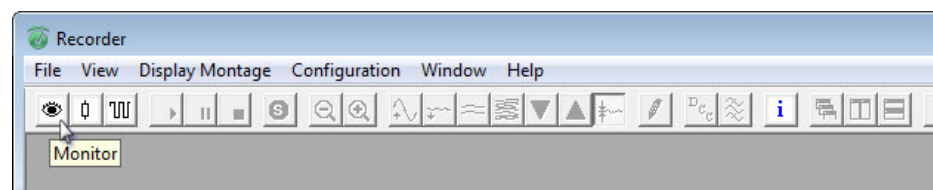
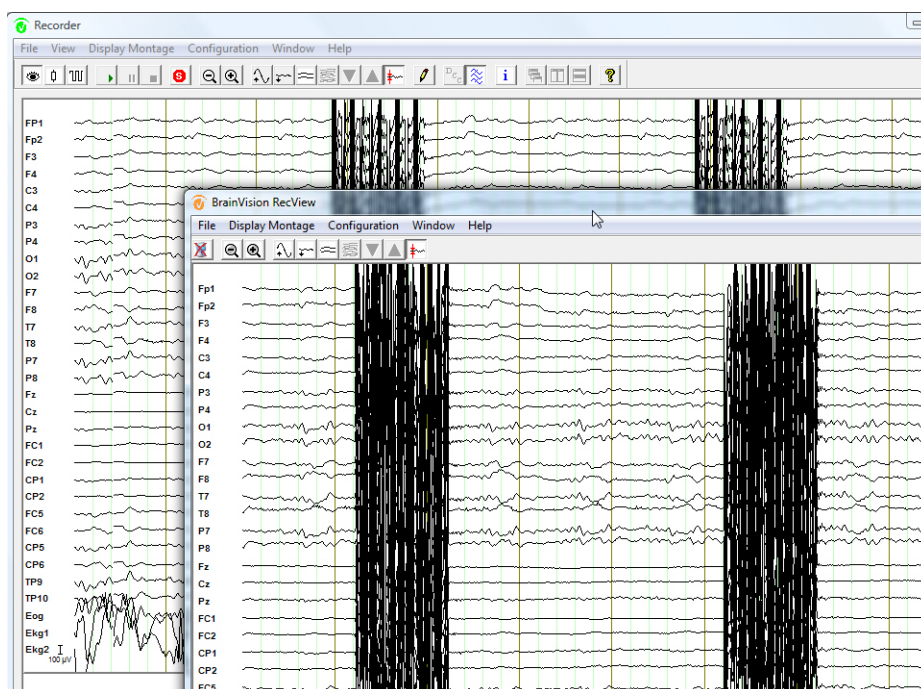


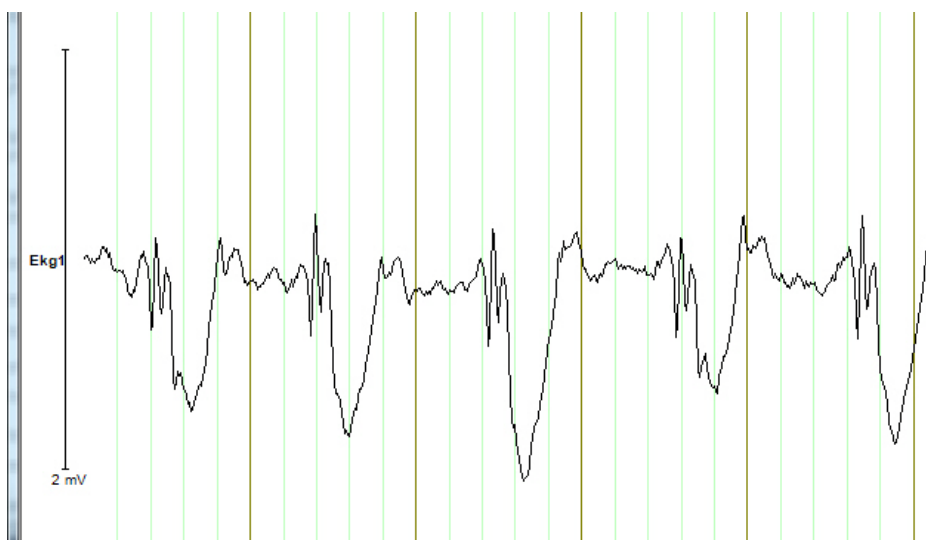
Figure 3-8. Simultaneous data view in the Recorder and RecView



You can select individual channel mode (see [Figure 3-9](#)) by double-clicking the name of the required channel. Double-clicking on this view in turn switches back to the overall view.

Individual channel mode

Figure 3-9. Individual channel mode



Activating/deactivating channels

To deactivate a channel and thus suppress the signal received, right-click the corresponding channel name. This opens a context menu. Choose *Switch Off 'channel name' Locally* to deactivate the channel in the active data window. Choose *Switch Off 'channel name' Globally* to deactivate the channel in all open data windows. To reactivate the channel, repeat the process and click the relevant menu item to remove the tick in front of the command.



It may, for instance, be sensible to deactivate channels if heavy interference on one channel hides other channels.

Figure 3-10. Global deactivation of a channel

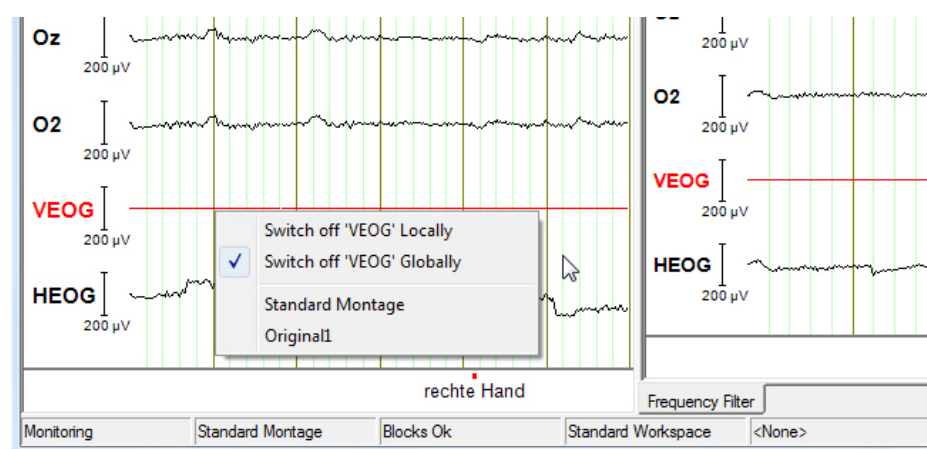
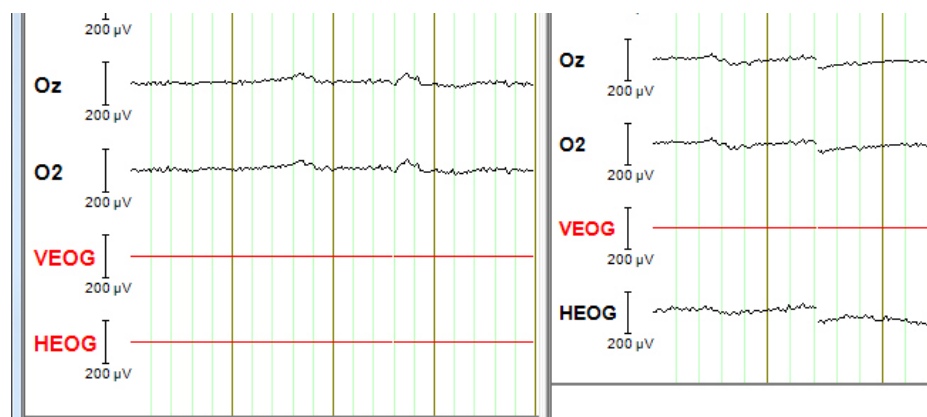


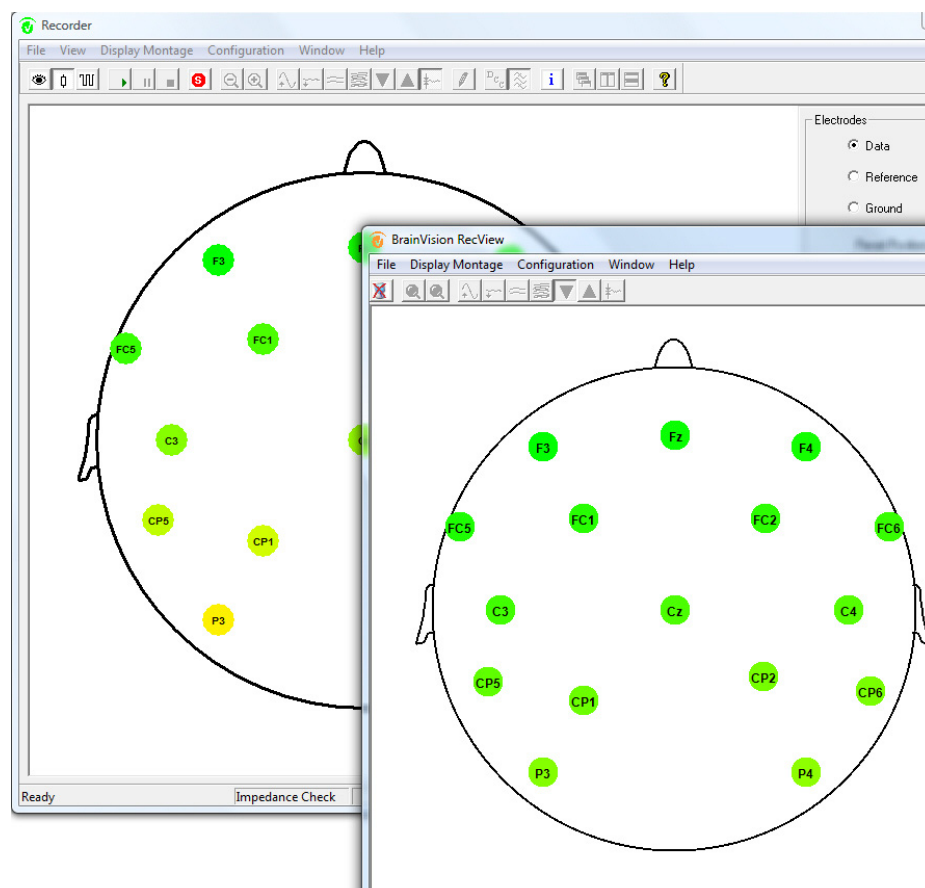
Figure 3-11. The VEOG channel has been deactivated globally and the HEOG channel locally



Impedance view


If you switch the Recorder to impedance mode, RecView also displays the impedances of the electrodes (see [Figure 3-12](#)).

Figure 3-12. Impedance mode in the Recorder and impedance view in RecView



3.3 Selecting a master filter



To make the following settings, disconnect RecView from the Recorder. To do this, click *Disconnect from Vision Recorder*  in the RecView toolbar.

If you wish, you can select a master filter. The master filter is used to filter the raw data sent by the Recorder before it is displayed in the main RecView window. The data is also pre-filtered before it is passed to all the other RecView filters.



For details on the combinations of filters that are permissible in the filter tree, refer to section 4.4 on page 47.

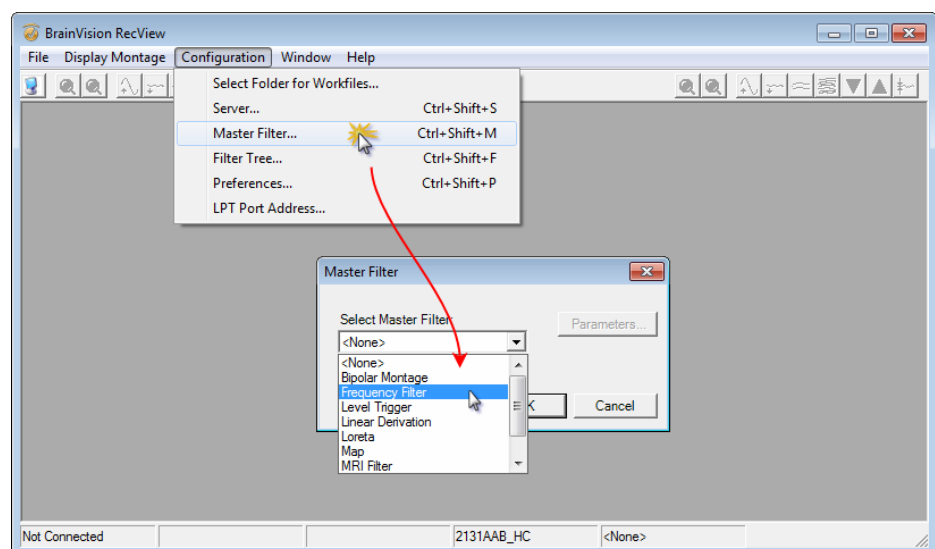
You can replace the master filter at any time, e.g. even after you have created a filter tree. It is not, however, possible to use every filter as a master filter. The Average filter, for example, requires segmented data and can therefore not be applied to raw data.



Filters that can typically be used to good effect are the MRI artifact filter and the Frequency filter.

To open the dialog box for selecting a master filter, choose *Configuration > Master Filter...* from the menu (see [Figure 3-13](#)).

Figure 3-13. Dialog box for selecting the master filter




To configure the master filter, click the *Parameters...* button. You will find detailed information on the filter-specific parameters in [Chapter 6](#) and [Chapter 7](#).

3.4 Constructing a filter tree

The filter tree permits sequential processing of the data. It also provides the possibility of branching.

It is not always necessary to use a filter tree. If, for instance, you only want to use the MRI artifact filter, you can choose it as the master filter.

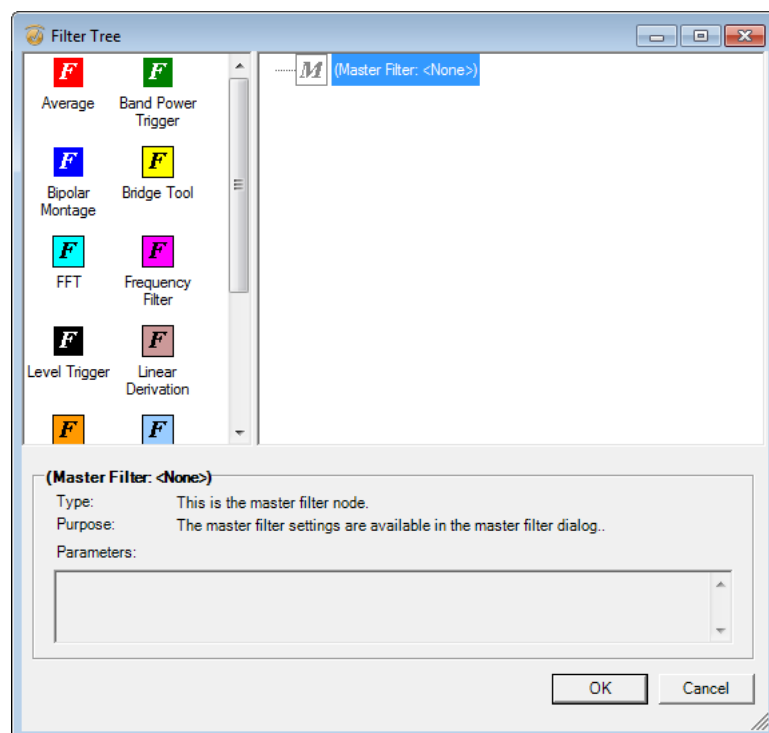
 **For information on selecting a master filter, see [Section 3.3 on page 44](#).**

To open the dialog box for creating a filter tree, choose *Configuration > Filter Tree...* from the menu. The *Filter Tree* dialog box is divided into two main windows (see [Figure 3-14](#)).

The left-hand window contains the filters installed in RecView. The filters are represented using different colored icons.

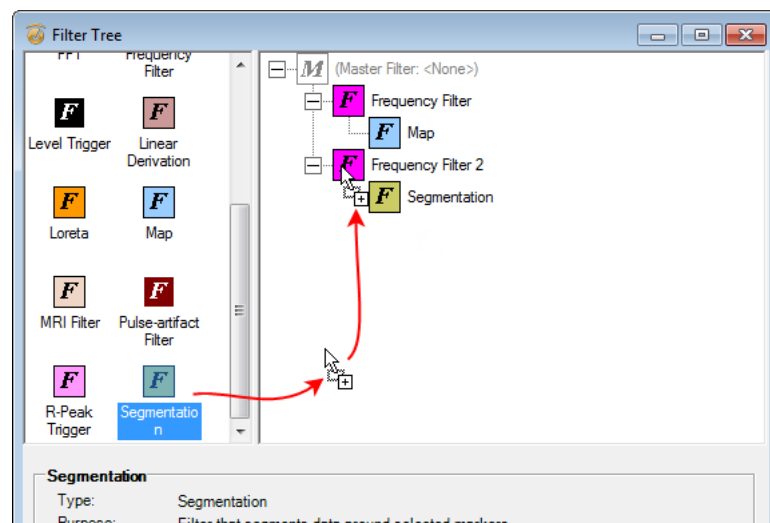
The right-hand pane contains the current filter tree starting at the root .

Figure 3-14. Empty filter tree



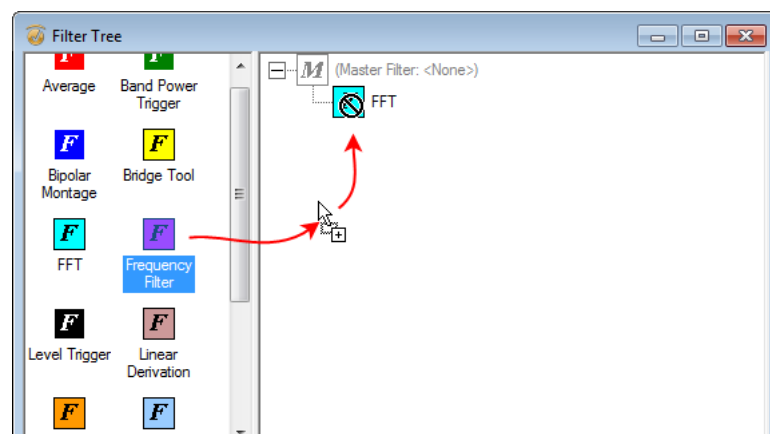
You create a filter tree by dragging filters from the left-hand window and dropping them in the right-hand window. You can also attach filters to the branches (filter icons) in the filter tree and thus add subnodes to the main filter nodes (see [Figure 3-15](#)).

Figure 3-15. Adding subnodes to main filter nodes by means of drag-and-drop



Certain filters can only handle specific input data. This means that certain combinations of filters are not possible (for more information, see [Table 3-1 on page 47](#)). If the output data type of a filter is not compatible with the input data type of the filter to be attached, it is not possible to chain these filters, thus avoiding interference. This is indicated by a prohibition icon. For example, you cannot attach a Frequency filter (input data type: time domain, real) to an FFT (output data type: frequency domain, complex) (see [Figure 3-16](#)).

Figure 3-16. Invalid filter combination: Frequency filter attached to FFT filter



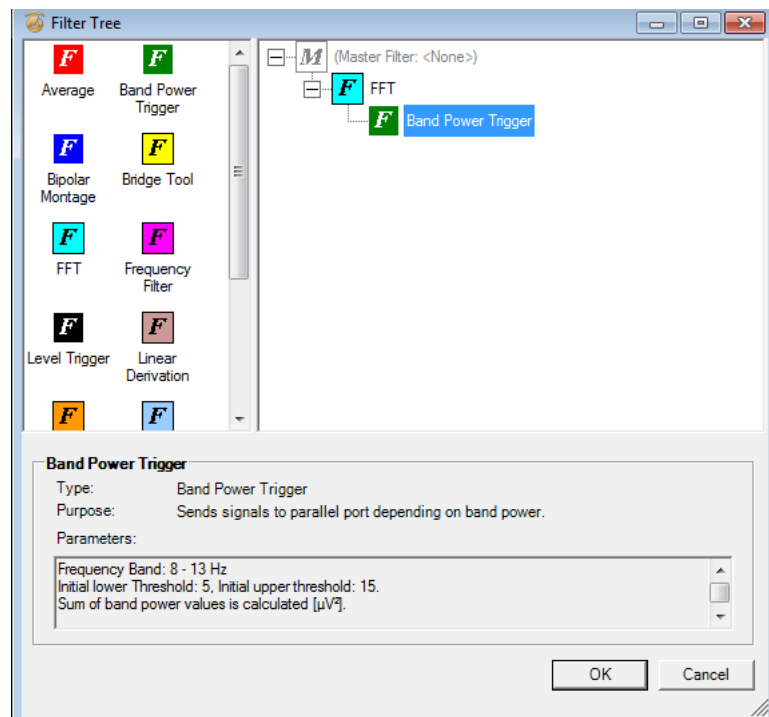
Filters can only ever be combined if their data types and segmentation types are compatible. **Combinations in the filter tree**
[Table 3-1](#) contains all the permitted filter combinations.

Table 3-1. Combinations in the filter tree

Filter	Input data type	Output data type	Input segmentation type	Output segmentation type
Average	Time domain, frequency domain, complex	Same as input data type	Segmented	Segmented
Band Power Trigger	Frequency domain, complex	–	Segmented	–
Bipolar Montage	Time domain	Time domain	Continuous, segmented	Corresponds to input segmentation type
Bridge Tool	Time domain	–	Continuous	–
FFT	Time domain	Frequency domain, complex	Continuous, segmented	Segmented
Frequency filter	Time domain	Time domain	Continuous	Continuous
Level Trigger	Time domain	Time domain	Continuous	Continuous
Linear Derivation	Time domain, frequency domain, complex	Same as input data type	Continuous, segmented	Corresponds to input segmentation type
LORETA	Time domain	Time domain	Continuous, segmented	Corresponds to input segmentation type
Map	Time domain, frequency domain, complex	Same as input data type	Continuous, segmented	Corresponds to input segmentation type
R-Peak Trigger	Time domain	Time domain	Continuous	Continuous
Segmentation	Time domain	Time domain	Continuous	Segmented
MRI Filter	Time domain	Time domain	Continuous	Continuous
Pulse-artifact Filter	Time domain	Time domain	Continuous	Continuous

The *Filter Tree* dialog box contains details on the currently selected filter below the two main windows. These details include the filter name, the filter type, a brief description of the filter and the filter-specific parameters that have been set (see [Figure 3-17](#)).

Figure 3-17. Details on the currently selected filter

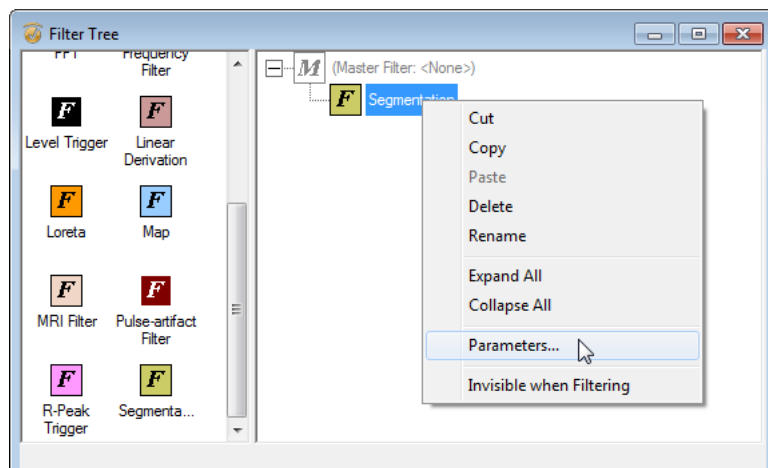


You will find detailed information on the filter-specific parameters in [Chapter 6](#) and [Chapter 7](#).

To change the parameters of a filter, right click the icon for this filter in the filter tree. This opens a context menu. Choose *Parameters...* from the menu (see [Figure 3-18](#)).

Alternatively, you can open the Parameters dialog box when you drag and drop a filter icon to the filter tree and/or when you double-click the corresponding filter node in the tree. You will find information on configuring these options in the description of the user settings (see also [Section 4.6 on page 68](#)).

Figure 3-18. Context menu for filters



Context menu for filters

The context menu contains the following functions in addition to *Parameters...*:

- ▶ You can use *Cut* to cut a filter from the filter tree.
- ▶ You can use *Copy* to copy a filter node.
- ▶ You can use *Paste* to insert the filter at the required position in the filter tree.
- ▶ *Delete* deletes a filter node (alternatively, you can select the filter you wish to delete and press).
- ▶ *Rename* renames a filter node (alternatively, you can select the filter you wish to rename and press <F2>).
- ▶ Use *Expand All* and *Collapse All* to expand and collapse all the filter nodes.
- ▶ Choose *Invisible when Filtering* if you want to use a filter in the filter tree, but do not wish to display the data. The names of invisible filters are shown in blue in the filter tree (see [Figure 3-19](#)).


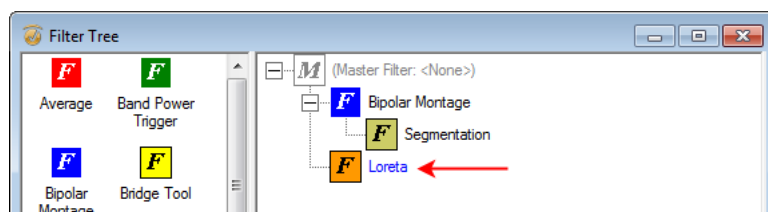
 **The function *Invisible when Filtering* can, for example, be of use if you want to use intermediate filters.**

Figure 3-19. Invisible LORETA filter



You must possess administrator privileges in order to use filters with LPT port control (Band Power Trigger, Level Trigger and R-Peak Trigger).

Using LPT port control

Under Windows® 7, 8.1 and 10, you must start RecView in Administrator mode even if you are already logged in as administrator at the computer. To run RecView as administrator, navigate to the RecView program folder, right-click the application *RecView.exe* and choose *Run as administrator* (see [Figure 3-20](#)).


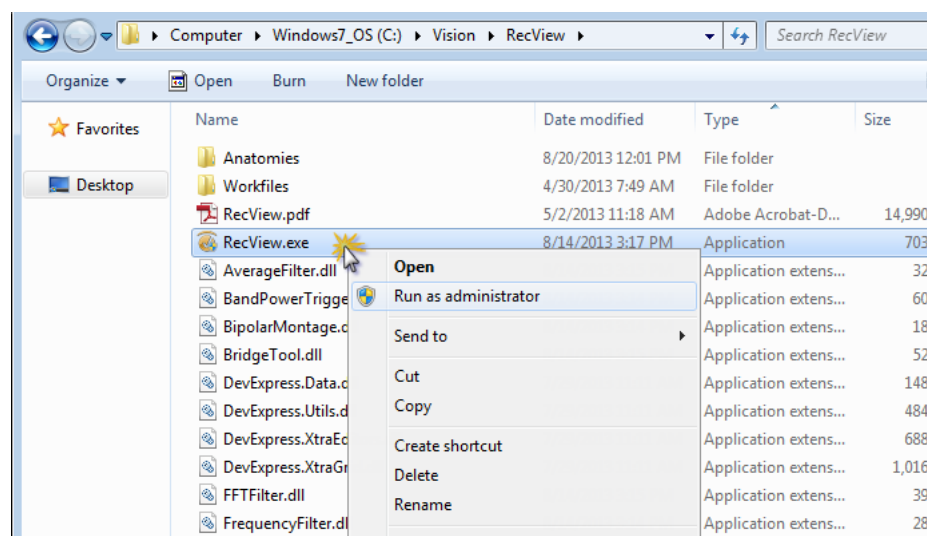
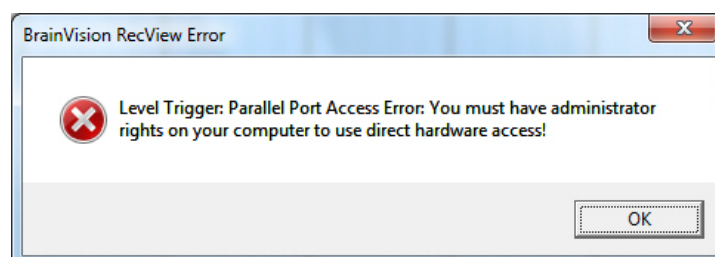
 **For information on other ways of running the program as administrator, refer to the Windows® user documentation.**



Figure 3-20. Right-clicking to run RecView as administrator



Otherwise, an error message is output and RecView terminates monitoring mode (see [Figure 3-21](#)). All the other filters in the filter tree may nevertheless continue to run in the background after you have closed this error message.

Figure 3-21. Example error message from the Level Trigger filter if the LPT port address is not specified

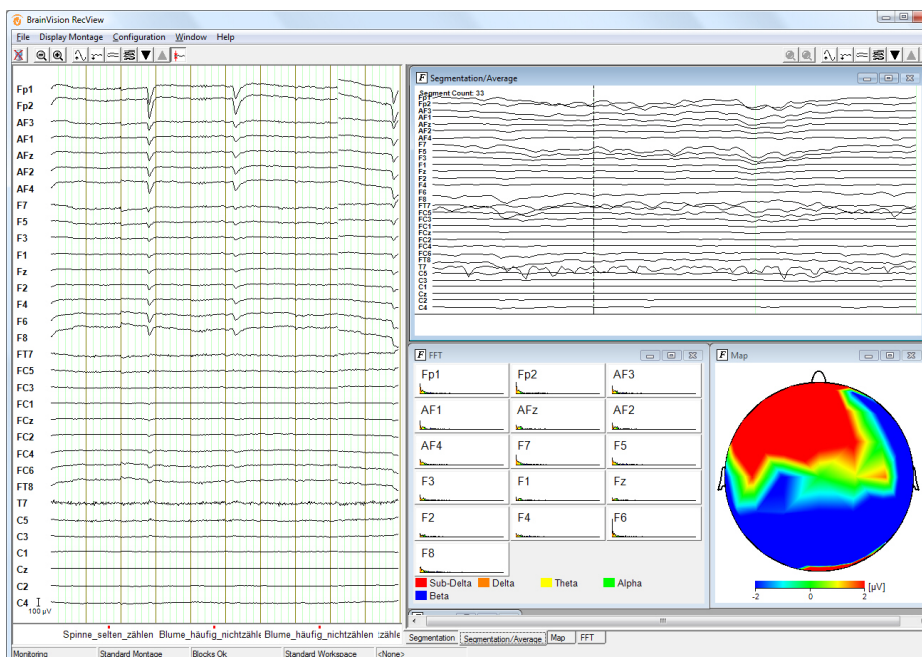


When you have completed the editing steps described here, click *Connect to Vision Recorder*  to establish a connection between RecView and the Recorder. Start the data view in the Recorder by clicking *Monitor* .

The RecView interface is now divided into two parts (see [Figure 3-22](#)): The main window (on the left) shows the data sent by the Recorder. A master filter may have been applied to this

data. Depending on the number of filter nodes created, the right-hand side of the interface contains one or more filter windows. This means that each visible filter node in the filter tree has its own data window.

Figure 3-22. Data representation with a filter tree



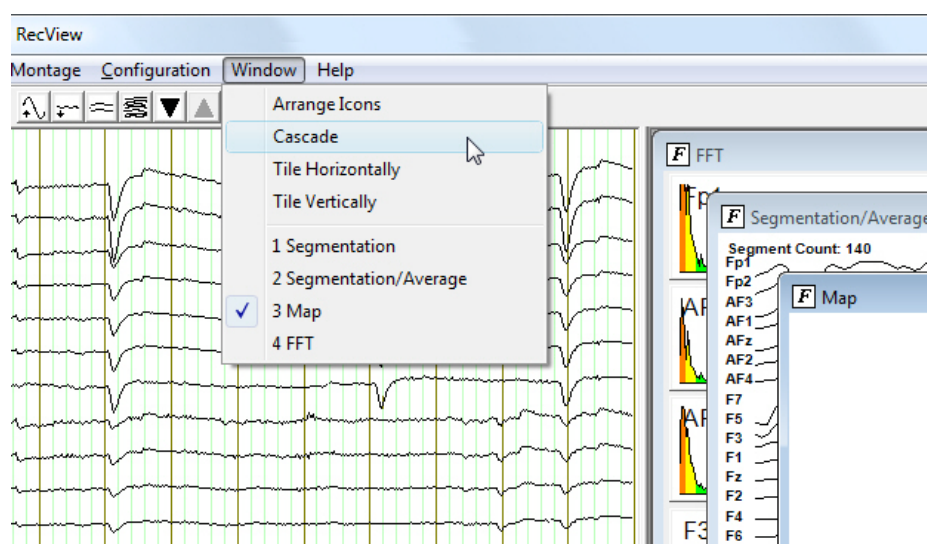
You can change the ratio between the main window (on the left) and the other filter windows by dragging the split bar between the windows to the left or right with the mouse.


The tabs below the filter windows allow you to switch between the individual filter windows (see [Figure 3-3 on page 39](#)).

You can change the arrangement of the filter windows using the *Window* menu (see [Figure 3-23](#)):

- ▶ *Cascade* cascades all the open filter windows one after another.
- ▶ *Tile Horizontally* arranges the windows one above the other.
- ▶ *Tile Vertically* arranges the windows next to each other.

Figure 3-23. Functions for arranging the filter windows

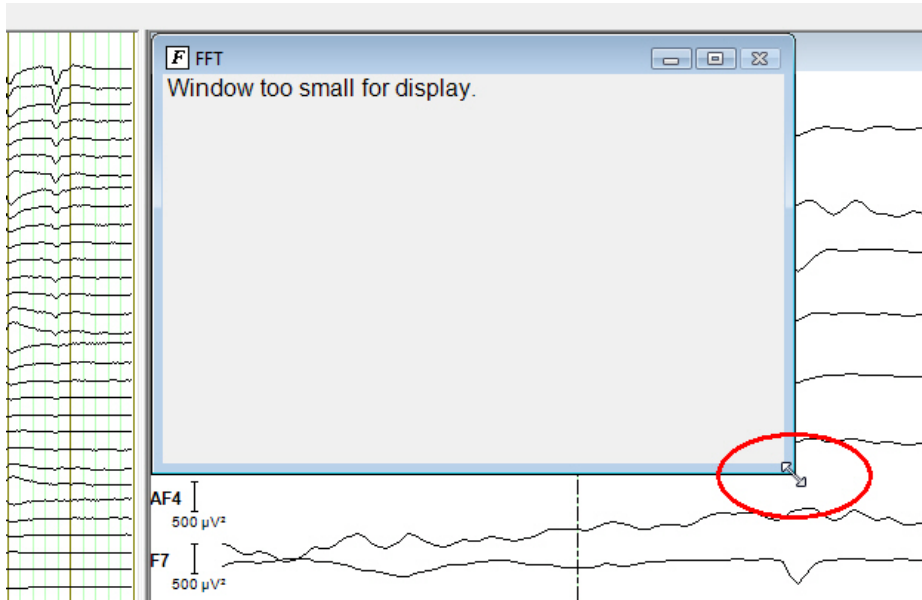


 **You will find a detailed description of the RecView user interface in [Section 3.1 as of page 35](#).**

At the top right of the RecView interface is a toolbar that applies to the currently active filter window. The functions and keyboard shortcuts corresponding to these buttons are the same as those of the main toolbar. However, note that you have to press the key combination *<Ctrl-Shift>* rather than just the *<Ctrl>* key to use the keyboard shortcuts.

If the error message *Window too small for display* appears, enlarge the relevant filter window with the mouse until the data is displayed correctly (see [Figure 3-24](#)).

Figure 3-24. Enlarging the data window to show the data correctly



3.5 The workspace concept

The filter tree you create is saved in a workspace. When RecView is first installed, a new workspace is automatically created with the name "Standard Workspace". Any changes you make to the filter tree are always saved in the current workspace.

If you want to define different filter trees, you must set up new workspaces:

- 1 To do this, choose *File > New Workspace* from the menu (see [Figure 3-25](#)).
- 2 The *Save As* dialog box appears.
- 3 Enter a meaningful name for the workspace in the *File name* text box.
- 4 Click *Save* when you have completed your entries (see [Figure 3-26](#)).

Figure 3-25. Creating a new workspace

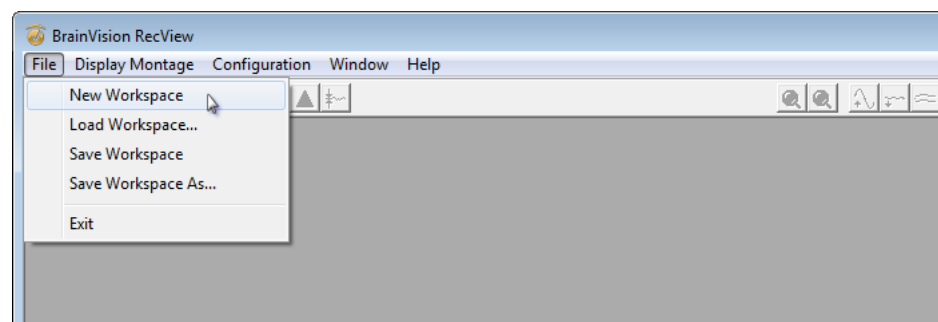
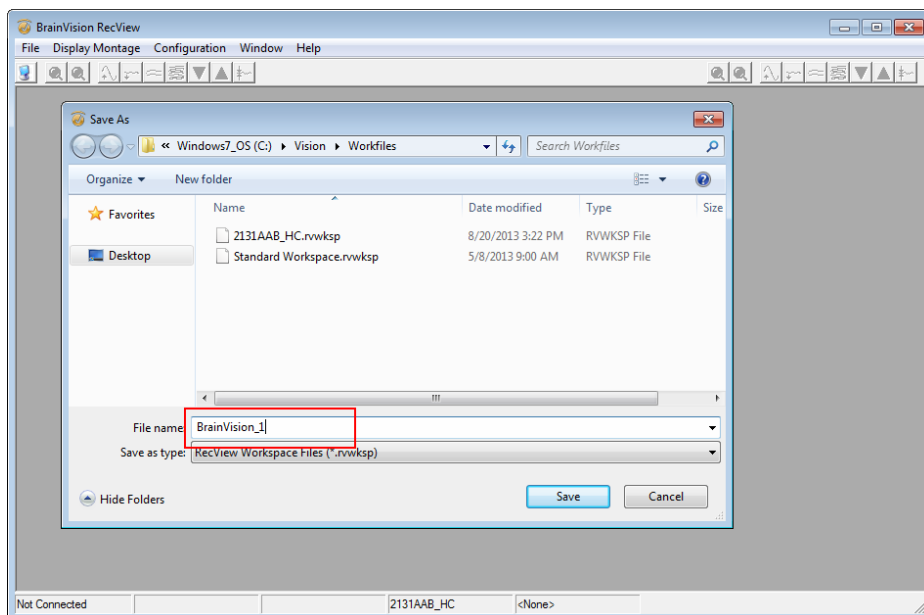
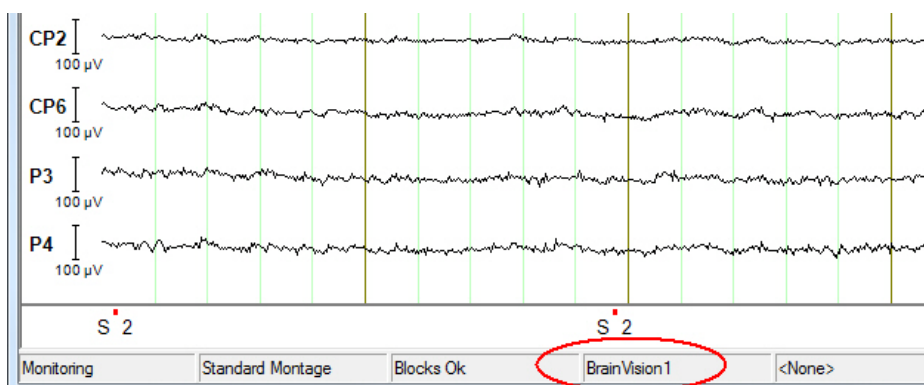



Figure 3-26. Saving the new workspace



- 5 The newly created workspace is now the current workspace (see Figure 3-27). It has taken over the settings of the previous workspace.

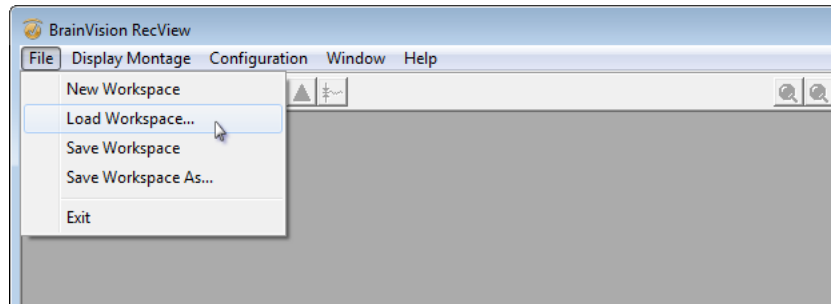
Figure 3-27. Newly created "BrainVision1" workspace



When you exit RecView a prompt will ask, if you want to save or discard the changes in the filter tree. 

You load an existing workspace by choosing *File > Load Workspace...* from the menu (see Figure 3-28).

Figure 3-28. Loading an existing workspace



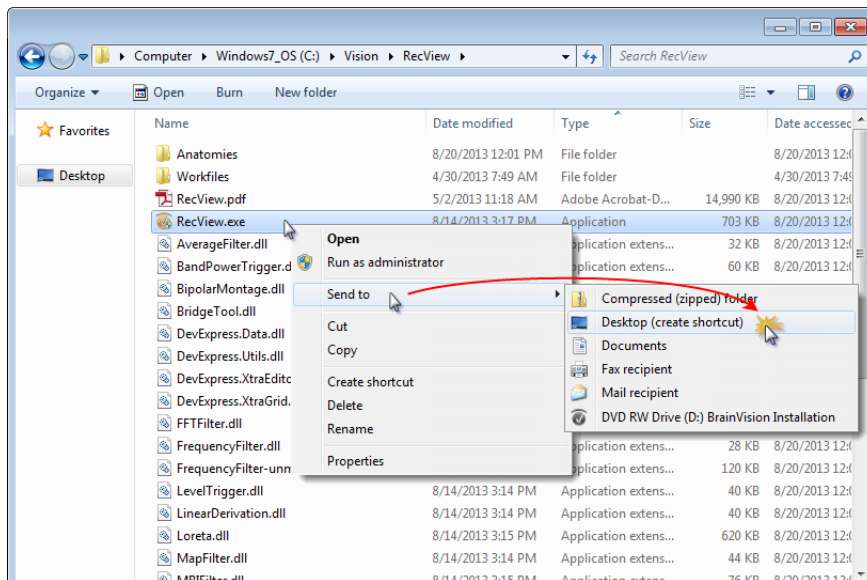
3.6 Command line parameters

A very convenient method for users who manage several workspaces at a time, is to load the desired workspace via a shortcut-icon. With this quick access functionality you can open RecView with the correct workspace and other parameters loaded. For each workspace you can create a separate shortcut.

To use this function do the following:

- ▶ Open the RecView directory.
- ▶ Right-click on file *RecView.exe* and select *Send to > Desktop (create shortcut)* ([Figure 3-29](#)).

Figure 3-29. Create shortcut on the Windows-Desktop

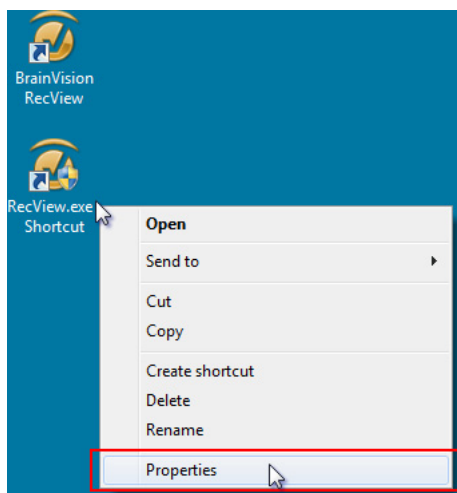


- The new shortcut-icon usually has the name *RecView.exe - Shortcut*.

You can rename this shortcut.

- Right-click on the shortcut and choose *Properties* (Figure 3-30).

Figure 3-30. Open the shortcut properties

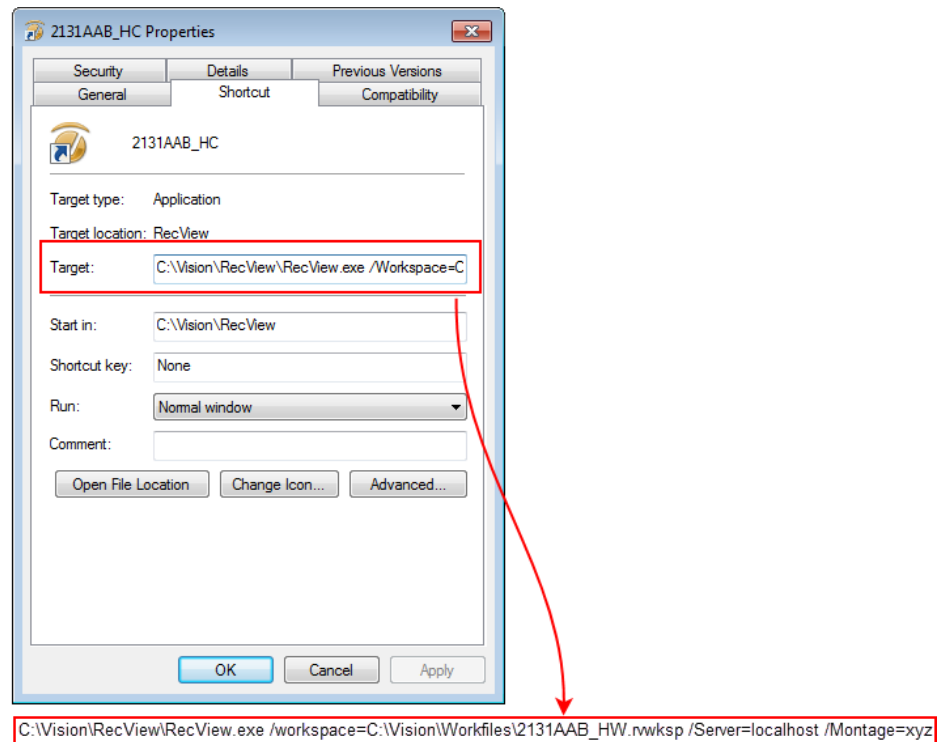


- Click on the tab *Shortcut*.

In the field *Target* you can add one or a combination of the following commands (see also [Figure 3-31](#)):

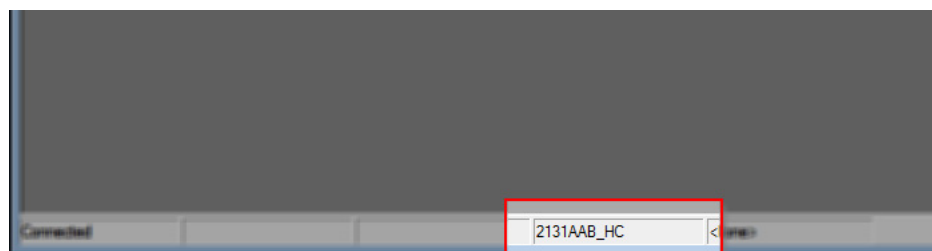
Command	Description and example
/Workspace=...	<p>Specifies the path to the workspace, e.g. /Workspace=C:\Vision\Workfiles\2131AAB_HC.rvwksp</p> <p>If the path contains spaces, then use quotation marks: /Workspace="C:\Vision\Workfiles\2131 AAB HC.rvwksp"</p>
/Server=...	<p>Specifies the IP-address or PC-name where BrainVision Recorder is running, e.g. /Server=localhost</p>
/Montage=...	<p>Specifies the Montage name, e.g. /Montage=xyz</p> <p>If the Montage name contains spaces, then use quotation marks: /Montage="x y z"</p> <p>The related file must be located within the <i>Workfiles</i> folder (see page 32). Only specify the file name WITHOUT its extension (*.MONT2).</p>

Example *Figure 3-31.* Editing the command line



Verify Workspace If you click on the shortcut, RecView starts and immediately opens the linked workspace (in the example: 2131AAB_HC.rwksp). In the status-bar of RecView you can verify, if the correct workspace has been loaded ([Figure 3-32](#)).

Figure 3-32. Verify correct workspace



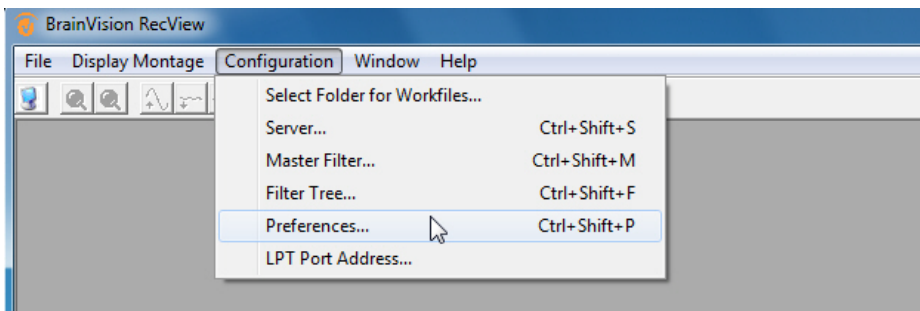
Windows creates the RecView shortcut on the Desktop, but you can move it to any other directory on your PC, network or external data storage. If you move it to a network location or external data storage, please make sure to open the shortcut from the PC on which the workspace is actually located.



Chapter 4 Configuring the user settings

To open the dialog box for configuring user settings, choose *Configuration > Preferences...* from the menu (see [Figure 4-1](#)). The dialog box is made up of six tabs whose functions are described below. Most of the configuration options relate to the way in which the data is represented.

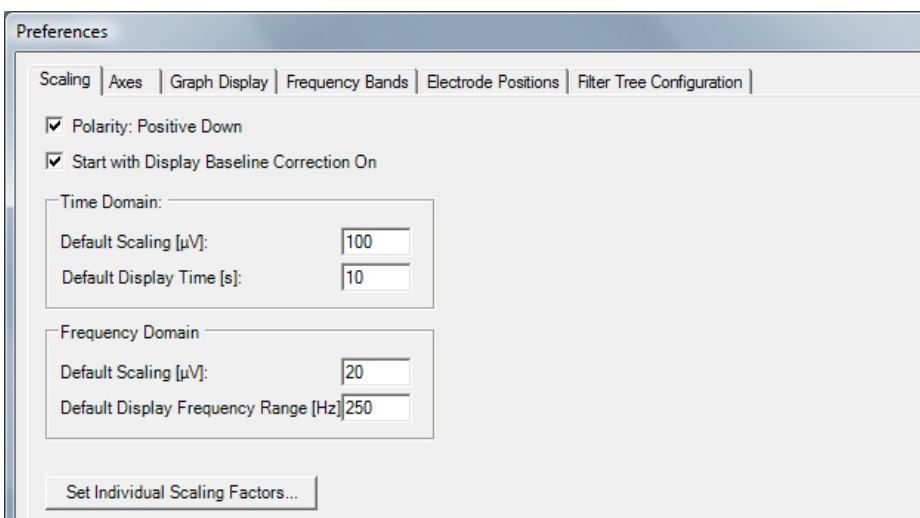
Figure 4-1. Calling the "Preferences" dialog box



4.1 Configuring the scaling

The *Scaling* tab is used to configure the scaling parameters.

Figure 4-2. Configuring the scaling parameters



You can make the following settings:

- ▶ The *Polarity: Positive Down* function defines the polarity of the displayed signal. If you select the check box, the axis for positive measured values points down.
- ▶ If you select the *Start with Display Baseline Correction On* check box, the baseline correction function in the data view is activated by default.
- ▶ *Default Scaling [μV]* specifies the default scaling used when data is first displayed. You can enter the values for data from the time domain and the frequency domain independently of each other.
- ▶ *Default Display Time [s]* specifies the interval represented in the time domain in seconds.
- ▶ *Default Display Frequency Range [Hz]* specifies the interval represented in the frequency domain in hertz. The frequency domain always starts at 0 Hertz.
- ▶ The *Set Individual Scaling Factors* function allows you to specify the channels that are to be displayed attenuated. In the table, enter the channel names and the associated scaling factors by which you want to reduce the scale of the signals (see [Figure 4-3](#)).


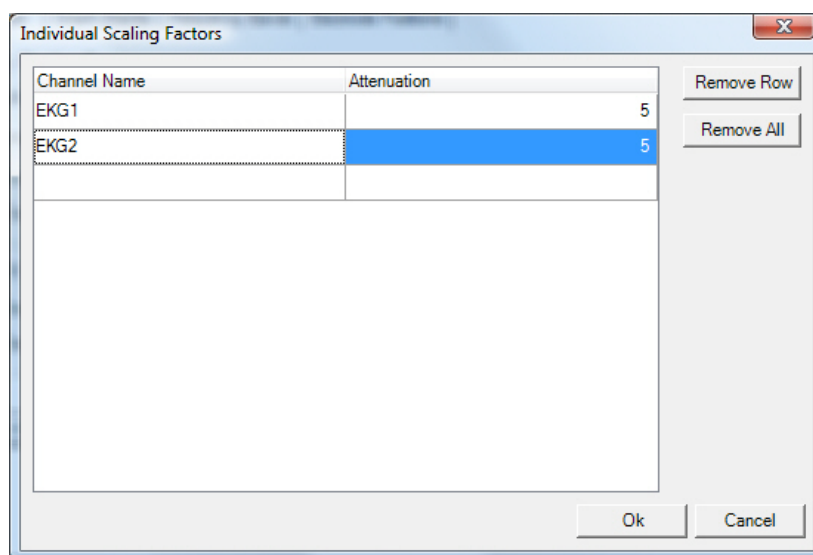
 **Individual scaling is desirable for ECG channels, for example, since otherwise they encroach badly on the curves of the EEG channels. The attenuation only affects the display of the data; it does not affect the data itself.**

Figure 4-3. Scaling selected channels

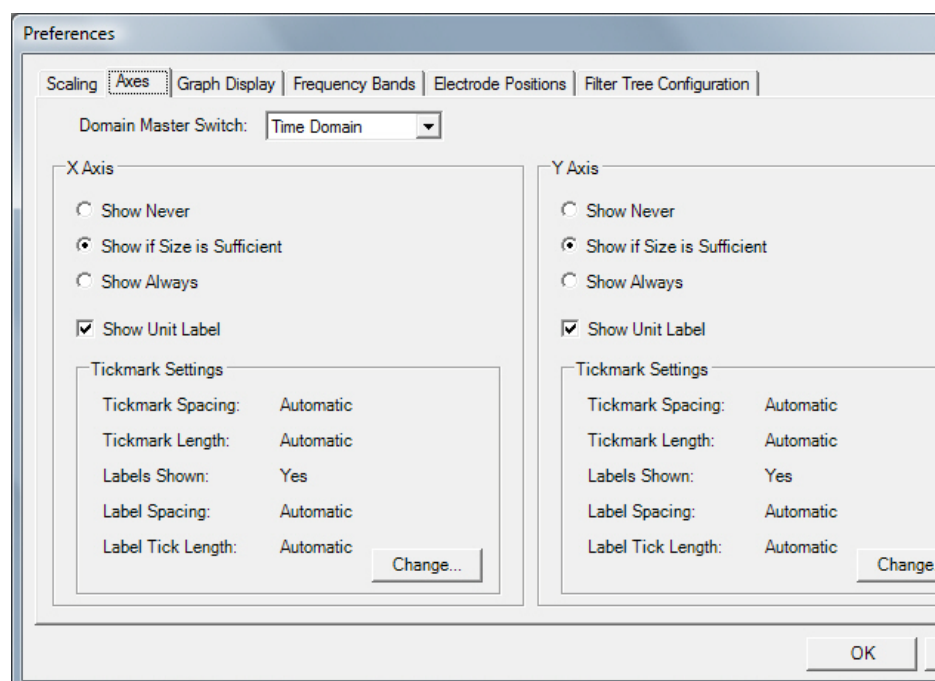


Channel Name	Attenuation
EKG1	5
EKG2	5

4.2 Configuring the axes

The Axes tab allows you to configure the x- and y-axes.

Figure 4-4. Configuring the axis parameters

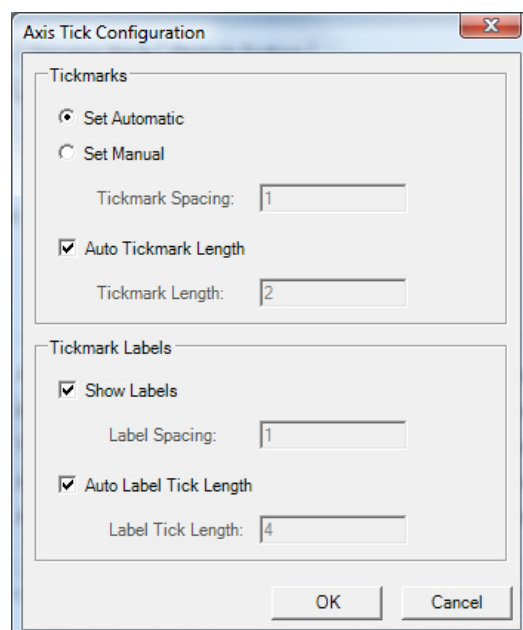


The *Domain Master Switch* drop-down list allows you to specify whether the settings refer to the *Time Domain* or to the *Frequency Domain*.

You can make the following settings separately for the x- and y-axes:

- ▶ The *Show Never* / *Show, if Size is Sufficient* / *Show Always* options allow you to specify whether the axis is not to be displayed, only to be displayed if there is enough space or always displayed.
- ▶ If you check the *Show Unit Label* box, the units (μV , s, Hz, etc.) of the axes are displayed.
- ▶ The *Tickmark Settings* group describes the intervals for the subdivisions of the axis. To change the settings for the arrangement, interval and labeling, click *Change....* The *Axis Tick Configuration* dialog box opens (see [Figure 4-5](#)).

Figure 4-5. Configuring the subdivisions of the axis (tickmarks)



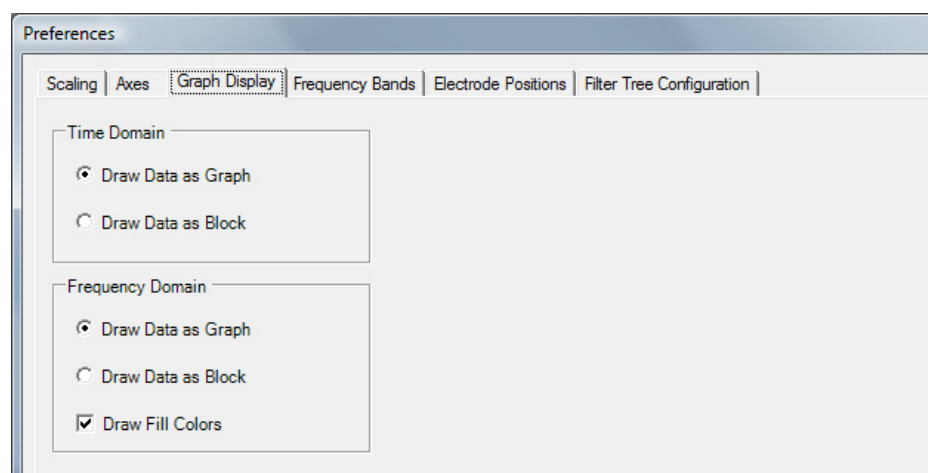
You can make the following settings in the *Axis Tick Configuration* dialog box:

- ▶ You can either have the intervals calculated automatically (*Set Automatic* option) or set them manually (*Set Manual* option).
- ▶ Enter the axis subdivision interval in the *Tickmark Spacing* text box and the length of the tickmark in the *Tickmark Length* text box.
- ▶ If you check the *Auto Tickmark Length* box, the length of the tickmark is determined automatically.
- ▶ The *Show Labels* check box is used to specify whether the subdivisions of the axis are labeled and if so at what intervals (*Label Spacing* text box). This specification determines the number of tickmarks after which a label is displayed.
- ▶ The *Label Tick Length* text box is used to specify the length of the labeled tickmarks. If you check the *Auto Label Tick Length* box, this length is determined automatically.

4.3 Graph display

The *Graph Display* tab is used to configure how graphs are displayed.

Figure 4-6. Configuring how graphs are displayed



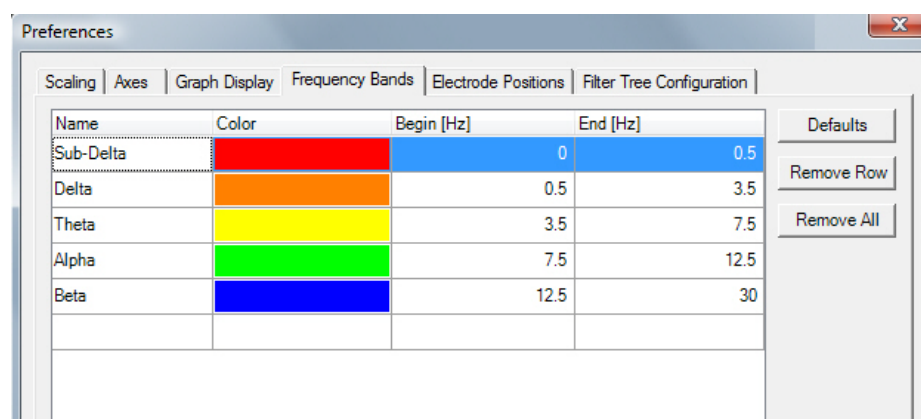
You can make the following settings:

- ▶ The *Draw Data as Graph* and *Draw Data as Block* options allow you to specify whether the individual data points are to be drawn as a graph or as discrete blocks. You can make this setting separately for the time domain and the frequency domain.
- ▶ For the frequency domain only, the *Draw Fill Colors* option allows you to specify whether the area under the graph is filled with colors. If you choose to do so, the frequency bands set on the *Bands* tab are highlighted in color (see [Section 4.4 as of page 66](#)).

4.4 Representation of the frequency bands

The *Frequency Bands* tab allows you to define frequency bands and assign colors to them. This is used when representing frequency data (e.g. FFT).

Figure 4-7. Defining frequency bands



You can make the following settings:

- ▶ In the table, you can specify the color of a band, its name and where it starts and ends (in which columns from left to right) in hertz. You change the color for the band by clicking on a color swatch in the *Color* column. This opens the color selection dialog box.
- ▶ To extend the table, click in an empty row and fill in a cell. A new row is then automatically added to the table.
- ▶ The *Remove Row* and *Remove All* buttons allow you to delete the selected row or all rows respectively.
- ▶ The *Defaults* button allows you to reset all the values modified in the table to their initial configuration.

4.5 Adjusting the electrode positions

RecView uses the 10/10 coordinate system for calculations which depend on the electrode positions (such as the map). If the names or positions you use differ from this system, you can specify them in the *Electrode Positions* tab.


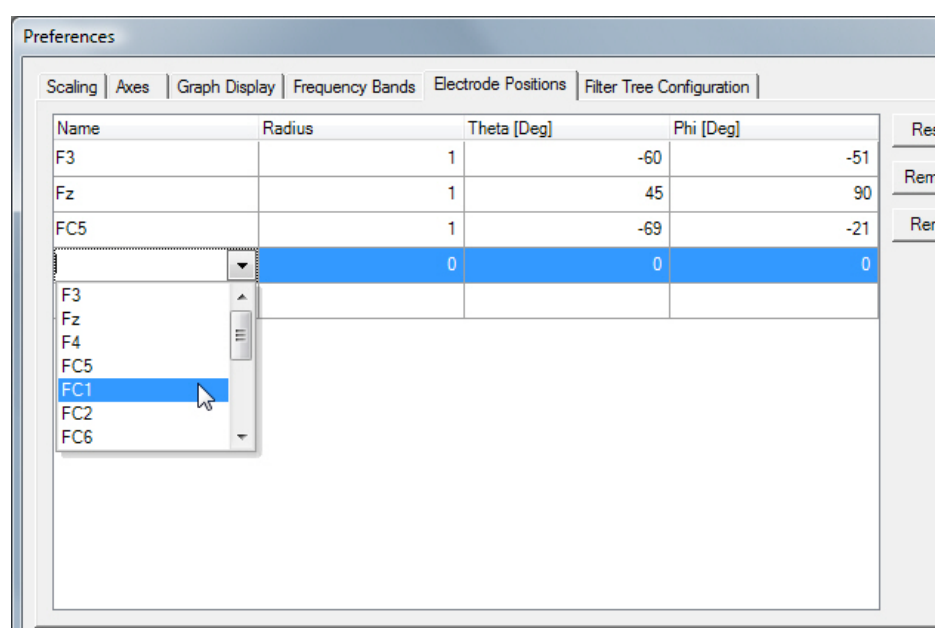

 You will find a description of the electrode coordinate system in [Appendix A](#) as of [page 133](#).

Figure 4-8. Selecting the electrode positions



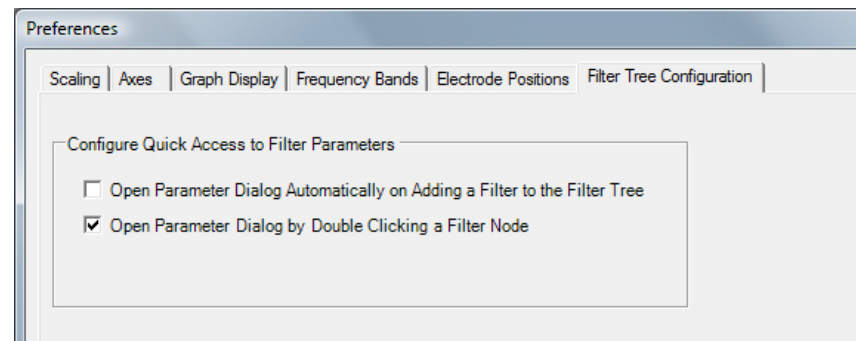
You can make the following settings:

- ▶ Once you have established a connection between RecView and the Recorder by means of *Connect to Vision Recorder* , you can select the names of the electrodes that are currently being used from a drop-down list in the *Name* column. Alternatively, you can enter the electrode names by hand.
- ▶ The *Remove Row* and *Remove All* buttons allow you to delete the selected row or all rows respectively.
- ▶ The *Reset Row* button allows you to undo the changes made for the channel.

4.6 Configuring fast access to the parameters dialog

In the *Filter Tree Configuration* tab, you can choose between two ways of configuring fast access to the filter parameter dialog: The dialog can be opened automatically whenever you drag and drop a filter icon to the filter tree and/or whenever you double-click the corresponding filter node in the tree.

Figure 4-9. Configuring fast access to the filter parameter dialog





Chapter 5 Montages

Montages enable channels to be reconnected in the software, i.e. new voltage references are assigned to the channels. Montages also serve to optimize the display of data, e.g. by combining frontal electrodes in one montage and occipital electrodes in another one. When a montage is selected, only those channels which have been assigned to it are displayed. The sequence of channels can also be changed using montages so that channels which were originally apart can be shown next to each other. A channel can also be displayed multiple times in a montage.

A montage is used for visualization purposes only. The resulting data only exists temporarily and is not passed to downstream filters.

The current version of RecView does not allow you to create montages. On the other hand, you can use all the montages created in the Recorder and the montages from the Analyzer with the exception of Laplacian Reference montages.

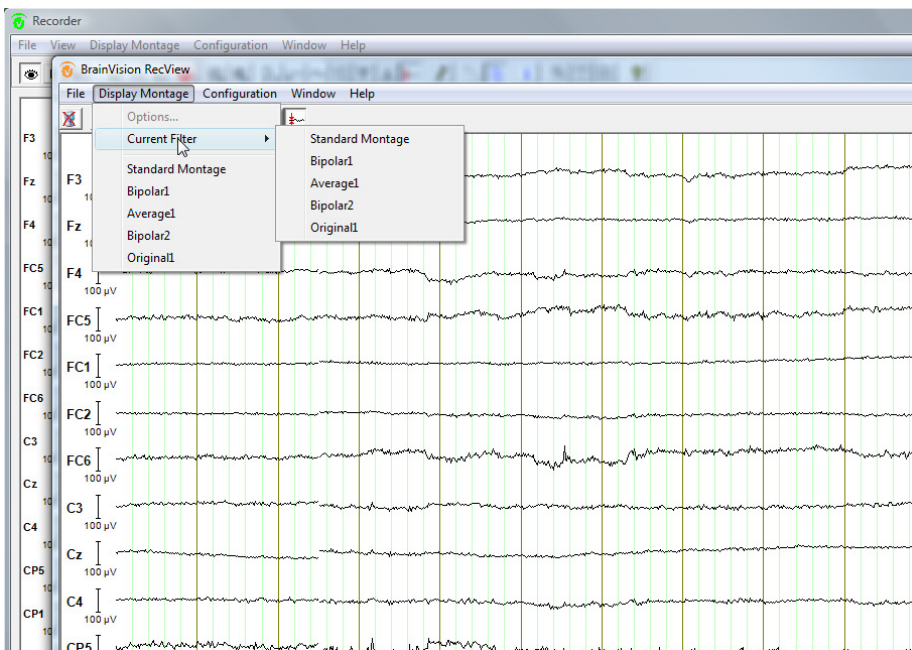
To show all the montages in the Work Files folder, click *Display Montage* in the RecView menu bar. Select a montage to apply it to the main window.

Choosing *Display Montage > Current Filter* from the menu lists all the montages for the active filter window if you have created a filter tree (see [Figure 5-1](#)). Always use the *Current Filter* function if you want to apply a montage to the active filter.



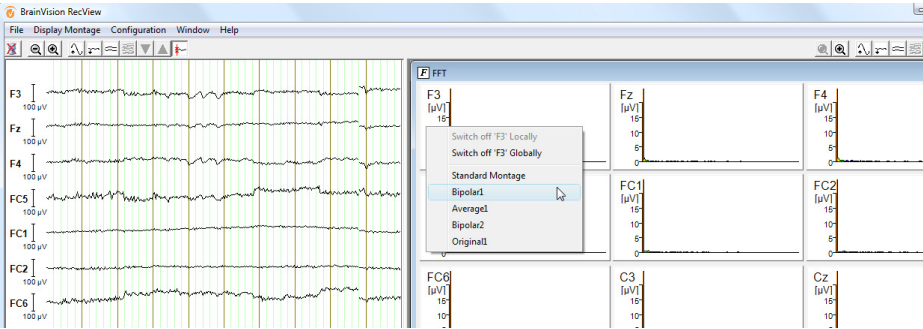
You should use the same Work Files folder for RecView as you do for the Recorder to allow you access to the Recorder montages.

Figure 5-1. Displaying and selecting montages (A)



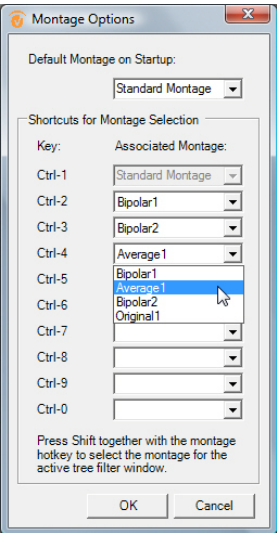
Alternatively, right-click in the data window and choose a new montage from the context menu (see [Figure 5-2](#)).

Figure 5-2. Displaying and selecting montages (B)



You can assign keyboard shortcuts to montages to allow you to switch between them (see [Figure 5-3](#)). Pressing these keyboard shortcuts activates the montages. To open the dialog box for selecting the keyboard shortcuts, choose *Display Montage > Options...* from the menu.

Figure 5-3. Assigning keyboard shortcuts to montages



You can freely assign the keyboard shortcuts *<Ctrl + 2>* through *<Ctrl + 0>* to the existing montages. *<Ctrl + 1>* is reserved for the default montage. If you have created a filter tree, you can use the shortcuts *<Ctrl + Shift + 1>* through *<Ctrl + Shift + 0>* to select the montage for the active filter window. You also have the option of selecting a montage that will be used by default when data is first displayed in RecView (*Default Montage on Startup*). ●

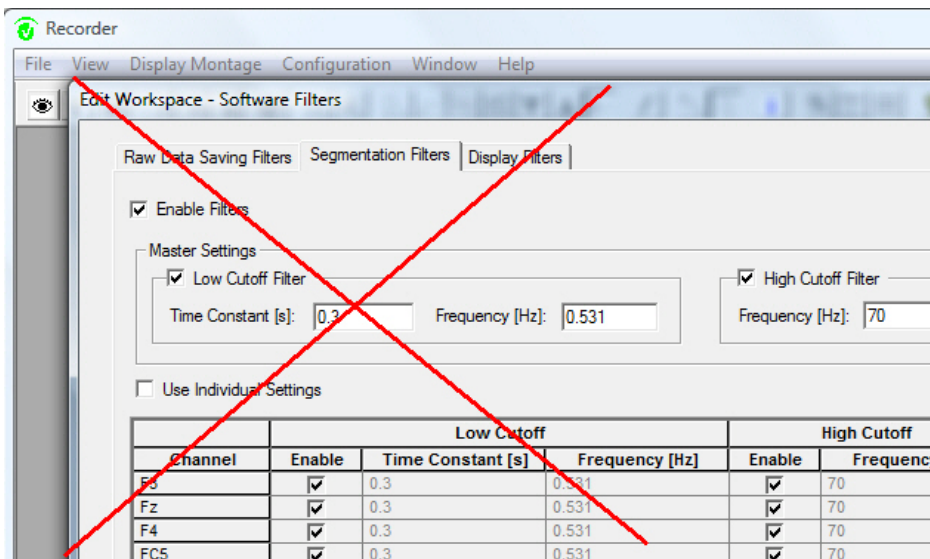


Chapter 6 Basic filters

Note that any software filters such as Segmentation Filters that are active in the Recorder have NO effect in RecView.



Figure 6-1. Software filters active in the Recorder have no effect in RecView



6.1 Average

Summary

The Average filter is used to average previously segmented data or frequency data. The Average filter also allows you to precisely define the period over which averaging is to be performed. You can define a given number of data blocks or a given window length over which the filter is to perform averaging. You can also calculate a weighted average value across the window, rectify the preceding signal and subtract the current average value from the current block.



Because RecView is an Online application, the average can only ever be drawn for all the segments present at the given time. As a result, the first segment is shown without change. Further segments have still not been passed to RecView by the Recorder at this time. As soon as the second segment is available to RecView, an average is drawn across these two segments, etc.

Settings

Figure 6-2. Parameters dialog box for the Average filter

Parameters for Average

☒ Enable Baseline Correction

☐ Interval Relative to Start of Segment

☒ Interval Relative to Marker

Interval Relative to Marker

☒ Based on Time

☐ Based on Datapoints

Start [ms]: -100

Start Point: 0

End [ms]: 500

End Point: 0

Duration [ms]: 600

Points: 1

☒ Enable Rectification

Rectification

☐ Absolute Values

☒ Squared Absolute Values

☒ Enable Weighted Averaging

Weighted Averaging

Window Form:

Window Length:

☒ Equal

10

☐ Triangular

☐ Exponential

Time Constant: 1.000

☒ Apply Zero-Phase Delay

☐ Subtract Weighted Average from Current Segment

OK

Cancel

You can perform an optional baseline correction prior to averaging. To do this, check the *Enable Baseline Correction* box.

You can now specify whether baseline correction is to be performed relative to the start of the segment (*Interval Relative to Start of Segment* option) or relative to the marker (*Interval Relative to Marker* option).

In both cases, the next group allows you to define whether the interval is to be determined on the basis of time (*Based on Time* option) or on the basis of data points (*Based on Data-points* option). If you choose to use time-based intervals, you enter the boundaries and duration of the interval in the text boxes *Start [ms]*, *End [ms]* and *Duration [ms]*. If you choose to use data-point-based intervals, you enter the start and end points and the number of data points in the text boxes *Start Point*, *End Point* and *Points*.

If you define an interval that does not lie within the segment boundaries, the program creates the intersection between the interval you select and the segment that is actually present. If the intersection is empty, no baseline correction is performed.



If you wish, you may rectify and prepare the signal blocks prior to averaging. To do this, select the *Enable Rectification* check box. The data blocks can be rectified by forming the absolute value (*Absolute Values* option) or by forming the squared absolute value (*Squared Absolute Values* option). The squared value is used to measure the power density spectrum.

To calculate a weighted average of the data blocks, check the *Enable Weighted Averaging* box. Enter the number of preceding (i.e. past) data blocks that are to be included in averaging in the *Window Length* text box. You can choose between three window functions:

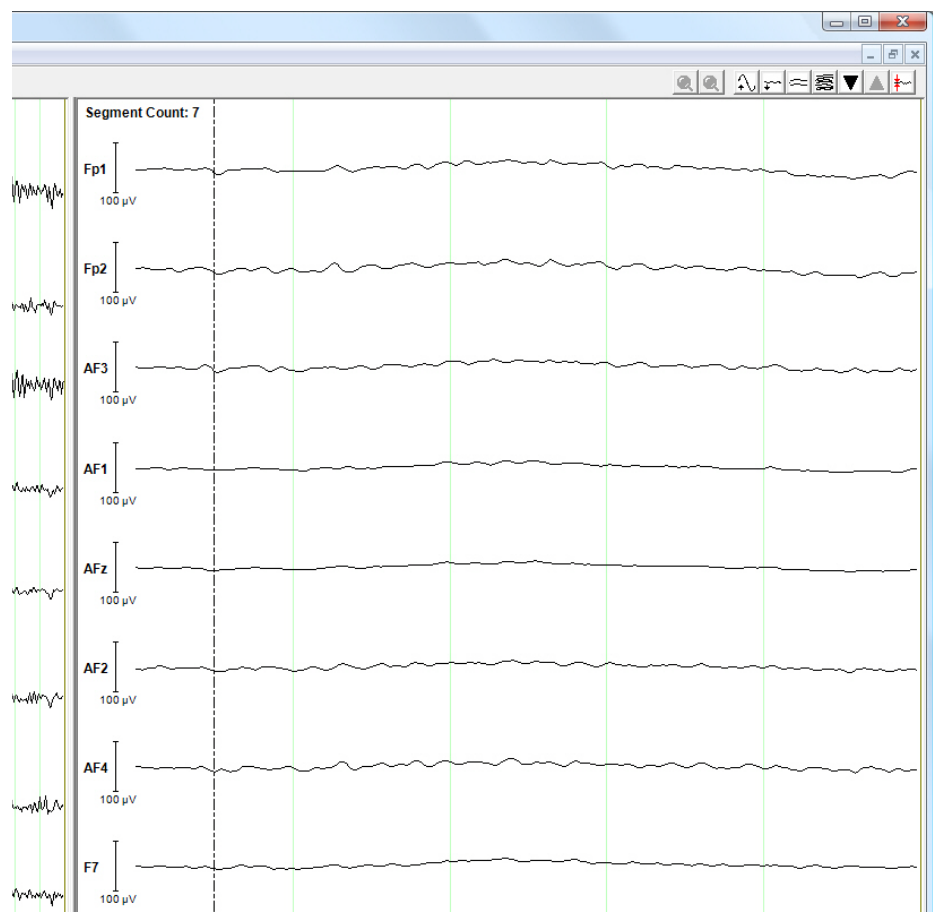
- ▶ *Equal*. The *Equal* option generates a symmetrical rectangular window. All the data blocks are weighted equally.
- ▶ *Triangular*. The *Triangular* option generates a symmetrical triangular window. As a result, at half the window length (*Window Length* box), the centrally located data block will have the greatest weighting.
- ▶ *Exponential*. The *Exponential* option generates a non-symmetrical window which falls exponentially on one side. The value of the time constant is required for a complete definition of this window that falls exponentially on one side. It comprises the same number of blocks as is specified in *Time Constant*.



By checking the *Apply Zero-Phase Delay* box, you are able to delay data output from the filter by half the window length, i.e. the filter supplies the averaged data to the view with a lapse of half a window length. Please note that in this case you must always select an even number for the window length since this is the only way of defining an unambiguous midpoint in the window.


If you want to depict current deviations from the long-term average value, check the *Subtract Weighted Average from Current Segment* box. This subtracts the stored average from the current segment.

Figure 6-3. Average filter



6.2 Band Power Trigger

The Band Power Trigger filter is used to send signals to the computer's LPT port as a function of their band power values. The use of this filter is particularly recommended within the framework of neurofeedback research.

The filter can only be used with frequency data (FFT-filtered data).
You must possess administrator permissions in order to use LPT port control. Under Windows® you must also start RecView in Administrator mode even if you are already logged in as administrator at the computer (see also  section 3.4 on [page 50](#)).

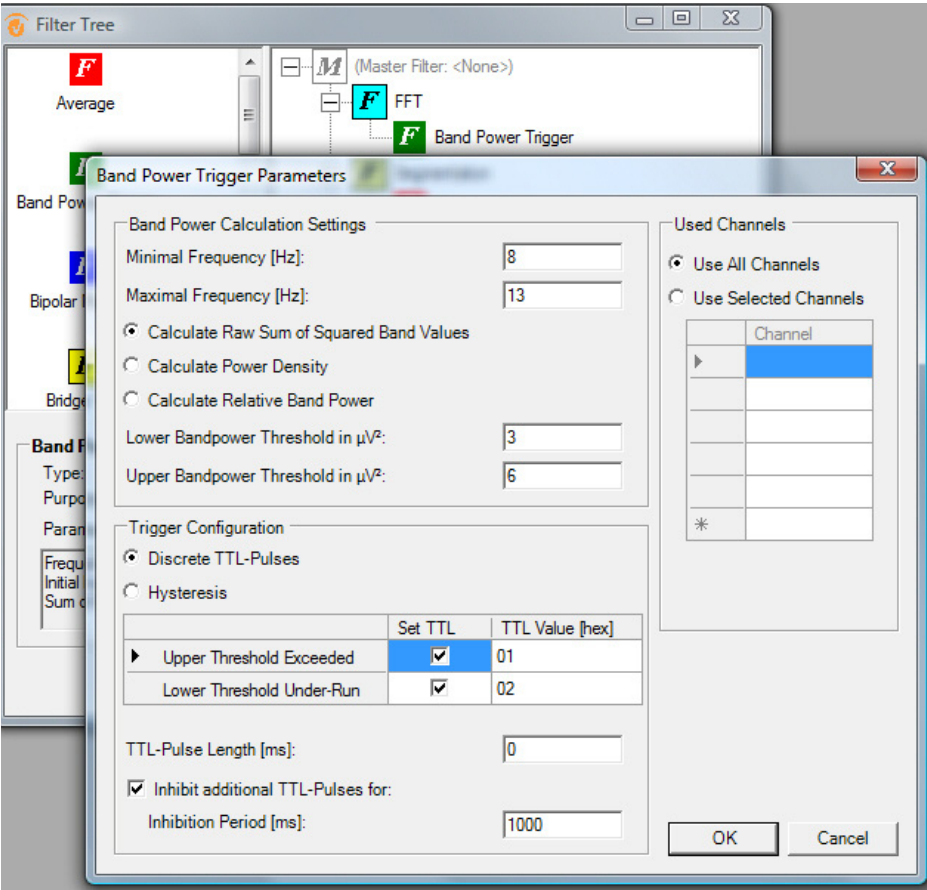
Summary

Prerequisites for use



Settings

Figure 6-4. Parameters dialog box for the Band Power Trigger filter



You can enter the limit values for the required frequency band in the *Minimal Frequency [Hz]* and *Maximal Frequency [Hz]* text boxes.

If the option **Calculate Raw Sum of Squared Values** is selected then the threshold values are specified in μV^2 . In the case of **Calculate Power Density**, these values are specified in $\mu V^2/Hz$ and in the case of **Calculate Relative Band Power**, they are specified in %.

There are three different ways of calculating the band power:

- *Calculate Raw Sum of Squared Band Values.* The squared values of all the frequency values within the previously defined frequency band are totaled. You should note that the number of totaled frequency values depends on the resolution.
- *Calculate Power Density.* The power density is displayed.
- *Calculate Relative Band Power.* The system calculates the ratio of the power within the defined frequency limit values to the power of the total spectrum of the signal.

For all three calculation options, you can enter an upper and lower threshold value in the *Lower Bandpower Threshold* and *Upper Bandpower Threshold* text boxes. A trigger is then sent to the LPT port if the value rises above or falls below these thresholds.

The channels selected in *Used Channels* are used for the calculation. The result is divided by the number of channels used.

In the *Trigger Configuration* group, you specify what trigger types and trigger values are sent to the LPT port: discrete TTL pulses or continuous TTL signals. The associated table contains the events *Upper Threshold Exceeded* and *Lower Threshold Under-Run*. *Upper Threshold Exceeded* indicates that the value specified in *Upper Bandpower Threshold* has been exceeded. *Lower Threshold Under-Run* indicates that the value has dropped below that specified in *Lower Bandpower Threshold*.

If you select the *Discrete TTL-Pulses* option then triggers are sent as TTL pulses to the LPT port. The status of the LPT port is reset to 0 after the period defined in *TTL-Pulse Length*. In this mode, both rows can be accessed in the table and TTL pulses can be configured for both events. You can check the associated boxes in the *Set TTL* column in the table to specify whether you actually want the event to release a trigger. The trigger value can be configured in the form of an 8-bit hexadecimal value (0 to FF) which you enter in the cell *TTL Value [hex]*.



In the *TTL-Pulse Length [ms]* text box, you specify the time after which the TTL pulse is reset to 0. If you enter the value 0 in the text box then it is reset immediately. Pulses that are reset immediately or very quickly (< 20 ms) cannot be displayed in the LPT status output. You should also note that the accuracy of the reset timer depends on the resolution of the Windows® internal system clock. It is therefore not possible to guarantee that timing will be accurate to the nearest millisecond.

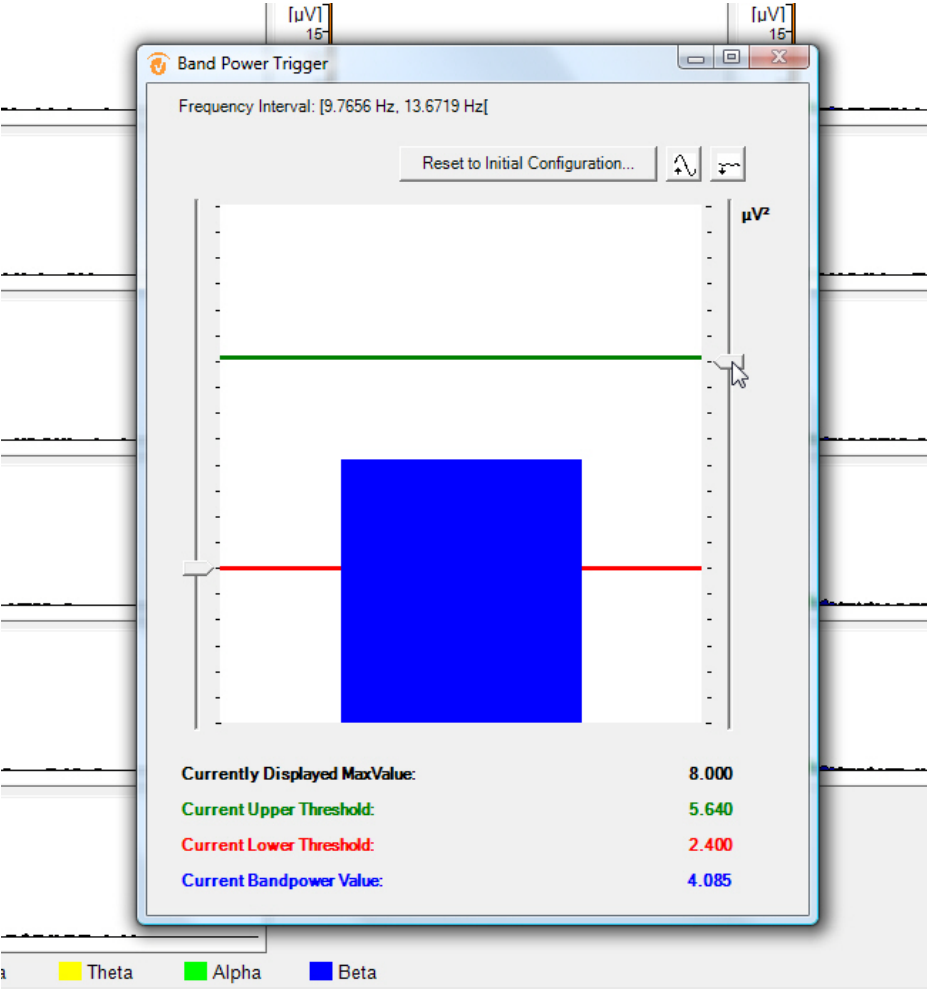
You should also note that TTL pulses are subject to temporal overlaps. This occurs if two (or more) events are detected within the period defined in *TTL-Pulse Length [ms]*. By default, in such cases the filter causes the trigger activated by the first event to be overwritten by any subsequent trigger. If you want to prevent triggers from being prematurely overwritten, check the *Inhibit additional TTL-Pulses for* box and specify the required inhibition period in the *Inhibition Period [ms]* text box. Events that are detected during the inhibition period do not trigger any additional TTL pulses.

If you enter identical values in the *Inhibition Period [ms]* and *TTL-Pulse Length [ms]* text boxes this prevents triggers from ever being overwritten. By choosing an inhibition period that is longer than the value specified in *TTL-Pulse Length [ms]*, you can prevent TTL pulses from occurring more frequently than you would want.

If you select the *Hysteresis* option then continuous TTL signals are sent as triggers to the LPT port. In the table, you can now only access the *Upper Threshold Exceeded* row, i.e. it is only possible to configure a TTL signal for the *Upper Threshold Exceeded* event. When the signal is sent to the LPT port, the LPT port status is retained until it is reset to the value 0 in response to the occurrence of the *Reset* event.

For a diagrammatic overview of the behavior of TTL pulses, see [Appendix D](#) of [page 141](#).



Figure 6-5. Band power trigger filter



In many cases it can be difficult to select appropriate threshold values at the start of an experiment. In addition, the behavior of the EEG data spectrum often changes over long periods of time (for example, if the test subject becomes tired during a comparatively long

Online configuration of the Band Power Trigger filter


experiment). For this reason, there are two slide controls which enable you to adjust the threshold values subsequently. The left-hand control adjusts the lower threshold value and the right-hand control the upper threshold value. After selecting a control, you can also adjust it at the keyboard using the *Up Arrow* and *Down Arrow* keys.

You can also use the *Scale Up*  and *Scale Down*  buttons to adjust the scaling in the normal way. When you perform scaling, it is possible that the two threshold values may no longer be visible in the display window because they are greater than the currently displayed maximum value. In this case, first drag the left-hand control (for the lower threshold value) and then the right-hand control back into the window. You can use the *Reset to Initial Configuration...* button to restore the parameter dialog settings to their initial values if you have changed them.



You should note that none of the adjustments you make in Online operation are persistent, i.e. the modified values are not saved as filter parameters.



If you want to identify the changes you have made during Online operation in your data, use the Recorder to set related "Comment" markers shortly after making each change. See the  Recorder User Manual for detailed information on how to add comments to your recording data in the form of markers.

6.3 Bipolar Montage

Montages enable channels to be reconnected on a software basis. The Bipolar Montage filter allows you to assign a channel a second channel as a new voltage reference. In this way, you define new channels that are derived from the difference in voltage between the two original channels.

Unlike the montages described in [Chapter 5](#), the Bipolar Montage filter is not used solely for visualization purposes, in other words, the data generated by the filter affects downstream filters.

You have the choice of either forming the difference from two consecutive channels in the channel list (*Each Channel Uses the Following Channel as Reference* option) or freely selecting the two reference channels using the table (*Define Reference Channels* option).

The *Clear all* button allows you to delete all specifications from the table.

If you check the *Display Old Channels* box, the original channels are displayed alongside the newly defined channels.

Summary

Settings

Figure 6-6. Parameters dialog box for the Bipolar Montage filter

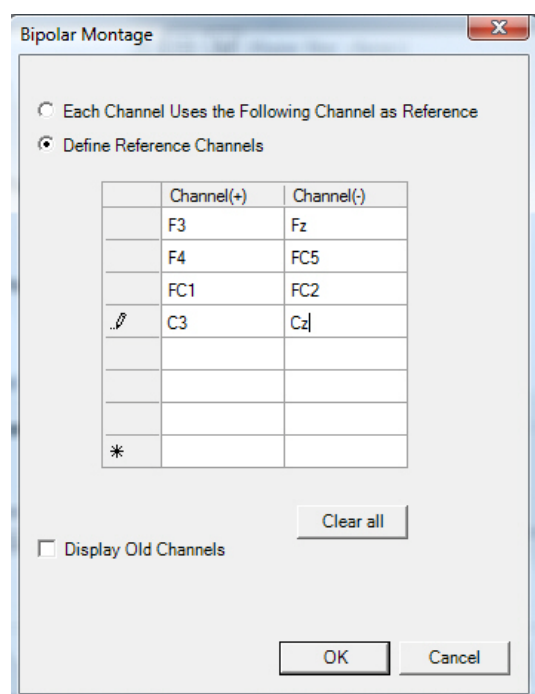
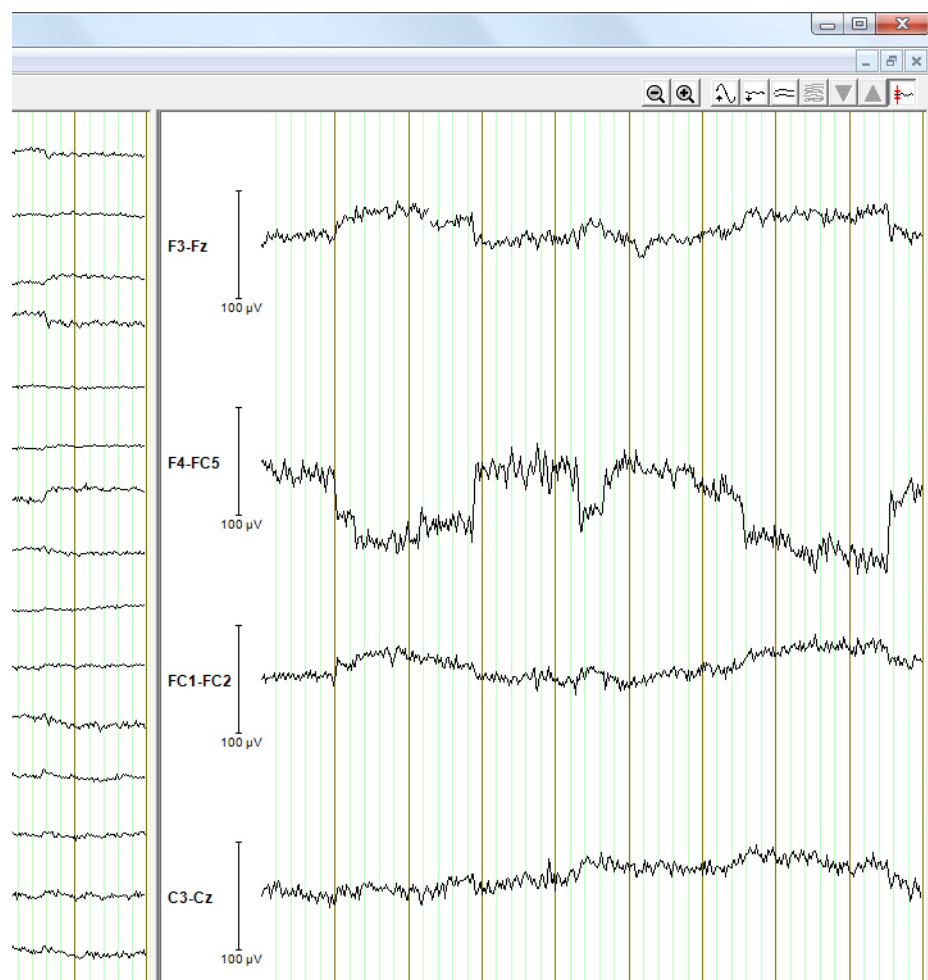


Figure 6-7. Bipolar Montage filter

6.4 Bridge Tool

You can use the Bridge Tool filter to detect any gel bridges that may potentially exist between neighboring channels. Gel bridges occur when the conductive gel that is used to reduce the skin's electrical resistance spreads across the skin of the test subject's head. This creates connections – or bridges – between neighboring electrodes and the corresponding channels are, for practical purposes, short-circuited. The signals in the affected channels have an abnormally high level of similarity. The Bridge Tool filter recognizes this abnormally high similarity between neighboring channels and displays this in graphical form.

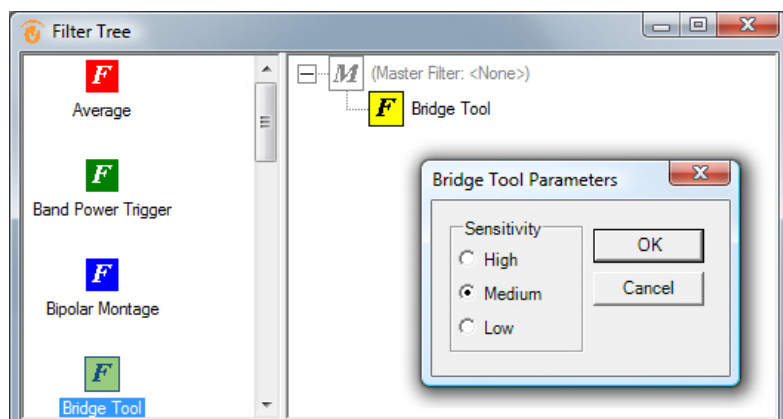
Using the Bridge Tool filter reduces the probability that you will create gel bridges when preparing the electrodes. In addition, the filter can help you achieve a long-term reduction in the time required for preparation by allowing you and your personnel to gain experience of the required amounts of gel. Once the potential presence of gel bridges has been detected, you must decide whether or not to continue with the measurement.

While you are performing impedance measurement using the actiCAP ControlSoftware or the Recorder, you can also run RecView in parallel. However, if you wish to reliably detect gel bridges, the actiCAP ControlSoftware and the Recorder must not be in impedance mode.

Summary

Deactivating Impedance mode

Figure 6-8. Filter tree with Bridge Tool filter and associated parameters dialog box



Settings

In the Bridge Tool filter's parameters dialog box, you can set the sensitivity to be used for the detection of gel bridges between two channels. If in doubt, you should choose *Low*. Of course, setting the sensitivity to *High* increases the probability that gel bridges that are genuinely present will be detected. At the same time, however, this also increases the probability of false alarms, i.e. gel bridges may be reported even though none actually exist. The opposite applies to the setting *Low*.

To obtain values that will help you decide on the optimum detection sensitivity more quickly, we recommend that you create a filter tree consisting of three Bridge Tool filters arranged in



parallel and assign each filter one of the three settings: *High*, *Medium*, *Low*. A bridge alarm should then only be interpreted as indicating a genuine bridge if it appears permanently when *Low* is set.

Start RecView. The right-hand window (filter window) contains a Paired Channel View covering all the electrode positions. If gel bridges are present, the view indicates red connecting lines between the relevant electrode positions after about a minute (see [Figure 6-9](#)).



You should note that due to the fact that the view is continuously updated, the red connection lines may disappear again.

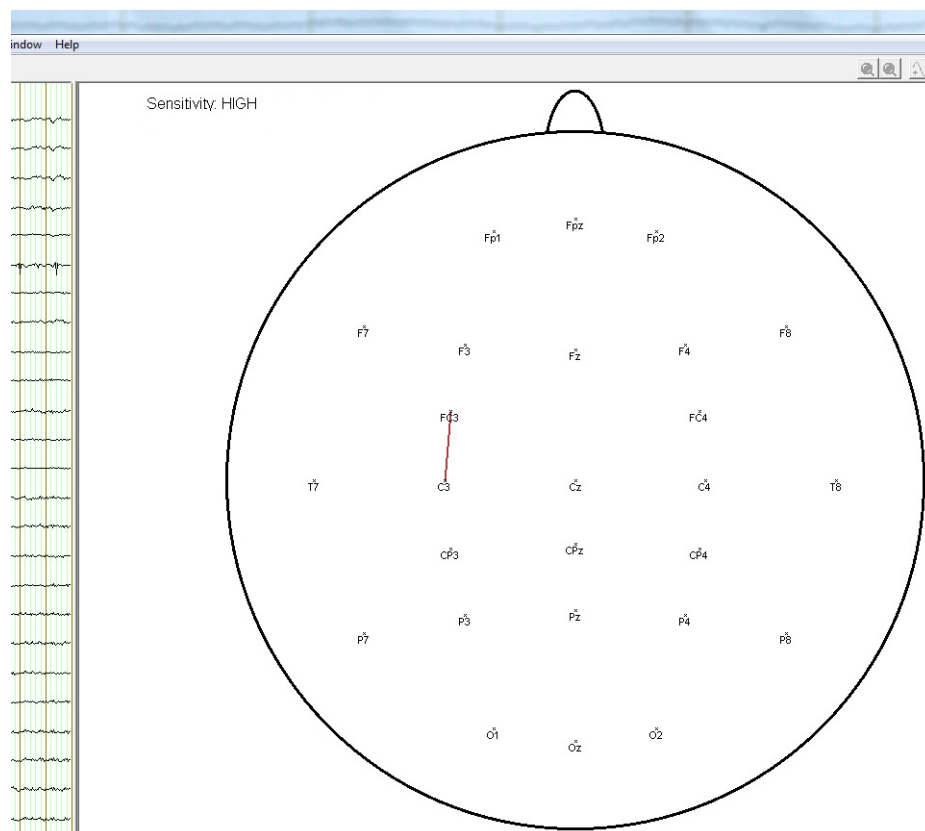
To reliably identify bridges and avoid creating any artifacts, do not apply any more gel. You should also make sure that the test subject keeps his/her eyes open, moves as little as possible and does not speak. If a connecting line is continuously displayed for several minutes then this very probably indicates a genuine gel bridge. If a line is only illuminated sporadically and then disappears again, then this is a false alarm and it is very probable that no gel bridge actually exists.

It is possible that the Bridge Tool filter may incorrectly interpret artifacts in the EEG as gel bridges. This is particularly likely if an electrode has just been filled with gel or if the test subject moves or talks. If the filter identifies more gel bridges than a fixed upper limit that is dependent on the number of channels used, then the Bridge Tool filter switches to *Automatic Mute Mode*. In this mode, the Paired Channel View statically displays all the potential gel bridges as dark red lines. If these lines are simply artifacts, the Bridge Tool filter switches back to normal mode as soon as the EEG is free of artifacts again and the indicated bridges have disappeared again.



If gel bridges are actually present and the static red lines persist, we recommend that you interrupt the measurement and prepare the electrodes again using a considerably smaller quantity of gel. As a guideline gel quantity, we recommend using approximately 10 cm³ of gel for 30 channels.



Figure 6-9. Displaying gel bridges in the Paired Channel View



Before performing any measurements with test subjects for research purposes, you should conduct a number of test data acquisitions in order to gain experience of the conditions of use of the Bridge Tool filter, for example concerning the test subject's hair length and head shape, the amount of gel to be applied and the position of the electrode cap.

Tips on the use of the Bridge Tool filter

If you still have little experience of preparing electrodes, we recommend that you should proceed as follows when using the Bridge Tool filter. This procedure is also useful if you want to use the Bridge Tool filter to train your personnel in cap preparation.

- 1 Fill 6 to 10 neighboring electrodes with gel and optimize the impedances (electrode LEDs glow green). When doing this, use as little gel as possible.
- 2 Use the Bridge Tool filter to perform regular checks of this group of neighboring electrodes for the presence of bridges during the preparation procedure. To do this, switch the Recorder software between impedance  and  monitoring mode.
- 3 If you detect a large number of gel bridges during the preparation stage, you must decide whether to interrupt or continue the measurement.

- 4 When you have finished preparing all the electrodes, apply the Bridge Tool filter again in order to obtain definitive information about the possibility of gel bridge formation.

If you already have a lot of experience of preparing electrode caps, we recommend that you proceed as follows when using the Bridge Tool filter in order to minimize the time spent preparing the electrodes:

- 1 Use as little gel as possible and attempt to obtain good average values for the impedances of all electrodes (electrode LEDs glow yellow).
- 2 When all the LEDs are glowing yellow or better, apply the Bridge Tool filter. The probability of gel bridges occurring now is extremely low.
- 3 Next fill the electrodes that are still glowing yellow with another very small quantity of gel until you reach the optimum impedance values (electrode LEDs glow green).
- 4 Apply the Bridge Tool filter again in order to obtain definitive information about the possibility of gel bridge formation.

Requirements relating to the test subject

Make sure that the test subject does not talk, move or close his/her eyes while the data is being checked using the Bridge Tool filter.

Practical experience concerning the number of electrodes

In our experience, it is possible to prepare a cap with 64 or 128 electrodes without a single gel bridge occurring – even with long-haired test subjects. In the case of caps using 256 electrodes, it is possible to apply the gel without forming bridges provided that you perform the preparations carefully.

Related publications

Tenke CE, Kayser J, A convenient method for detecting electrolyte bridges in multichannel electroencephalogram and event-related potential recordings, *Clin Neurophysiol.* 2001 Mar, 112(3):545-50.

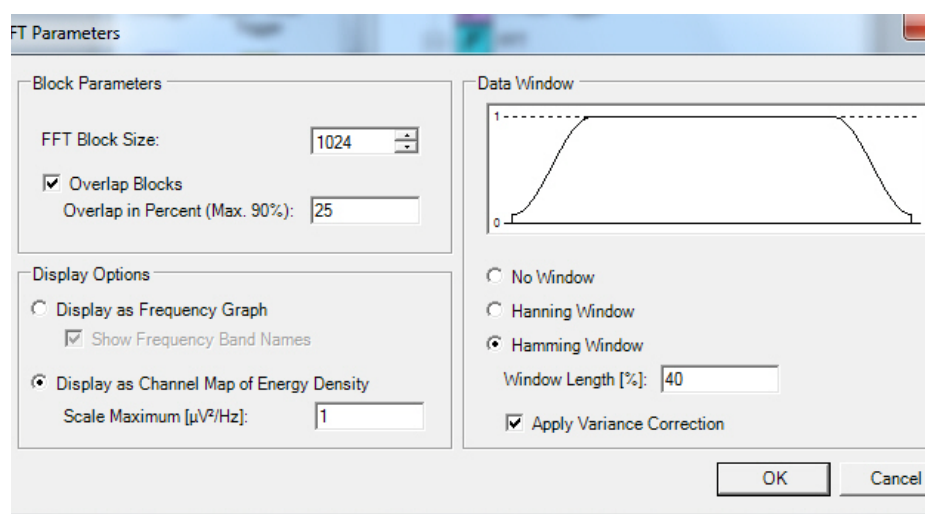
Tenke CE, Kayser J, A convenient off-line method for detecting electrolyte bridges in multichannel ERP recordings, *Psychophysiol.* 2000, 37:94.

Greischar LL, Burghya CA, et al., Effects of electrode density and electrolyte spreading in dense array electroencephalographic recording, *Clin Neurophysiol.* 2004 Mar, 115(3):710-20.

6.5 FFT (Fast Fourier Transform)

The FFT filter transforms data from the time domain into the frequency domain. The resulting data indicates the extent to which the individual frequencies are present in the EEG between 0 Hz and at most half the sampling rate.

Figure 6-10. Parameters dialog box for the FFT filter



FFT Block Size allows you to specify the block size used for calculation, expressed as a number of data points. You can only select powers of 2. The larger the block size, the less often the representation will be updated. *But we recommend that you do not select too few data points, as this may overload the computer and possibly cause data blocks to be lost.*

Because the block size must always be a power of 2, the required block size is always zero-padded to the next power of 2 with segmented data. This means that a data block that does not already have a length corresponding to a power of 2 is padded with zeros.

If you check the *Overlap Blocks* box, the blocks are not processed sequentially, but are instead overlapped. The percentage by which the blocks are to be overlapped is specified in the *Overlap in Percent (Max. 90%)* text box. This value is restricted to 90%. If, for example, you select an overlap of 75%, only 25% of the data points are new as of the first data block. The advantage of overlapped processing of the data blocks lies in improved continuity in data representation (see [Figure 6-13](#)).

Note that the overlap function is not available for segmented data.

If you select the *Display as Frequency Graph* option, the FFT data is displayed as frequency graphs for each channel. The *Show Frequency Band Names* check box allows you to switch the graph labeling on and off.

Summary

Settings

Defining the block size



Display options

If you check the *Display as Channel Map of Energy Density* box, a map of the energy density distribution is displayed for each frequency band. You can also set the scaling for the map in *Scale Maximum* [$\mu V^2/Hz$].

FFT data window



In the same way as the Periodic option for the FFT in the Analyzer, RecView configures the right-hand margin of the window in such a way as to optimize the analytical characteristics of the window for its periodic continuation.

Since the FFT assumes that the segment will be periodically continued, artifacts occur in high frequency ranges due to jumps to the segment boundaries. We advise using a window function to eliminate these artifacts. In the *Data Window* group, you can specify the type of the FFT data window. The following three options allow you to choose between different window types: *No Window*, *Hanning Window* and *Hamming Window*. In the *Window Length [%]* text box, you enter the window length as a percentage of the segment length. The window function is displayed graphically in the filter's parameters dialog box.

If you select the *Apply Variance Correction* check box, the power in the EEG signal is identical before and after the application of the FFT, even when a window function is used.

In both representations (frequency graph or map), double-clicking enlarges it to occupy the entire filter window (see [Figure 6-11](#)). If you double-click in the filter window again, you switch back from individual-channel mode to the original view.

Figure 6-11. FFT in the frequency graph view using individual-channel mode

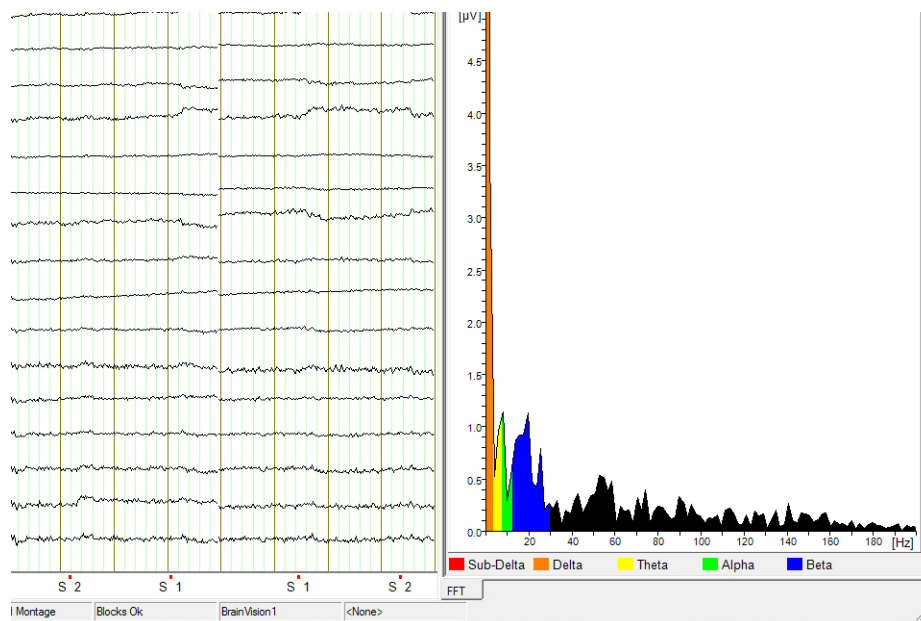


Figure 6-12. FFT in the map view

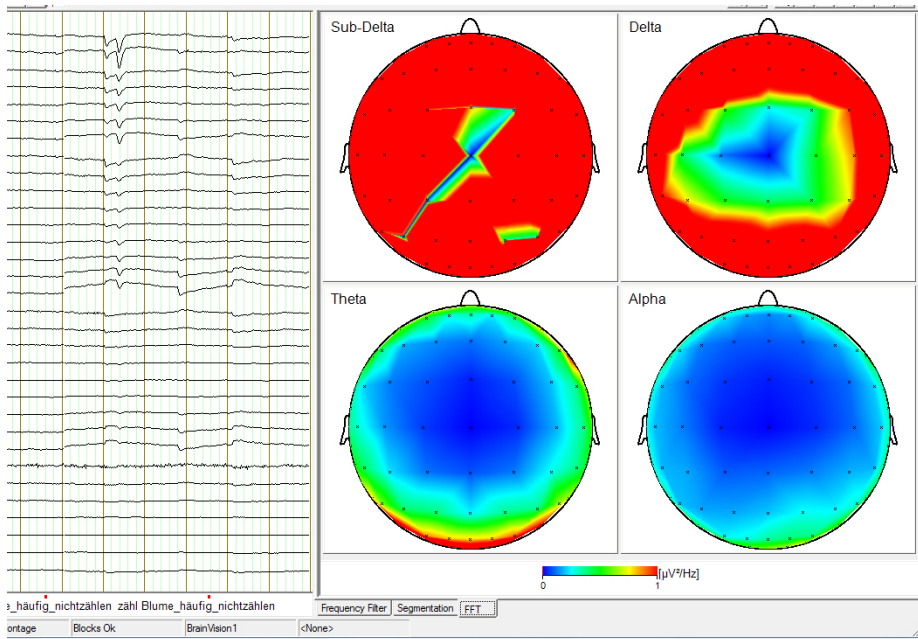
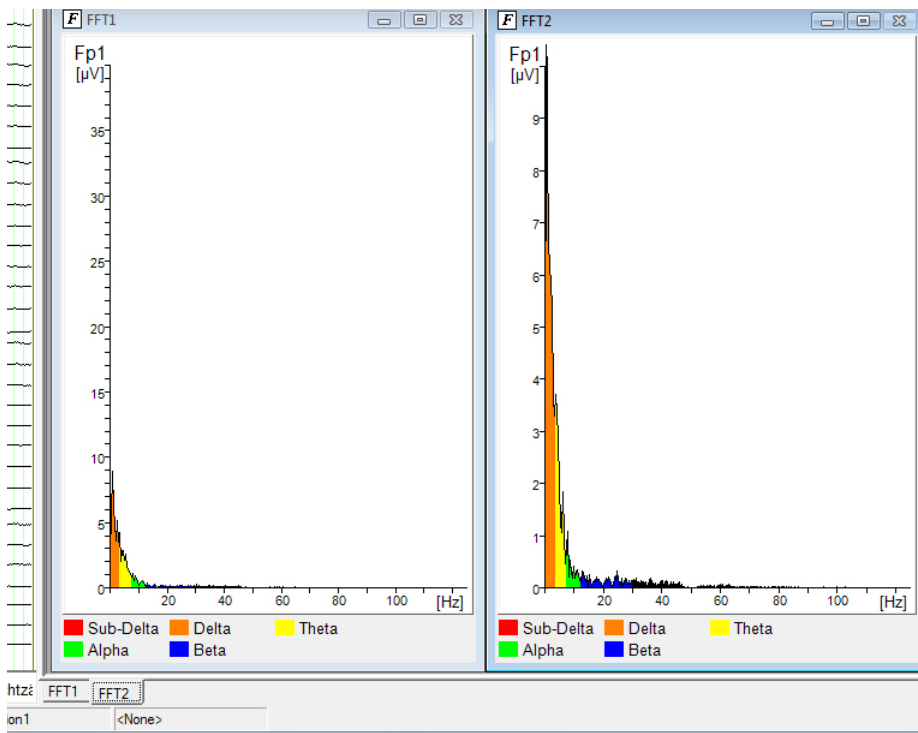


Figure 6-13. FFT filter without overlap (left) and with overlap (right)



6.6 Frequency Filter

Summary

The Frequency Filter is used to restrict the bandwidth to a particular frequency range. It also allows you to select a 50 or 60 Hz notch filter.

Settings

Check the appropriate box – *Low Cutoff Filter*, *High Cutoff Filter*, *Notch Filter* – to specify what filter is to be used (high-cutoff, low-cutoff, notch).

In the case of the Low Cutoff Filter, enter the lower frequency threshold in *Cutoff Frequency [Hz]*. The *Slope [dB/oct]* drop-down list allows you to determine the slope of the filter.

As with the Low Cutoff Filter, in the case of the High Cutoff filter, enter the upper frequency threshold in *Cutoff Frequency [Hz]* and the filter slope in *Slope [dB/oct]*.

In the case of the Notch Filter, you can select a *Frequency [Hz]* of 50 or 60 Hz. The slope of this filter is fixed at 48 dB/octave and cannot be selected explicitly.

Figure 6-14. Parameters dialog box for the Frequency filter

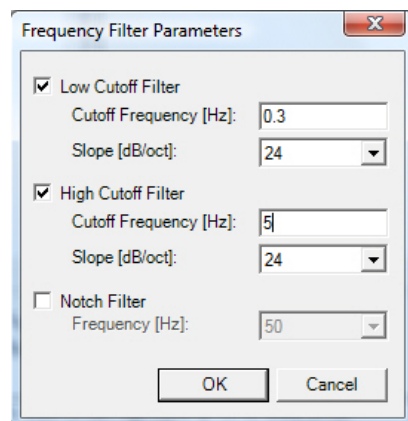
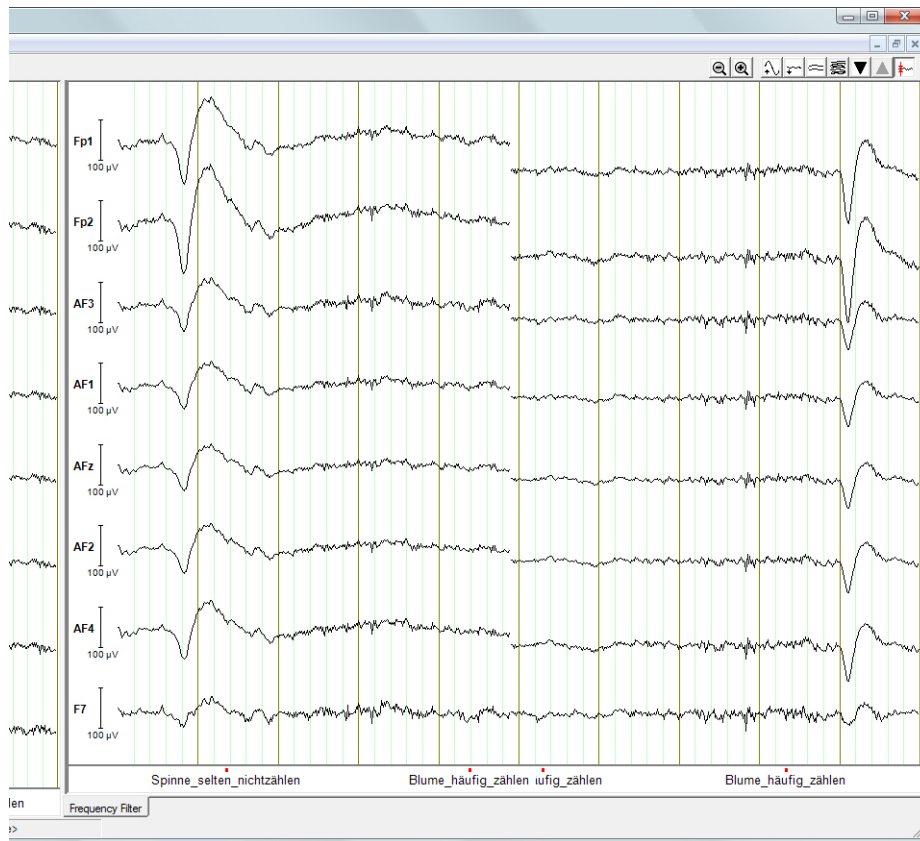


Figure 6-15. Frequency filter



6.7 Level Trigger

Summary

The Level Trigger filter allows you to set markers or send configurable signals to the computer's LPT port as a function of the voltage curve for a selected EEG channel. The use of this filter is particularly recommended within the framework of neurofeedback research.

Prerequisites for use

The filter can only be used with time data.



You must possess administrator permissions in order to use LPT port control. Under Windows®, you must also start RecView in Administrator mode even if you are already logged in as administrator at the computer (see also section 3.4 on [page 50](#)).

Settings

Figure 6-16. Parameters dialog box for the Level Trigger filter

Level Trigger Parameters

Level Settings

Name	Channel	Threshold	Direction	Reset Value
R	Fp1	-300	Negative	-250

Time Tolerance [ms]: 5

Trigger Configuration

☐ Discrete TTL-Pulses
☒ Hysteresis

	Set Marker	Set TTL	TTL Value [hex]
▶ Threshold Value Exceeded	<input checked="" type="checkbox"/>	<input checked="" type="checkbox"/>	01
Peak Found	<input type="checkbox"/>	<input type="checkbox"/>	02
Reset Value Under-Run	<input type="checkbox"/>	<input type="checkbox"/>	03

TTL-Pulse Length [ms]: 15

☐ Inhibit additional TTL-Pulses for:
Inhibition Period [ms]: 1000

You define the threshold value in the *Level Settings* group. You specify a name for the threshold that you want to search for in the *Name* column. In the drop-down list in the *Channel* column, you choose the channel on which the threshold is to be searched for. You specify the threshold in μV in the *Threshold* column.

In the drop-down list in the *Direction* column, you specify the direction of the voltage curve in which the threshold violation is defined. "Positive" means that the corresponding trigger or marker is set when the voltage is rising and the threshold is reached. "Negative" means that the corresponding trigger or marker is set when the voltage is falling and the threshold is reached.

Depending on the direction set in *Direction*, the event *Peak* (see also second row of the table in the *Trigger Configuration* group) indicates the occurrence of a local maximum or minimum value.

In the *Reset Value* column, enter the value in μV at which the event *Reset Value Under-Run* is provoked (see description on this page). This value is usually identical with the *Threshold* but you can set another value for certain purposes. If the direction is positive, the value obtained must be below this one before a new *Threshold Value Exceeded* event can be provoked; if the direction is negative, the value obtained must be above this one.

In the *Time Tolerance [ms]* text box, you can enter an interval during which the EEG curve must rise or fall uniformly after reaching a local minimum or maximum in order to make it possible for the minimum or maximum to be recognized as such. A marker is set for the minimum or maximum within this interval. You should adjust the size of the interval to the steepness of the edges of the trigger channels.

You should note that RecView requires at least the time specified in *Time Tolerance [ms]* in order to reliably detect a peak after its actual occurrence.



In the *Trigger Configuration* group, you specify what trigger types and trigger values are sent to the LPT port: discrete TTL pulses or continuous TTL signals. The associated table contains the events *Threshold Value Exceeded*, *Peak* and *Reset Value Under-Run*. Depending on the direction specified in *Direction*, *Threshold Value Exceeded* indicates that the value set in *Level Settings* has been exceeded exceeded or under-run. *Reset Value Under-Run* indicates that the value has fallen below the specified value. *Peak Found* indicates the first local minimum or maximum that occurs during the period between the threshold being exceeded and the reset.

Please note that RecView sends a single trigger or sets a single marker during the period between *Threshold Value Exceeded* and *Reset Value Under-Run*. It does this at the first detected local minimum or maximum. All further local minimums and maximums during the interval between *Threshold Value Exceeded* and *Reset Value Under-Run* are ignored.



If you select the *Discrete TTL-Pulses* option then triggers are sent as TTL pulses to the LPT port. All three rows are accessible in the table and TTL pulses can be configured for all three events. You can check the associated boxes in the *Set TTL* column in the table to specify that a trigger is actually to be sent to the LPT port. The trigger value can be configured in the form of an 8-bit hexadecimal value (0 to FF) which you enter in the cell *TTL Value [hex]*.

The TTL pulse is reset after the time specified in the text box *TTL-Pulse Length [ms]*; if the text box has the value 0 then the pulse is reset immediately.

Pulses that are reset immediately or very quickly ($< 20\text{ ms}$) cannot be displayed in the LPT status output. You should also note that the accuracy of the reset timer depends on the resolution of the Windows® internal system clock. It is therefore not possible to guarantee that timing will be accurate to the nearest millisecond.





For a diagrammatic overview of the behavior of TTL pulses, see [Appendix D](#) as of [page 141](#).

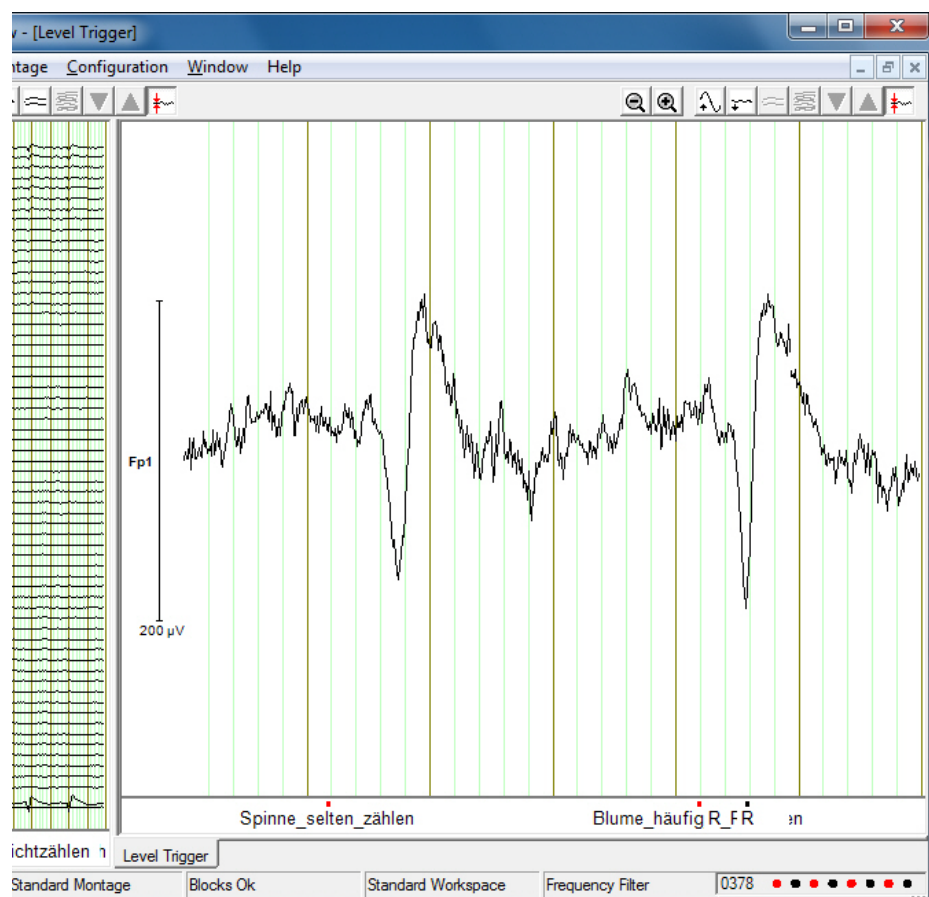
You should also note that TTL pulses are subject to temporal overlaps. This occurs if two (or more) events are detected within the period defined in *TTL-Pulse Length [ms]*. By default, in such cases the filter causes the trigger activated by the first event to be overwritten by any subsequent trigger. If you want to prevent triggers from being prematurely overwritten, check the *Inhibit additional TTL-Pulses for* box and specify the required inhibition period in the *Inhibition Period [ms]* text box. Events that are detected during the inhibition period do not trigger any additional TTL pulses.

If you enter identical values in the *Inhibition Period [ms]* and *TTL-Pulse Length [ms]* text boxes this prevents triggers from ever being overwritten. By choosing an inhibition period that is longer than the value specified in *TTL-Pulse Length [ms]* then you can prevent TTL pulses from occurring more frequently than you would want.

If you select the *Hysteresis* option then continuous TTL signals are sent as triggers to the LPT port. In the table, you can now only fully access the *Threshold Value Exceeded* row, i.e. it is only possible to configure a TTL signal for the *Threshold* event. When the signal is sent to the LPT port, the LPT port status is retained until it is reset to the value 0 in response to the occurrence of the *Reset* event.


You can also set a marker for each of *Threshold Value Exceeded*, *Peak Found* and *Reset Value Under-Run* by checking the corresponding box in the *Set Marker* column. Please note that the Peak marker is set at the time when the peak is recognized as such. In the data, it therefore appears offset from the real peak by the value specified in *Time Tolerance*.

Figure 6-17. Level Trigger filter



6.8 Linear Derivation

Summary

 **Linear Derivation filter in RecView compared to the Linear Derivation transform in the Analyzer**

The Linear Derivation filter allows you to generate new channels through linear combinations of existing channels. The new channels are calculated from coefficients that are assigned to existing channels based on the following formula: New channel = coeff1 * channel1 + coeff2 * channel2 +

Unlike the operation of the Analyzer's Linear Derivation transform, RecView does not know the input channels that are present in the data set at the time of parameter entry. If you do not read the coefficient matrix from a file, you must therefore enter the channel names manually.



Here, you should note that you do not need to enter all the input channels but only those that you require for the generation of the new channels that you wish to create. For example, if, in a data set, you want to generate a new channel as the sum of the input channels 0.3*Fp1 and 0.33*Fp2 then the specifications entered in [Figure 6-18](#) are sufficient, even if the input data contains further channels.

Figure 6-18. Generating the new channel from the combination of the input channels Fp1 and Fp2

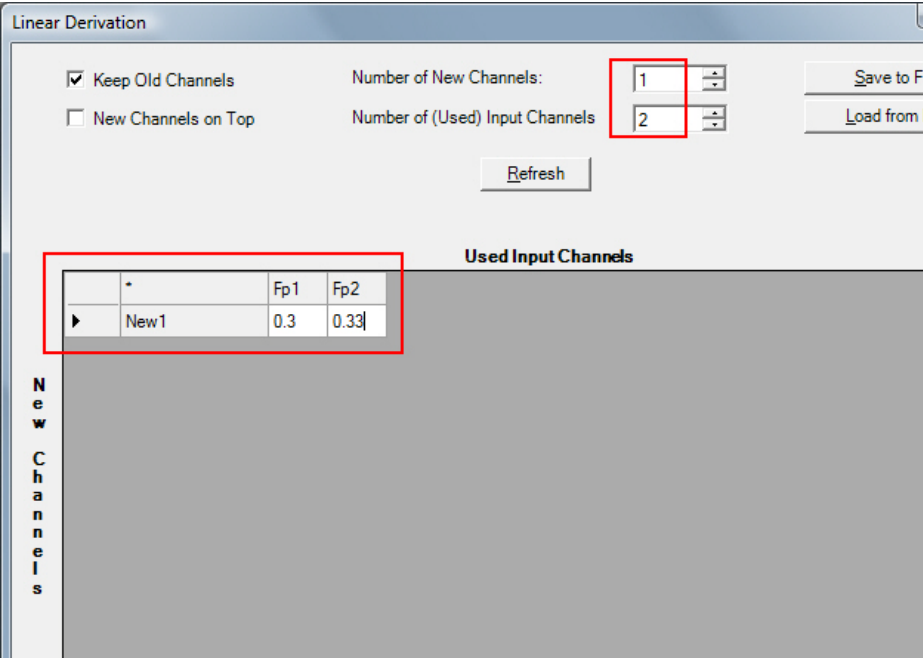


Figure 6-19. Parameters dialog box for the Linear Derivation filter

		Fp1	Fp2	AF3	AF1	AFz	AF2
F00		-0.01886879	0.01950607	0.05276779	-0.005698975	0.01113171	0.0010865
F01		-0.01216254	0.02667836	0.02508937	0.0003135398	-0.01188219	-0.0165563
F02		-0.01004132	0.02798324	0.002041995	-0.0009478853	0.01980104	0.0068015
F03		0.005132434	0.001959419	0.007568133	0.0158857	0.005495728	0.0069618
F04		0.0002894236	0.005805029	0.001035406	-0.01009123	0.008764028	-0.0020466
F05		-0.005706147	-0.03689781	-0.008421344	0.02429723	0.002569839	0.0045098
F06		-0.05768489	0.01407431	0.03182536	0.09146169	-0.009975952	0.0030411
F07		-0.009691566	-0.005631357	0.009835472	0.0364661	-0.01229902	-0.0007360
F08		0.0183203	-0.01267678	0.008130919	0.0008843155	0.0004004566	-0.0013863
F09		-0.01496931	-0.01919437	-0.02875056	0.0248083	0.02428289	0.0198049
F10		0.04581244	-0.005888857	0.0203287	0.002257296	-0.03781291	-0.0246052
F11		0.02250922	0.051467507	0.004212121	0.01405285	0.02787696	0.0088251

If you select the *Keep Old Channels* check box, the old channels are included in the new data set; that makes the new channels additional channels. If you do not check the box, the new data set consists only of the new channels.

If you select the *New Channels on Top* check box, the new channels are listed first.

In the *Number of New Channels* text box, you specify the number of new channels you require. You enter the number of input channels in the *Number of (Used) Input Channels* text box. You can use the *Refresh* button to update the coefficient matrix.

As an alternative to the manual entry of the input channels, you can also read in a coefficient matrix from a text file by clicking the *Load from File...* button. If you choose this method then you do not need to edit the channel matrix in RecView. The matrix must have the following structure:

Table 6-1. Structure of the channel matrix that is to be read in

	Channel1	Channel2	Channel3
New1	Coefficient ^a	Coefficient	Coefficient
New2	Coefficient	Coefficient	Coefficient

a. The decimal separator used in the coefficients is the decimal point (.)

Settings

Method 1: Manual entry in the channel matrix

Method 2: Reading in the LDR matrix



You can also read in ICA matrices that have been exported from the Analyzer or coefficient matrices that have been generated and stored using the Analyzer's Linear Derivation transform. Reading in exported ICA matrices permits the Online output of ICA components that have been calculated offline using the Analyzer.

To save the matrix, click *Save to File...*. The *Remove Line* and *Remove Column* buttons allow you to delete the selected rows or columns from the matrix.

Figure 6-20. Generating new channels using the Linear Derivation filter

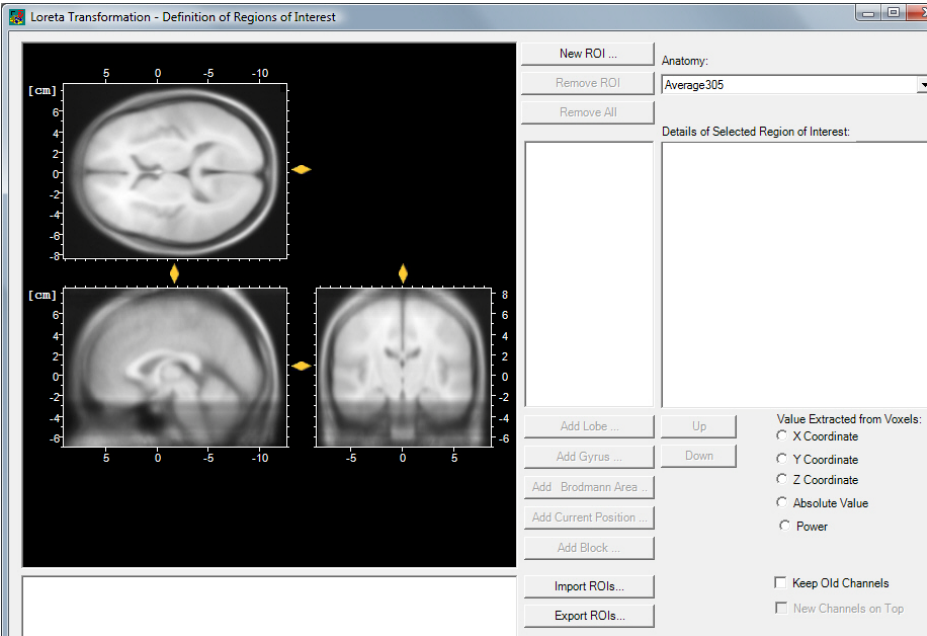


6.9 LORETA

The LORETA filter allows you to view the EEG data as LORETA data over the time domain. Regions of interest (ROIs) are defined for this purpose. Each ROI is displayed in RecView as a virtual channel.

The virtual MR anatomical images are made available by the Montreal Neurological Institute of McGill University.

Figure 6-21. Parameters dialog box for the LORETA filter



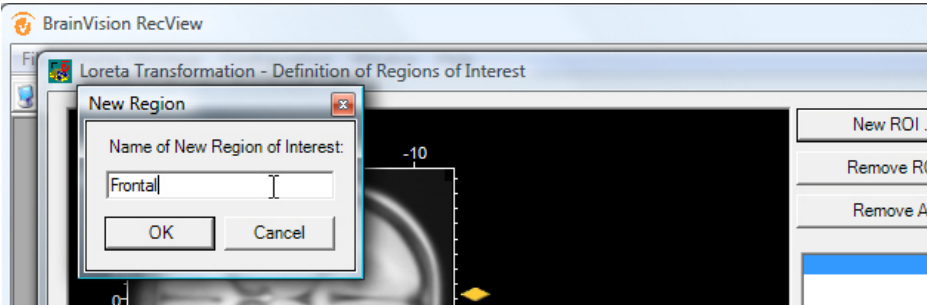
Summary

Settings

In the LORETA filter dialog box, click *New ROI...* to create a new ROI (see Figure 6-22). The *New Region* dialog box appears, in which you can enter the name of the new ROI. The name you enter here is also the name of the virtual channel.

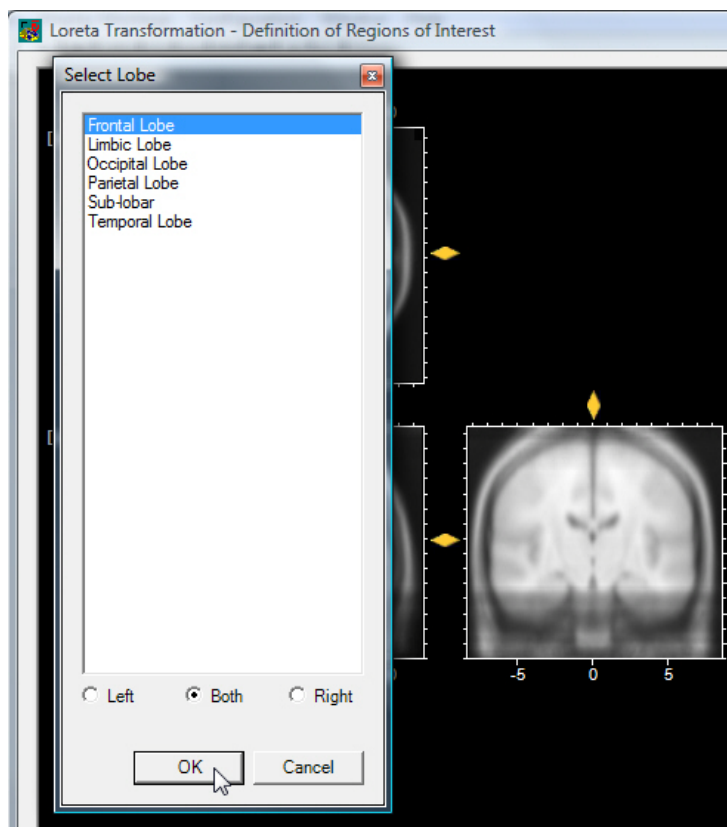
Defining the ROIs

Figure 6-22. Creating an ROI



To add lobes to the ROI, click *Add Lobe...*. The *Left*, *Both* and *Right* options allow you to choose whether the left, right or both lobes are to be added (see [Figure 6-23](#)).

Figure 6-23. Adding lobes

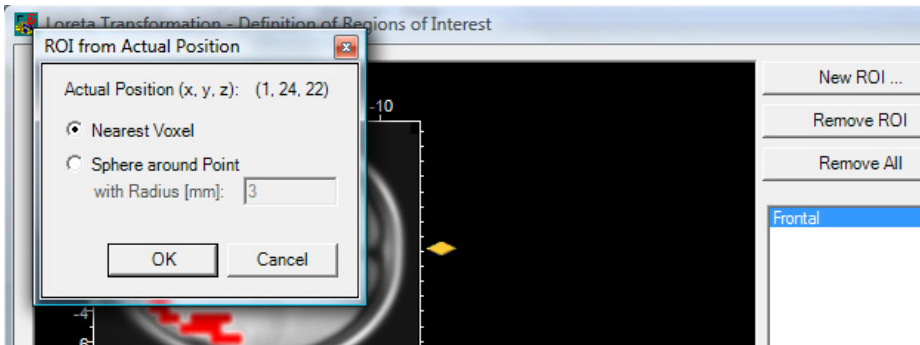


In the same way as selecting lobes, you can use the *Add Gyrus...* and *Add Brodmann Area...* buttons to add gyri and Brodmann areas to the ROI.

The ROIs are defined (block, point, circle) using the MNI coordinate system.

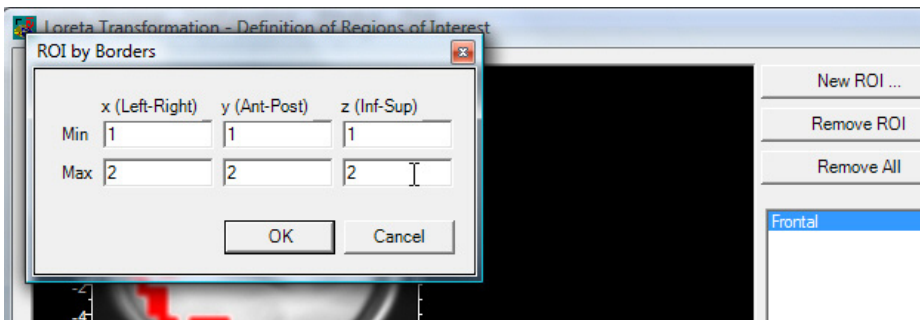
The *Add Current Position...* button allows you to add a specific position to the ROI (see [Figure 6-24](#)). You can choose whether to add the nearest voxel to the mouse pointer (by selecting the *Nearest Voxel* option) or to define a sphere with a specified radius around the current position (by selecting the *Sphere around Point* option).

Figure 6-24. Adding a specific position



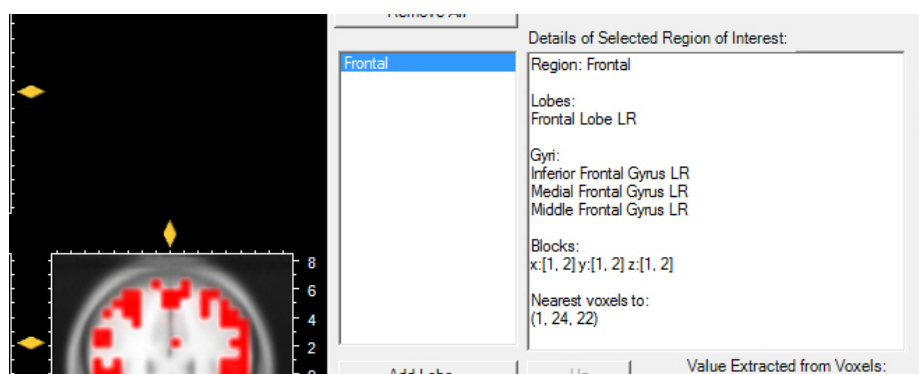
The *Add Block...* button allows you to add a rectangular block, whose limits you can specify (see [Figure 6-25](#)).

Figure 6-25. Adding a block



The *Details of Selected Region of Interest* box lists all the specifications shown above (see [Figure 6-26](#))

Figure 6-26. Part of the LORETA filter dialog box, containing a list of the components of the ROI "Frontal"



Other settings

The *Anatomy* drop-down list allows you to choose between various virtual MR anatomical images.

The *Remove ROI* and *Remove All* buttons allow you to remove ROIs individually or all at once.

In the *Value Extracted from Voxels* group, you can specify which value is to be calculated for the virtual channel from the corresponding ROI. You can choose the x-coordinate, y-coordinate, z-coordinate, absolute value of the coordinates or power (square of the value).

The *Keep Old Channels* check box allows you to specify whether the original channels are to be retained. The *New Channels on Top* check box allows you to specify whether the virtual channels are to be displayed before the original channels in the filter window.

The *Up* and *Down* buttons allow you to specify the order of the ROIs in the data set.

The *Import ROIs...* button allows you to read in ROIs that have already been created. The *Export ROIs...* button allows you to export ROIs you have created as an XML file so that they can be used subsequently.

The *Export Blank ROIs File* button exports voxel data, including the anatomical data, in a CSV file. You can open this file in Excel, for example, define the ROIs manually and reimport them as a CSV file.



If you edit this CSV file, it is essential to make sure that you do not change the number or sequence of the rows in the table. Otherwise errors may occur when you import the file again.

The values in CSV files are separated by commas and not, as in earlier versions of the transform, by semicolons. Please note this when exchanging data with other programs and when reading older CSV files.

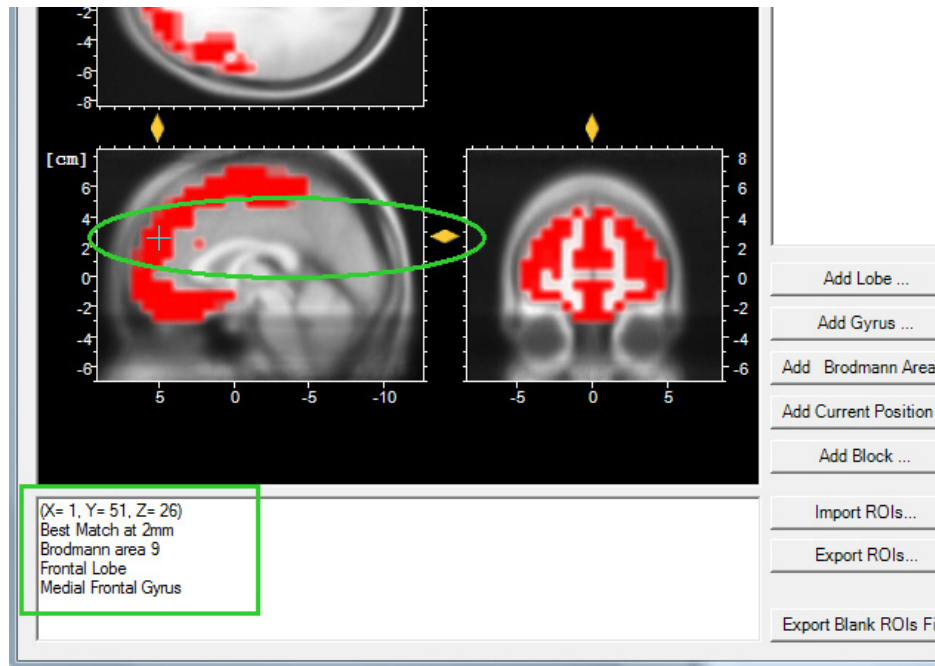
Navigation

You can navigate in the cross-sections or layers of the tomography either by using the mouse to move the four yellow sliders on the borders of the cross-sections in the desired direction or by clicking a point in the cross-section and using the mouse wheel to scroll up and down. When you click in a cross-section, the position of the sliders is updated.

An information field is displayed below the 3D anatomies. This refers to the position of the mouse and contains the following information in the following sequence (see [Figure 6-27](#)):

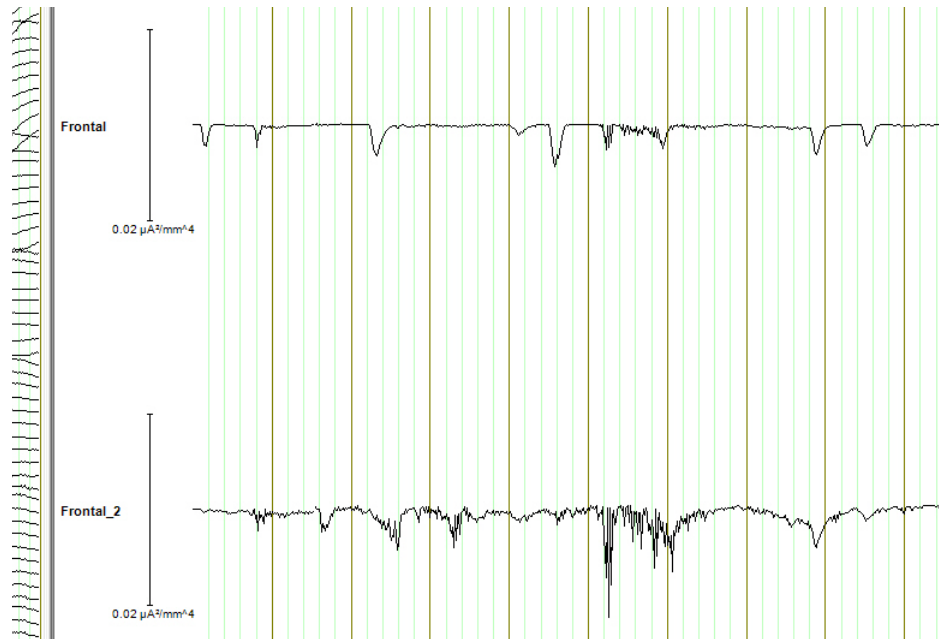
- ▶ The parentheses contain the cross-section coordinates of the current position of the mouse pointer (crosshair). When you move the mouse pointer around the cross-section, the coordinates displayed change accordingly.
- ▶ The value for *Best Match at* specifies the distance from the current mouse position of the next voxel containing stored physiological data.
- ▶ The next three lines indicate the associated anatomical data of the brain areas in the vicinity of the mouse pointer.

Figure 6-27. Display of the mouse pointer in the cross-section and the information field



When the LORETA filter is used, each ROI is represented as a virtual channel (see [Figure 6-28](#)).

Figure 6-28. Virtual channels "Frontal" and "Frontal_2"

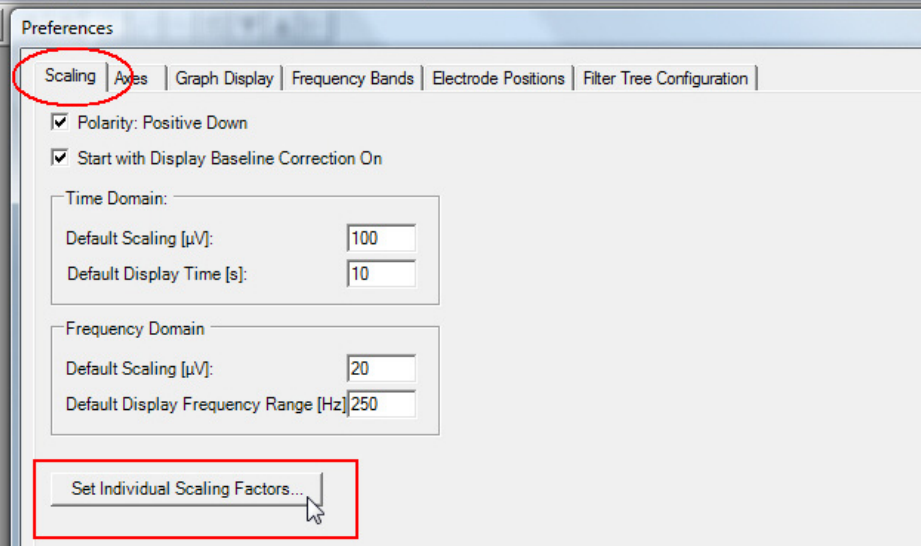


Because very flat data is displayed if the unit $\mu\text{A}^2/\text{mm}^2$ is used, we recommend that you scale the data upwards considerably in the LORETA filter window. In the *Preferences* menu, specify individual scaling for your virtual ROI channels to avoid having to re-scale the data subsequently each time a new connection is established between the Recorder and RecView. When you do this, assign unique names that are not used in the original data set to the ROI channels.

Scaling the virtual ROI channels

To open the dialog box for configuring preferences, choose *Configuration > Preferences...* from the menu. On the *Scaling* tab, click *Set Individual Scaling Factors...* (see [Figure 6-29](#)).

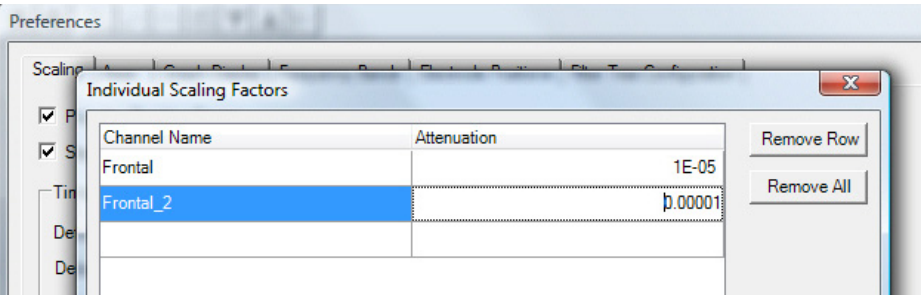
Figure 6-29. Performing individual scaling of the the ROI channels (A)



In the *Individual Scaling Factors* dialog box, specify the required channel name in *Channel Name* and the attenuation factor for this virtual channel in *Attenuation*. As shown in the example (see [Figure 6-30](#)), we recommend that you choose a factor of 0.00001.



Figure 6-30. Performing individual scaling of the ROI channels (B)



6.10 Map

Summary

The Map filter shows the interpolated voltage distribution over the surface of the head. This is done using the electrode positions and the voltages at the individual electrodes. You can apply the Map filter to continuous and segmented time data and to frequency data.

Continuous time data

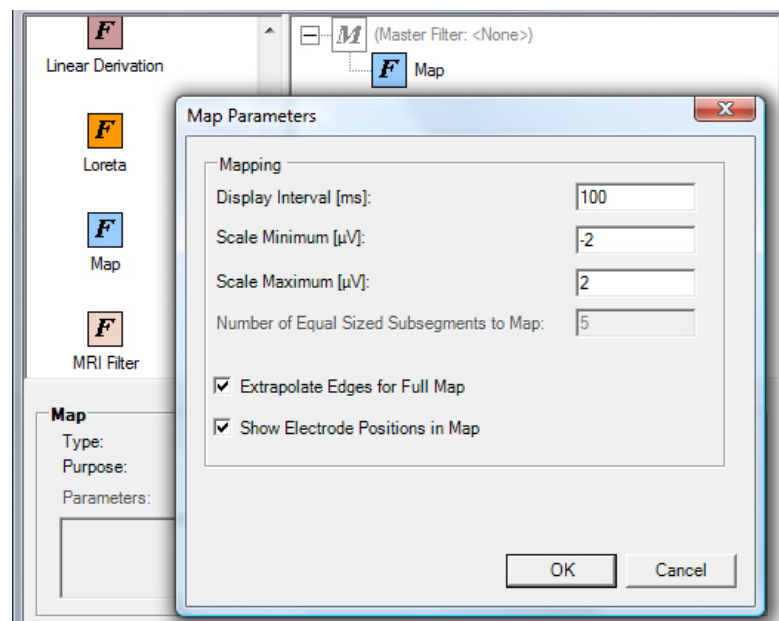
If you apply the Map filter to continuous data, a Map is displayed over a defined time interval.

Enter the interval for which the data points of each channel are averaged before they are used for calculating the Map in the *Display Interval [ms]* text box.

Enter the lower and upper limits of the scale in the *Scale Minimum [μ V]* and *Scale Maximum [μ V]* text boxes.

The *Number of Equal Sized Subsegments to Map* text box is not enabled if you apply the Map filter to continuous time data.

Figure 6-31. Configuring the Map filter for continuous time data



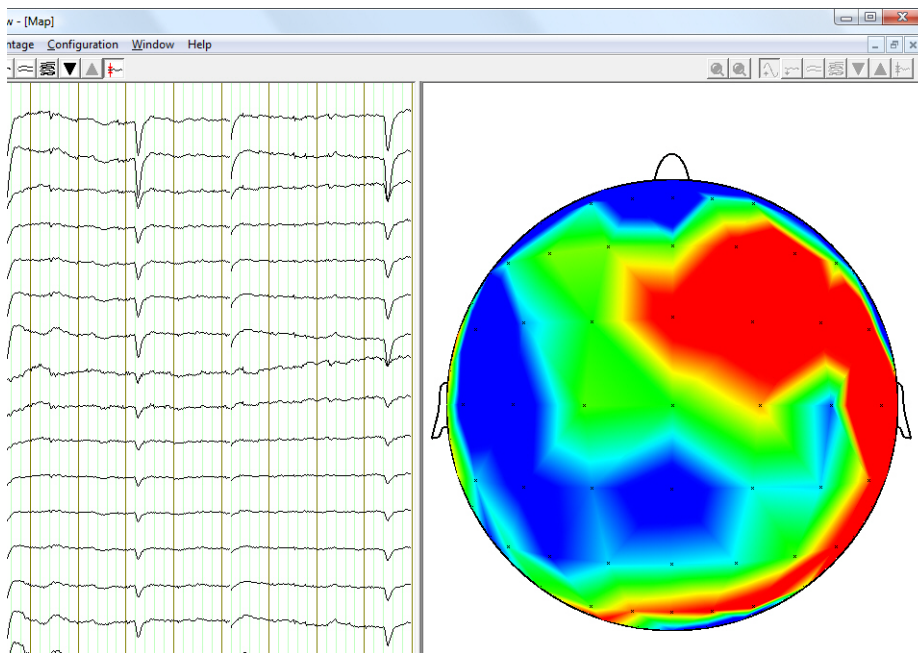
If you check the *Extrapolate Edges for Full Map* box, all the electrodes present in the visible portion of the sphere are shown. The data required for this representation is extrapolated.

If you check the *Show Electrode Positions in Map* box, the electrodes appear as small dots on the Map.

If you are using your own naming conventions for electrodes, you can enter the electrode positions by choosing *Configuration > Preferences ...* from the menu and choosing the *Electrode Positions* tab (see also [Section 4.5 on page 67](#)).



Figure 6-32. Map filter for continuous time data



If you apply the Map filter to segmented data, you are able to show the average voltage distribution of the entire segment or of several partial segments of equal size.

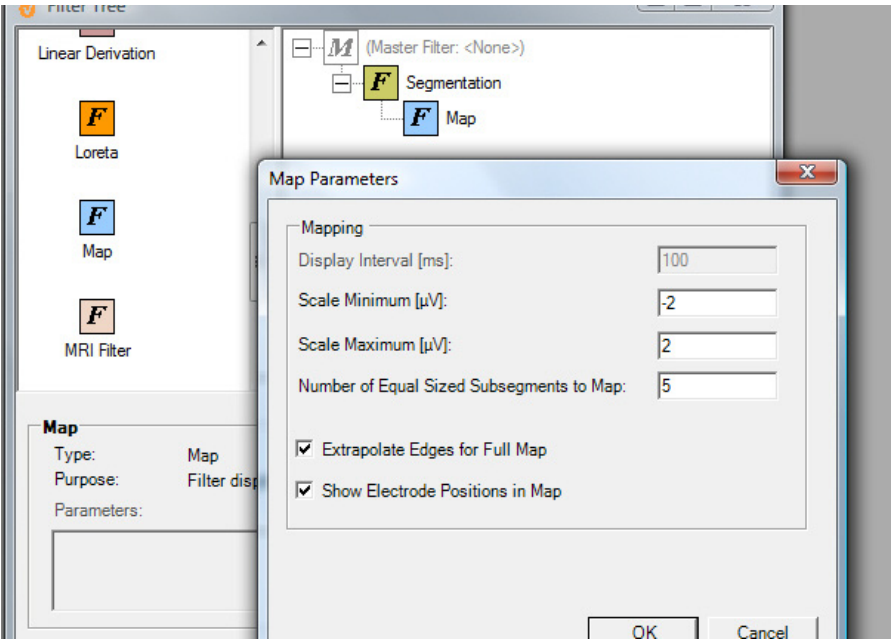
Segmented time data

The settings for segmented time data are the same as those for continuous time data with the following exceptions:

- ▶ The *Display Interval [ms]* text box is not available.
- ▶ In the *Number of Equal Sized Subsegments to Map* text box, you specify the number of partial segments to be displayed per segment. When the partial segments are represented as a Map, the data points for each channel that belong to each partial segment are averaged before they are used for interpolation.

The *Scale Minimum [μV]*, *Scale Maximum [μV]*, *Extrapolate Edges for Full Map* and *Show Electrode Positions in Map* functions are still available (see also the description under [Continuous time data on page 104](#) in this section).

Figure 6-33. Configuring the Map filter for segmented time data




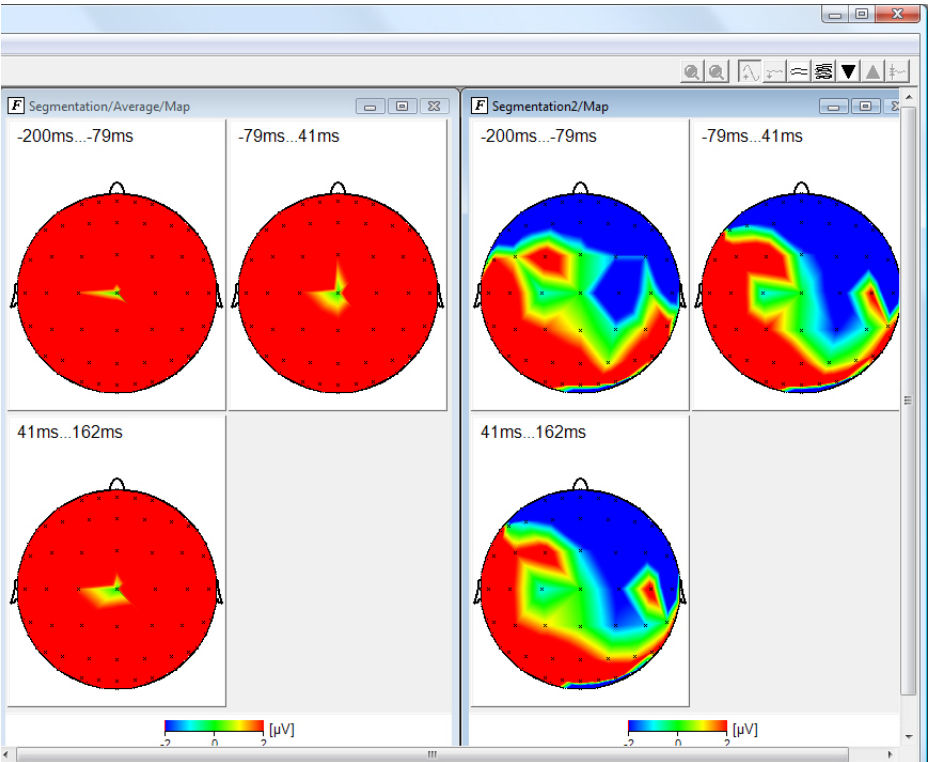
 You are able to append an **Average** filter to the **Segmentation** filter in order to view both the segments and the average as a map.

Figure 6-34. Map filter for segmented and averaged time data



If you apply the Map filter to frequency data, a Map is shown for each frequency band. To change the assignment of colors to the frequency bands, choose *Configuration > Preferences...* from the menu. In the *Preferences* dialog box, select the *Frequency Bands* tab and make the adjustments you require (see also [Section 4.4 on page 66](#)).

In the case of frequency data, you can only set the upper limit of the scale (in the *Scale Minimum* [$\mu\text{V}^2/\text{Hz}$] text box). In addition, the *Extrapolate Edges for Full Map* and *Show Electrode Positions in Map* functions are available (see also the description under [Continuous time data on page 104](#) of this section).

Frequency data

Figure 6-35. Configuring the Map filter for frequency data

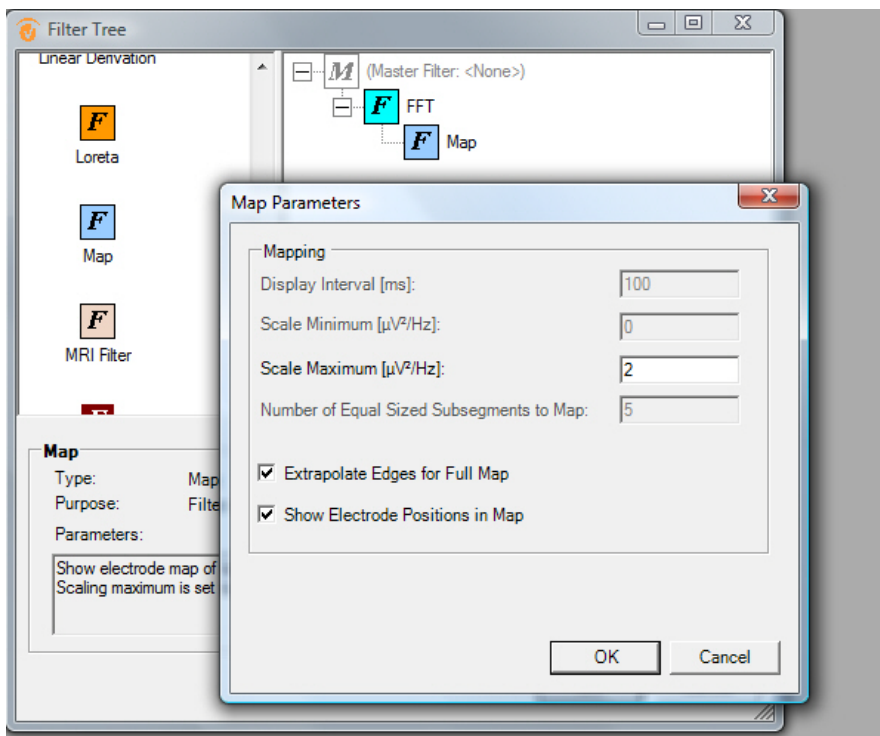
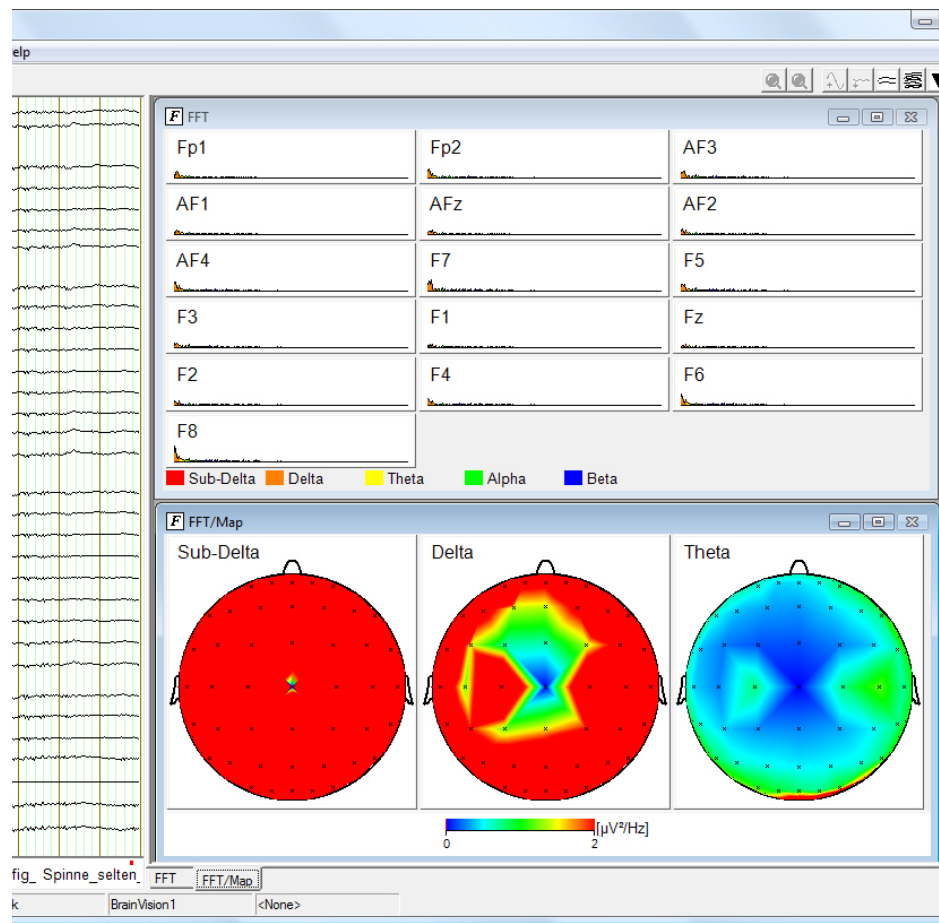


Figure 6-36. Map filter for frequency data



6.11 R-Peak Trigger

The R-Peak Trigger filter is used to detect R-peaks in data sets that are not recorded in the MR scanner.

The filter can only be applied to continuous time data which provide a good ECG signal (R-peaks).

The filter cannot be applied to data which is recorded in the MR scanner because the characteristic curve of the ECG signal is much less well-defined in MR data.


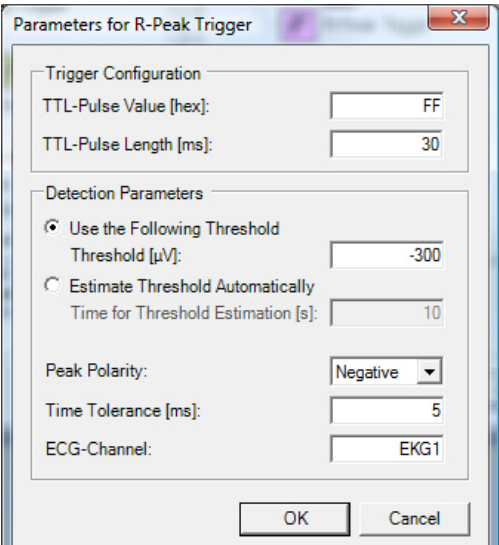
You must possess administrator permissions in order to use LPT port control. Under Windows®, you must also start RecView in Administrator mode even if you are already logged in as administrator at the computer (see also  section 3.4 on [page 50](#)).

Figure 6-37. Parameters dialog box for the R-Peak Trigger filter



The R-Peak Trigger filter detects R-peaks in the EEG. If detection is successful, a marker is set and a trigger is sent in the form of a TTL pulse to the LPT port. The trigger value can be configured in the form of an 8-bit hexadecimal value (0 to FF) which you enter in the cell *TTL-Pulse Value [hex]*. The TTL pulse is reset after the time specified in the text box *TTL-Pulse Length [ms]*; if the box has the value 0 then the pulse is reset immediately.

Pulses that are reset immediately or very quickly (< 20 ms) cannot be displayed in the LPT status output. You should also note that the accuracy of the reset timer depends on the resolution of the Windows® internal system clock. It is therefore not possible to guarantee that timing will be accurate to the nearest millisecond.

Summary

Prerequisites for use



Settings



You specify the threshold that is to be used in *Detection Parameters*:

- If you have set a threshold manually, activate the *Use following Threshold* option and, in the *Threshold [μ V]* text box, enter a voltage whose violation is to trigger the search for an R-peak.



To specify a value manually, you should record the ECG signal and search for suitable values (see [Figure 6-38 on page 111](#) and the accompanying explanation). This manual definition is only suitable for data sets with a very regular ECG signal.

- To perform an automatic search for a suitable threshold value, activate the *Estimate Threshold Automatically* option. The filter uses a variance criterion to decide where to set the threshold. In the text box *Time for Threshold Estimation [s]*, enter the period in seconds during which the filter is to search for a suitable threshold. A sensible value is 10. You should not use any value greater than 15.

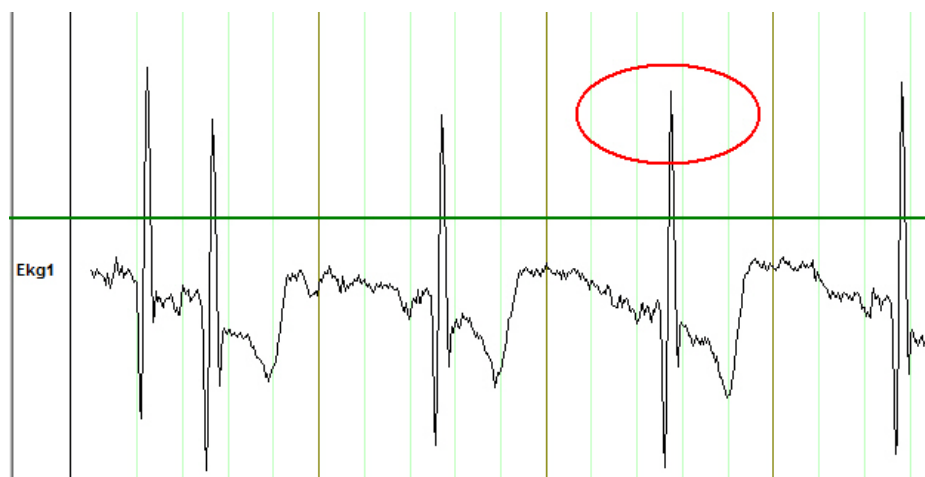
When the period specified in *Time for Threshold Estimation [s]* has elapsed, the threshold value is updated at periodic intervals. This results in a continuous and more stable detection of R-peaks.

You enter the polarity of the R-peaks in the *Peak Polarity* text box. To determine the polarity, view the data briefly in RecView or in the Recorder.

In the *Time Tolerance [ms]* text box, you can enter an interval during which the ECG curve must rise or fall uniformly after reaching a local minimum or maximum in order to make it possible for the minimum or maximum to be recognized as such. Please note that the R-peak marker is set at the time when an R-peak is recognized as such. In the data, it therefore appears offset from the real R-peak by the value specified in *Time Tolerance*. The ideal length of the *Time Tolerance* interval depends on the characteristics of the R-peaks. In [Figure 6-38](#), the R-peak in the ECG curve rises very steeply. After reaching the local minimum, the curve falls steeply again. As a result, a comparatively short time interval should be chosen in this case.

On the basis of the ECG curve characteristics, you should also choose the polarity and – if you are not using automatic detection – a suitable *Threshold* value. In our example (see [Figure 6-38](#)), we select "Negative" for *Peak Polarity* since the upward R-peaks are better defined than the downward ones. For the *Threshold*, we also choose a voltage value which approximates to the straight line drawn in on the graph (this only affects the option *Use following Threshold*).

Figure 6-38. Negative ECG curve (negative polarity) with steep R-peaks



You should enter the channel with the best signal quality among the recorded ECG channels in the *ECG Channel* text box.

Figure 6-39. R-Peak Trigger filter



6.12 Segmentation

Summary

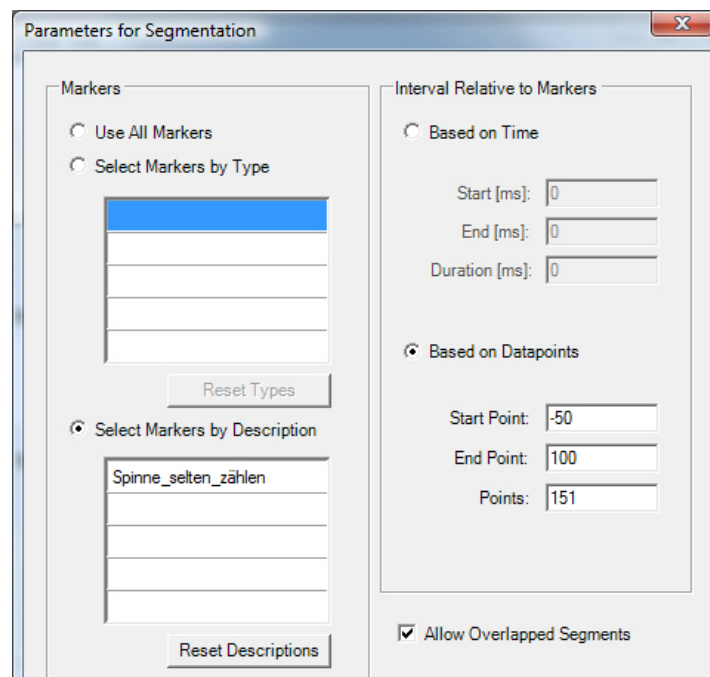
The Segmentation filter allows you to cut out segments of the complete data set of the EEG on the basis of all markers or selected markers.



Note that in contrast to the Analyzer, it is not possible to select the marker names or marker types (e.g. stimulus, reaction, instruction) from a drop-down list, as this information is unknown to the program at the time the parameters are passed. Consequently, you must enter the names and type descriptions manually. The entries are not case-sensitive.

Settings

Figure 6-40. Parameters dialog box for the Segmentation filter



Select the markers to be used in the *Markers* group:

- Select the *Use All Markers* option to use all the markers in the data set.
- To use certain types of marker, select the *Select Markers by Type* option and enter the required types in the relevant list. To use certain marker names, select the *Select Markers by Description* option and enter the required names in the relevant list.

The *Reset Types* and *Reset Descriptions* buttons allow you to reset your entries for the marker types or marker names.

The *Interval Relative to Markers* group allows you to specify the size of the interval to be segmented relative to the markers. You can choose between a time-based specification (*Based on Time*) and a data-point-based specification (*Based on Data Points*).

If you choose to use time-based intervals, you enter the boundaries and duration of the interval in the text boxes *Start [ms]*, *End [ms]* and *Duration [ms]*.

If you choose to use data-point-based intervals, you enter the start and end points and the number of data points in the text boxes *Start Point*, *End Point* and *Points*.

Check the *Allow Overlapped Segments* box to specify that overlapping segments are permitted. If you do not check this box, markers are ignored that are too close to the previous marker.


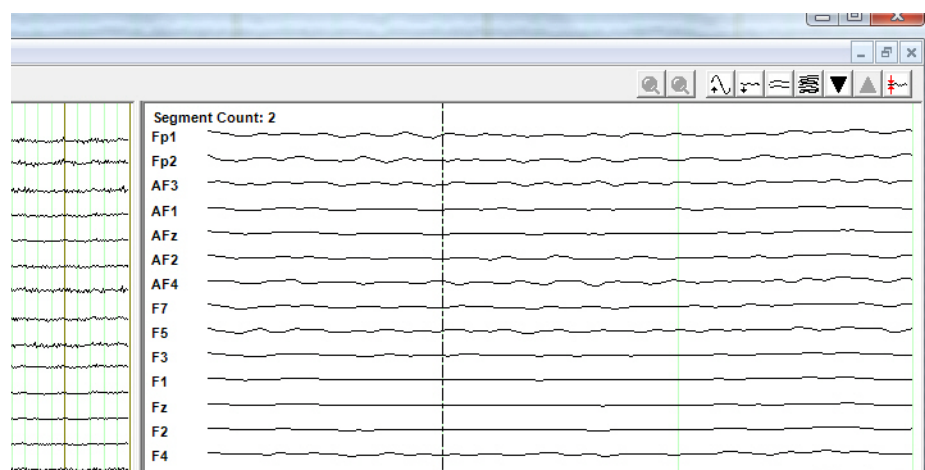
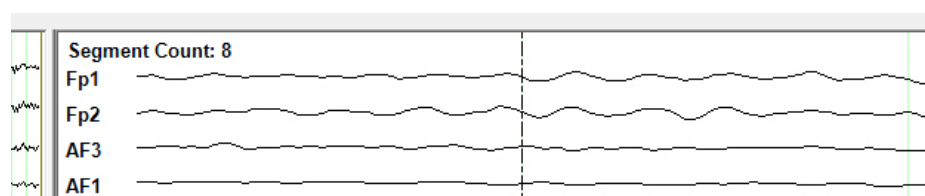
 **Note that in contrast to the Analyzer, the values for the time-based text boxes are not automatically converted to the corresponding number of data points or time points if you change the specification method.**

Figure 6-41. Segmentation filter



The number specified in *Segment Count* (in the top left of the filter window) specifies what segment is currently being displayed. The "Time Zero" marker (dashed horizontal line) is also displayed.

Figure 6-42. Display of the segment number and the "Time Zero" marker



A segment that is detected is displayed until the next segment can be displayed in its entirety. This means that only the current segment is ever displayed. ●



Chapter 7 Optional filters

7.1 MRI filter

If EEG data is recorded in an MR scanner, the signals are subject to considerable interference.

In this context, we distinguish between two primary categories of artifacts:

- 1 **Scanner artifact.** A scanner artifact is caused by the alternating magnetic field during the scanning process.
- 2 **Cardioballistic artifact.** A cardioballistic artifact is caused by the strong static magnetic field combined with movements of the electrodes in time with the heart frequency of the test subject.

The MRI artifact filter allows you to considerably reduce artifacts belonging to the first category. The EEG signals then become clearly visible again and you can now identify saturated channels or channels subject to other interference.

Correction is carried out on the basis of averaging. In principle, recurring intervals are averaged in phase with artifact generation. This causes the randomly distributed EEG signals to be dropped from the averaged curve, ideally leaving only the external influence of the scanner. This is now used as a template and is subtracted from the individual sections in a second step. What is left is the useful signal.

The MRI artifact filter is simple to use. However, the Time of Repetition (TR), i.e. the time between two consecutive gradients, must be exactly known to an accuracy of one sampling interval.

Template drift compensation

Template drift is the temporal offset of the scanner TR relative to an integer multiple of the sampling interval of the EEG amplifier. This happens either because the TR has not been matched to the sampling rate of the amplifier or because the amplifier and the scanner have a slightly different interpretation of the exact length of 3000 ms, for example. It is, for instance, possible that the scanner in reality requires 3000.025 ms to complete a TR cycle. In our example, this causes the data points of the subsequent TR to be measured 0.025 ms too early. Thus, the measured values for the artifact in the data points of the subsequent TR no longer exactly match those which are stored in the template. This has a negative impact on the quality of correction.

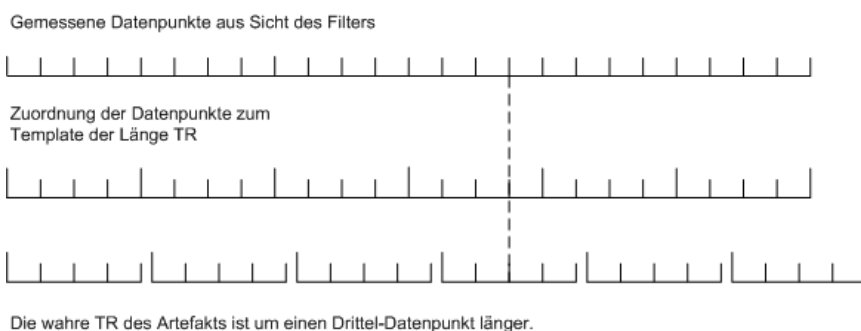
Because the difference between the true TR of the scanner and the nominal TR of the filter is constant for the whole duration of the measurement, each of these drifts adds up and, over time, the quality of the template is destroyed.

It is not possible to specify the TR with an accuracy greater than one sampling interval, as the algorithm works with data points separated by one sampling interval. This means that even if the TR is specified as accurately as possible, it is possible for an offset to arise.

Summary

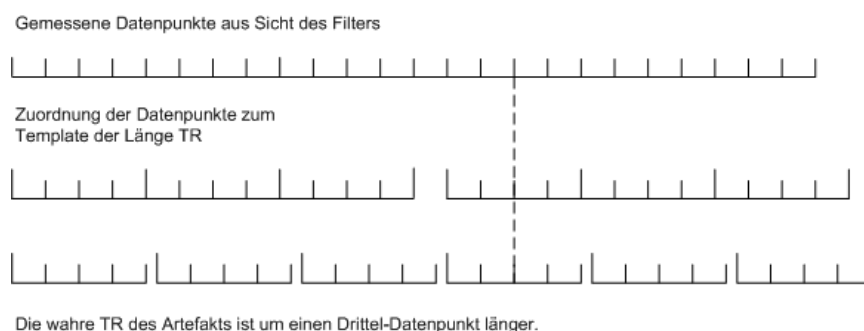
Initial methodological considerations

The following diagram shows an example of template drift. The true TR of the scanner is one third of a data point longer than the nominal TR. The top part of the diagram shows the times at which data points are measured and how they are assigned to the template. The bottom part shows the times at which the artifact repeats in reality. The value of the artifact at the time at which the fourth data point of the fourth TR was measured (highlighted in the diagram) is actually the value of the artifact at the time at which the third data point of the first TR was measured. If this data point is included in the templates, without compensating for the template drift, this results in a discrepancy.



The MRI artifact filter is able to determine the template drift and also calculate which point of the template a measured data point should be assigned to. If the template drift exceeds the value of one sampling interval, then the start of the artifact is shifted by one or more data points. However, interference still occurs because some TR sections are offset by a fraction of the sampling interval with respect to the template.

The diagram shows how the filter compensates for the template drift in the fourth TR by shifting the template in relation to the measured data points.

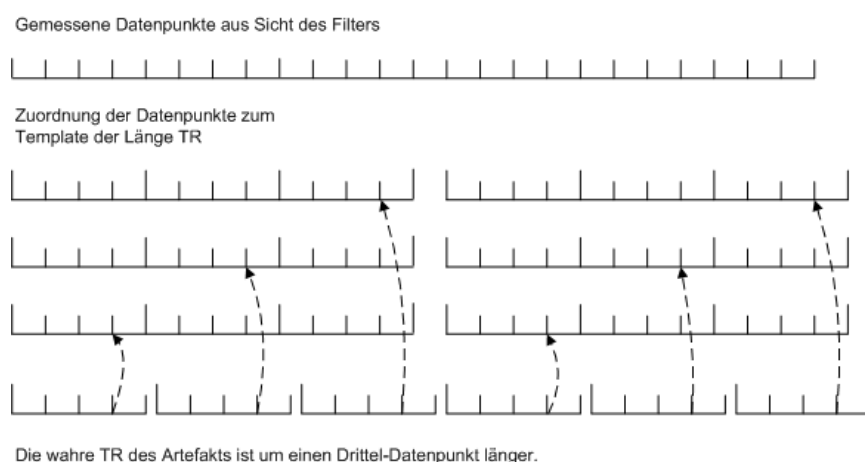


In order to improve the quality of the correction still further, the filter actually uses several templates. The template drift of the first point is determined for every section of the TR, and only those data points from TR sections in which the template drift has a similar value are included in each template. The individual templates can be seen as being "offset by a given fraction of the sampling interval".

If several templates are used, the number of TR sections added to each template after a specified period is reduced proportionally. The more TR sections a template contains, the more

meaningful the data will be that is corrected using this template. For this reason, the number of templates used should not be too large; three is a suitable value.

The following diagram shows the filter with three templates and indicates which data point is added to which template. Depending on the value by which the first point of a TR section is offset in relation to the TR of the scanner, the data points are included in different templates. The top template contains data points with the template drift of $2/3$ of a sampling interval and the bottom template contains points with no template drift.



Because the difference between the true and nominal TR is not generally an exact fraction of the sampling interval, it cannot be assumed that this method can completely compensate for discrepancies arising from template drift. Nevertheless, the quality of the correction is improved.

Template drift detection

The MRI artifact filter uses a procedure to automatically determine the template drift from the data. This is necessary if the user does not know the exact value of the template drift. Template drift detection works reliably if the TR is known to an accuracy of one sampling interval. Scanner timing discrepancies greater than one sampling interval can be compensated for by setting an adjusted TR.

The template drift is determined by observing the marked, narrow peaks in the data. A peak of this type cannot come from the normal EEG signal, as this does not generally have gradients of a comparable magnitude.

By comparing the positions of the peaks of different TR sections, it is possible to determine the template drift between the sections in real-time, even if a TR section has only been partially read.

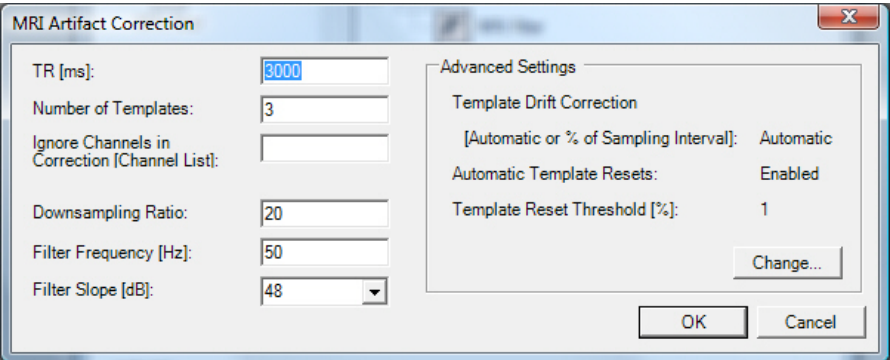
This method is particularly suitable for comparing consecutive TR sections. Because template drift is the result of a constant discrepancy between the scanner and the amplifier, it

remains constant between two consecutive TR sections. As a result, the average can be drawn across a large number of individual measurements of the template drift, giving a value which is not subject to temporary interference in the data. The template drift with relation to the measured artifact can be determined subsequently for a TR section which has already been read. This is achieved by adding the section-to-section drift to the known drift of the previous section and also by directly calculating the template drift in relation to the first TR section measured. Combining these values permits accurate determination of the template drift.

In order to assign the measurement data of the new TR section to a suitable template from the very start, the template drift of the section must be known before the data is measured. However, at this time the template drift of the TR section which has just been processed is known, as is the template drift between two consecutive sections. The template drift of the new section can be predicted on the basis of these values.

Basic settings of the MRI artifact filter

Figure 7-1. Parameter dialog box for the MRI artifact filter



The *TR [ms]* text box specifies the time of repetition.



In the *Number of Templates* text box, you can specify how many templates the filter establishes in order to improve correction quality in the event of template drift. This value should be 1 if there is no template drift. If there is template drift, a value greater than 1 can improve the correction quality. However, because each TR interval is only incorporated in one of these templates, a higher value here means that it takes longer until the templates become meaningful. A sensible value is 3.

In the *Ignore Channels in Correction* text box, you can specify a comma-separated list of channel names which are not to be corrected by the filter.

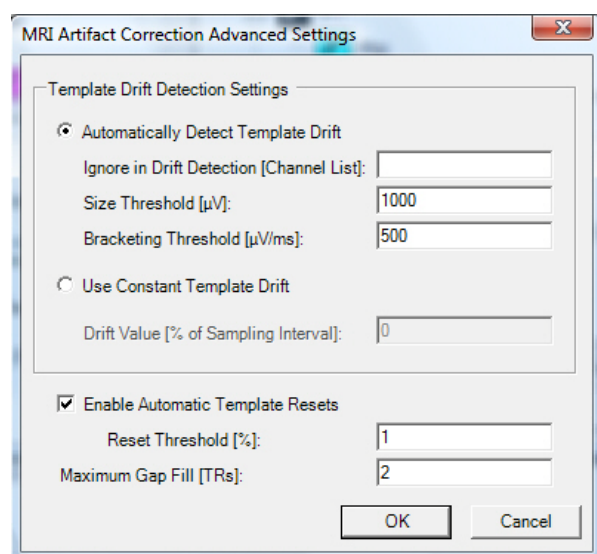
You are also able to reduce the sampling rate of the corrected data after the actual scanner artifact correction has taken place in order to increase the speed with which the subsequent nodes in the filter tree can work. *Downsampling Ratio* is the factor by which the sampling rate is reduced. For example, a value of 20 means that a 5000 Hz signal is converted to a 250 Hz signal.

The reduced sampling rate data is fed through a Butterworth low-pass filter in order to remove remaining noise. The *Filter Frequency* and *Filter Slope* text boxes specify the filter frequency and the slope of the characteristic curve of the filter.

Advanced settings which only rarely need to be changed are available if you click the *Change...* button.

Figure 7-2. Advanced configuration of the MRI artifact filter

Advanced settings



If the TR has been specified correctly, the default settings for automatic template drift detection are as a rule suitable for processing the data reliably. However, it is possible that modifications need to be made for particular sets of measurement data in order to adjust the method to the particular conditions that apply to this data.

Select the *Automatically Detect Template Drift* option to use automatic template drift detection.

In the *Ignore in Drift Detection [Channel List]* text box, you can specify a list of channel names which are not to be used for drift correction. The list is separated by commas. This allows you to prevent individual channels with extremely atypical data from negatively impacting the template drift detection process.

The *Size Threshold [µV]* parameter specifies the minimum size of the peaks which are used for template drift detection.

The *Bracketing Threshold [µV/ms]* text box specifies the gradient that delineates the peaks from the neighboring data points. Minima are only used if this gradient is exceeded. It can be necessary to reduce the values in these boxes if the overall strength of the artifacts or the typical artifact gradients are lower than the default values.




We recommend that you always use automatic template drift detection and adjust your settings accordingly. Even if the drift is known in advance, the automatic detection facility can be useful in order to compensate for discrepancies that occur over time.

Select the *Use Constant Template Drift* option to deactivate automatic template drift detection. This only makes sense if drift correction fails on the measured data or if the template drift is known in advance with a high degree of accuracy.

If automatic template drift detection is deactivated, you can specify a constant drift between two consecutive TR sections in the *Drift Value [% of Sampling Interval]* text box. The drift is specified as a percentage (negative or positive value) of a sampling interval. A value of -30 would mean that the nominal TR of the filter is 30/100 of a sampling interval shorter than the actual TR of the scanner.

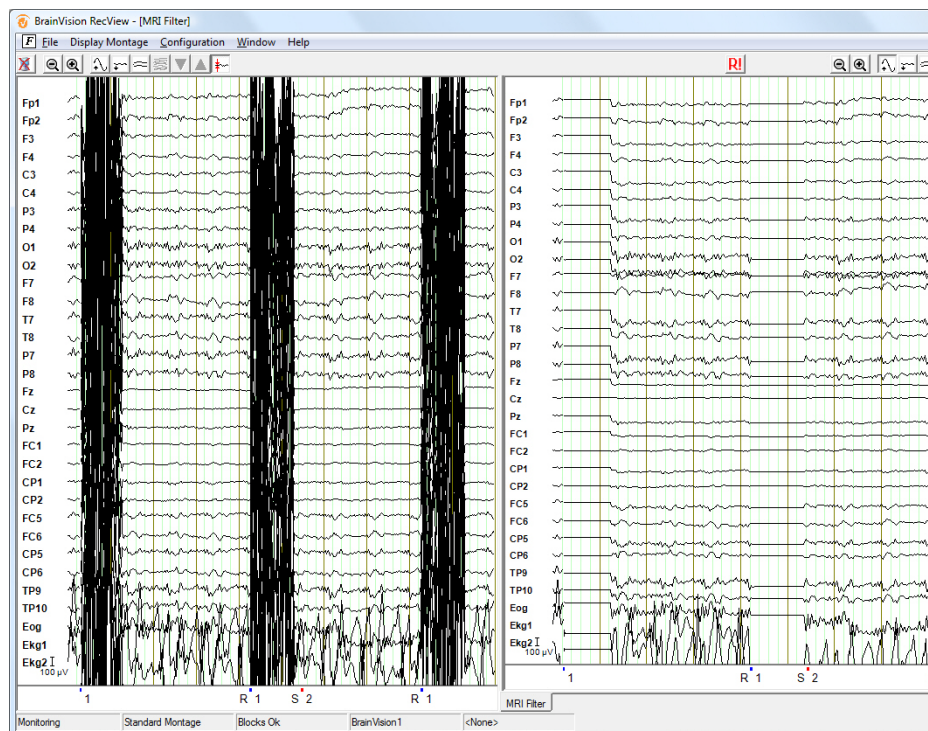


If you check the *Enable Automatic Template Resets* box, the filter automatically rebuilds its templates if changes in the artifact cause the correction quality to drop below a particular value. You should deactivate this automatic facility if the filter rebuilds its templates when this is not required. You can rebuild the templates at any time by clicking the *Reset Averaging Templates*  button in the toolbar.

The correction quality is determined on the basis of the proportion of large gradients remaining in the corrected data. If there are a large number of high gradients in the corrected data, this is an indication that the artifact has not been removed reliably. It is however possible that some large gradients remain in data which has nevertheless been corrected sufficiently well. The *Reset Threshold [%]* text box allows you to specify the percentage of data which is permitted to contain large gradients.

If the filter encounters gaps in the measurement data, this is an indication of temporary overloading of the computer on which you are running the program. The filter will attempt to bridge a gap of this type to avoid aborting the current correction. The value in the *Maximum Gap Fill [TRs]* text box specifies the maximum number of TRs that are bridged.

Figure 7-3. MRI artifact filter



7.2 Pulse-artifact filter

The Pulse-artifact filter detects the heartbeats, i.e. the R-peaks on a specified ECG channel, and initiates a correction process for the EEG channels for every detected pulse period. The functionality of the filter falls into the following phases:

Downsampling

Since it is necessary for the filter to process a large quantity of input data in a relatively small time, its performance improves inversely to the sampling rate of the input data. For this reason, the filter has an optional preprocessing stage that allows you to reduce the sampling rate of the input data.

The training phase

In order to detect the position of the R-peak on the ECG channel, the Pulse-artifact filter must find and store a pulse pattern with a distinct R-peak. This is done within a fixed period when the filter first starts to be used. This period is referred to as the training phase in this document. The default value for the duration of the training phase is 15 s. You can change this

Summary

duration. During the training phase, the pulse is neither marked nor corrected. If no pulse pattern is detected after the planned training phase, the training phase is repeated with reference to the following sections until a pulse pattern is successfully detected.

Pulse detection

After the training phase has been completed, the actual pulse detection process starts. This involves a combined procedure using correlation and amplitude criteria that compares the period of the pulse pattern with the current period. If the correlation lies above a previously defined limit and the amplitude lies within previously defined limits, an R-peak marker is set at the position on the time axis at which the R-peak was set in the pulse pattern.

Correction

The pulse artifacts are corrected simultaneously on all EEG channels that you have not excluded from correction. During this process, a period defined by entering a time prior to the R-peak and a time after the R-peak is corrected. In order to correct this period, a template is used which is derived by averaging the previous pulse periods and then selecting this value from the current data period.

Figure 7-4. Parameters dialog box for the Pulse-artifact filter

Settings

Pulse-artifact Filter Parameters

Detection Parameters

Pulse Reference Channel:

Look for a Model Pulse [s]:

Minimal Pulse Period (ms):

☒ Mark Pulse Peaks.

Minimal Correlation:

Minimal Amplitude:

Maximal Amplitude:

Suppress Marker Display

☒ Hide Markers with Description(s):

Correction Parameters

Number Pulses in Average:

Correction before Peak (ms):

Correction after Peak (ms):

Excluded from Correction:

Downsampling before Correction

☒ Do Downsampling.

☒ Downsampling to 250 Hz.

Downsampling with a Factor of:

You can configure the pulse detection parameters in *Detection Parameters*:

- Pulse Reference Channel:** ECG reference channel. RecView checks whether a valid channel has been specified and outputs an error message if the channel is not present. The error message also indicates which channel will be used instead of the missing channel, namely the last channel in the workspace's channel table.
- Look for a Model Pulse (s):** Length of the training phase
- Minimal Pulse Period (ms):** Minimum distance between two R-peaks
- Mark Pulse Peaks (checkbox):** Specifies that detected R-peaks are to be marked with R markers
- Minimal Correlation:** Contains the correlation threshold (default: 0.6)
- Minimal Amplitude:** Contains the lower amplitude threshold (default: 0.6).
- Maximal Amplitude:** Contains the upper amplitude threshold (default: 1.2).

Correction Parameters Contains the correction parameters:

- Number Pulses in Average:** Number of preceding pulse beats that are to be taken into account for the currently used correction template (default: 10).
- Correction Before Peak (ms):** Distance between the start of the correction interval and the R-peak.
- Correction After Peak (ms):** Distance between the R-peak and the end of the correction interval.

Excluded from Correction: Channels that are not to be corrected. Enter a comma between the channel names. It is usual to exclude the ECG channels from correction to make it easier to identify whether the R-peaks are set correctly or whether the detection or correction parameters need to be adjusted.

Under *Downsampling before Correction*, you can use

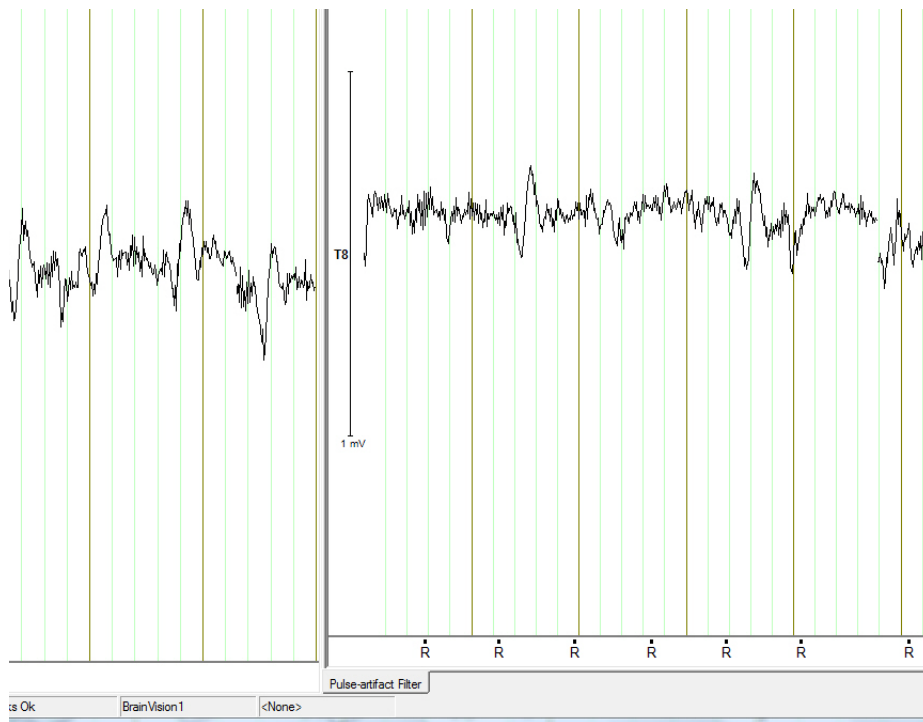
Do Downsampling: To specify whether downsampling is to be performed as a preparatory step or not. If you check this box then the *Downsampling to 250 Hz* checkbox is also activated.

Downsampling to 250 Hz: If you check this box then the sampling rate is automatically reduced to 4 ms (250 Hz). Alternatively, enter the downsampling factor you require as an integer in the *Downsampling with a Factor of* text box.

You can use *Suppress Marker Display* to hide markers:

Hide Markers With Description(s): Check this box if you want to hide specific markers in RecView. Enter the marker name in the *Suppress Marker Display* text box (e.g. R128). If you enter more than one marker name, separate the names with commas. Any markers you hide in this way are not removed but are simply no longer included in the display. As a result, you can continue to use these markers, for example when performing subsequent segmentation.

Figure 7-5. R-peak marker and correction of a channel




Downsampling is mandatory for inputs of 5000 Hz and more if the filter is to function efficiently. We also recommend automatic downsampling to 250 Hz in this case.

 **Notes on use**

If incorrect R-peaks are to be marked, enter a higher value in the *Minimal Pulse Period (ms)* text box. If this does not result in any improvement, increase the value in the *Minimal Correlation* text box by one tenth (e.g. from 0.7 to 0.8) or reduce the value range of the acceptable amplitude correlation (e.g. from 0.6 to 1.2 to 0.7 to 1.1, etc.).

If R-peaks are skipped, reduce the value in the *Minimal Pulse Period (ms)* text box. If this does not result in any improvement, increase the value in the *Minimal Correlation* text box by one tenth (e.g. from 0.7 to 0.6) or reduce the value range of the acceptable amplitude correlation (e.g. from 0.6 to 1.2 to 0.5 to 1.3).

If the R-peaks are identified correctly, but the artifacts are not corrected, the selected correction interval is too coarse. The Pulse-artifact filter does not permit any overlapping correction periods. This means that the sum of the values *Correction before Peak* and *Correction after Peak* must be smaller than the minimum actual period between two successive R-peaks.

Because the pulse artifact template is not continuously rebuilt despite the fact that the resting pulse of the test subject may change during measurement, it could be helpful to reset the template. You can rebuild the templates at any time by clicking the *Reset Template in Pulse-artifact Filter*  button in the toolbar.



Chapter 8 Programming user-defined filters

Chapter 8 contains programming instructions for developing user-defined filters. *Please note that Brain Products is unable to provide any support with respect to implementation details.* We shall supply descriptions and examples of filter implementations.

8.1 Overview

You can extend RecView to include filters you have programmed yourself. Filters are made up of program libraries that use the Microsoft .NET runtime environment.

The following requirements apply if you wish to develop your own filters:

- ▶ A general knowledge of programming.
- ▶ Knowledge of a .NET programming language; our examples use C#.
- ▶ Understanding of the terms "interface", "class" and "attribute" in the context of .NET.
- ▶ A development environment for .NET components for .NET Version 4.0. Our sample projects were developed using Microsoft Visual Studio 2010.

Copy the compiled filter DLL into the program folder so that RecView is able to find it.

You will find help and examples in the folder *RecView\Filter Development* on the BrainVision Application Suite USB.

A filter is always implemented in the form of a collection of interfaces within a class. A special filter attribute describes the filter for RecView.

The interface and structure descriptions and the filter attribute class are contained in the file *RecorderInterfaces.dll*, which is located in the program folder. This must be referenced in all filter projects.

You will find a precise description of the structure of the interfaces, classes and attributes in the help file *RecViewInterfaces.chm* located in the subfolder *Filter Development*.

For notes on debugging user-defined filters using Visual Studio 2010 Express C#, see the file *Debugging RecView Filters with Visual Studio 2010 Express Edition C#.pdf* in the *Filter Development* subfolder.

8.2 Interfaces

The following interfaces can or must be implemented:

`IDataIn` (mandatory)

This interface is mandatory. It receives the data, setup information and status information from the previous filter.

`IDataOut` (optional)

If the results of the filter are to be passed to RecView so that they can be viewed or distributed to further filters, you must implement this interface. It establishes the connection between the filter and another `IDataIn` interface supplied by RecView.

`IFilterParameters` (optional)

This interface allows you to enter parameters. Parameters are stored in text format in the workspace file by RecView. The interface receives or supplies the text and displays a user dialog box on request.

`ISimpleView` (optional)

This interface is used for simple visualization of data. The data is displayed in a window outside the RecView frame using the methods of the interface. If you have implemented this interface, you cannot implement the `IDataOut` interface. This means that the filter represents an endpoint in the filter tree.

`IDataView` (optional)

This interface is also used for visualization, but has a far more complex structure. It integrates visualization into RecView itself. It is also able to handle the existing buttons for scaling and setting the time etc. Because it is so complex, we shall not deal with the `IDataView` interface here. We recommend that you use `ISimpleView` instead.

`IUITools` (optional, "UI" = "User Interface")

This allows you to provide users with buttons on a toolbar in order to perform corrections interactively, for instance. You can also output information in one of the fields of the status bar.

The following paragraphs list some examples of filters using different interface combinations:

- ▶ The frequency filter uses the interfaces `IDataIn`, `IDataOut` and `IFilterParameters`. If this filter only allowed fixed frequencies, it would not be necessary to use the `IFilterParameters` interface.
- ▶ The map implements `IDataIn`, `IDataOut`, `IFilterParameters` and `IDataView`. `IDataView` is implemented because `RecView` is not able to represent topographical data implicitly.
- ▶ The MRI artifact filter implements the interfaces `IDataIn`, `IDataOut`, `IFilterParameters` and `IUITools`. `IUITools` is used to allow the user to reset the template used while the data is being displayed.
- ▶ A simple biofeedback filter can be implemented using a combination of `IDataIn` and `ISimpleView`. You will find an example of this on the BrainVision Application Suite USB in the folder *Filter Development\Samples\SimpleViewExampleFilter* below the `RecView` folder.
- ▶ You can also develop a filter which only implements `IDataIn`. The data can then, for instance, be exported over the serial interface. You could also write the data to hard disk.



If you want to use the examples in debug mode, you will find the relevant information in the file **Debugging RecView Filters with Visual Studio 2010 Express Edition C#.pdf** in the **Filter Development** subfolder on the **BrainVision Application Suite USB**.

8.3 Programming examples

The sample projects are located in the *RecView\Filter Development\Samples* folder on the BrainVision Application Suite USB.

Compiled versions of the projects are located on the USB in the folder *RecView\Filter Development\Samples\Binaries*. If you wish to test these projects, copy them to the program folder.

Sample filter 1

We shall look at the filter in the subfolder *RecView\Filter Development\Samples\FlatChannelFilter* in detail below. While you are reading the following explanations, you should have the help file *RecorderInterfaces.chm* open.

It is usually possible to compile the project without difficulty using Microsoft® Visual Studio 2010. You may have to adjust the reference to *RecViewInterfaces.dll* in the project, since it could reference an invalid folder. Do this by deleting the reference and then creating it again, specifying the correct path. As we have already said, the file is located in the RecView program folder.

The job of this filter is to allow a channel selected by the user to be deactivated, i.e. all the values on the channel are set to 0.

Here, we shall look at the file *TestFilter.cs* containing the class `TestFilter`.

The class contains one filter attribute. Without this attribute, RecView would ignore the class. The first element of the attribute (`id`) is a GUID. This is a 128-bit value which uniquely identifies the filter. If RecView finds several filters with the same GUID, only the first of these is loaded. You should therefore generate a genuine GUID in Visual Studio, for instance by choosing *Tools > Create Guid*.

The `displayName` parameter defines the text which appears in menus etc. `Description` is a short help text.

The next four parameters describe which input and output data types and which segmentation types are permitted. In our example, we have the type `DataTypes.TimeDomain` for both input and output data type. This means that the filter expects and returns data from the time domain. The permitted input segmentation types are described by `SegmentationTypes.Continuous | SegmentationTypes.Segmented`. This means that the filter can use both continuous and segmented data. The output segmentation type is identified by the designation `SegmentationTypes.ByParent`. This segmentation type indicates to the program that the output segmentation type is determined by the input type, i.e. the output type of the upstream filter. The same logic must be used if you use a filter with a multi-value input and output data type. You will find a list of available data types and segmentation types with descriptions in the file *RecViewInterfaces.chm*.

The following parameters are reserved and must be set to 0. The last (and optional) filter attribute indicates whether the filter directly addresses hardware components. In this case, it does not matter whether you omit the attribute or set it to the value `HWAccess.None`. If you want your filter to access the parallel port, you should set the value to `HWAccess.LPTPort`. If RecView detects a filter whose hardware access attribute has this value then the RecView LPT port status display becomes visible.

The `IDataOut` interface receives an `IDataIn` interface via the `Connect()` method. This interface is stored in the private variable `dataReceiver`. The `Connect()` method is always called before any other method of the `IDataIn` interface.

The methods of the `IDataIn` interface forward the parameters passed to them to `dataReceiver`. Depending on the task involved, these parameters may be modified or unmodified. In our example, the setup is modified in `IDataIn.Start()` in order to change the name of the channel whose values are to be set to 0. The modified copy is then forwarded to `dataReceiver`. `IDataIn.AddData()` also selects the same procedure, namely modification of a copy, for the received data.

Never modify the original data if this was passed in the form of an object reference. Any change might affect other filters.



The `IFilterParameters` interface receives and returns a text via the `Parameters` property. This text can easily be converted to and from parameter variables using the `XmlSerializer` class of .NET.

`IFilterParameters.EditParameters()` opens a dialog box where the user can enter parameter variables.

Sample filter 2

Another example filter, the `SimpleViewExampleFilter` already mentioned, displays a "smiley" whose smile depends on the proportion of alpha waves in the total spectrum of the EEG. The proportion of alpha waves is also displayed in numeric form on the top left of the output window.

This filter only accepts complex frequency data as supplied by FFT. This means that frequency analysis within the filter is extremely simplified, because the FFT filter has already converted the data to frequency data.

In this case, the `IDataIn` interface is implemented as well as the `ISimpleView` interface. The window in which the data is displayed is not bound to the RecView interface, but can be moved freely. This allows you to use the entire screen for biofeedback output.

Sample filter 3

The final example – `ExampleParallelPortAccess` – illustrates how the parallel port can be controlled using a filter which you define yourself. Your filter does not need to implement any interface in order to control the parallel port.

Instead, you simply need to use the methods of the class `ParPortAccess` which is present in the file *RecViewInterfaces.dll*. Use the public methods

```
bool Init(InfoProvider info, out string sMessage),
ParportAccess.Write(byte signal) and
byte ParPortAccess.Read() as described in the example.
```

Note the use of a constructor with `Infoprovider-Delegate` as parameter. If you want to make use of the possibility of monitoring the operation of your filter in the RecView LPT port status display, add the entry `HWAccess.LPTPort` to your filter attributes as in the example. Please note that you need administrator permissions in order to use this type of filter.





Appendix A Electrode coordinate system

The electrode coordinate system used in RecView is explained below. This coordinate system is used wherever electrode positions are needed, e.g. in mapping.

The axis system is defined in such a way that the z-axis runs through the vertex. The x-axis points to the right, and the y-axis to the front.

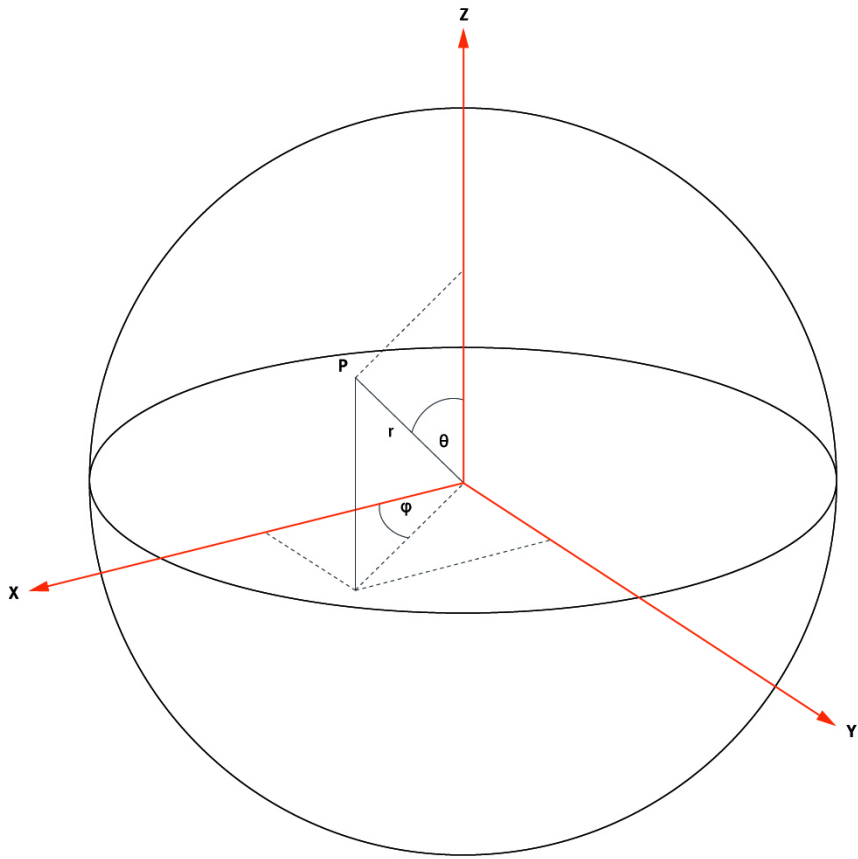
Spherical coordinates are used to specify a point on the head. A set of coordinates consists of the three variables r , θ and ϕ (radius, theta and phi).

The radius r specifies how far the point is away from the center of the coordinate system. It is stated in millimeters. The only exceptions are $r = 0$ and $r = 1$. $r = 0$ signifies an invalid position, for instance when the position of an electrode is not known, $r = 1$ means that a standard diameter has been chosen for the radius. This can be used when the surface of the head is approximated by the surface of a sphere.

ϕ specifies the angle between the x-axis and the projection of the line connecting the point and the coordinate origin on the xy plane. $\phi > 0$ applies to the front right and rear left quarter of the sphere and $\phi < 0$ to the front left and rear right.

θ is the angle between the z-axis and the line connecting the point and coordinate origin. In the left hemisphere, $\theta < 0$. In the right hemisphere, $\theta > 0$.

Figure A-1. Coordinate system for electrodes





Appendix B Installing the RecView license from the Brain Products web site

RecView can only be used if you have purchased a sub-license for the Recorder. If you purchased sub-licenses at the same time as you purchased the Recorder, the sub-license file is included on a USB data carrier supplied with the software. All sub-licenses that you have purchased can be downloaded from the Brain Products web site.

Appendix C describes how to download and install sub-licenses that you purchase subsequently.

To activate the downloading of sub-licenses, your USB license dongle must first be registered. To do this, choose *Downloads & Support* > *Product Registration* at www.brainproducts.com.

To register your dongle, enter the external and internal serial ID of your dongle, your name, university and email address in the product registration form (see [Figure B-1](#)). The external serial ID is printed on your dongle. You can find out the internal serial ID using the *Serial ID Check Program* available on the web site. Further information is available at www.brainproducts.com/productreg.php. Once your registration has been processed, you will receive a confirmation mail.

Downloading sub-license files

Figure B-1. Data entry form for product registration

After you have received the confirmation mail, you can log in (see [Figure B-2](#)) to download your files by proceeding to the Login page. Use the login data you received by mail.

Figure B-2. Login form

Login

Home

About Brain Products

Projects & References

Workshops & Events

Products & Applications

Distributors

Downloads & Support

Order & Return Shipment

Login

Username

URA10125

Password

•••••

Login

If you do not have a login yet, please register [here](#). If your login does:

Please note that cookies have to be accepted to login.

Now you can select and download the sub-license file *License File for Analyzer 1 and/or Recorder* from the download area under *Downloads & Support > Downloads* (see [Figure B-3](#)).

Figure B-3. Download area for sub-license files

Events

» [Register your product here](#)

BrainVision Analyzer 1 >

BrainVision Analyzer 2 >

BrainVision CapTrak >

BrainVision PyCorder >

BrainVision Recorder >

BrainVision RecView >

Dongle Driver >

Electrode Caps (Montages, Workspaces, Electrode Coordinate Files) & actiCAP ControlSoftware >

OpenViBE for Brain Products >

Operating Instructions & User Manuals >

Software Development Kits (SDKs) >

Tools (File Converter, TriggerBox, etc.) >

Tutorials & SetUp Poster >

Brain Products License Files

Our main software products BrainVision Recorder and BrainVision Analyzer are protected by USB keys.

For the newer Sentinel HASP dongle technology (since 2013) Add-on licenses are stored directly on the USB-key so that **no additional license file is required**.

For older dongles, which used a different technology, the licenses for additional functionality have to be provided in so-called "sub-licenses", which have to be installed using a BrainVision license file. The license file has to be executed on every local installation of the software following the instructions provided [here](#).

To check whether these are being recognized, please navigate to *Help > About* in BrainVision Analyzer or Recorder to see whether your Add-on licenses are listed there.

In case you require a **BrainVision Analyzer 2** license file or you have questions on sublicenses for **Add channels** or **Analyzer Video**, please contact our Scientific Support team ([Send Email](#)) indicating the number printed on your dongle.

The license file for **BrainVision Recorder Video**, **RecView** or **RecView MR correction** can be downloaded below. For further questions on BrainVision Recorder Video, RecView or RecView MR correction please contact our Technical Support team ([Send Email](#)) indicating the number printed on your dongle.

27-06-2019

License File for BrainVision Recorder Video, RecView, RecView MR correction

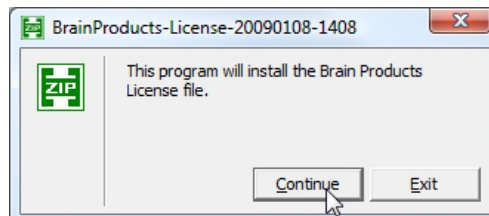
Type: zip Size: 76.5 KB

A sub-license file is an executable file. It automatically installs the sub-license in the correct folder.


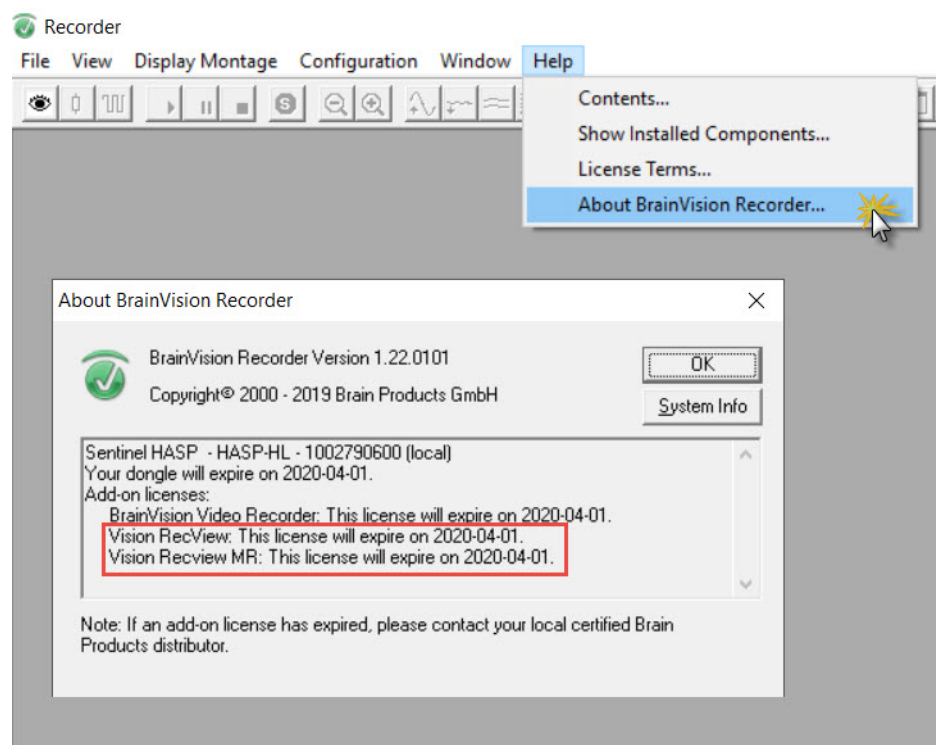
Installing sub-license files

Start the executable file and then click *Continue* to install the sub-license (see [Figure B-4](#)). Then follow the instructions in the automatic installation routine.

Figure B-4. Installing sub-licenses



You can check what sub-licenses are active by choosing *Help > About BrainVision Recorder...* from the Recorder menu (see [Figure B-5](#)).

 Figure B-5. Displaying sub-licenses in the Recorder


The installed sub-license is stored in the Windows® system folder as a file with the extension .bplcs.



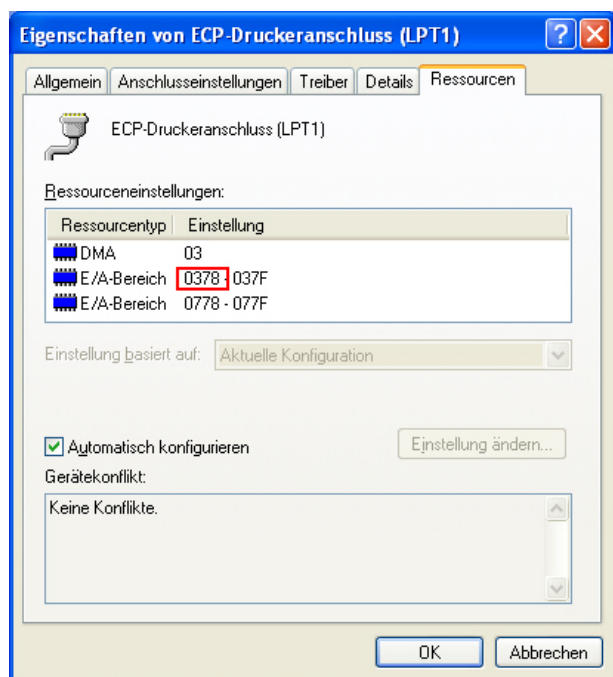
Appendix C How can I find the address of the LPT port?

If your computer has only one parallel port (LPT1) then its hardware address is usually 0378 (default value). If your computer has a second parallel port then its hardware address is usually 03F8.

If the default address is not the correct address then you can identify the address as follows:

- 1 Open the Windows® Device Manager.
- 2 In the Device Manager, choose the entry *Ports (COM and LPT)*.
- 3 To do this, right-click the line *ECP (LPTx) Printer Port* and choose *Properties* from the context menu that appears.
- 4 The dialog box *ECP Printer Port (LPTx) Properties* appears.
- 5 In this dialog box, choose the *Resources* tab (see [Figure C-1](#)). You can see the first start address in the *I/O range* under *Resource Settings*.

Figure C-1. Displaying the address of the LPT port in the Windows® Device Manager





Appendix D Behavior of TTL pulses in different parameter configurations

On page 143 of Appendix E, you will find a diagrammatic representation of the behavior of the TTL pulses in response to different parameter configurations of the Band Power Trigger filter (see also [Section 6.2 as of page 75](#)) and Level Trigger filter (see also [Section 6.7 as of page 90](#)).

A: "Hysteresis" mode

Trigger Configuration

☐ Discrete TTL-Pulses

☒ Hysteresis

	Set TTL	TTL Value [hex]
▶ Upper Threshold Exceeded	<input checked="" type="checkbox"/>	01
Lower Threshold Under-Run	<input checked="" type="checkbox"/>	02

TTL-Pulse Length [ms]:

☒ Inhibit additional TTL-Pulses for:

Inhibition Period [ms]:

(The curve at pin 0 is displayed.)

The depictions in B and C indicate the settings you can make to prevent signals from being overwritten prematurely.



B: "Discrete TTL-Pulses" mode without inhibition period

Trigger Configuration

☒ Discrete TTL-Pulses

☐ Hysteresis

	Set TTL	TTL Value [hex]
▶ Upper Threshold Exceeded	<input checked="" type="checkbox"/>	01
Lower Threshold Under-Run	<input checked="" type="checkbox"/>	02

TTL-Pulse Length [ms]:

☐ Inhibit additional TTL-Pulses for:

Inhibition Period [ms]:

(The curve at pin 0 and pin 1 is displayed.)

C: "Discrete TTL-Pulses" mode with specified inhibition period

Trigger Configuration

☒ Discrete TTL-Pulses

☐ Hysteresis

	Set TTL	TTL Value [hex]
▶ Upper Threshold Exceeded	<input checked="" type="checkbox"/>	01
Lower Threshold Under-Run	<input checked="" type="checkbox"/>	02

TTL-Pulse Length [ms]:

☒ Inhibit additional TTL-Pulses for:
Inhibition Period [ms]:

(The curve at pin 0 and pin 1 is displayed.)

D: "Discrete TTL-Pulses" mode with specified inhibition period

Trigger Configuration

☒ Discrete TTL-Pulses

☐ Hysteresis

	Set TTL	TTL Value [hex]
▶ Upper Threshold Exceeded	<input checked="" type="checkbox"/>	01
Lower Threshold Under-Run	<input type="checkbox"/>	02

TTL-Pulse Length [ms]:

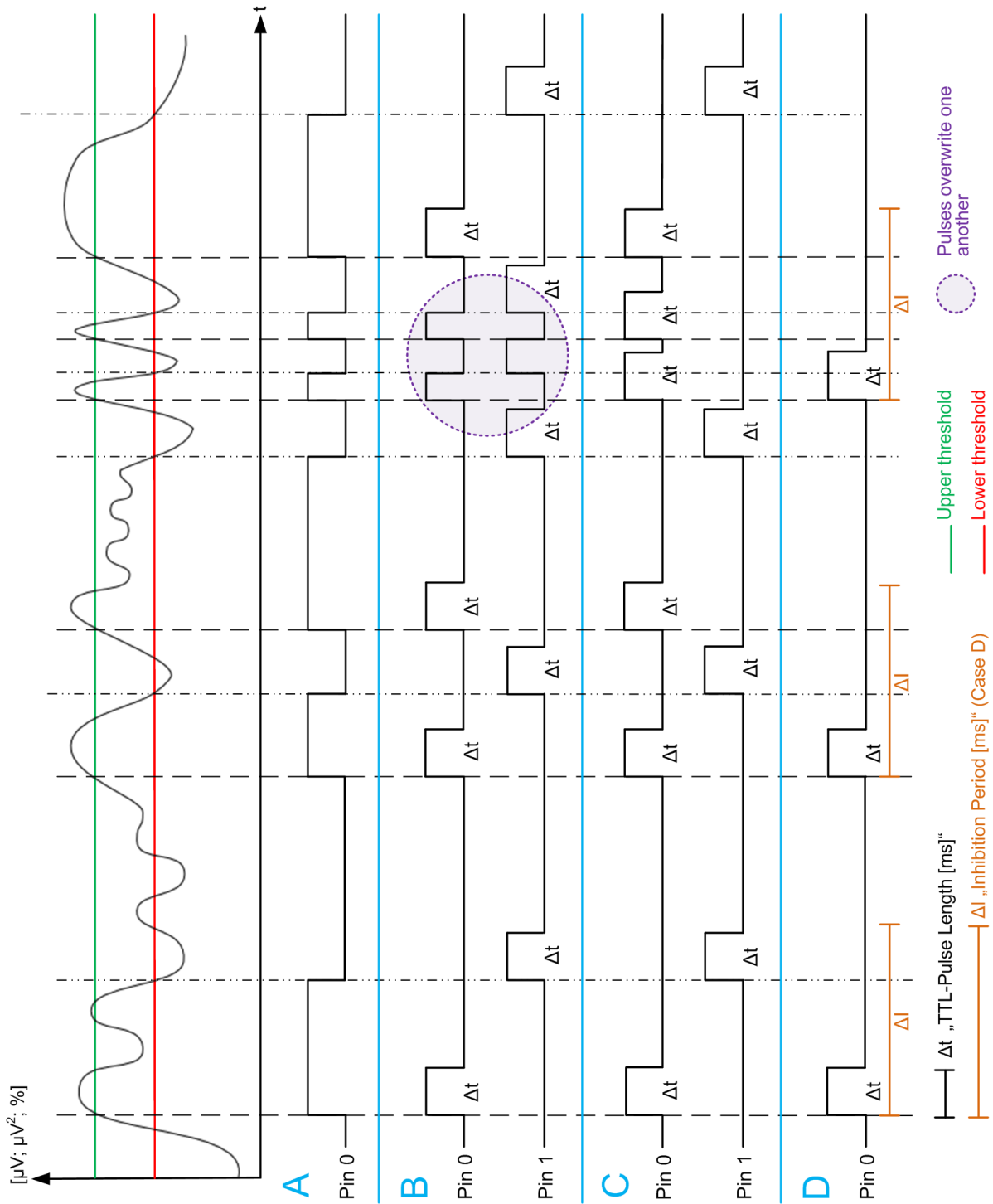
☒ Inhibit additional TTL-Pulses for:
Inhibition Period [ms]:

(The curve at pin 0 is displayed.)



You should note that the accuracy of the reset timer and the inhibition period timer depends on the resolution of the Windows® internal system clock. It is therefore not possible to guarantee that timing will be accurate to the nearest millisecond.

Figure D-1. Diagrammatic representation of the behavior of TTL pulses





Appendix E Legal notes

WinRing0

RecView uses the WinRing0 library from OpenLibSys.org in order to control the parallel port. In compliance with the conditions of the modified BSD license, we reproduce the redistribution conditions here. The Copyright text refers only to the WinRing0 files present in the distribution (WinRing0.dll, WinRing0x64.dll, WinRing0.sys, WinRing0x64.sys, WinRing0.vxd):

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Notes for RecView users in the USA

You should note that the use of our devices and software other than for the intended use described in the present User Manual may represent an infringement of certain industrial property rights arising out of US patent number 5,445,162. You should therefore note that the following procedures for use must be observed.

Recording must be performed outside the MRI room. The PC or laptop used to record and store the signals must not be located in the MRI room. Brain Products GmbH accepts no liability in the event of any non-compliance with these instructions and the original intended use.

We accept no liability for loss or damage caused to your devices by strong magnetic fields if laptops or computers are located in the MRI room. This does not just apply in the USA, but worldwide.

The manual or automatic triggering of the MRI based on the detection of special wave forms during the monitoring of inbound data may potentially result in the infringement of patent. Brain Products GmbH accepts no liability or responsibility in the event of the improper use of our devices and/or software for such purposes.

The BrainAmp MR and BrainAmp MR plus amplifiers and the BrainVision Recorder recording software are not able to send triggers based on the detection of special wave forms in an EEG (e.g. spikes). You can find further information on the US patent office's web site at <http://www.uspto.gov> (patent number 5,445,162 and referral). Alternatively, please contact Brain Products GmbH directly.

BrainVision RecView is able to send triggers. The use of this function within the framework of the above-mentioned patent-protected procedure should be avoided in the USA. You can find further information on the US patent office's web site at <http://www.uspto.gov> (patent number 5,445,162 and referral). Alternatively, please contact Brain Products GmbH. ●

List of abbreviations

BCI Brain Computer Interface

ECG Electrocardiogram

EDA Electrodermal activity

EMG Electromyogram

EOG Electrooculogram

FFT Fast Fourier Transform

fMRI Functional magnetic resonance imaging

ICA Independent Component Analysis

LDR Linear derivation

LORETA Low Resolution Brain Electromagnetic Tomography

LPT Line Print Terminal

MNI Montreal Neurological Institute

MRI Magnetic Resonance Imaging

ROI Region of Interest

TCP/IP Transmission Control Protocol/Internet Protocol

TR Time of Repetition

TTL Transistor-transistor logic

Glossary

A

actiCAP ControlSoftware: Software from Brain Products that allows the actiCAP active electrode system to be controlled and configured. The actiCAP ControlSoftware can also be controlled from the Recorder.

Amplitude: Maximum deflection of the EEG curve in μV measured from peak to trough.

Analyzer: Software from Brain Products for analyzing EEGs and other physiological signals and which is able to read and evaluate different file formats from various vendors.

Artifact: All potential shifts in the EEG recording that do not have their source in the cortex. Artifacts can be subdivided into those related to the test subject (physiological artifacts) and technical interference. Technical artifacts can be caused by faulty electrodes, defects in the apparatus or technical interference.

Average: Formation of arithmetic mean using segmentation (total value of the points divided by the number of segments). This is performed separately for each EEG channel.

Average: see *DELETE THIS MARKER*.

B

Baseline: An assumed horizontal line marking the vertical zero point in the EEG (voltage = 0).

Bipolar connection: Montage type in which the differences between two channels are calculated (see also *Montage*).

BrainAmp family: Amplifiers from Brain Products with 32 channels each (can be extended) that can be used in different fields (laboratory acquisition, combined EEG-fMRI measurements, EEG-TMS measurements, etc.).

D

Digital port: Parallel interface over which data can be transferred between a computer and peripheral devices.

Dongle: Pluggable copy protection device.

Drift: Drifts are temporal shifts between the averaged artifact curve and the scanner artifact of each interval. This drift is caused when the time of repetition (TR) of the scanner is

not a multiple of the sampling rate of the amplifier. Consequently, the artifacts of the individual intervals drift by a fraction of a sampling interval even if the "Scan Start" markers are positioned perfectly.

H

High-cutoff filter: Filter that reduces the amplitude of high-frequency digitized signals.

I

Impedance measurement: Recorder operating mode for measuring the resistance of the electrodes.

Impedance: Resistance between the electrode and the head skin.

Interval: A section of the EEG signal defined by its starting point and length or by its starting point and end point within the signal.

L

Low-cutoff filter: Filter that reduces the amplitude of low-frequency digitized signals.

LPT port: see *Parallel port*.

M

Marker: Markers indicate a point in time or a period within the EEG. A marker can be an item of stimulus information that is used to ascertain evoked potential. It can also mark a new segment or indicate that a DC offset correction was carried out at a certain time. Markers are used for orientation during segmentation.

Monitoring: Observation of the EEG signals on screen.

Montage: Reconnection of the channels in the software whereby new voltage references are assigned to the channels.

P

Polarity: The polarity setting determines whether the axis for positive measurements points up or down on EEG curves.

R

Raw file: The EEG file obtained directly during recording without any modifications.

RDA (remote data access): Remote access to the Recorder or the transfer of data from the Recorder to RecView. In this process, the Recorder acts as the server and RecView as a client.

Resolution: Specifies the granularity with which the value range of the EEG signal is subdivided during digital acquisition. A higher resolution means finer granularity and more accurate acquisition of the original signal. Unit: μV .

S

Sampling rate: Number of data points measured per second when acquiring an EEG digitally.

Scaling: In the context of displaying the EEG signal, scaling is the assignment of an amplitude value in μV to an interval.

Segment: A section of the EEG resulting from segmentation (q.v.).

Segmentation: Subdivision of the EEG into different segments (epochs). Segmentation can be based on a number of different criteria. On the one hand, segmentation is understood to be a preliminary stage in the analysis of evoked potentials. Epochs of the same length are generated relative to a reference marker (a stimulus, for example). This results in a data set consisting of a sequence of segments or epochs. On the other hand, segmentation is understood to be the preparation of separate processing steps for different sections of an EEG, for example for the analysis of different stages before and after medication.

Server: The address of the computer on which the Recorder software is running (see also *RDA*).

Sub-license: File associated with the dongle and which can be used to enable optional functions; Extension: .bplcs.

T

Ten-ten system (10-10 system): One additional electrode is positioned between each of the electrodes of the 10-20 system (q.v.).

Ten-twenty system (10-20 system): Internationally recognized, standardized method for positioning electrodes on the head. The skull is measured from defined anatomical points. The distance between neighboring electrodes is either 10% or 20% of the measured distances.

Trigger: Pulse generated by a device or software program and which initiates an operation. A presentation software package can, for example, generate a trigger each time an image appears. The trigger can be sent to the amplifier via the parallel port of the computer and recorded by the Recorder as a marker simultaneously with the EEG. EEG activity (e.g. an EEG signal of sufficient amplitude or length) can also be used to generate a trigger pulse that starts a process (e.g. control of a program).

TTL pulse: Transmission to the LPT port of a trigger signal which is reset to the value 0 after a (relatively) short period.

TTL signal: Transmission to the LPT port of a trigger signal which persists though to the reception of a given reset event at the LPT port; when the reset event is received, the value is reset to 0.

V

View: Method of representing the EEG, such as the grid view, the head view, and the mapping view. A view determines how the channels are arranged in the window, for example.

W

Workfile: A file containing information on workspaces (*.rvwksp), montages (*.mont) and other user-defined settings.

Workspace: Storage location for files, the processing steps performed at the EEG data. File name extension: .rvwksp.

Subject index

A

actiCAP ControlSoftware 81
 Administrator mode 50, 75, 90, 109, 132
 Analyzer 23, 69, 86, 94, 96, 112, 113
 artifact (see also scanner artifact and cardioballistic artifact) 82, 86
 averaging 72
 pulse artifact correction 122
 scanner artifact correction 115
 weighted 73
 axes
 configuring 63
 subdivisions 64

B

bandwidth 88
 baseline correction 36, 62, 73
 block indicator 37
 Butterworth high-cutoff filter 119

C

cardioballistic artifact 115
 correcting 121–125
 channel
 activating/deactivating 42
 creating 79, 94, 94–96
 reconnecting 79
 coefficient matrix 94, 95
 Command line options 56
 coordinate system
 for electrodes 133
 for voxels 98

D

data loss 37
 data representation
 configuring 36
 incorrect 52–53
 simultaneous 41
 downsampling 121, 124, 125

E

ECG 110
 channel 62, 111, 121
 data 109
 electrode
 changing position 67, 105
 coordinate system 133
 detecting gel bridges 81
 preparing 83–84

F

FFT (Fast Fourier Transform) 85
 data window 86
 filter tree 45
 creating 45, 46
 displaying 50
 editing 49
 filter windows
 arranging 35, 52
 switching between 37
 filters
 combining 46–47
 configuring 48
 configuring parameter dialog access 68
 invalid combinations 46
 invisible 49
 parameters 48
 programming (see also programming) 127
 renaming 49
 valid combinations 47

firewall 30

frequency band 75

- assigning a color 66
- configuring 66, 107

frequency data 66, 72, 75, 104, 107–108, 131

frequency graph 85

G

gradient 115, 117, 119, 120

graph

- configuring 65

H

Hamming window 86

Hanning window 86

high-cutoff filter 88

I

ICA component 96

ICA matrix 96

impedance view 42

individual channel mode 41, 86

inhibition period 76–77, 92, 141, 142

installation

- conditions (see also system requirements) 23
- Windows® 24
- Windows® 7, 8.1, 10 24

K

keyboard shortcut 36, 37, 52

L

license 23

- downloading 135
- installing 27–28, 137

low-cutoff filter 88

LPT port

- controlling 37, 49, 75, 76–77, 90–92, 109, 131
- identifying the address 139
- programming example 132
- specifying the address 32, 37
- status display 131, 132
- trigger 75, 90, 109

M

Map 86, 104

- for segmented data 105

marker

- displaying 39
- for comments 78
- for peak 92
- for R-peak 110, 122, 125
- hiding 124
- segmenting on 112
- setting 90, 91, 109

master filter 37

- selecting 44

menu bar 35

Microsoft .NET Framework 127

montage

- keyboard shortcuts 70
- showing 35, 37, 69
- switching between 70

MR data 115

MR scanner 21, 109, 115

N

neurofeedback 75, 90
notch filter 88

O

overlapping 85, 87, 113

P

polarity 110
power density 73, 76, 86
program
 starting 31
 status 37
program folder 50, 127, 130
program information
 displaying 35
programming
 interfaces 128
 RecViewInterfaces.dll 127, 130, 132
 sample filter 130, 131, 132
pulse (ECG)
 detecting 122

R

RDA server
 activating 29–30
Recorder 23, 31, 71, 72, 78, 81, 83, 102, 110, 146
 connecting to 31, 36, 40
 disconnecting from 36, 44
 impedance mode 42, 81, 83
 missing connection to 40
 monitoring mode 83
 montage 69
 RDA server 29–30

sub-license 28, 135–138
unblocking 30

rectification 72–73
reference channel 79, 123
ROI (Region of Interest) 97
 channel 97
 configuring 97–100
 exporting 100
 importing 100
R-peak 109, 110–111, 121, 123, 124, 125

S

sampling interval 115
sampling rate
 reducing (see also downsampling) 118, 121
scaling 39, 61
 configuring 61
 individual scaling factors 62, 102
 ROI channel 102
scanner artifact 115, 119
 correcting 115
segment
 displaying 113
segmentation 112
status display 37
 LPT port 76, 91, 109
sub-license (see also license) 135
system requirements 23

T

TCP/IP network connection 23, 30
template drift compensation 115–117
template drift detection 117, 119–120
test subject
 requirements placed on 82, 84
threshold 76, 90, 91, 92, 110

- time data 90, 104–106
- Time of Repetition (TR) 115–118, 119
 - configuring 118
- Time Zero marker 113
- toolbar 35–37
- topography 104
- trigger 75, 76, 77, 90, 91, 92, 109
- TTL pulse 37, 76–77, 91, 109, 141–143
- TTL signal 76, 77, 91, 92

U

- USB dongle 28, 135
- USB license dongle 25

V

- voltage difference 79

W

- window function
 - averaging 73–74
 - FFT 86
- work files 31
 - folder 31, 69
- workspace 35, 37, 54, 128
 - creating 54
 - loading 55–56
 - saving 55

Z

- zero padding 85